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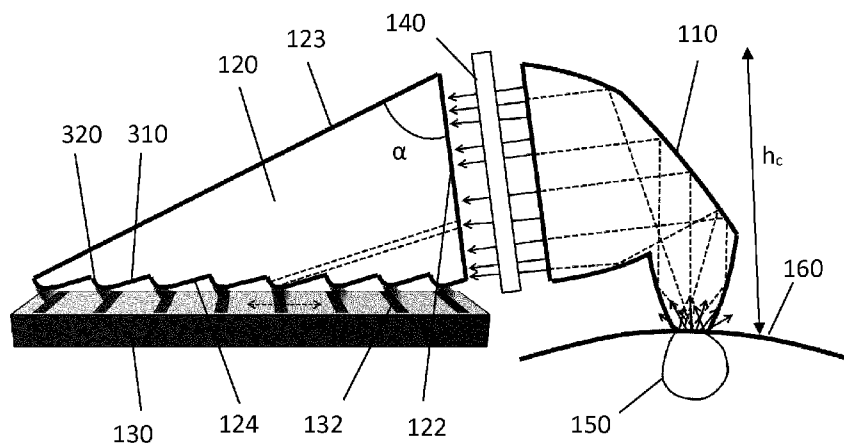


FIG. 1a

(57) Abstract: A spectrometer (100) for characterizing a radiation beam, the spectrometer (100) comprising an optical radiation guiding system comprising a collimator (110) for collimating the radiation beam into a collimated radiation beam, and a beam shaper (120) for distributing the power of the collimated radiation beam over a discrete number of line shaped fields, the spectrum of the collimated radiation beam being delivered to each of the discrete number of line shaped fields, and a spectrometer chip (130) wherein the spectrometer chip (130) is adapted for processing the radiation in a discrete number of line shaped fields coming from the beam shaper (120).



## Optical spectrometer with matched étendue.

### Field of the invention

The invention relates to techniques for non-invasive measuring of analytes. In particular, the present invention relates to techniques for non-invasive measuring of analytes in skin or other tissue using  
5 Raman spectroscopy. In addition to non-invasive measurements of analytes in the human body, the method can also be used to measure the properties of produce, fluids, textile, etc.

### Background of the invention

Raman spectroscopy is a known optical technique for identifying molecules. The identification is based on vibrational information specific to chemical bonds and symmetry of molecules. The technique  
10 provides a fingerprint by which molecules may be uniquely identified. Consequently, Raman spectroscopy can be used as a qualification and quantification technique for detecting analytes of interest in a sample.

As optical, non-destructive technique, Raman spectroscopy also be used for identifying targets of interest in medical applications, for example identifying molecules in the skin of an individual and to  
15 estimate the total number of such molecules in the volume probed. One application that has been envisaged in the past is the sensing of glucose in a living creature.

Nevertheless, as for most optical techniques, the response signal when measuring glucose is very limited. To monitor glucose in a living creature, a small signal variation is to be measured while a significant amount of background signal is present. Therefore it is important that a detector based on  
20 Raman spectroscopy has a high sensitivity.

Raman scattering will lead to a light signal that is isotropic, i.e. emitting in all directions. The spectrometer needs to capture light propagating in all angles as much as possible. In addition, since light scatters readily in skin, the light that is available at the skin surface is spread out over a substantial area (1 mm<sup>2</sup> or more, depending on the illumination scheme used). This creates the  
25 challenge of collecting light over all angles and a large area, i.e. a large étendue (proportional to area times solid angle), which is a fundamental challenge in optics since spectrometers that are able to collect and process a light signal with a large étendue are challenging to design and build.

Moreover due to the differences in the local geometry of the skin (e.g. different thicknesses and microstructure of the various layers that make up skin) for different positions on the skin as well as for  
30 different individuals, it is difficult to quantify the concentration of a particular analyte without performing calibration steps for each individual separately. Therefore, to obtain a reproducible technique, advantageously calibration is performed systematically. This is typically a time consuming and cumbersome process that limits the applicability of the Raman technique for doing accurate routine non-invasive measurements of important analytes such as glucose, cholesterol, ethanol, etc.

Together with the required high sensitivity and the need for calibration, another requirement typically is the ease of use of the sensor for the user. For example in case of glucose sensing, sensing typically needs to be performed at least a couple of times a day. Conventional Raman systems typically are large optical systems and cannot be used for convenient day-to-day glucose monitoring. Efforts have been made to miniaturise optical Raman systems. Some suggestions have been made in the past to use an implantable sensor, an example thereof being described in US patent application 13/415,392. Whereas implantable sensors have the advantage of being easy in use and even allow continuous monitoring once they have been implanted, such implantable sensors require accurate packaging while maintaining access to the tissue or fluids to be measured and also require a surgical step for implanting them.

There is still a need for a good Raman based optical sensor, with high sensitivity, good accuracy and advantageously with good ease of use for the user.

#### **Summary of the invention**

It is an object of embodiments of the present invention provide an optical system for detecting a light spectrum whereby the optical system has a high coupling factor with the light source. It is an advantage of embodiments of the present invention that the optical system is able to accept a large étendue of the light source. It is an advantage of embodiments of the present invention that the étendue can be matched. It is an advantage of embodiments of the present invention that a cheap, compact and sensitive Raman based device can be obtained, allowing determination of the concentration of analytes in tissue.

The above objective is accomplished by a method and device according to the present invention.

In one aspect, the present invention relates to an optical system for characterizing a radiation beam, the spectrometer comprising an optical radiation guiding system comprising a collimator for collimating the radiation beam into a collimated radiation beam, and a beam shaper for distributing the power of the collimated radiation beam over a discrete number of line shaped fields, and a spectrometer chip wherein the spectrometer chip is adapted for processing the radiation in a discrete number of line shaped fields coming from the beam shaper. The optical system may be a spectrometer. By increasing the number of waveguides of the optical system,, the overall spectrometer étendue can be increased to match the source étendue. It is an advantage of embodiments of the present invention that a very large number of incoupling gratings can be realized. The collimated radiation beam may be directed substantially in a single direction with a maximum angular spread of 20°.

According to embodiments of the present invention, the beam shaper thereby is configured such that the spectrum of the collimated radiation beam entering the beam shaper is being delivered to each of the discrete number of line shaped fields. In other words, the beam shaper is configured to not split the collimation radiation beam into spectrally different sub-beams for the different discrete line shaped fields, but rather is configured for splitting the collimation radiation beam in power over the

different line shaped fields. The beam shaper may distribute the collimation radiation beam equally over the discrete line shaped fields, the whole spectrum thus being distributed to each of the discrete line shaped fields, The beam shaper thus may be adapted for performing a power distribution without inducing a spectrum distribution (the spectral components are not split over the different line shaped fields.

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The system processes the different line shaped fields spectrally after the line shaped fields have been split by the beam shaper.

The beam shaper may have a wedge shape. It is an advantage of embodiments of the present invention that collimated radiation entering the wedge can be spread out over a large area while allowing to keep the height of the system limited. The latter advantageously improves the wearability of the device.

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The collimator and the beam shaper may be arranged so that the beam shaper can receive radiation via a wedge entrance area being the short side of the wedge. It is an advantage of embodiments of the present invention that system with limited height can be obtained, resulting in improved wearability.

15

The beam shaper may be shaped so that radiation incident orthogonally at a wedge entrance area is guided directly to the wedge exit area without first being reflected at another surface of the wedge.

At least part of the collimator may have a 3D parabolic or hyperbolic shape. It is an advantage of embodiments of the present invention that accurate beam collimation can be obtained.

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The collimator may have an entrance point and is shaped so as to fold an irradiation beam between the entrance point and an output of the collimator. It is an advantage of embodiments of the present invention that a compact optical system can be provided.

The beam shaper may comprise an exit area for directing the radiation to the discrete number of line shaped fields, the exit area having a waved or stepped pattern. It is an advantage of embodiments of the present invention that the light refracted on the exit area of the wedge and that the refraction is location dependent.

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The waved or stepped pattern may comprise a plurality of first segments and a plurality of second segments, the second segments interconnecting the first segments, neighbouring first segments being positioned at a distance shorter than the length of the first segments and oriented substantially parallel with an orthogonal direction to an entrance area of the beam shaper.

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The second segments may be curved. It is an advantage of embodiments of the present invention that radiation which is refracted by a second segment can be focused on a line of the spectrometer chip. The first segments may have an equal length and/or the second segments may have an equal length and shape.

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The spectrometer chip may comprise a plurality of detection channels, each detection channel may comprise an incoupling grating, an outcoupling grating, a spectrally dependent transmission system

wherein the incoupling grating may be coupled with the outcoupling grating through the spectrally dependent transmission system and wherein the incoupling gratings of the different detectors may be arranged on a discrete number of lines. The incoupling grating and/or outcoupling grating may be shared over a number of detectors. It is an advantage of embodiments of the present invention that a  
5 distribution of the incoupling gratings over a discrete number of lines allows to increase the number of single mode waveguides as more space is available compared to only one line of incoupling gratings. It is an advantage of embodiments of the present invention that the wedge is designed such that, when light from a light source is distributed by the wedge over a discrete number of line shaped fields, the spacing and orientation of the line shaped fields arriving at the spectrometer chip corresponds with  
10 the spacing and orientation of the incoupling gratings. This results in a high coupling factor between the light source and the spectrometer chip.

The spectrally dependent transmission system may be a Fabry-Perot system.

A first rejection filter may be present between the collimator and the beam shaper for rejecting an excitation radiation. According to embodiments of the present invention, a second rejection filter may  
15 be present between the beam shaper and the spectrometer chip and/or a third rejection filter may be implemented in the spectrally dependent transmission system using Bragg grating.

The optical system may be integrated in a wristband. It is an advantage of embodiments of the present invention that by wearing the wristband a good contact between the entrance of the collimator and the skin can be realized. It is an advantage of embodiments of the present invention that a good  
20 wearability of the sensing system is obtained.

The present invention also relates to the use of an optical system as described above as a glucose sensor. It is an advantage of embodiments of the present invention that a glucose level of a patient or a variation therein can be measured without disturbing the patient too much, i.e. that a glucose measurement can be done without substantially hampering patient comfort. During use, the  
25 measured spectra may be correlated with a reference glucose spectrum for increasing the signal to noise ratio. It is an advantage of embodiments of the present invention that the signal to noise ratio can be increased if a standard response of a particle or molecule to be detected can be used as reference spectrum.

Embodiments of the present invention also relate to a detector system wherein the detector system  
30 comprises an optical system mounted on an optical printed circuit board and a read-out printed circuit board wherein the read-out printed circuit board is connected with the optical printed circuit board for digitizing the optical signal and/or processing the digitized result. It is an advantage of embodiments of the present invention that the read-out printed circuit board and the optical system are directly connected reducing the overall noise in the detector system. In some embodiments, the optical system  
35 and/or the read-out system may be integrated in a wristband.

The present invention also relates to an optical radiation guiding system comprising a collimator for collimating radiation beam into a collimated radiation beam, and a beam shaper for distributing the power of the collimated radiation beam over a discrete number of line shaped fields. The beam shaper thus may be adapted for performing a power distribution without inducing a spectrum distribution  
5 (the spectral components are not split over the different line shaped fields.

According to embodiments of the present invention, the beam shaper thereby is configured such that the whole spectrum of the collimated radiation beam is being delivered to each of the discrete number of line shaped fields. In other words, the beam shaper is configured to not split the collimation radiation beam into spectrally different sub-beams for the different discrete line shaped fields, but  
10 rather is configured for splitting the collimation radiation beam in power over the different line shaped fields.

Particular and preferred aspects of the invention are set out in the accompanying independent and dependent claims. Features from the dependent claims may be combined with features of the independent claims and with features of other dependent claims as appropriate and not merely as  
15 explicitly set out in the claims.

These and other aspects of the invention will be apparent from and elucidated with reference to the embodiment(s) described hereinafter.

## 20 **Brief description of the drawings**

FIG. 1a shows a schematic drawing of an optical system in accordance with embodiments of the present invention.

FIG. 1b shows a schematic drawing of an alternative wedge in accordance with an embodiment of the present invention.

25 FIG. 2 shows a TEM image of a second rejection filter in accordance with embodiments of the present invention.

FIG. 3 shows a schematic drawing of a spectrometer chip in accordance with embodiments of the present invention.

FIG. 4 shows an example of a glucose spectrum as can be obtained with Raman spectroscopy as can be  
30 used in embodiments of the present invention.

FIG. 5 shows a glucose spectrum and a measured glucose spectrum including shot noise measured using an optical system during a 10 sec integration time in accordance with embodiments of the present invention.

FIG. 6 shows a glucose spectrum and a measured glucose spectrum including shot noise measured using an optical system during a 120 sec integration time in accordance with embodiments of the present invention.

FIG. 7 shows a glucose histogram measured using an optical system during a 10 sec integration time  
5 accordance with embodiments of the present invention.

FIG. 8 shows a glucose histogram measured using an optical system during a 120 sec integration time accordance with embodiments of the present invention.

FIG. 9 shows a Clarke error grid representing measurements (10 seconds integration time) in accordance with embodiments of the present invention.

10 FIG. 10 shows a Clarke error grid representing measurements (120 seconds integration time) in accordance with embodiments of the present invention.

FIG. 11 provides a schematic 3D drawing of a detector system in accordance with embodiments of the present invention.

FIG. 12 provides a schematic 3D drawing of a detector system comprising a wrist band in accordance  
15 with embodiments of the present invention.

FIG. 13 shows the transmission of a waveguide in accordance with embodiments of the present invention.

FIG. 14 shows the transmission of a waveguide in accordance with embodiments of the present invention.

20 FIG. 15 shows the transmission of a waveguide in accordance with embodiments of the present invention.

FIG. 16 shows an incoming spectrum as can be processed in a system according to an embodiment of the present invention.

FIG. 17 shows the transform of the spectrum in function of the waveguide index in accordance with  
25 embodiments of the present invention.

FIG. 18 shows an incoming spectrum and the reconstructed spectrum in accordance with embodiments of the present invention.

FIG. 19 shows an incoming spectrum as can be processed in a system according to an embodiment of the present invention.

30 FIG. 20 shows an incoming spectrum and the reconstructed spectrum in accordance with embodiments of the present invention.

The drawings are only schematic and are non-limiting. In the drawings, the size of some of the elements may be exaggerated and not drawn on scale for illustrative purposes.

Any reference signs in the claims shall not be construed as limiting the scope.

35 In the different drawings, the same reference signs refer to the same or analogous elements.

**Detailed description of illustrative embodiments**

The present invention will be described with respect to particular embodiments and with reference to certain drawings but the invention is not limited thereto but only by the claims. The drawings described are only schematic and are non-limiting. In the drawings, the size of some of the elements may be exaggerated and not drawn on scale for illustrative purposes. The dimensions and the relative dimensions do not correspond to actual reductions to practice of the invention.

Furthermore, the terms first, second and the like in the description and in the claims, are used for distinguishing between similar elements and not necessarily for describing a sequence, either temporally, spatially, in ranking or in any other manner. It is to be understood that the terms so used are interchangeable under appropriate circumstances and that the embodiments of the invention described herein are capable of operation in other sequences than described or illustrated herein.

Moreover, the terms top, under and the like in the description and the claims are used for descriptive purposes and not necessarily for describing relative positions. It is to be understood that the terms so used are interchangeable under appropriate circumstances and that the embodiments of the invention described herein are capable of operation in other orientations than described or illustrated herein.

It is to be noticed that the term "comprising", used in the claims, should not be interpreted as being restricted to the means listed thereafter; it does not exclude other elements or steps. It is thus to be interpreted as specifying the presence of the stated features, integers, steps or components as referred to, but does not preclude the presence or addition of one or more other features, integers, steps or components, or groups thereof. Thus, the scope of the expression "a device comprising means A and B" should not be limited to devices consisting only of components A and B. It means that with respect to the present invention, the only relevant components of the device are A and B.

Reference throughout this specification to "one embodiment" or "an embodiment" means that a particular feature, structure or characteristic described in connection with the embodiment is included in at least one embodiment of the present invention. Thus, appearances of the phrases "in one embodiment" or "in an embodiment" in various places throughout this specification are not necessarily all referring to the same embodiment, but may. Furthermore, the particular features, structures or characteristics may be combined in any suitable manner, as would be apparent to one of ordinary skill in the art from this disclosure, in one or more embodiments.

Similarly it should be appreciated that in the description of exemplary embodiments of the invention, various features of the invention are sometimes grouped together in a single embodiment, figure, or description thereof for the purpose of streamlining the disclosure and aiding in the understanding of one or more of the various inventive aspects. This method of disclosure, however, is not to be interpreted as reflecting an intention that the claimed invention requires more features than are expressly recited in each claim. Rather, as the following claims reflect, inventive aspects lie in less



than all features of a single foregoing disclosed embodiment. Thus, the claims following the detailed description are hereby expressly incorporated into this detailed description, with each claim standing on its own as a separate embodiment of this invention.

Furthermore, while some embodiments described herein include some but not other features  
5 included in other embodiments, combinations of features of different embodiments are meant to be within the scope of the invention, and form different embodiments, as would be understood by those in the art. For example, in the following claims, any of the claimed embodiments can be used in any combination.

In the description provided herein, numerous specific details are set forth. However, it is  
10 understood that embodiments of the invention may be practiced without these specific details. In other instances, well-known methods, structures and techniques have not been shown in detail in order not to obscure an understanding of this description.

Where in embodiments of the present invention reference is made to "étendue", reference is made to the geometrical extent of light in an optical system. It characterizes how spread out the light  
15 is.

Where in embodiments of the present invention reference is made to "N", reference is made to the total number of waveguides on the chip. In embodiments of the present invention N varies between 1,000 and 10,000,000, e.g. between 100,000 and 5,000,000. The number of waveguides is a function of the étendue of the optical signal that need to be measured. The total étendue of the  
20 collection of waveguides should ideally exceed the étendue of the light signal that impinges on the chip. Practical considerations such as maximum reticle size and cost of the chip may result in a lower practical optimum. The étendue per waveguide is of the order of  $\lambda^2$ . So if the light signal has an étendue of  $1 \text{ mm}^2$ , approximately 1,000,000 waveguides are needed to match the étendue of the light signal for  $\lambda = 1 \text{ }\mu\text{m}$ .

25 Where in embodiments of the present invention reference is made to "L", reference is made to the total number of different spectral responses. In embodiments of the present invention L varies between 50 and 500.

Where in embodiments of the present invention reference is made to "M", reference is made to the number of repeats. Hereby L is equal to the total number of waveguides N divided by the total number  
30 of different spectral responses. In embodiments of the present invention M varies between 200 and 10000.

In a first aspect, the present invention relates to an optical system for characterizing a radiation beam, e.g. a radiation beam captured after interaction with an object to be characterized. Embodiments of the present invention allow to obtain high sensitivity, whereby advantageously the  
35 étendue of the incoming radiation source is accepted and is substantially maintained in the optical system.

Embodiments of the present invention can for example be used for identifying molecules (e.g. for glucose quantification in tissue or interstitial fluid under the skin of a person). Embodiments of the present invention may for example be used for quantifying molecular presence/concentration in heavily scattering objects. For applications that target the skin, this may include e.g. glucose but  
 5 quantification of other biomolecules also may be performed. In embodiments of the present invention the optical system comprises an optical radiation guiding system comprising a collimator for collimating the radiation beam into a collimated radiation beam. Such a collimate radiation beam may be a radiation beam whereby the spread of the radiation is limited, e.g. may be a radiation beam of radiation with a maximum angular spread of 20°. In embodiments of the present invention the optical  
 10 system also comprises a beam shaper for distributing the power of the light coming from the collimator over a discrete number of line shaped fields. The beam shaper thereby is configured such that the spectrum of the collimated radiation beam entering the beam shaper is being delivered to each of the discrete number of line shaped fields. In other words, the beam shaper is configured to not split the collimation radiation beam into spectrally different sub-beams for the different discrete line  
 15 shaped fields, but rather is configured for splitting the collimation radiation beam in power over the different line shaped fields.

It is to be noticed that prior to entering the beam shaper, the excitation radiation can be filtered partly or fully from the collimated radiation beam.

In embodiments of the present invention the optical system 100 furthermore comprises a  
 20 spectrometer chip wherein the spectrometer chip is adapted for processing the radiation in a discrete number of line shaped fields coming from the beam shaper. In embodiments of the present invention, advantageously the étendue is conserved.

By way of illustration, embodiments of the present invention not being limited thereby, standard and optional features of the optical system will be discussed in more detail. Reference will be  
 25 made to the drawings, an exemplary optical system 100 being shown by way of illustration in FIG. 1a.

In some exemplary embodiments of the present invention the collimator expands the cross-section of the light beam in exchange for collimation. In embodiments of the present invention the collimator redirects the radiation from an incoming radiation beam into a single direction with a maximum angular spread of 20°, preferably 10°. In embodiments of the present invention the exit area  
 30 of the collimator is between 3 and 80 mm<sup>2</sup>, more preferably between 5 and 20 mm<sup>2</sup>, for example 10 mm<sup>2</sup>. In embodiments of the present invention the entrance area of the collimator is between 0,25 and 10 mm<sup>2</sup>, more preferably between 0.5 and 2 mm<sup>2</sup>, for example 1 mm<sup>2</sup>.

In some embodiments of the present invention the collimator may have a 3D parabolic shape. The ratio between the entrance area and exit area may for example equal

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$$\frac{Area_{exit}}{Area_{entrance}} = \frac{1}{(\sin \theta)^2} = 10$$

Hereby  $\theta$  is the angular spread. If  $\theta = 20^\circ$  the ratio between exit area and entrance area is equal to 10. This illustrates the relation between the expansion of the cross-section of the light beam and the collimation of the light beam.

In some preferred embodiments of the present invention the collimator 110 is designed such that, when a radiation beam is provided at the entrance of the collimator 110, the actual beam path is folded, as shown by way of example in FIG. 1a. In embodiments of the present invention the radiation beam may be folded over an angle between  $30^\circ$  and  $150^\circ$ , e.g. over an angle between  $60^\circ$  and  $120^\circ$ .

In an exemplary embodiment of the present invention the excitation zone has an étendue of  $1 \text{ mm}^2$  and the incoming radiation corresponds with a diffuse source generating  $10^8$  photons/second. In operation, the radiation is firstly collimated by the collimator 110, in a next stage it is distributed over a discrete number of line shaped fields by the wedge 120, after which it is detected by the spectrometer chip 130. This operation is explained for the exemplary embodiment of the present invention illustrated in FIG. 1a. In the exemplary embodiment of FIG. 1a the entrance of the collimator 110 has an area of  $1 \text{ mm}^2$ . The radiation at the entrance 150 may correspond with a diffuse source generating not collimated light, stemming from an irradiated tissue or interstitial fluid, e.g. at the skin. The angular spread of the radiation ranges between  $0^\circ$  and  $90^\circ$ , so that the radiation coming out of the diffuse scattering source, e.g. the skin, may be shaped as a full 90 degrees half cone. The radiation at entrance in the illustrative example has a photon flux of  $10^7$ - $10^8$  photons/sec. The radiation (e.g. Raman light leaving the skin) goes through a collimator 110 in which the area of the radiation is expanded and the radiation gets collimated. The exit area of the collimator of the exemplary system schematically presented in FIG.1a is  $30 \text{ mm}^2$  and the angular spread of the outgoing radiation is  $10.5^\circ$ . The radiation leaving the collimator has an étendue of  $1.2 \text{ mm}^2$ . The photon flux at the output of the collimator 110 equals  $0.8 \times 10^8$  photons/sec in the example. The incoming light is oriented and collimated by reflection on the side walls of the collimator. The reflection may be based on total internal reflection or by a metallic coated surface with a high reflectance. The shape typically is optimized for redirecting the radiation and collimating it. The collimation part may be designed such that it resembles or is equal to a compound hyperbolic concentrator or a compound parabolic concentrator. Nevertheless, also other collimator elements based on lenses could be used. In advantageous embodiments of the present invention, the collimator is limited in height. The height  $h_c$  of the collimator in the example of FIG. 1a is about 5 mm.

As indicated above, in embodiments of the present invention a beam shaper 120 is present between the collimator 110 and the spectrometer chip 130. The beam shaper 120 distributes the radiation coming from the collimator 110 over a discrete number of line shaped fields. The radiation coming from the collimator enters the beam shaper at the beam shaper entrance area 122 and leaves the beam shaper at the beam shaper exit area 124. The beam shaper and the collimator advantageously are arranged so that collimated radiation is guided directly, or after filtering, towards

the entrance region of the beam shaper. The entrance area of the beam shaper thereby may be parallel with the exit area of the collimator. Alternatively the entrance area of the beam shaper may be not parallel with the exit area of the collimator. The entrance area of the collimator shown in FIG. 1a and the exit area of the collimator are not fully parallel. In embodiments of the present invention the beam shaper 120 advantageously may have the shape of a wedge. Thereby the wedge 120 has a wedge entrance area 122 oriented towards the exit area of the collimator 110 and a wedge exit area 124 oriented towards the spectrometer chip 130. In the exemplary embodiment illustrated in FIG. 1a the cross-section of a wedge 120 is shown. The drawing is not at scale.

In at least some embodiments of the present invention, the radiation, after entering the wedge, will first reflect at the upper area of the wedge 123, thus being reflected downwards to an exit area of the wedge. Through shaping of the exit area, the radiation can then be focused in a detection zone. This principle is shown in FIG. 1a.

In at least some embodiments of the present invention the angle between the wedge entrance area 122 and the upper area of the wedge 123 is  $90^\circ$  so that irradiation entering the wedge perpendicularly to the wedge entrance does not hit the upper edge first but hits the wedge exit area 124 first. As the drawing in FIG. 1b is not at scale the angle  $\alpha$  which is  $90^\circ$  in the exemplary embodiment of the present invention is not preserved in the drawing of the same exemplary invention. The enlarged portion in FIG. 1b illustrates how the reflection of the radiation occurs.

In some embodiments of the present invention the wedge exit area 124 has a waved or stepped pattern. In the cross-section orthogonal to the wedge entrance area 122 and the wedge exit area 124 as shown in FIG. 1a and 1b, a stepped pattern can be seen for the wedge exit area 124. The stepped exit area 124 thereby comprises first segments 310 which in some embodiments may be surfaces oriented orthogonally to the wedge entrance area 122. The distance between neighboring first segments 310 may be smaller than the length of the first segments 310. The stepped shape moreover comprises second segments 320 interconnecting the first segments 310. The second segments 320 may be flat surfaces or curved surfaces. The second segments 320 may be cylindrically shaped surfaces. The waved/stepped exit area of the present example schematically shown in FIG. 1b comprises a plurality of second segments spread over a distance of 20 mm. The radiation is reflected by total internal reflection at the second segments 320 of the wedge exit area 124 towards the first segments and thus towards the spectrometer chip 130. This can be seen in the enlarged portion of FIG. 1b. In some embodiments of the present invention the first segments 310 may have an equal shape so that the line shaped fields are equal in width. In some embodiments of the present invention the second segments 320 have an equal length and shape. In some embodiments, the width of the line that is illuminated is compatible with two incouplers in the spectrometer chip 130, the two incoupler coupling into two opposite directions.

The area of the wedge exit area 124 in the example schematically illustrated in FIG. 1a equalled  $200 \times 10 \text{ mm} \times 0.01 \text{ mm}^2 = 20 \text{ mm}^2$ . The étendue of the light leaving the wedge 120 was  $\pi \cdot 0.6 \text{ mm}^2$ . The light leaving the wedge 120 has an angular spread  $10^\circ$  and a photon flux of  $0.2 \times 10^8$  photons/sec. From this exemplary embodiment it can be concluded that it is an advantage of  
 5 embodiments of the present invention that the overall collection efficiency can be above 10% and that the étendue is conserved as much as possible. The combination of the large number of input waveguides and the specific light guiding structure thus conserves the étendue as much as possible. If the input is compared with the output, 60% is reached, while the total photon count is still 20%. As known, the étendue is limited by the smallest étendue of the system, and while the étendue of the  
 10 totality of the emitted light will increase, the étendue of the light reaching the grating couplers will have decreased, due to the limitations of the optics.

In embodiments of the present invention the optical system 100 also comprises a spectrometer chip 130 wherein the spectrometer chip 130 is enabled for detecting radiation coming from the beam shaper 120. In embodiments of the present invention the spectrometer chip 130  
 15 comprises a plurality of detectors 210. Each detector comprises an incoupling grating 220, an outcoupling grating 230, and a spectrally dependent transmission system 240. The incoupling grating 220 is coupled with the outcoupling grating 230 through the spectrally dependent transmission system 240 and the incoupling gratings 220 of the different detectors 210 are arranged on a discrete number of lines. The incoupling gratings 220 typically may be arranged such that they are in line with the line  
 20 shaped radiation fields created by the beam shaper.

In an exemplary embodiment of the present invention the spectrometer chip comprises 200 lines wherein radiation is received. The height of the active part of the spectrometer chip equals 20 mm. This corresponds with a distance  $d_i$  between the lines of 0.1 mm. Each line in the spectrometer chip comprising around  $2000 \times 2$  waveguides. In this exemplary embodiment the total number of  
 25 waveguides and incoupling gratings  $N$  therefore is equal to  $200 \times 2 \times 2000 = 800,000$ . It is an advantage of embodiments of the present invention that the spectrometer étendue can be increased because the total number of waveguides can be large because of the spatial heterodynisation. By decreasing the distance  $d_i$  between the lines, the total number of lines can be increased even more given the same total height. The spectrometer étendue  $\varepsilon$  of the incoupling zone equals:

$$30 \quad \varepsilon = N \times \lambda^2 = 2000 \times 2 \times 200 \times (850 \text{ nm})^2 = 0.58 \text{ mm}^2$$

Hereby  $\lambda^2 = (850 \text{ nm})^2 = 0.72 = 0,72 \text{ } \mu\text{m}^2$  is the étendue of a waveguide.

In the exemplary embodiment described above the spectrometer étendue is up to  $0.58 \text{ mm}^2$  per photonics layer. With denser arrangements of waveguides, larger étendues per photonics layer may be possible. Multiple photonics layers can also be stacked to achieve higher overall étendues.

35 In the exemplary embodiment the width of a line equals 10 mm. In general, the width essentially depends on the output width of the collimator. In embodiments of the present invention

the distance between the lines  $d_i$  may vary depending on the resolution that is to be obtained. The distance between the lines may be set by the maximum length required to match the spectral resolution of the spectrometer. For the glucose spectrum, one may want to resolve peaks with a width of about 2 to 3 nm. In one example, the distance between the lines may vary between 20 $\mu$ m and 2mm, more preferably between 50 $\mu$ m and 1mm. In the exemplary embodiment the number of different spectral responses  $L$  equals 200. Therefore the number of waveguides per spectral type  $M$  equals: 800,000/200 = 4,000, or in other words on average 4,000 waveguides are used per spectrally different output of the spectrometer.

In embodiments of the present invention the spectrally dependent transmission system 140 is a Fabry-Perot system. Other compact structures with spectrally tunable transmission can be used as spectrally dependent transmission system 140. For example: a Mach-Zhender interferometer or a ring resonator, etc. In embodiments of the present invention the signal level is increased when the number of photons at the output of the spectrometer chip 130 is increased. The photon output of the spectrometer chip 130 is proportional to the étendue multiplied with the average photon transmission probability. The étendue per waveguide/incoupling grating 220 is limited. It is an advantage of embodiments of the present invention that a high photon output can be realized using a Fabry-Perot type spectrally dependent transmission system 140.

FIG. 13, FIG. 14, and FIG. 15 show the transmission ( $T_j(\lambda)$ ) of a waveguide in an optical system according to an embodiment of the present invention. A Fabry-Perot type spectrally dependent transmission system 140 is assumed. The length of the waveguide is 0.03 mm in case of FIG. 13, 0.1 mm in case of FIG. 14 and 0.5 mm in case of FIG. 15. The figures show the transmission in function of the wavelength. The transmission is measured at the outcoupling grating 230. FIG. 16 shows the incoming spectrum. The spectral intensity  $S(\lambda)$  is shown in function of the wavelength. FIG. 17 shows the transform of the spectrum response as a function of the waveguide index when the same spectrum is inserted in every waveguide. FIG. 17 shows:

$$r_j = \int T_j(\lambda)S(\lambda)d\lambda$$

wherein  $j$  is the waveguide index,  $S$  is the incoming spectrum, and  $T_j$  is the transmission of waveguide  $j$ . In embodiments of the present invention the input spectrum may be reconstructed based on the measurement results. The spectrum may be reconstructed using a least square fit. Such a reconstruction is shown in FIG. 18. FIG. 18 shows the input spectrum 1910 and shows the reconstructed spectrum 1920. The spectrum is reconstructed based on the measurement result shown in FIG. 17. In embodiments of the present invention a complete reconstruction of the input spectrum is not required (e.g. for the estimation of a glucose concentration). FIG. 19 shows an input spectrum with a double peak. One at 885 nm and one at 875 nm. FIG. 20 shows the input spectrum 2110 as well as the reconstructed spectrum 2120.

By decreasing the length of the spectrally dependent transmission system to 50  $\mu\text{m}$  a spectrometer chip 130 with a height of 20 mm can comprise 200 lines instead of 40. By increasing the number of waveguides with a factor 5, also the chip étendue is increased with a factor 5 to 0.58  $\text{mm}^2$ . It is an advantage of embodiments of the present invention that by decreasing the height of the spectrometer chip 130 the matching can be improved. In an exemplary embodiment comprising 4000  
5 waveguides per spectral response characteristic all 4000 waveguides need to be matched since the response will be added to obtain a  $\text{SNR} > 1$ .

In some embodiments a first rejection filter 140 may be present between the collimator 110 and the beam shaper 120. The first rejection filter may for example be provided for rejecting an  
10 excitation beam used for optically exciting a region of interest at one wavelength, whereas a radiative response at another wavelength is expected. In particular embodiments of the present invention the optical density of the first rejection filter may be above 6 for wavelengths between 675 nm and 830 nm. In the exemplary embodiment of FIG. 1 the light coming from the collimator 110 enters the rejection filter 140. The light coming from the rejection filter 140 enters the wedge 120 at the wedge  
15 entrance area 122 and leaves the wedge at the wedge exit area 124. The wedge entrance area 122 has an area of 30  $\text{mm}^2$ . The étendue of the light is 1.2  $\text{mm}^2$ . The light entering the collimator has an angular spread of 10.5° and a photon flux of  $0.4 \times 10^8$  photons/sec.

In embodiments of the present invention a second rejection filter also may be present between the beam shaper 120 and the spectrometer chip 130. In embodiments of the present  
20 invention the second rejection filter may be an on-chip long pass rejection filter using multilayer  $\text{SiO}_2/\text{a-SiC:H}$ . The optical density of the second rejection filter may be above 3. An exemplary embodiment thereof optimized for rejection at 532 nm is shown in FIG. 2.

The number of filters is not limited to 1 or 2. In some embodiments a third rejection filter also may be implemented inherently by using a single mode waveguide with a Bragg grating. The optical  
25 density of the third rejection filter may be above 1. Also a fourth rejection filter is present between the photonic chip and the imager/detector. The optical density of the fourth rejection filter may be above 4.

In embodiments of the present invention the overall optical density thus obtained may be above 9.

30 The optical system 100 according to embodiments of the present invention can be used in several types of products. Below is described how it is used as a glucose sensor. When used as a glucose sensor the following signal to noise ratios are to be considered:

-  $\text{SNR}_{\text{peak, glucose}}$ : the signal to noise ratio of the Raman spectral signal for glucose in deionized water measured at strong glucose Raman peaks, for example the 1126  $\text{cm}^{-1}$  peak being the glucose peak  
35 providing the strongest signal. In this case no strong fluorescence or Raman background is present.

-  $SNR_{peak, skin}$ : the signal to noise ratio of the Raman spectral signal for glucose in skin measured at strong glucose Raman peaks. In this case strong background fluorescence and other Raman signals lead to large shot noise.

-  $SNR_{system}$ : the signal to noise ratio of a glucose concentration measurement after analysis of spectrum. This value is higher than the  $SNR_{peak, skin}$  because information from multiple peaks is combined.

The signal to noise ratio assuming only glucose in water can be estimated as follows:

$$SNR_{peak, skin} = \frac{P_{glucose} \cdot t_{int} \cdot \eta_{IC} \cdot \eta_{det}}{\sqrt{P_{glucose} \cdot t_{int} \cdot \eta_{IC} \cdot \eta_{det}}}$$

wherein:

10  $P_{glucose}$  is the glucose spectrum

$\eta_{IC}$  is the incoupling efficiency being the overall incoupling efficiency of the optical system,

$\eta_{det}$  is the detector efficiency

and  $t$  is the integration time.

An example of the glucose spectrum multiplied with the detector efficiency is illustrated in FIG. 4.

15 The signal to noise ratio of the Raman spectral signal for glucose in skin assuming a background signal that is 1000 times stronger than the noise signal in DI water can be estimated as follows:

$$SNR_{peak, skin} = \frac{P_{glucose} \cdot t_{int} \cdot \eta_{IC} \cdot \eta_{det}}{\sqrt{P_{glucose} \cdot t_{int} \cdot \eta_{IC} \cdot \eta_{det} + P_{background}}}$$

wherein:

20  $P_{background} = 1000 \max (P_{glucose})$ .

FIG. 5 shows the measured spectrum 610 after an integration time of 10 seconds and the spectrum without noise 620. FIG. 6 shows the measured spectrum 710 after an integration time of 120 seconds and the spectrum without noise 720. Given a glucose spectrum  $P_{glucose} \times \eta_{det}$  a  $SNR_{peak, skin}$  of 1.7 can be obtained after a 10 seconds integration time and a  $SNR_{peak, skin}$  of 6 can be obtained after a 120

25 seconds integration time.

In embodiments of the present invention the glucose signal is estimated by least square fitting the glucose spectrum with each of the measured spectra. When assuming a known and stable background an increased signal to noise ratio can be obtained. After a 10 seconds integration time the obtained  $SNR_{system}$  is 4.0 instead of  $SNR_{peak, skin}$  of 1.7. This is illustrated in FIG. 7. The estimated glucose concentration for a set of measurements on a sample without glucose is shown (810) as well as on a sample with 40 mg/dl of glucose (820). The histograms 830 and 840 are also shown. After a 120 seconds integration time the obtained  $SNR_{system}$  is 13 instead of  $SNR_{peak, skin}$  of 6. This is illustrated in FIG. 8. The estimated glucose concentration for a set of measurements on a sample without glucose is shown (910) as well as on a sample with 40 mg/dl of glucose (920). The histograms 930 and 940 are also shown. 500 fits were done without glucose (noise is seen as glucose contribution), and 500 fits

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with glucose at 40 mg/dl. 40 mg/dl is the minimum physiological concentration of glucose. The  $SNR_{system}$  is expected to scale with the  $\sqrt{\text{number of strong peaks} = 6} \sim 2.5$ . This corresponds with the results shown in FIG. 7 and FIG. 8 when applying the following formula:

$$SNR_{system} = \frac{S}{\sqrt{2}\sigma}$$

5 wherein S and  $\sigma$  are as shown in the FIG. 7.

FIG. 9 and FIG.10 show a Clarke error grid for the  $SNR_{system}$  after a ten seconds integration time and 120 seconds integration time respectively. The incoupling efficiency  $\eta_{ic}$  of both is equal to 2%, the detector efficiency  $\eta_{det}$  is equal to 30%. A background signal 1000 times stronger than the glucose signal is assumed. According to the FDA guidance 95% of the measurements should fall in zone A, less than 5% should fall in zone B, and 0% should fall in zones C, D or E. The  $SNR_{system}$  corresponding with FIG. 9 is equal to 3.9 and the  $SNR_{system}$  corresponding with FIG. 10 is equal to 13. From the graphs it can be concluded that a  $SNR_{system} > 4$  at the lowest physiological concentration of (40 mg/ dl) is sufficient for glucose concentration. It is an advantage of embodiments of the present invention that this signal to noise ratio can be obtained.

15

In a second aspect, the present invention relates to a detector system 1200. The detector system 1200 comprises an optical system 100 as indicated above being part of or being mounted on an optical printed circuit board 1210, including the optical part of the spectrometer. The detector system 1200 moreover comprises a read-out printed circuit board 1220 for reading out the optical signal received from the optical part of the spectrometer described in the first aspect. The read-out printed circuit board 1220 is connected with the optical printed circuit board 1210. The read-out printed circuit board 1220 digitizes the optical signal coming from the optical system 100 and/or processes the digitized result. An exemplary embodiment thereof is shown in FIG. 11.

In embodiments of the present invention the detector system 1200 comprising a wristband 25 1310. The optical system 100 and the read-out printed circuit board 1220 are integrated in the wristband 1310. In the exemplary embodiment illustrated in FIG. 12 the dimensions  $d_w$ ,  $t_w$ , and  $w_w$  are indicated. These dimensions may be as follows:  $d_w = 6.5$  cm,  $t_w = 7.4$  mm, and  $w_w = 14$  mm. Due to the small thickness of the optical system, the wristband can be limited in height, resulting in a high degree of wearability.

30

In a third aspect, the present invention also relates to an optical radiation guiding system comprising a collimator and beam shaper as described in the first aspect, without the optical part of the spectrometer being present. Such an optical radiation guiding system thus may be a separate component. Features and advantages thereof may be as described in the first aspect.

35

In the following aspects the RAMAN spectrometer in the embodiments of the present invention corresponds with an optical system according to the previous aspects of the present invention.

5 In a fourth\_aspect of the disclosure, an integrated circuit for performing spectroscopy on tissue is presented. The device comprises: a first optical unit comprising: a RAMAN spectrometer; an OCT spectrometer; an interferometer optically coupled to the OCT spectrometer; and a light coupler, positioned to couple scattered and reflected light from illuminated tissue into the RAMAN and OCT spectrometer; and an imaging region optically coupled to the RAMAN and OCT spectrometer.  
10 According to an embodiment of the disclosure, the integrated circuit further comprises at least a second optical unit, wherein the imaging region is optically coupled to the RAMAN and OCT spectrometer of each optical unit. According to an embodiment of the disclosure, the first optical unit further comprises an IR spectrometer optically coupled to the light coupler; and further comprising an infrared imaging region optically coupled to the IR spectrometer.

15

In a fifth aspect of the disclosure, an integrated circuit for performing spectroscopy on tissue is presented. The device comprises: a first optical unit comprising: a RAMAN spectrometer; an IR spectrometer; a light coupler, positioned to couple scattered and reflected light from illuminated tissue into the RAMAN and IR spectrometer; an imaging region optically coupled to the RAMAN spectrometer; and an infrared imaging region optically coupled to the IR spectrometer. According to an  
20 embodiment of the disclosure, the integrated circuit further comprises at least a second optical unit; wherein the imaging region is optically coupled to the RAMAN spectrometer of each optical unit; and wherein the infrared imaging region is optically coupled to the IR spectrometer of each optical unit. According to an embodiment of the disclosure, the first optical unit further comprises: an OCT spectrometer optically coupled to light coupler; and an interferometer optically coupled to the OCT spectrometer; and wherein the imaging region is optically coupled to the OCT spectrometer. According to an embodiment of the disclosure, the integrated circuit further comprises at least a second optical unit; wherein the imaging region is optically coupled to the RAMAN and OCT spectrometer of each optical unit; and wherein the infrared imaging region is optically coupled to the IR spectrometer of  
30 each optical unit. According to an embodiment of the disclosure, the integrated circuit further comprises at least one optical waveguide distributor for distributing a light beam of a light source on the integrated circuit thereby allowing simultaneous illumination of different locations of tissue. According to an embodiment of the disclosure, the integrated circuit further comprises at least one through-hole thereby allowing illumination of tissue through the integrated circuit. According to an  
35 embodiment of the disclosure, the integrated circuit further comprises at least one rejection filter located to allow, when in operation, only scattered light reaching the RAMAN spectrometer. According

to an embodiment of the disclosure, the integrated circuit comprises a plurality of active electronic component layers thereby forming a three-dimensional integrated circuit wherein each active electronic component layer comprises the first optical unit or the at least one second optical unit. The integrated circuit may be a 3D (stacked) integrated circuit comprising different layers, each layer comprising an optical unit. According to an embodiment of the disclosure, the light coupler of the first or the at least one second optical unit of each active electronic component layer is configured to couple light with a different wavelength into the RAMAN spectrometer. Each light coupler of an optical unit present in a layer of the 3D integrated circuit may be configured to couple light with a specific wavelength in a spectrometer. The wavelength ranges of different light couplers may be adjacent to allow in coupling of light with wavelengths falling within a specific wavelength range. According to an embodiment of the disclosure, one or more photodiodes of the imaging region comprise a spectral filter for spectrally resolving RAMAN scattered light. At least one photodiode in the imaging region, which may be present in an active electronic component layer of the integrated circuit, may comprise a spectral filter. Different photodiodes of the imaging region may comprise different spectral filters.

In a sixth aspect of the disclosure, a wearable system for non-invasive measuring of the concentration of an analyte in tissue is presented. The system comprising: an integrated circuit according to an embodiment of the disclosure; a first light source optically coupled to the integrated circuit and configured to emit a laser beam for performing Raman spectroscopy; a second light source optically coupled to the integrated circuit and configured to emit a broadband light beam for performing OCT spectroscopy or IR spectroscopy; read-out electronics electrically coupled to the integrated circuit and configured to read out and correlate spectroscopic data from the RAMAN and IR spectrometer or from the RAMAN and OCT spectrometer and to determine the concentration of an analyte using the correlated spectroscopic data. According to an embodiment of the disclosure, the system further comprises a third light source optically coupled to the integrated circuit and configured to emit a broadband light beam for performing IR spectroscopy or OCT spectroscopy; and wherein the read-out electronics is further configured to read out and correlate spectroscopic data from the RAMAN, OCT and IR spectrometer and determine the concentration of an analyte using the correlated spectroscopic data.

According to an embodiment of the disclosure, the second light source is a low coherent light source or a very wide bandwidth source and the third light source is low coherent light source or a very wide bandwidth source.

According to an embodiment of the disclosure, the system further comprises at least one optical reflector adapted to couple light from a light source in the integrated circuit.

According to an embodiment of the disclosure, the tissue is skin tissue and the system is completely packaged in a wearable casing and the wearable casing is adapted to press the integrated circuit against the skin tissue of an individual when worn thereby allowing scattered and reflected light from

illuminated skin tissue to be received by the integrated circuit. According to an embodiment of the disclosure, the wearable casing is a wristband, the size of the wristband being adaptable to allow pressing of the integrated circuit against the skin of an individual when worn. According to an embodiment of the disclosure, the wearable casing is a watch comprising a watch strap, the size of the watch strap being adaptable to allow pressing of the integrated circuit against the skin of an individual when worn.

In a seventh aspect of the disclosure, a method for non-invasive measuring of the concentration of analyte in tissue using the wearable system is presented. The method comprises: simultaneously obtaining spectra of Raman scattered light at different locations of the tissue; obtaining an optical model of the tissue; correlating the obtained spectra of Raman scattered light with the obtained optical model; determining the concentration of the analyte using the correlated data.

According to an embodiment of the disclosure, obtaining an optical model of the tissue comprises determining thicknesses and optical properties of different layers of the tissue. According to an embodiment of the disclosure, the tissue is skin tissue and obtaining an optical model of the tissue comprises obtaining a skin model of skin tissue underneath the sensor, the skin model comprising information on thickness and optical properties of different layers of the skin tissue. According to an embodiment of the disclosure, the skin model further comprises information on the refractive index of interstitial fluid and blood in the skin tissue. According to an embodiment of the disclosure, the analyte is glucose. According to an embodiment of the disclosure, obtaining an optical model of the tissue is done using IR spectroscopy and/or using OCT spectroscopy. According to an embodiment of the disclosure, simultaneously obtaining spectra of Raman scattered light of the tissue at different locations and obtaining an optical model of the tissue is performed simultaneously.

In an eighth aspect of the disclosure, the system may be used for measuring the concentration of glucose in living tissue.

**Claims**

- 1.- An optical system (100) for characterizing a radiation beam, the optical system (100) comprising:
  - an optical radiation guiding system comprising
    - a collimator (110) for collimating the radiation beam into a collimated radiation beam, and
    - 5       - a beam shaper (120) for distributing the power of the collimated radiation beam over a discrete number of line shaped fields, the spectrum of the collimated radiation beam entering the beam shaper being delivered to each of the discrete number of line shaped fields, and
    - a spectrometer chip (130) wherein the spectrometer chip (130) is adapted for processing the radiation in a discrete number of line shaped fields coming from the beam shaper (120).
- 10   2.- An optical system (100) according to claim 1, wherein the beam shaper (120) has a wedge shape.
- 3.- An optical system (100) according to claim 2, wherein the collimator and the beam shaper are arranged so that the beam shaper can receive radiation via a wedge entrance area (122) being the short side of the wedge.
- 15   4.- An optical system (100) according to any of claims 2 to 3, wherein the beam shaper is shaped so that radiation incident orthogonally at a wedge entrance area is guided directly to the wedge exit area without first being reflected at another surface of the wedge.
- 5.- An optical system (100) according to any of the previous claims, wherein at least part of the collimator (110) has a 3D parabolic shape.
- 20   6.- An optical system (100) according to any of the previous claims, wherein the collimator 110 has an entrance point and is shaped so as to fold an irradiation beam between the entrance point and an output of the collimator.
- 7.- An optical system (100) according to any of the previous claims, wherein the beam shaper comprises an exit area for directing the radiation to the discrete number of line shaped fields, the exit area having a waved or stepped pattern.
- 25   8.- An optical system (100) according to claim 7, wherein the waved or stepped pattern comprises a plurality of first segments (310) and a plurality of second segments (320), the second segments interconnecting the first segments, neighbouring first segments being positioned at a distance shorter than the length of the first segments and oriented substantially parallel with an orthogonal direction to an entrance area of the beam shaper.
- 30   9.- An optical system (100) according to claim 8, wherein the second segments (320) are curved.
- 10.- An optical system (100) according to any of the previous claims, wherein the spectrometer chip (130) comprises a plurality of detection channels (210), each detection channel comprising:
  - an incoupling grating (220),
  - 35       - an outcoupling grating (230),

- a spectrally dependent transmission system (240) wherein the incoupling grating (220) is coupled with the outcoupling grating (230) through the spectrally dependent transmission system (240) and wherein the incoupling gratings (220) of the different detectors (210) are arranged on a discrete number of lines.

- 5 11. An optical system (100) according to claim 10, wherein the spectrally dependent transmission system (240) is a Fabry-Perot system.
- 12.- An optical system (100) according to any of the previous claims, wherein a first rejection filter (140) is present between the collimator (110) and the beam shaper (120) for rejecting an excitation radiation.
- 10 13.- An optical system (100) according to any of the previous claims, the optical system being integrated in a wristband.
- 14.- Use of an optical system (100) according to any of the claims 1 to 13 as a glucose sensor.

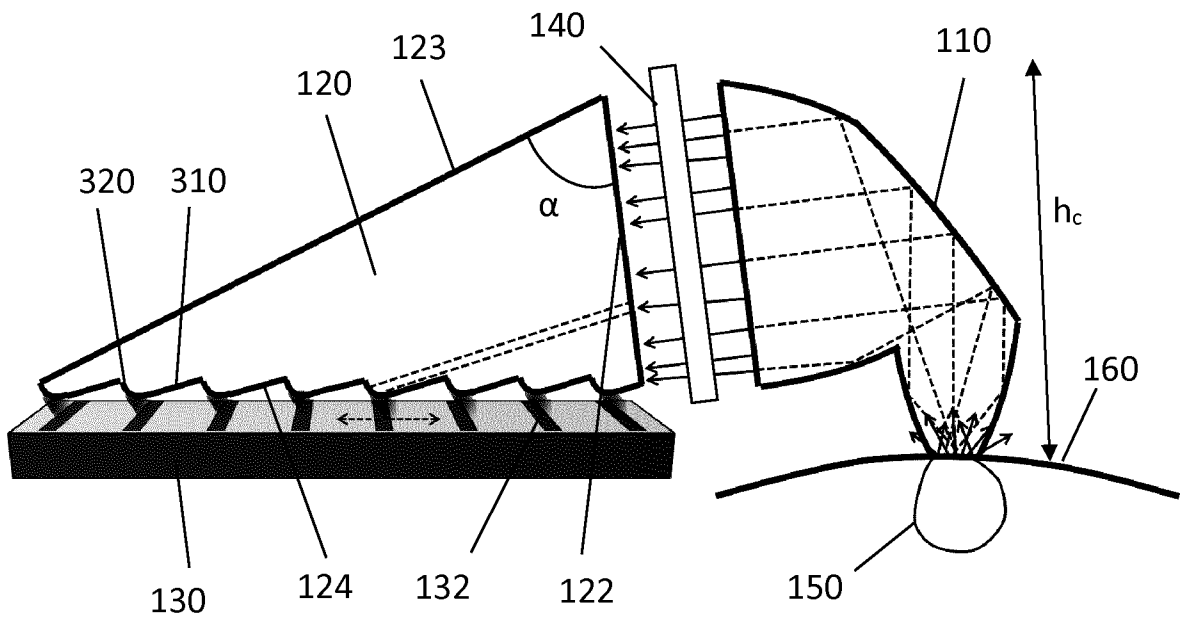


FIG. 1a

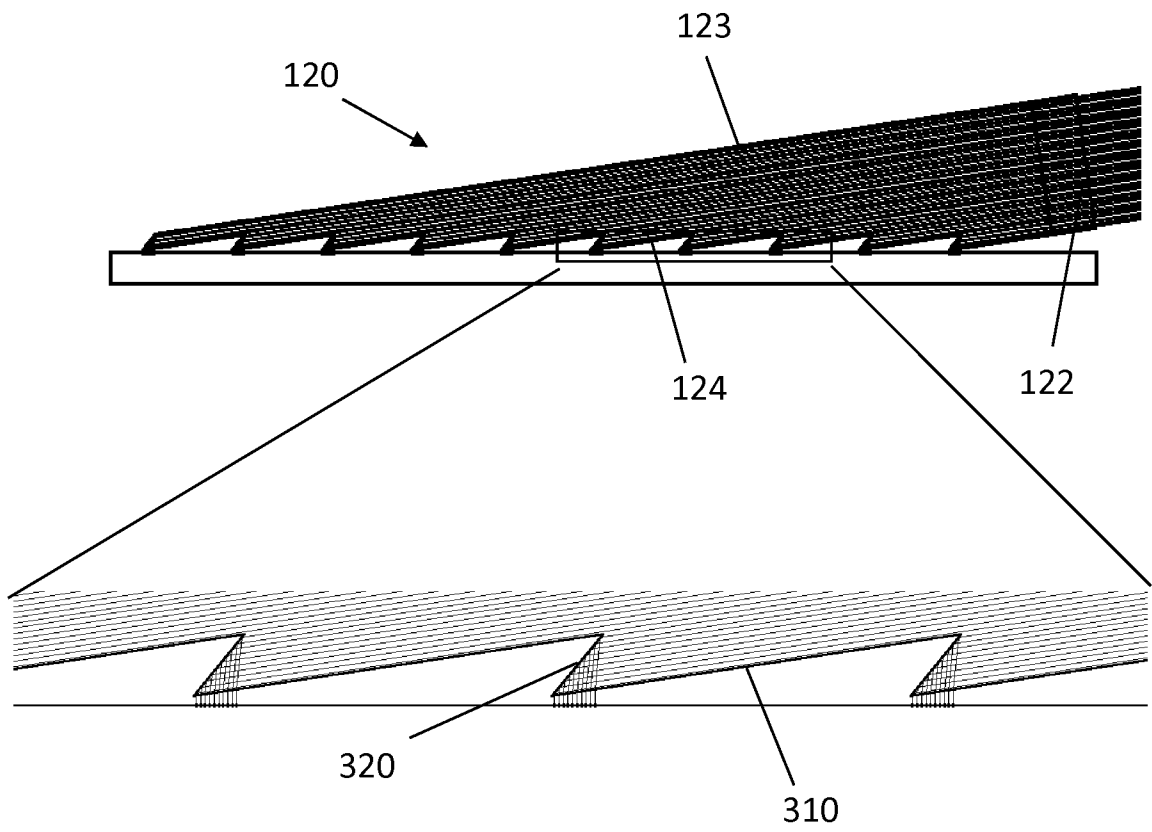


FIG. 1b

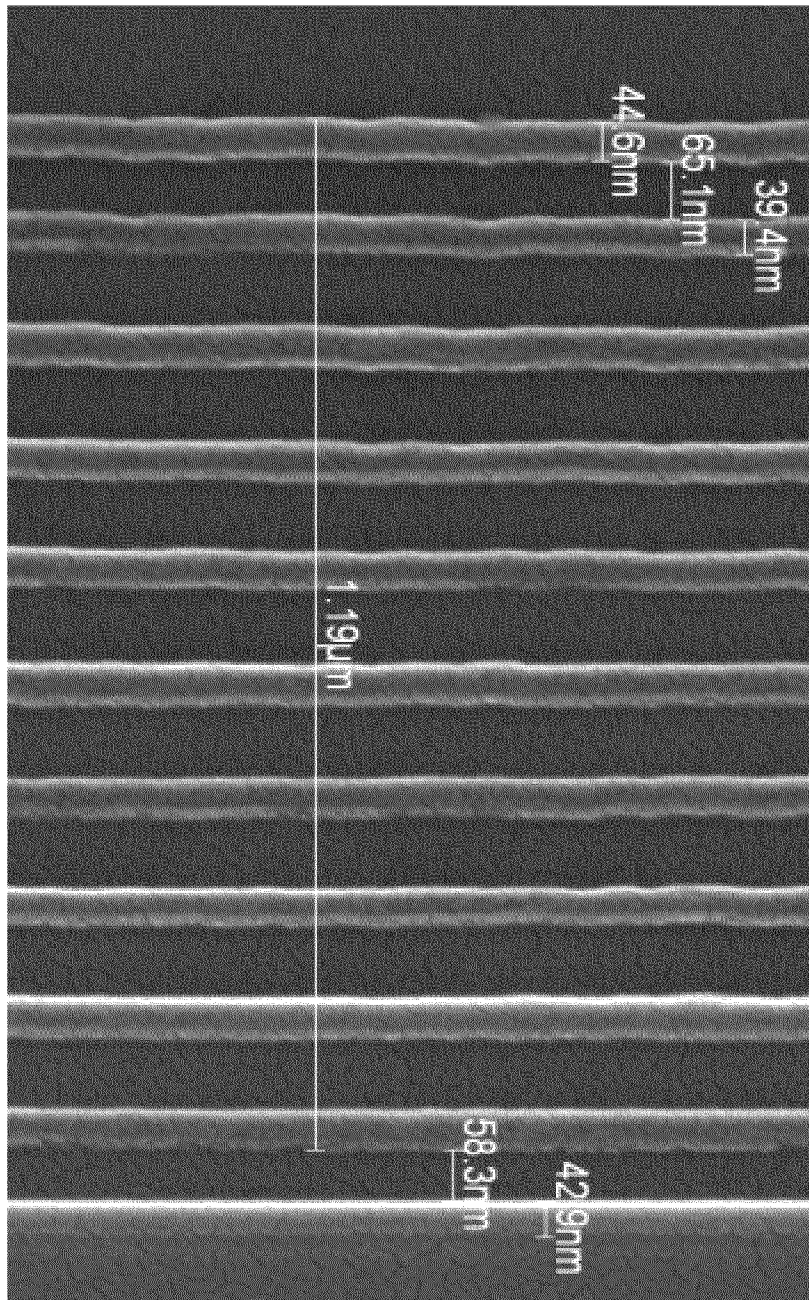


FIG. 2



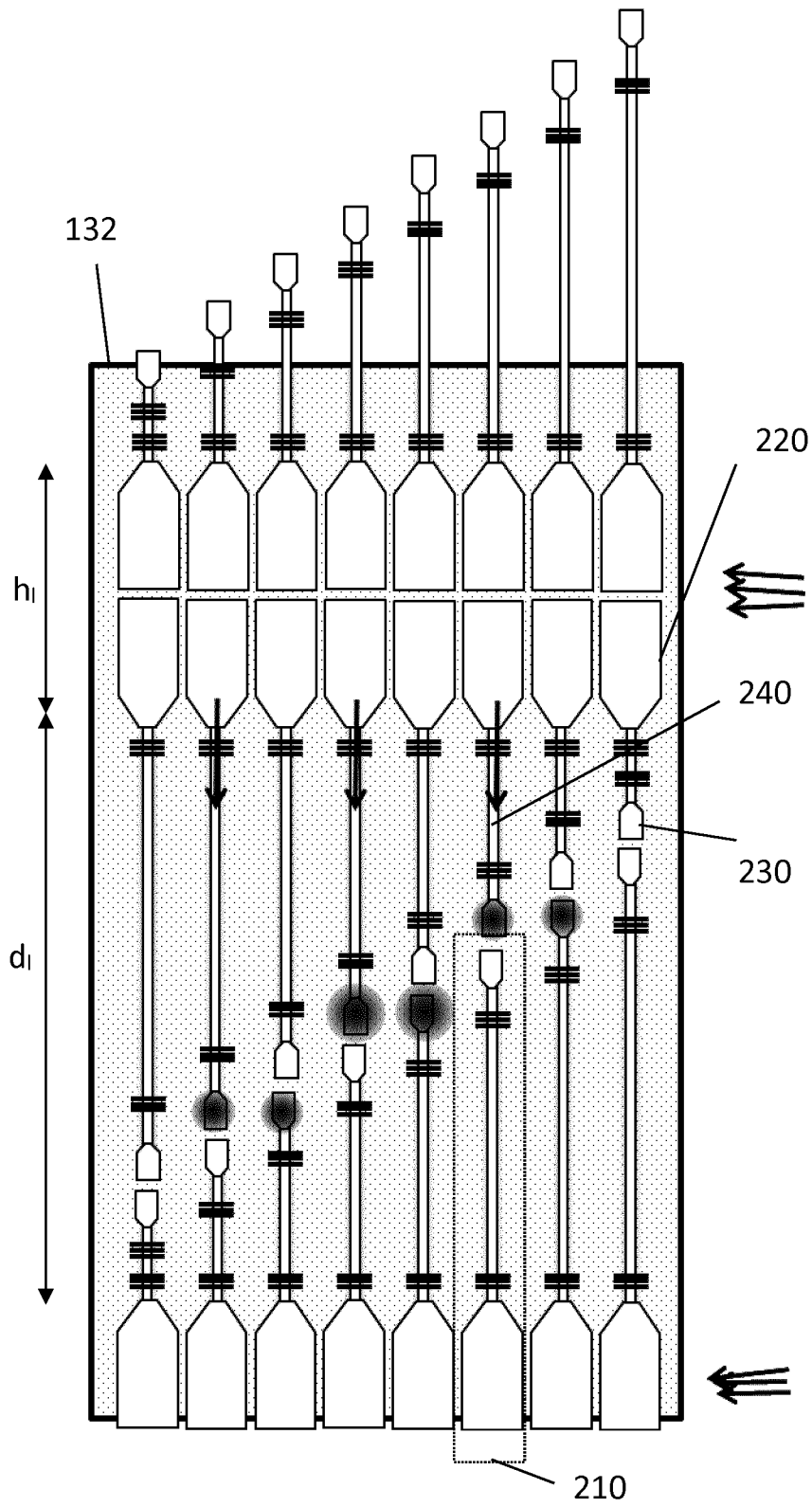
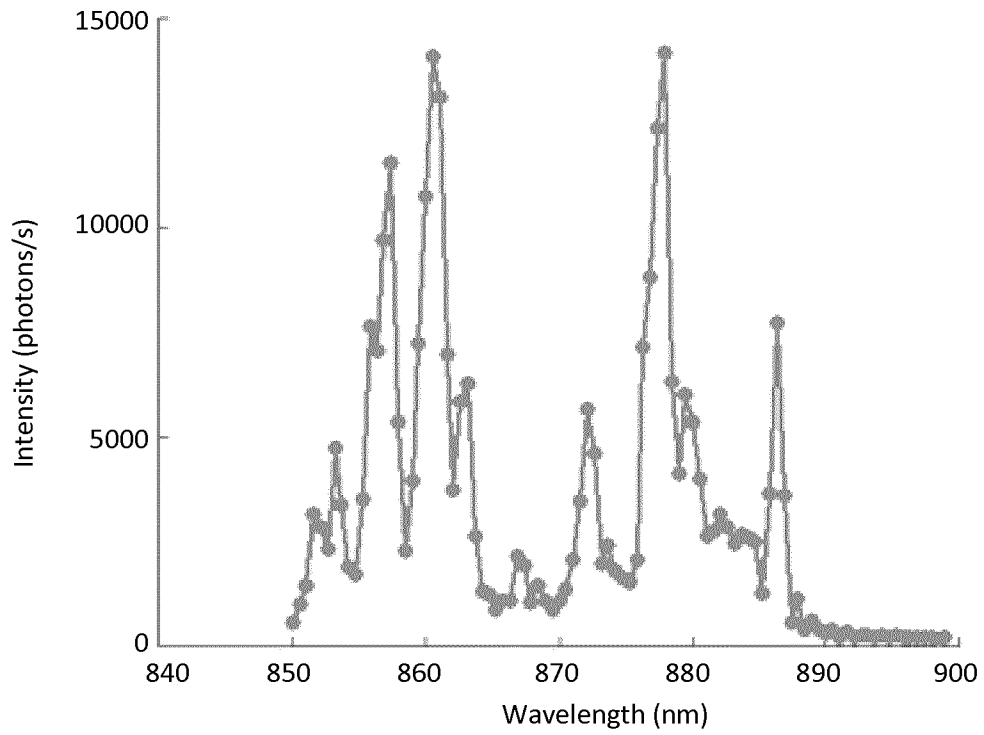
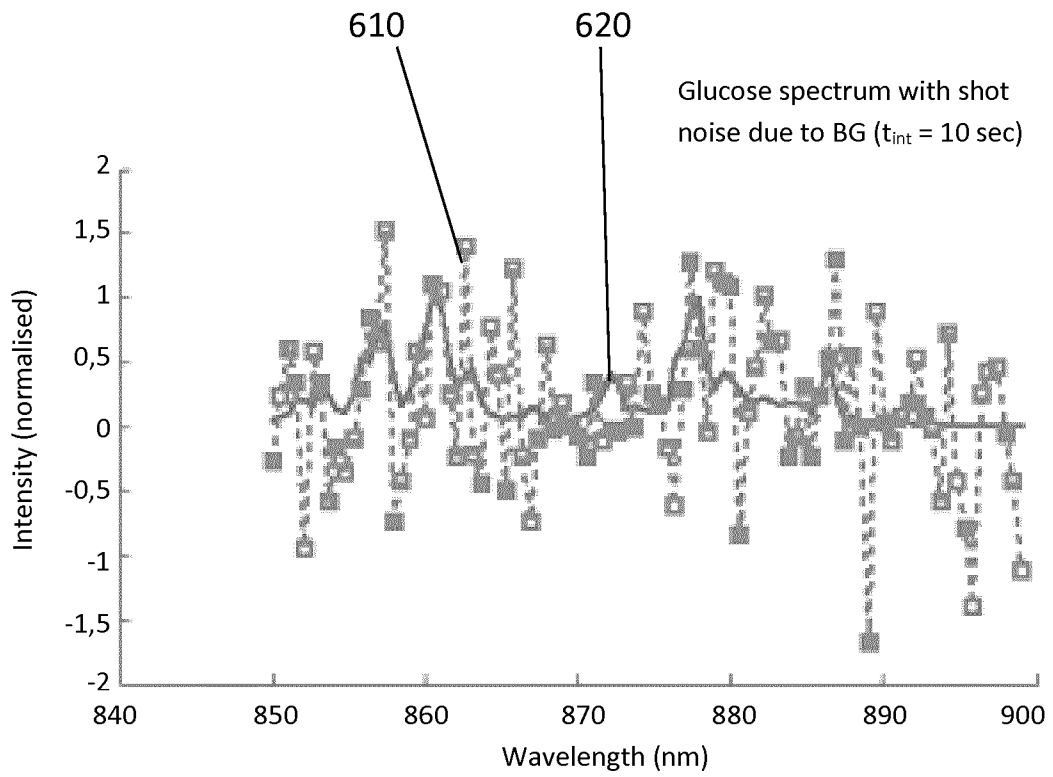


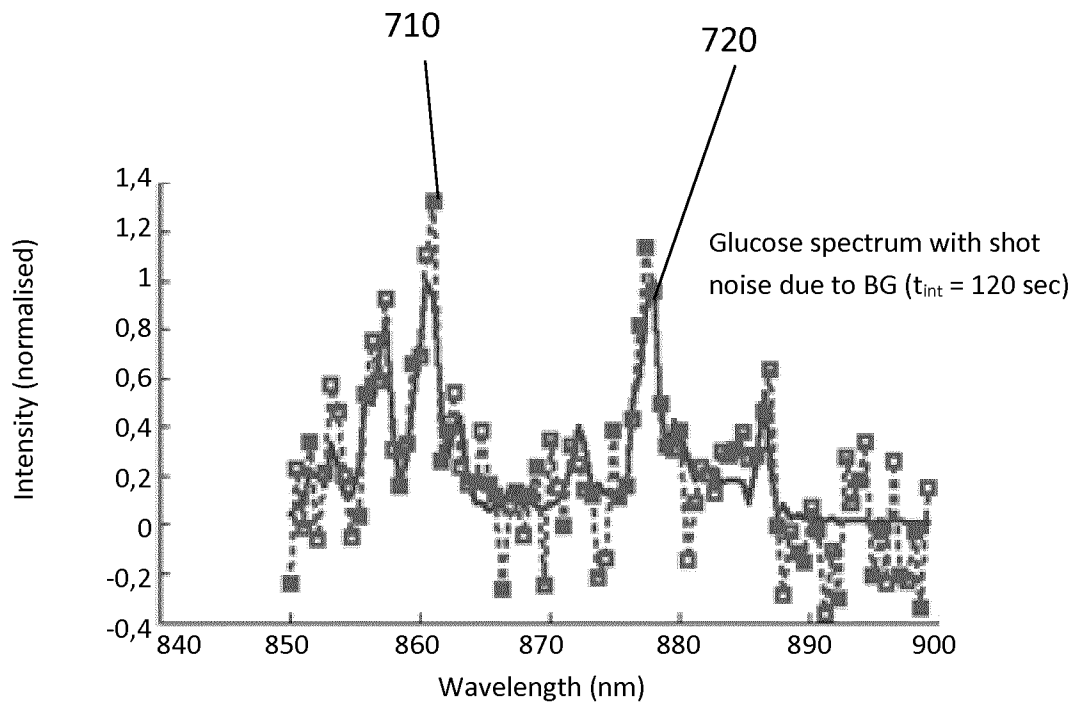
FIG. 3



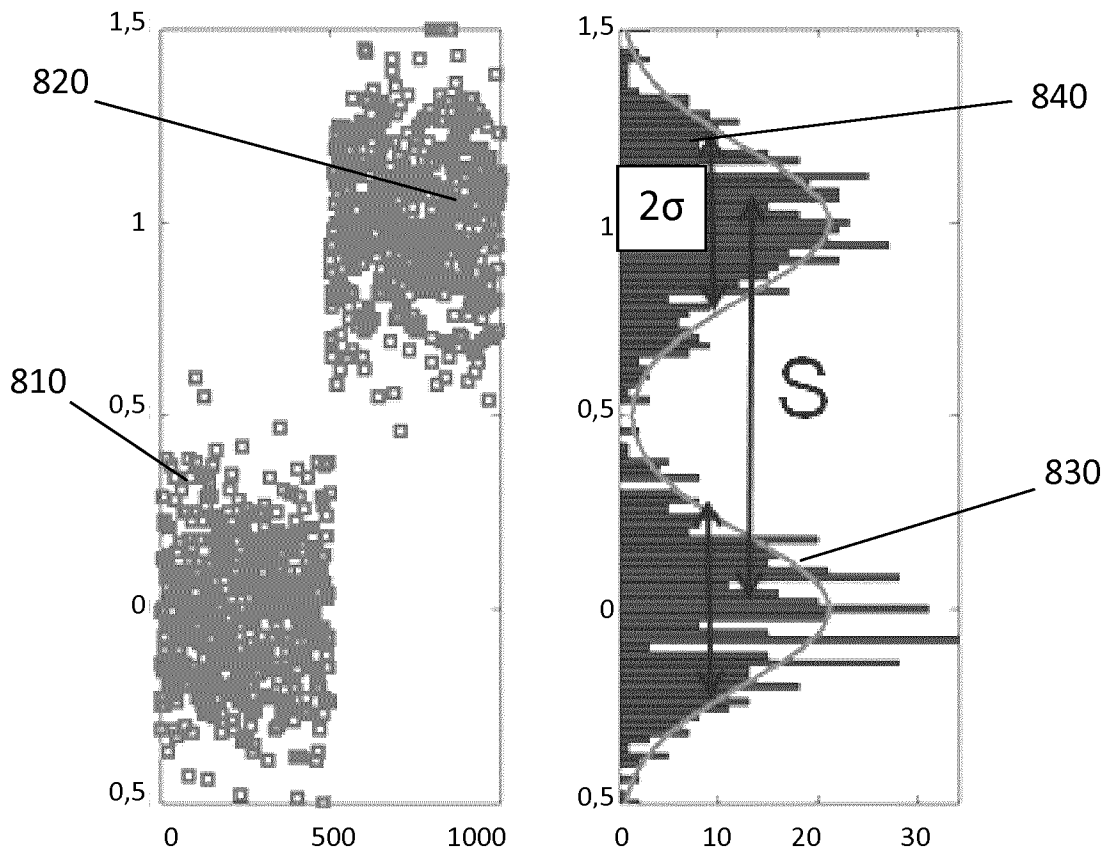
**FIG. 4**



**FIG. 5**



**FIG. 6**



**FIG. 7**

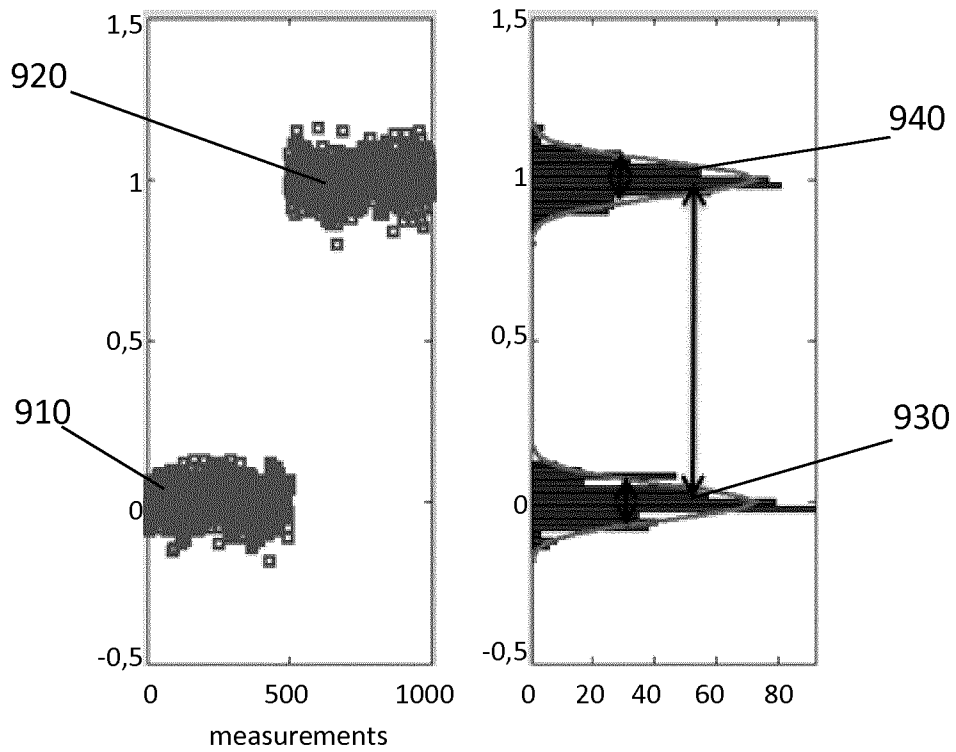


FIG. 8

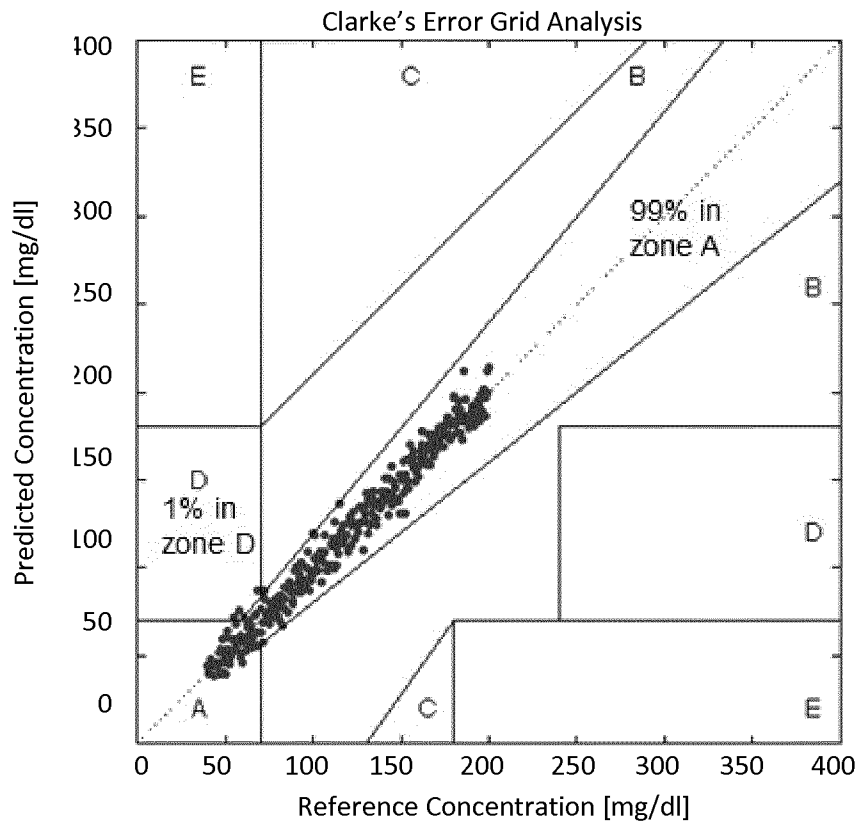
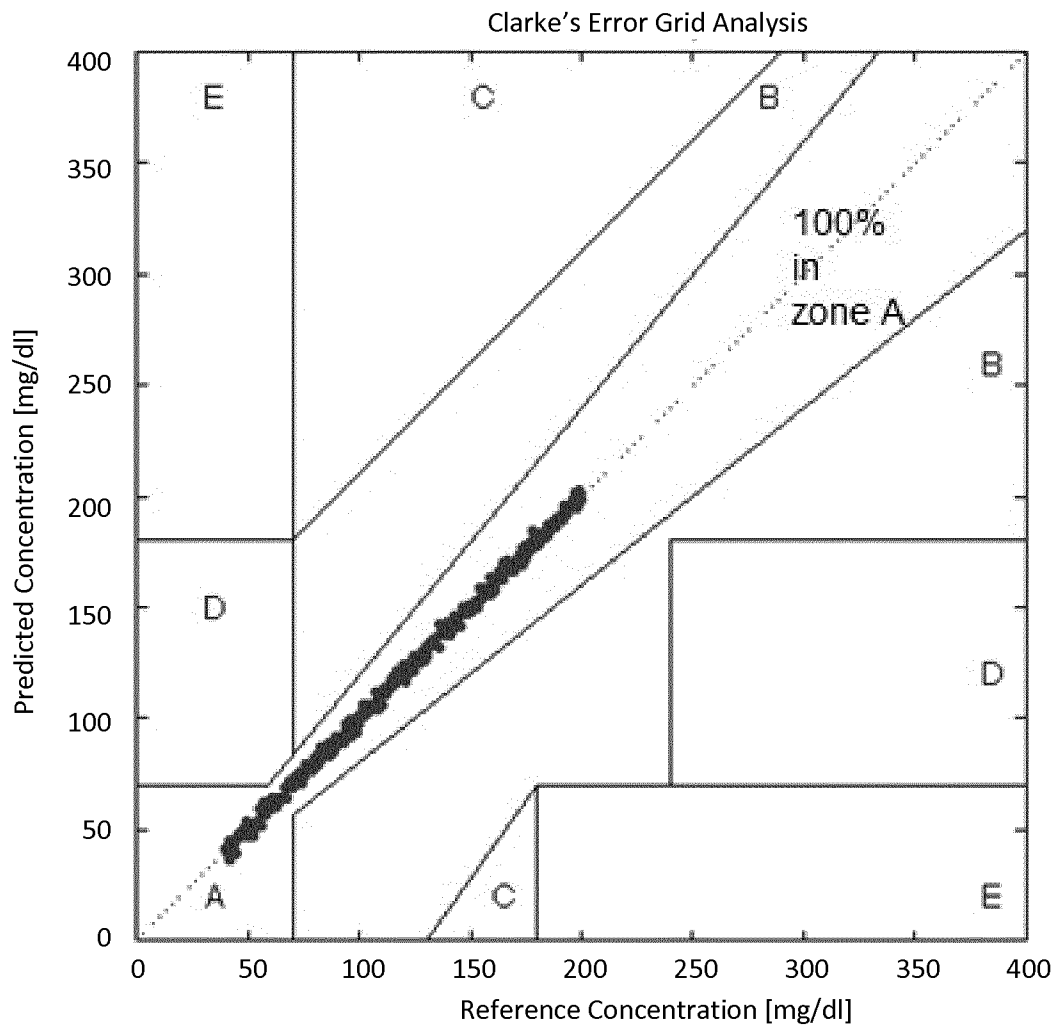
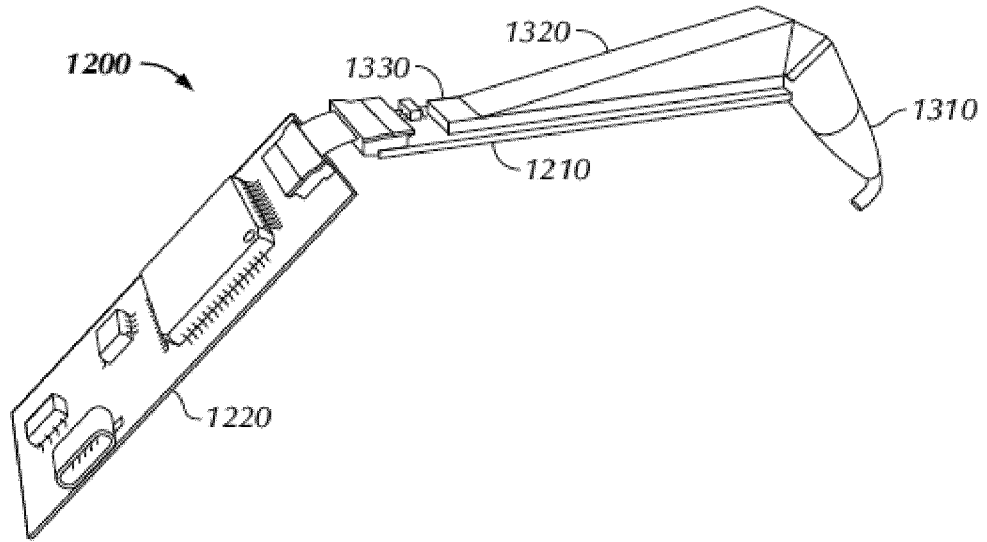


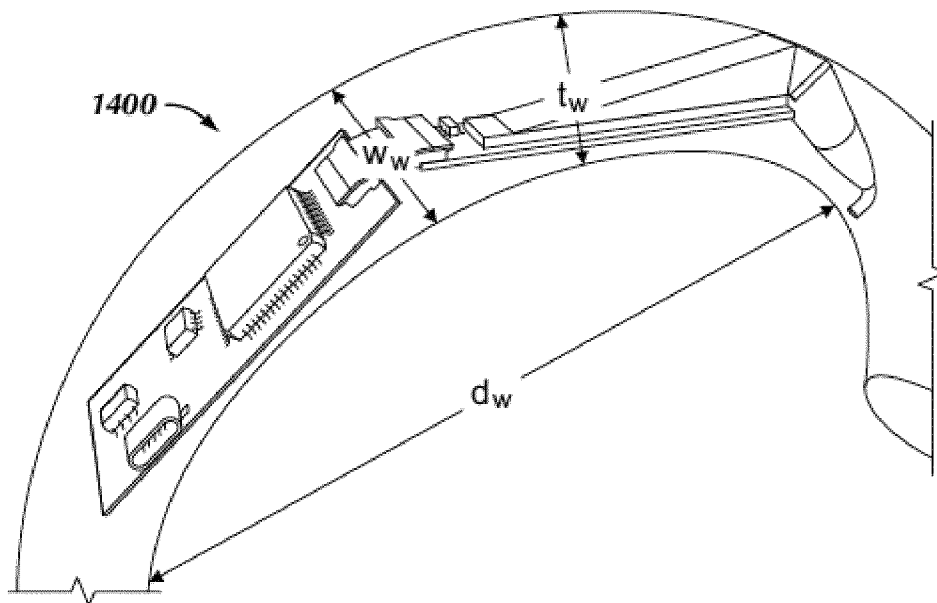
FIG. 9



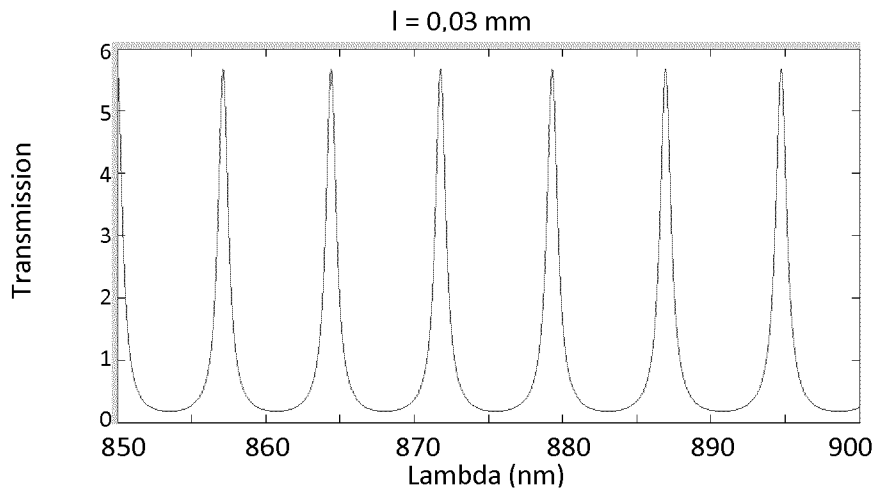
**FIG. 10**



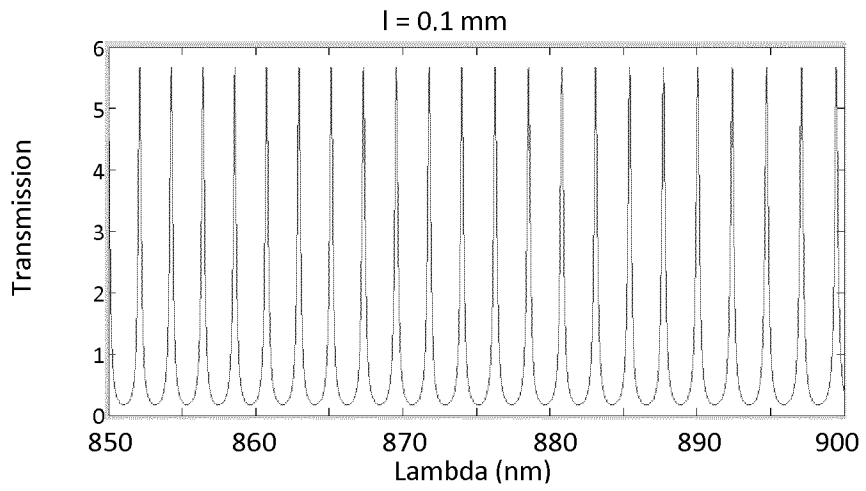
**FIG. 11**



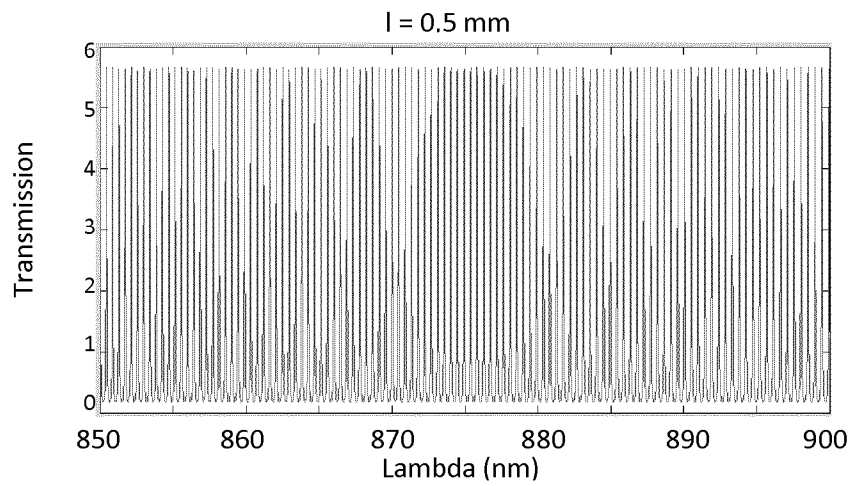
**FIG. 12**



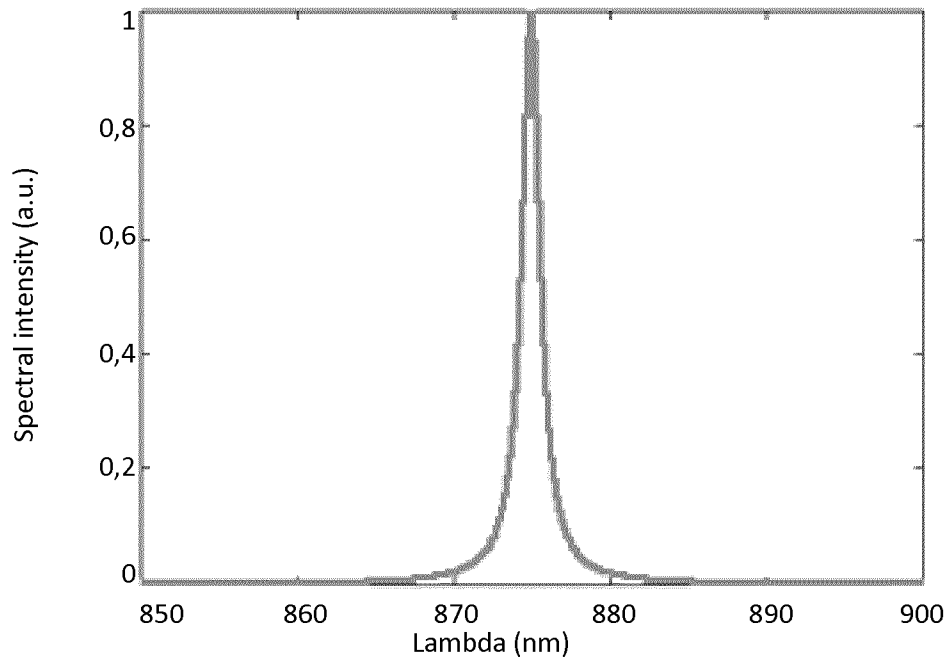
**FIG. 13**



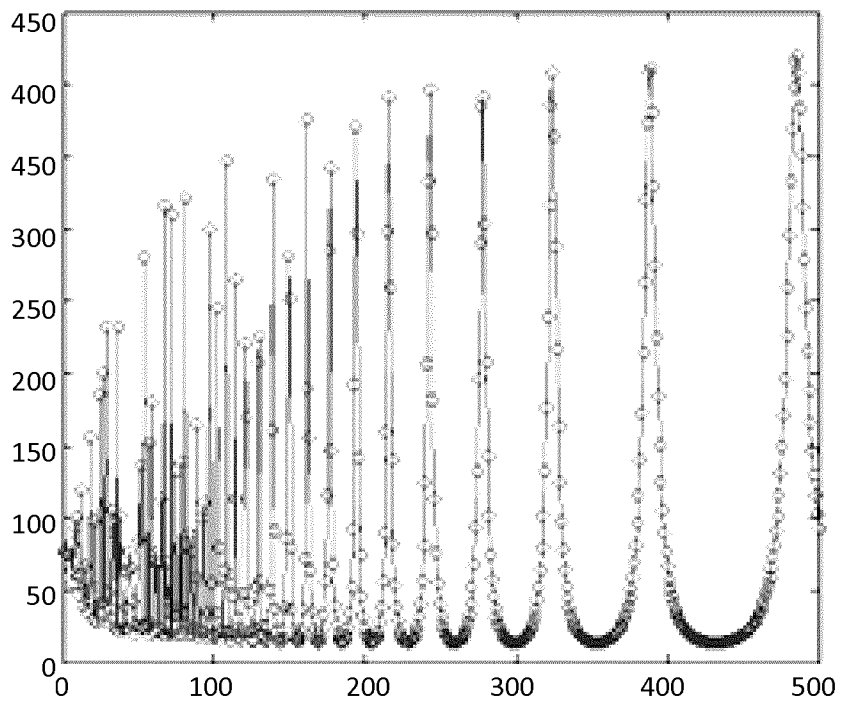
**FIG. 14**



**FIG. 15**

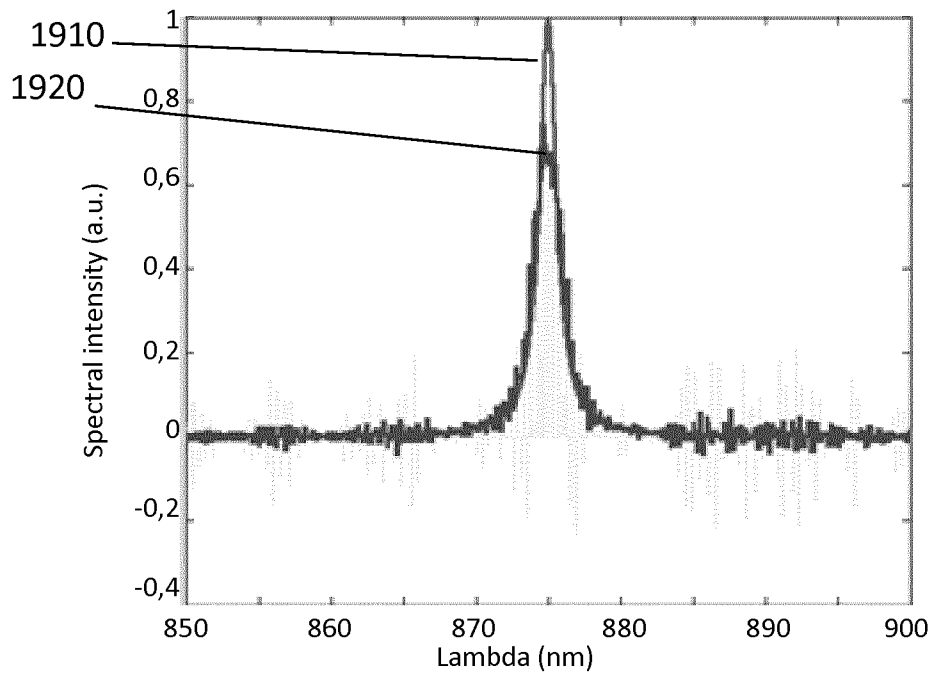


**FIG. 16**

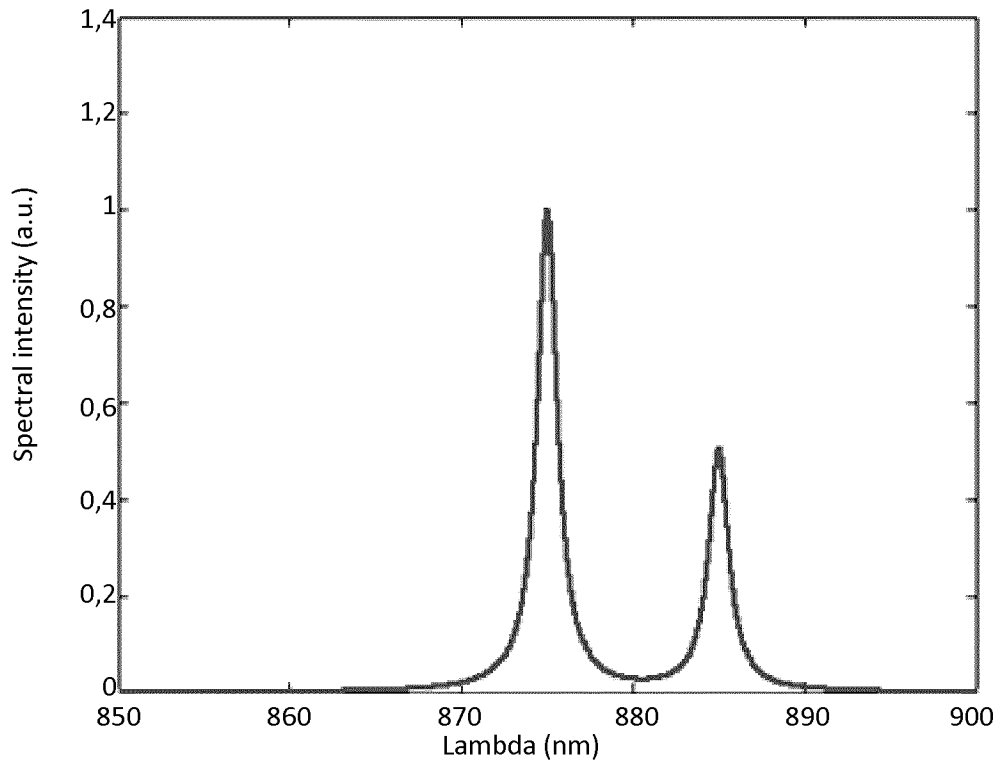


**FIG. 17**

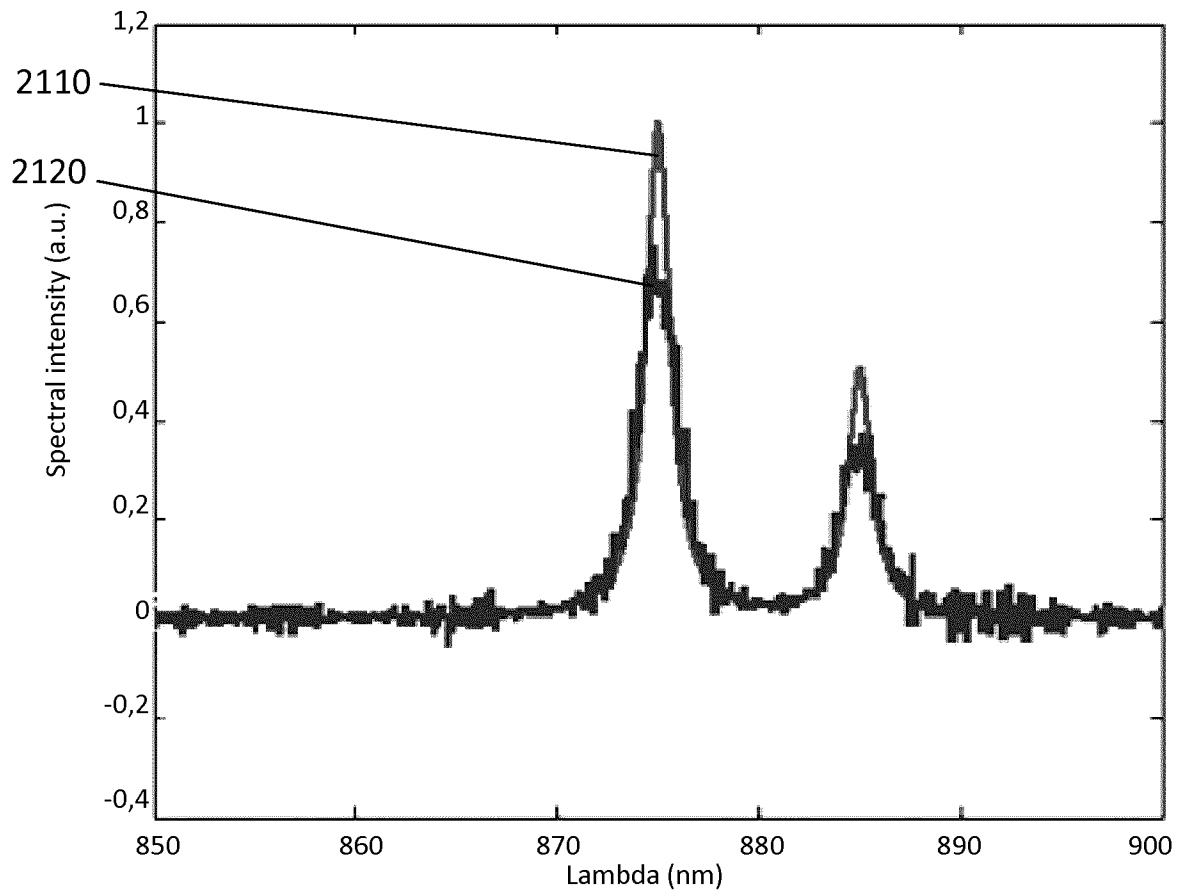




**FIG. 18**



**FIG. 19**



**FIG. 20**

INTERNATIONAL SEARCH REPORT

International application No  
PCT/EP2015/054225

A. CLASSIFICATION OF SUBJECT MATTER  
 INV. G01N21/65 G01J3/02 G01J3/36 G01J3/44  
 ADD.  
 According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED  
 Minimum documentation searched (classification system followed by classification symbols)  
 G01N G01J G02B  
 Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)  
 EPO-Internal, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
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A	US 2012/275189 A1 (LAINE JEFFREY A [US] ET AL) 1 November 2012 (2012-11-01) paragraph [0013] - paragraph [0018] paragraph [0025] - paragraph [0027] figures 1-4,5c,6 -----	1,14
A	US 5 011 284 A (TEDESCO JAMES M [US] ET AL) 30 April 1991 (1991-04-30) column 3, line 25 - line 49 column 4, line 24 - line 45 figures 1,2 -----	1-14
	-/--	

Further documents are listed in the continuation of Box C.

See patent family annex.

\* Special categories of cited documents :

<p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier application or patent but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p>	<p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art</p> <p>"&amp;" document member of the same patent family</p>
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Date of the actual completion of the international search  27 May 2015	Date of mailing of the international search report  03/06/2015
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Name and mailing address of the ISA/ European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Fax: (+31-70) 340-3016	Authorized officer  Verdoodt, Erik
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## INTERNATIONAL SEARCH REPORT

International application No  
PCT/EP2015/054225

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
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