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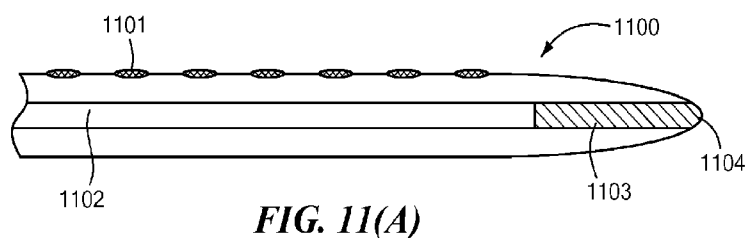


FIG. 11(A)

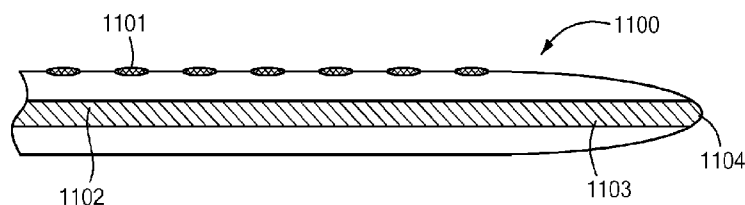


FIG. 11(B)

(57) Abstract: A cochlear implant electrode includes an implantable electrode carrier having an outer surface with electrode contacts for electrically stimulating nerve tissue of the inner ear of a patient. A drug lumen is within the electrode carrier and adapted to receive a therapeutic fluid. The drug lumen contains delivery openings to the outer surface of the electrode carrier and a hydrogel matrix disposed between the drug lumen and the one or more delivery openings and adapted to swell in volume when exposed to the therapeutic fluid. The hydrogel matrix is adapted to control diffusion of the therapeutic fluid from the drug lumen through the delivery openings to the outer surface of the electrode carrier.



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TITLE

Hydrogel-Filled Drug Delivery Reservoirs

[0001] This application claims priority from U.S. Provisional Patent 61/112,818, filed November 10, 2008, and U.S. Provisional Patent 61/243,209, filed September 17, 2009, which are incorporated herein by reference.

FIELD OF THE INVENTION

[0002] The present invention relates to medical implants, and more specifically to implantable drug delivery systems for the inner ear.

BACKGROUND ART

[0003] There is increased interest in implantable drug delivery systems to deliver therapeutic fluids to targeted internal tissues such as the inner ear. Drug eluting electrode leads with cortico steroids have been used successfully in the past with cardiac pacemaker electrodes to reduce the contact impedance. In addition, silicone elastomer loaded with a pharmacological agent has been used as an eluting structure in several applications such as birth control, vascular injury treatment, and stents. There also have been attempts to deliver medicine to the inner ear, for example to promote healing after implantation of cochlear implant electrode.

[0004] But materials that release a therapeutic substance do not necessarily have a desirable linear release rate and/or may not be refillable (e. g. NuvaRing® birth control device). Large complex implantable drug delivery pumps (e.g. from tricumed Medizintechnik GmbH) are known for implantation in body regions such as the abdomen for delivering significant amounts of therapeutic fluids into the circulatory system. However this technology is designed to deliver relatively large amounts of drugs in body locations which are less fragile and which allow greater implant dimensions than the inner ear.

[0005] In US 2009/062896 A1, the inventor describes a nonlinear release profile as illustrated in his Fig.13. His Fig. 16 shows that this release profile is achieved by loading

different forms of the drug dexamethasone, such as dexamethasone salt and dexamethasone base, into a storage lumen.

[0006] WO0241666 describes an electrode carrier having a drug impregnated bioresorbable gel that when implanted in a patient releases the drug over time. During manufacture, the electrode must be soaked in the liquid drug for long enough to absorb the chemical. Then the liquid must be dried out for packaging and shipment, and when the electrode is implanted, it absorbs fluid and reforms the gel which then releases the drug over time.

SUMMARY OF THE INVENTION

[0007] Embodiments of the present invention are directed to a cochlear implant electrode that includes an implantable electrode carrier having an outer surface with electrode contacts for electrically stimulating nerve tissue of the inner ear of a patient. A drug lumen is within the electrode carrier and adapted to receive a therapeutic fluid. The drug lumen contains delivery openings to the outer surface of the electrode carrier and a hydrogel matrix disposed between the drug lumen and the one or more delivery openings and adapted to swell in volume when exposed to the therapeutic fluid. The hydrogel matrix is adapted to control diffusion of the therapeutic fluid from the drug lumen through the delivery openings to the outer surface of the electrode carrier.

[0008] The drug lumen may be adapted to contain a treatment period amount of therapeutic fluid for an extended treatment period. The hydrogel matrix may be based on a three-dimensional network of cross-linked hydrophilic polymer chains, for example, made of hyaluronic acid. The hydrogel matrix may have a mesh size small enough to resist entry of bacteria. The hydrogel matrix may fill some or all of the volume of the lumen. The hydrogel matrix may have an adjustable pore size which controls diffusion rate of the therapeutic fluid.

[0009] The therapeutic fluid may include dexamethasone, for example, the electrode array may be adapted to release between 5 μg and 600 μg of dexamethasone during an initial 24 hour period of use. There may be a refilling arrangement for refilling the drug

lumen in an implanted electrode with additional therapeutic fluid.

BRIEF DESCRIPTION OF THE DRAWINGS

[0010] Figure 1 shows an embodiment of an implantable drug delivery system.

[0011] Figure 2 shows another embodiment of an implantable drug delivery system using a charge drive arrangement.

[0012] Figure 3 shows principles of a magnetic drive arrangement as used by another embodiment of the present invention.

[0013] Figure 4 shows an embodiment having a volume of therapeutic fluid in a delivery catheter.

[0014] Figure 5 shows an embodiment having a semi-permeable filter in the form of a drug delivery rod.

[0015] Figure 6 shows an embodiment in which an implantable delivery catheter is connected to the body of an implant housing.

[0016] Figure 7 shows another embodiment having a primary reservoir and a secondary reservoir connected by a diffusion channel.

[0017] Figure 8 shows an embodiment having one or more internal control surfaces to form a control labyrinth that promotes controlled flow of fluid.

[0018] Figure 9 shows an embodiment having a pressure control element between the primary reservoir and the secondary reservoir for preventing pressure transients.

[0019] Figure 10 shows a device having a delivery syringe and a receiver syringe in accordance with an embodiment of the present invention.

[0020] Figure 11 A-B shows an embodiment of an electrode having an inner drug lumen with a hydrogel matrix that fills some or all of the lumen.

[0021] Figure 12 shows a hydrophilic polymer network used for a hydrogel matrix according to one embodiment.

[0022] Figure 13 A-B shows drug diffusion characteristics of drug lumens with and without a hydrogel matrix.

[0023] Figure 14 shows drug release profile curves for drug lumens with and without a hydrogel matrix.

[0024] Figure 15 shows an arrangement for loading therapeutic fluid into a drug lumen.

[0025] Figure 16 A-C shows how an embodiment of a drug lumen and hydrogel matrix is filled with a therapeutic fluid.

DETAILED DESCRIPTION OF SPECIFIC EMBODIMENTS

[0026] Various embodiments of the present invention are directed to implantable drug delivery apparatuses and methods. Embodiments include a fillable and refillable implantable drug delivery system which does not increase its internal pressure while refilling. And electrical and/or magnetic pulses can be used to displace molecules within the therapeutic fluid within the apparatus. Such embodiments and techniques are useful for delivering a solution of a therapeutic fluid into target tissue such as a body cavity like the cochlea. Embodiments also include one or more subcutaneous drug delivery reservoirs that are transcutaneously refillable without increasing pressure. Embodiments also maintain homogeneity of a therapeutic fluid within a drug delivery reservoir as the drug diffuses to the outside of the reservoir. Embodiments of the invention also include an implantable electrode carrier having a drug lumen that contains a hydrogel matrix which allows diffusion over time of a therapeutic fluid from the lumen into tissue adjacent to the electrode carrier.

[0027] Figure 1 shows an embodiment of an implantable drug delivery system **100** that includes a subcutaneous primary reservoir **101** that holds a primary volume of a therapeutic fluid. The primary reservoir **101** includes an input port septum **104** for receiving the therapeutic fluid and a corresponding an output port septum **105** for removing fluid. A diffusion channel **103** provides a fluid communication path from the primary reservoir **101** to a secondary reservoir **102** that holds a secondary volume of the therapeutic fluid. The secondary reservoir **102** includes a drug permeable surface **107** such as a drug permeable membrane, slits or holes for diffusion of the therapeutic fluid into nearby tissue, and a priming septum **106** for fluid exchange within the secondary reservoir **102**. It may be useful in such an arrangement to mix the therapeutic fluid with an osmotic agent such as a saline solution for promoting and accelerating diffusion of the therapeutic fluid out of the secondary reservoir **102**. The embodiment shown in Fig. 1 also includes a channel coil **108** that surrounds the diffusion channel **103** for inducing ionic displacement of fluid within the diffusion channel from one reservoir to the other.

[0028] The system may be filled with therapeutic fluid before implantation by inserting a needle of a delivery syringe containing the therapeutic fluid into the input port septum **104**. A needle of a receiver syringe is inserted into the priming septum **106** and the therapeutic fluid is injected from the delivery syringe into the primary reservoir **101** while the receiver syringe withdraws fluid from the secondary reservoir **102**, thereby priming the reservoirs with the therapeutic fluid. After priming the system, the needles are removed from the septums and the drug delivery system is ready to be subcutaneously implanted in a selected position in a patient, for example, adjacent to the skull of the patient for use with a cochlear implant system.

[0029] The implantable drug delivery system **100** allows refilling of the reservoirs **101** and **102**, either with the same therapeutic fluid or with a new therapeutic fluid with a different molecular content. The refilling process does not raise pressure either within the internal volume of the drug delivery system **100** or in the surrounding tissue and fluid region outside the secondary reservoir **102**. No special bacterial filter is needed because molecular diffusion preferentially occurs through the ion permeable membrane drug delivery surface **107**, or through punctures in the drug delivery surface **107** that are smaller

than bacteria size.

[0030] Figure 2 shows another similar embodiment of an implantable drug delivery system **200** which has just a single primary septum **201** on top of the primary reservoir **101**. And instead of a channel coil arrangement, this embodiment uses a charge driver arrangement to for displacing the therapeutic fluid within the apparatus by driving electrically charged molecular substances within the therapeutic fluid. Specifically, a pulse generator **204** (e.g., from an implantable stimulator) generates a drive signal to an active electrode **202** in the primary reservoir **101**. A ground electrode **203** in the secondary reservoir **102** completes the current path. A drive signal based on charge balanced asymmetric pulses such as the example shown in the bottom of Fig. 2 then can drive electrically charged molecular substances within the therapeutic fluid, for example, to displace the therapeutic fluid from the primary reservoir **101** to the secondary reservoir **102** over time to replenish the secondary reservoir.

[0031] Instead of placing the ground electrode **203** inside the secondary reservoir **102**, in some embodiments it may be external to the secondary reservoir **102**. Such an arrangement allows a drive signal based on charge balanced asymmetric pulses to displace the therapeutic fluid from the primary reservoir **101**, through the secondary reservoir **102**, and by active diffusion through the drug permeable surface **107** into the nearby tissue, e.g., into the surrounding cochlear fluid or extra-cellular fluid. Such a charge driver arrangement may be especially effective if there are small ionic channels between the polymer matrix of the drug permeable surface **107** and the surrounding tissue. These can be created by punctures made with a small needle, laser ablation of holes, use of an ion permeable membrane, and/or one or more slits from scalpel, any of which may provide an improved passage for the flow of complex charged molecules in the therapeutic fluid to flow from inside the secondary reservoir **102** out into the surrounding fluids and tissues.

[0032] Using a balanced charge drive signal may help avoid undesirable corrosion of the electrodes **202** and **203**. The pulse generator **204** advantageously may be located within the housing of a cochlear implant stimulator, which typically are designed to deliver charge balanced symmetric or asymmetric pulses. Alternatively the drive signal may be

based on use of tri-phasic pulses to provoke a net charge displacement in one direction of the electrodes. The associated insulated wiring for such embodiments both to and from the pulse generator **204** and between the electrodes **202** and **203** may run within the interior volume of the reservoirs, or within or along the walls and surfaces of the apparatus structures.

[0033] Rather than a charge drive arrangement as depicted in Fig. 2, some embodiments may use a magnetic drive arrangement based on the principles shown in Figure 3 for displacing the therapeutic fluid within the apparatus by driving magnetic molecular substances within the therapeutic fluid. Instead of electrodes **203** and **204**, a magnetic driver arrangement uses a repeller magnet **301** and an attractor magnet **302** that set up a magnetic field between them that displaces the therapeutic fluid within the apparatus by driving magnetic molecular substances **303** within the therapeutic fluid. In the example shown in Fig. 3, this drives the magnetic molecules away from the repeller magnet **301** to create a region of lower molecular concentration **305** in the vicinity, while a higher molecular concentration **304** region develops near to the attractor magnet **302** located, for example, outside the secondary reservoir to exert a magnetic attractive force on magnetic molecular substances within the therapeutic fluid and pull them through the drug permeable surface into the nearby tissue. Alternatively, the attractor magnet **302** may be located within the secondary reservoir to displace the therapeutic fluid from the primary reservoir to the secondary reservoir over time to replenish the secondary reservoir. The magnets **301** and/or **302** may usefully be covered by a protective encapsulation layer.

[0034] Figure 4 shows another embodiment of an implantable drug delivery apparatus in which the arrangement of the primary reservoir **101** and its input septum **104** and output septum **105** are as in Fig. 1, but the secondary reservoir **401** is elongated to form a delivery catheter that encloses the secondary volume. Thus, the proximal end of delivery catheter secondary reservoir **401** is in fluid communication with the input septum **104** while the distal end includes an output septum **403** for removing fluid from the secondary reservoir **401** when filling or refilling the system. A drug permeable surface **402** such as an ion permeable diffusion membrane diffuses the therapeutic fluid into the surrounding tissues and fluids.

[0035] In some embodiments, the interior of the secondary reservoir **401** may include a semi-permeable filter such as the drug delivery rod **502** shown in Figure 5 for mechanically filtering fluid flow through the catheter. In the example shown, the drug delivery rod **502** may be in the specific form of a drug eluting gel or drug eluting polymer such as a drug eluting silicone rod. Such a drug delivery rod **502** is then embedded or incorporated into the main superstructure of the secondary reservoir **401**, which may be, for example, a silicone matrix **501**. The silicone matrix **501** may include a slit opening **503** that allows hydration of the drug eluting material by the surrounding fluid. In some embodiments, the elongated form of the secondary reservoir **401** may be pre-shaped to have a bend in it to accommodate placement around internal body structures. Or the secondary reservoir **401** may be flexible to be bendable around such internal body structures.

[0036] Figure 6 shows another embodiment in which an implantable delivery catheter **401** is connected to the body of an implant housing **603**, such as a cochlear implant stimulator housing. In such an embodiment, the delivery catheter **401** may be an internal volume within a stimulator electrode array which is implanted, for example, in the cochlea of a hearing impaired patient. The electrode array in such an embodiment includes a drug permeable surface as described above (e.g., an ion or molecule permeable membrane and/or an arrangement of multiple diffusion slits or holes) through which the therapeutic fluid diffuses into the surrounding tissue or fluid. In the embodiment shown, the therapeutic fluid is delivered to the delivery catheter **401** via an arrangement of an input septum **601** over an input port **602**, through an input channel **604** and the implant housing **603**. In another embodiment, there may be simply an input septum **601** without a discernable defined input port **602** as such. In either configuration, priming septum **106** may be used before implantation to withdraw existing fluid within the delivery catheter **401** to initially fill the system. After implantation, additional therapeutic fluid can be periodically added transcutaneously through the input septum **601**, which located is just under the skin of the patient.

[0037] Figure 7 shows another embodiment having a primary reservoir **701** and a

secondary reservoir **702** connected by a diffusion channel **703**. The secondary reservoir **702** includes a priming septum **710** and a drug delivery surface **711** as described above with regards to other embodiments. In addition, an input channel **708** provides fluid communication between the primary reservoir **701** and an input port **706** having an input septum **704**. Similarly, an output channel **709** also provides fluid communication between the primary reservoir **701** and an output port **707** having an output septum **705**.

[0038] Initial filling of the system may occur before implantation using the input septum **704** and priming septum **710**. After implantation, the system can be filled/replenished using a delivery syringe containing the therapeutic fluid to refill the primary reservoir **701** transcutaneously through the skin of a patient into the input septum **704**, while a receiver syringe under negative pressure (i.e., withdrawing the plunger) permits air or old fluid to be withdrawn transcutaneously through the output septum **705** and the skin into the receiver syringe, thereby refilling/replenishing the primary reservoir **701**. After the therapeutic fluid has been introduced into the primary reservoir **701**, both the delivery syringe needle and the receiver needle are removed.

[0039] Embodiments may also include an internal flow control arrangement for correctly and reliably directing fluid flow within the primary reservoir, for example to maintain a desired concentration of therapeutic fluid within the fluid in the reservoir. For example, Figure 8 shows a primary reservoir **800** having one or more internal control surfaces **801** to form a control labyrinth that promotes controlled flow of fluid within the primary reservoir **800**. Fig. 8 A shows use of a single control surface **801**, in other embodiments, there may be multiple such control surfaces arranged to form a more complicated control labyrinth. For example, a capillary tube arrangement such as the one shown at the bottom of Fig. 9 may be used as a control labyrinth within the primary reservoir **800**.

[0040] Embodiments may also include a pressure control element between the primary reservoir and the secondary reservoir for preventing pressure transients between the primary reservoir and the secondary reservoir. Limiting pressure transients between the primary reservoir and the secondary reservoir during fluid filling operations also serves to prevent pressure transients in the surrounding tissue and fluid region outside the secondary

reservoir. For example, such a pressure control element may be in the specific form of a check valve arrangement at the opening to the diffusion channel such as single flap check valve **901** or double flap check valve **902**. If pressure increases in the primary reservoir during fluid filling, the check valve **901** or **902** closes to prevent a pressure transient in the secondary reservoir. Alternatively, a capillary tube arrangement **903** at the beginning of the diffusion channel may serve the same purpose by allowing diffusion but providing significant resistance to any pressure driven fluid flow.

[0041] To maintain constant pressure in the reservoirs, the fluid flow into and out of the system needs to be coordinated in volume and flow rate. This can be achieved with a device or arrangement which takes in and out of the reservoir, the same amount of fluid, at the same time and the same flow rate. Figure 10 shows one example of such a fluid replacement device **1000** which contains in a single housing both a delivery syringe **1001** having a delivery piston **1003** and a receiver syringe **1002** having a receiver piston **1004**. Connected to each piston is a piston coupling rod **1005** which rotates about a coupling axis **1006** so that when the delivery piston is pushed into the delivery syringe **1001**, the coupling rod **1005** rotates to push out the receiver piston **1004** the same amount.

[0042] Embodiments of the present invention also are directed to a cochlear implant electrode as shown in Figure 11 A-B that includes an implantable electrode carrier **1100** having an outer surface with electrode contacts **1101** for electrically stimulating nerve tissue of the inner ear of a patient. A drug lumen **1102** is within the electrode carrier **1100** and adapted to receive a therapeutic fluid, for example, a treatment period amount of a therapeutic fluid such as dexamethasone. So the drug lumen **1102** may contain a treatment volume of dexamethasone to release between 5 μg and 600 μg of dexamethasone during an initial 24 hour period of use.

[0043] The drug lumen **1102** also contains one or more delivery openings **1104** to the outer surface of the electrode carrier **1100**. A hydrogel matrix **1103** is disposed between the drug lumen **1102** and the one or more delivery openings **1104** and adapted to swell in volume when exposed to the therapeutic fluid. The hydrogel matrix **1103** is adapted to control the diffusion of the therapeutic fluid from the drug lumen **1102** through the one or

more delivery openings **1104** to the outer surface of the electrode carrier **1100**. In the embodiment shown in Fig. 11A, the hydrogel matrix **1103** fills a portion of the drug lumen **1102** nearest the opening. Fig. 11B shows a similar embodiment where the hydrogel matrix **1103** fills the entire volume of the drug lumen **1102**.

[0044] The hydrogel matrix **1103** may be based on hyaluronic acid in a three-dimensional network. Figure 12 shows a hydrophilic polymer network **1200** that forms multiple cross-linked hydrophilic polymer chains which include closed loops **1201** and dangling ends **1202**. The polymer network **1200** also includes cross-linking points **1203** and polar groups **1204** that make the polymer hydrophilic. The hydrogel matrix **1103** acts as a host to the therapeutic fluid inside the drug lumen **1102**. The hydrogel matrix **1103** allows the drug lumen **1102** to store the molecules of the therapeutic fluid both in a dry status (for example on the shelf) and in a wet status (for example when implanted). When the polymer network **1200** is immersed in water **1205** it increases in volume, and the therapeutic fluid can diffuse out from the drug lumen **1102** through the polymer network **1200** at a diffusion rate that is controlled by the pore size of the hydrogel matrix **1103** which preferably also is small enough to resist entry of bacteria.

[0045] In specific embodiments, the hydrogel matrix **1103** may be non-degradable, partially biodegradable, or fully biodegradable. It would be possible to arrange the hydrogel matrix **1103** in the drug lumen **1102** so that some sections of the lumen are filled with biodegradable hydrogel, while other sections have non-degradable hydrogel. The hydrogel matrix **1103** is vacuum- and temperature-resistant such that it is suitable for sterilization.

[0046] In an embodiment where the drug lumen **1102** is partially filled with a hydrogel matrix **1103** (e.g., Fig. 11B), the hydrogel matrix **1103** can act as a diffusion gate for the therapeutic fluid. A diffusion gate could also be one or more small delivery openings (for example punctures or slits) in the side wall of the drug lumen **1102**. When the concentration of the therapeutic fluid is greater within the drug lumen **1102** than outside the electrode carrier **1100** so as to form a concentration gradient, then the therapeutic fluid will diffuse out of the drug lumen **1102** over time into target tissue adjacent to the

electrode carrier **1100**.

[0047] It is useful to compare the characteristics of an implantable electrode carrier **1100** containing a drug lumen **1102** both with and without a hydrogel matrix **1103**. Figure 13A shows the drug diffusion characteristics for a drug lumen **1102** without a hydrogel matrix **1103** at the one or more delivery openings **1104**, where a flat concentration gradient develops while the therapeutic fluid diffuses out of the drug lumen **1102**. Curve A in Figure 14 shows the resulting non-linear drug release profile over time with large release rates in the beginning and lower release rates towards the end of the release time. Figure 13B shows the drug diffusion characteristics for a drug lumen **1102** with a hydrogel matrix **1103** at the one or more delivery openings **1104** where the drug diffusion coefficient in the section without the hydrogel matrix **1103** is much higher than the drug diffusion coefficient in the section with the hydrogel matrix **1103**. Thus, the diffusion rate through the hydrogel matrix **1103** is the time dependent factor rather than diffusion rate within the section of the drug lumen **1102** without the hydrogel matrix **1103**. This allows enough time for the drug concentration within the drug lumen **1102** to even out, resulting in a steep concentration gradient in the section with the hydrogel matrix **1103** as seen in Fig. 13B. While the drug lumen **1102** releases the therapeutic fluid, the drug concentration gradient changes less in the section with the hydrogel matrix **1103** which leads to a more linear drug release profile as shown in Curve B of Fig. 14.

[0048] After mixing the hydrogel material from its constituent compounds, the hydrogel stays in liquid form for a period. The liquid hydrogel material can be easily positioned either partially or fully into the drug lumen **1102**, for example, by injection. Polymerization of the hydrogel material then occurs within the drug lumen **1102** ending with the hydrogel matrix **1103** being solid and fixed within the drug lumen **1102**. To mechanically fix the hydrogel matrix **1103** within the drug lumen **1102**, the front end of the drug lumen **1102** can be closed and one or more delivery openings **1604** provided at the side of the lumen as shown in Figure 16. This type of design prevents the hydrogel matrix **1103** from popping out of the drug lumen **1102** when fluid pressure is applied.

[0049] The hydrogel matrix **1103** also acts as a flow resistor and pressure resistance. In a

refillable reservoir arrangement such as the one shown in Figure 4, a primary reservoir is flushed using two fluid septums **104** and **105**. Such a refilling procedure could cause pressure differentials that could be transferred to fragile pressure sensitive regions such as the inner ear. A hydrogel matrix **402** can be used to avoid such behavior. The hydrogel matrix **402** minimizes the flow of liquid out of the tip of the reservoir so that the therapeutic fluid is only released by diffusion through the hydrogel matrix **402** and is not actively driven by the refilling pressure.

[0050] If an electrode has a drug lumen **1102** which uses a permeable membrane with its one or more delivery openings **1104**, then it is not possible to fill the lumen because the air it contains cannot be released. But if there is a permanent outlet to release this air, then body fluids and/or bacteria may enter the drug lumen **1102**. Figure 15 shows an arrangement for loading therapeutic fluid **1506** into a drug lumen **1502** containing a hydrogel matrix **1503** and a pin hole **1505** near the delivery opening **1504** that allows air to be released from the drug lumen **1502** while filling it with the therapeutic fluid **1506** from a drug syringe **1507**. After filling, the pin hole **1505** does not release any liquid from the drug lumen **1502**. In some embodiments, the therapeutic fluid **1506** can be loaded into a drug lumen **1502** while the hydrogel material is dry. The therapeutic fluid **1506** can be injected through a septum or similar structure at the back end of the drug lumen **1502** while air is released through the pores of the dry hydrogel. Once the liquid of the therapeutic fluid **1506** begins to flow through the dry hydrogel material, it swells up into a hydrogel matrix **1503** and seals the one or more delivery openings **1504** at the front end of the drug lumen **1502**. In some embodiments, the delivery openings **1504** may include a permeable membrane to further benefit this arrangement.

[0051] Figure 16A shows an electrode carrier **1600** having an empty drug lumen **1602** which does not initially contain any therapeutic fluid, but which does contain the dry hydrogel material. This is a convenient shelf-stable form in which to transport and store the electrode carrier **1600** prior to implantation by a surgeon in a patient. The therapeutic fluid may be added at any convenient time after manufacturing, e.g., directly prior to implantation. Then during surgery the surgeon can decide what kind of medication he requires and then inject the therapeutic fluid with a syringe into the empty drug lumen

1602 as shown in Fig. 16B. During the drug injection, the air can be released from the drug lumen **1602** through the dry hydrogel material. The initial volume of the dry hydrogel material is just a fraction (e.g. up to 20%) of its final volume when wet into the swollen hydrogel matrix **1603**. As the injected therapeutic fluid contacts the dry hydrogel material, the hydrogel matrix **1602** starts swelling within a very short time (seconds to minutes) and closes the delivery openings **1604** at the tip of the electrode **1600**. As shown in Fig. 16C, the therapeutic fluid is now slowly released by the swollen hydrogel matrix **1603**.

[0052] Although various exemplary embodiments of the invention have been disclosed, it should be apparent to those skilled in the art that various changes and modifications can be made which will achieve some of the advantages of the invention without departing from the true scope of the invention.

CLAIMS

What is claimed is:

1. A cochlear implant electrode comprising:
an implantable electrode carrier having an outer surface including a plurality of electrode contacts for electrically stimulating nerve tissue of the inner ear of a patient; and
a drug lumen within the electrode carrier adapted to receive a therapeutic fluid and containing:
 - i. one or more delivery openings to the outer surface of the electrode carrier, and
 - ii. a hydrogel matrix disposed between the drug lumen and the one or more delivery openings and adapted to swell in volume when exposed to the therapeutic fluid;wherein the hydrogel matrix is adapted to control diffusion of the therapeutic fluid from the drug lumen through the one or more delivery openings to the outer surface of the electrode carrier.
2. An electrode according to claim 1, wherein the drug lumen is adapted to contain a treatment period amount of therapeutic fluid for an extended treatment period.
3. An electrode according to claim 1, wherein the hydrogel matrix has an adjustable pore size which controls diffusion rate of the therapeutic fluid.
4. An electrode according to claim 1, wherein the hydrogel matrix is based on hyaluronic acid.
5. An electrode according to claim 1, wherein the hydrogel matrix is based on a three-dimensional network of cross-linked hydrophilic polymer chains.
6. An electrode according to claim 1, wherein the hydrogel matrix has a mesh size small enough to resist entry of bacteria.

7. An electrode according to claim 1, wherein the therapeutic fluid includes dexamethasone.
8. An electrode array according to claim 1, wherein the electrode is adapted to release between 5 μg and 600 μg of dexamethasone during an initial 24 hour period of use.
9. An electrode according to claim 1, further comprising:
a refilling arrangement for refilling the drug lumen in an implanted electrode with additional therapeutic fluid.

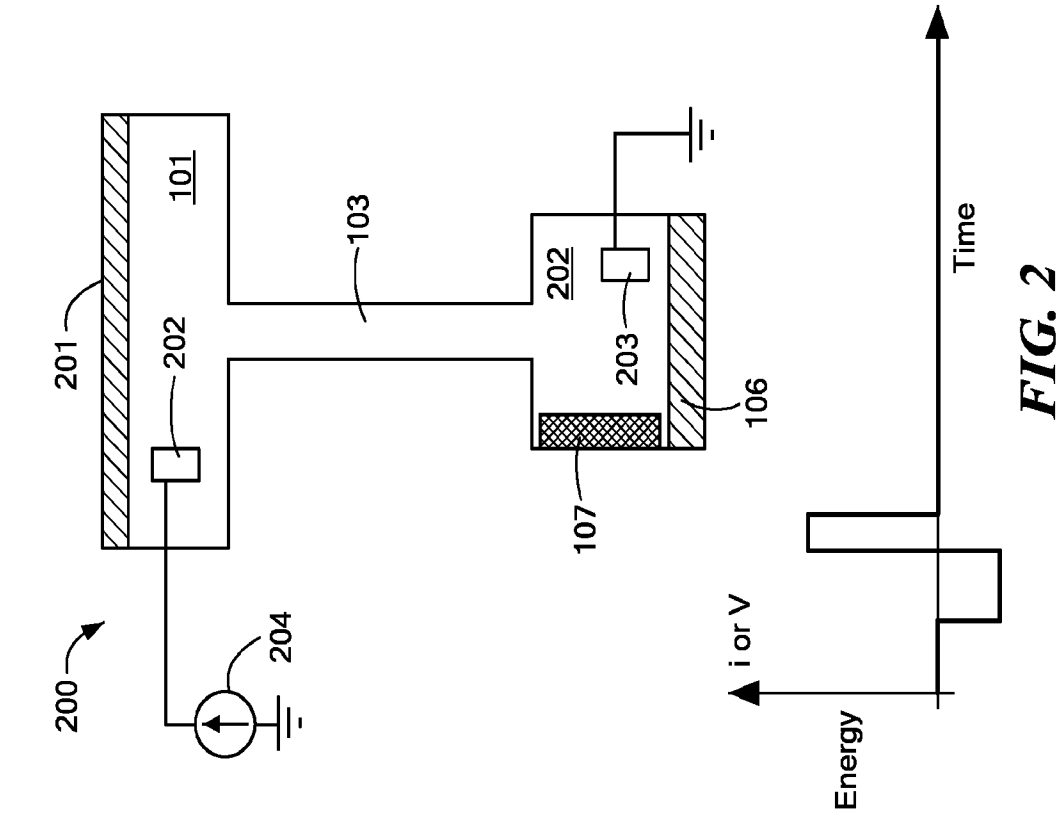


FIG. 1

FIG. 2

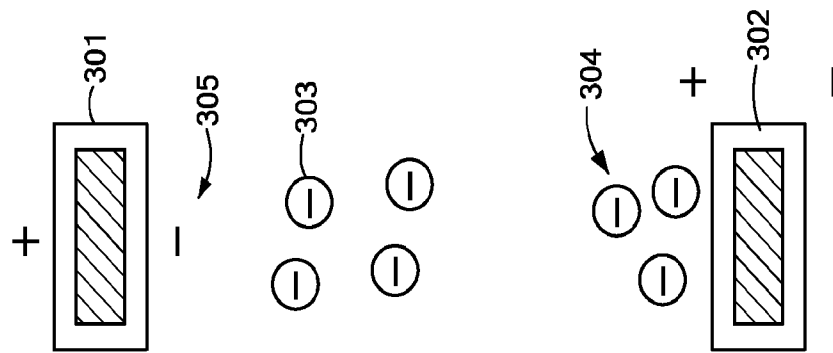


FIG. 3

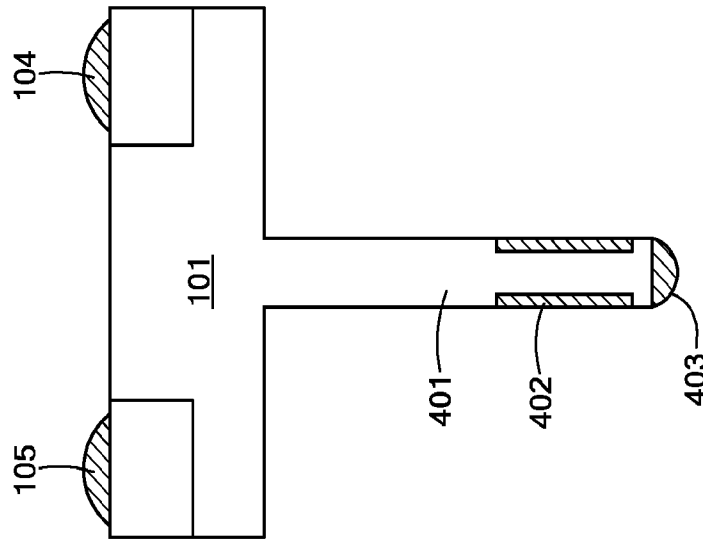


FIG. 4

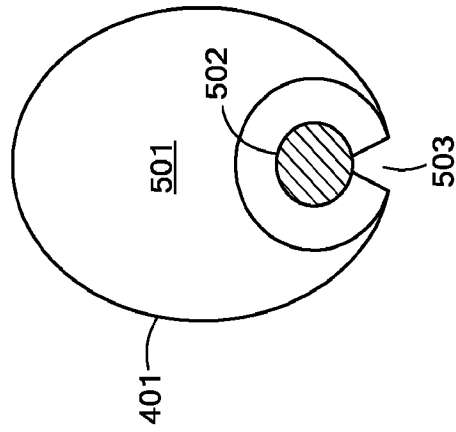


FIG. 5

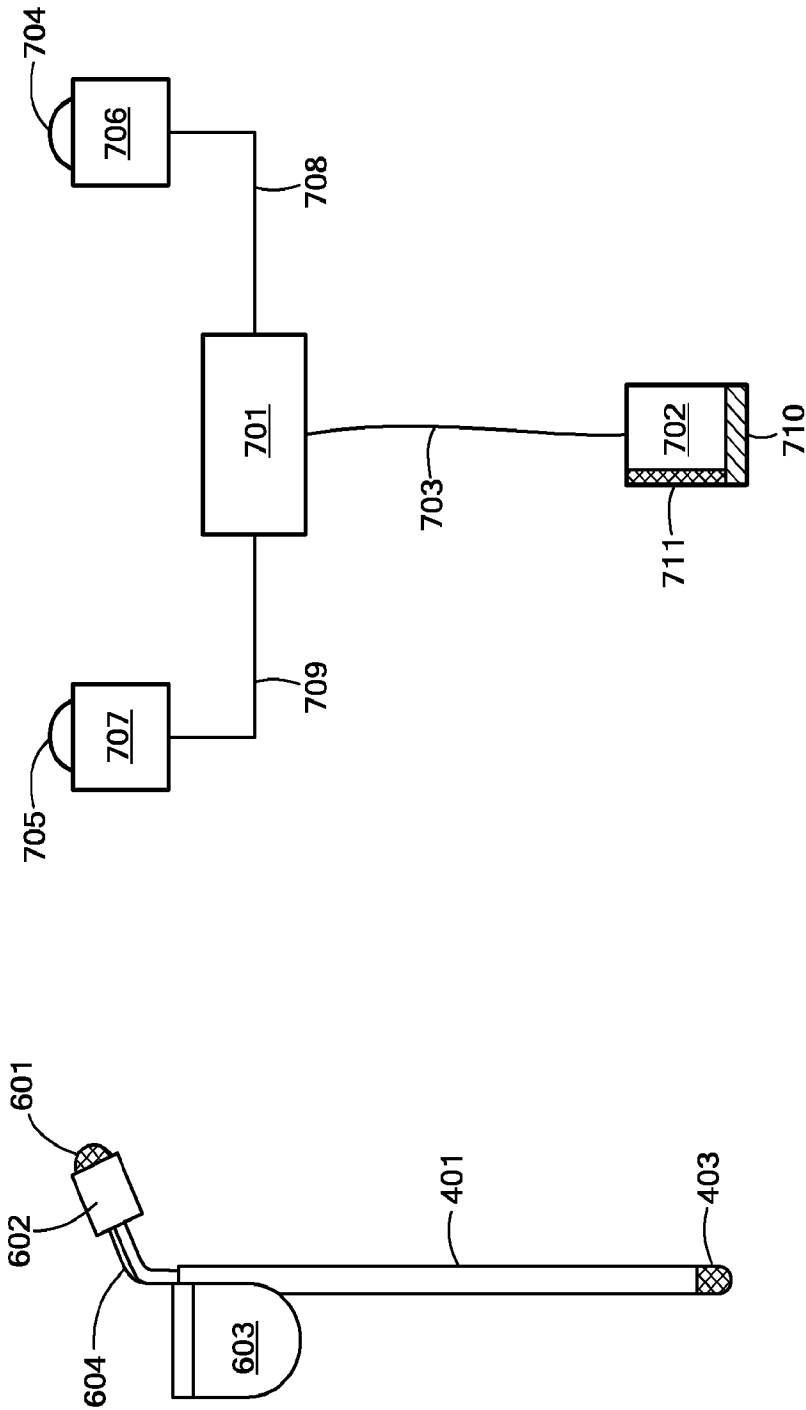


FIG. 6

FIG. 7

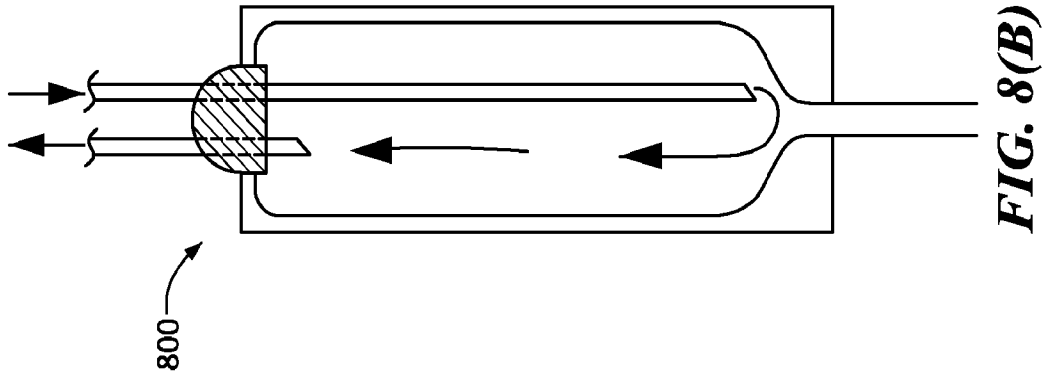


FIG. 8(B)

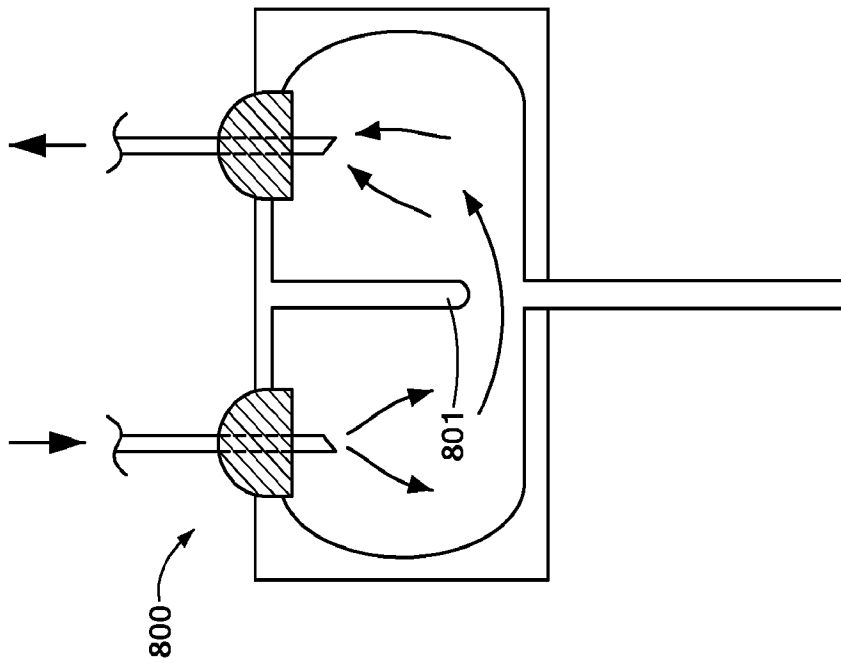


FIG. 8(A)

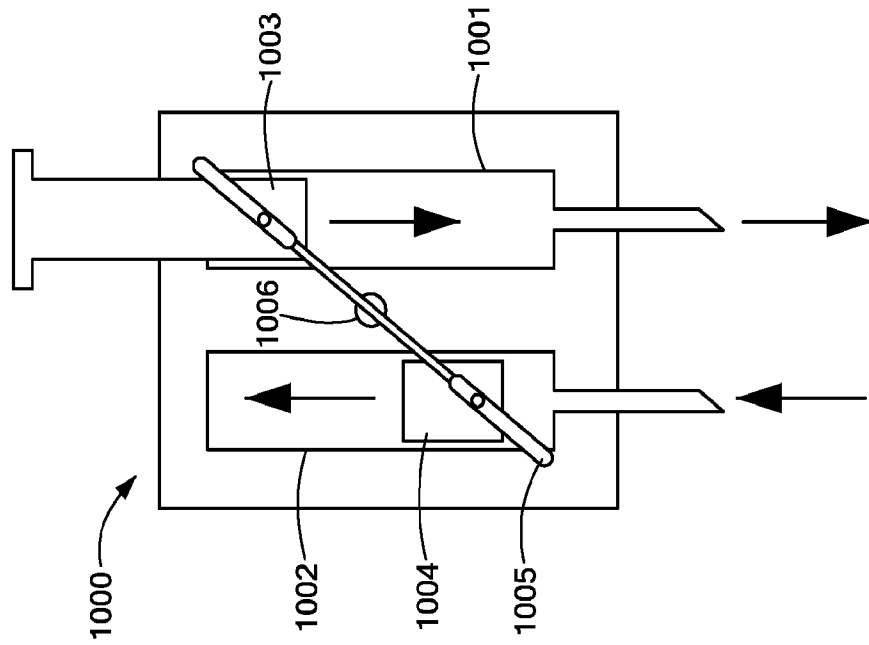


FIG. 10

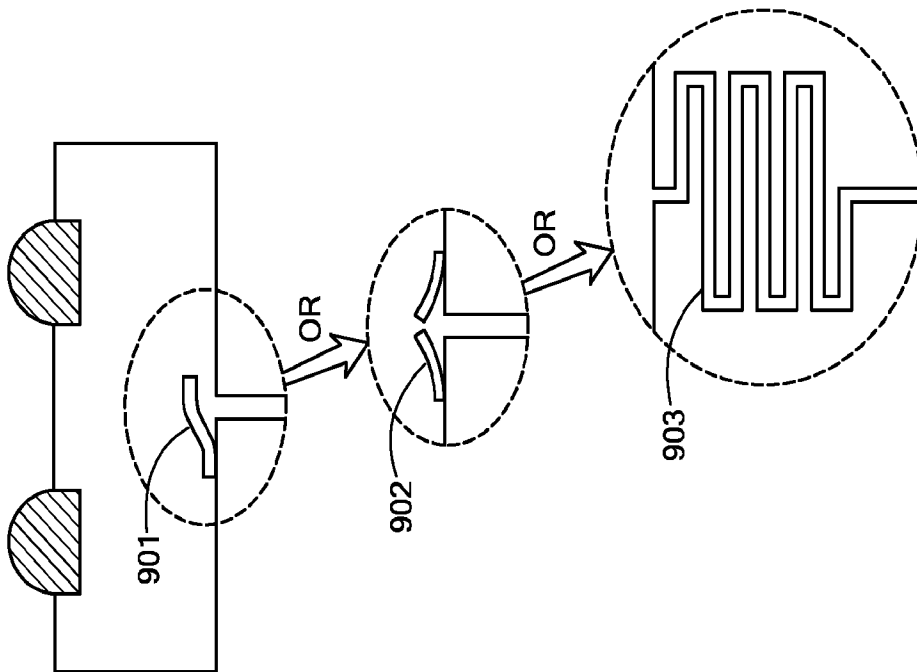


FIG. 9

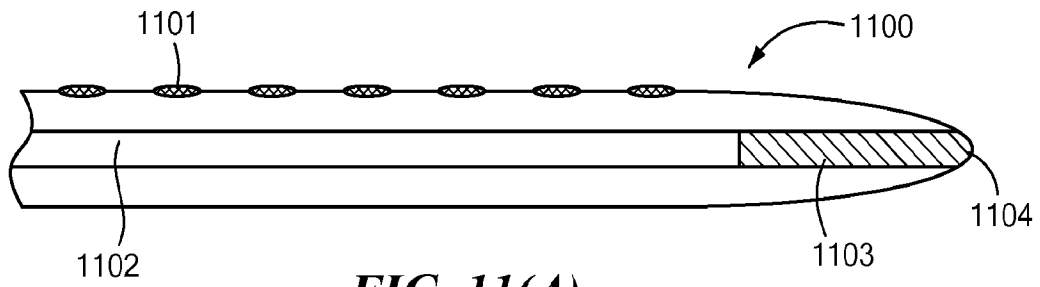


FIG. 11(A)

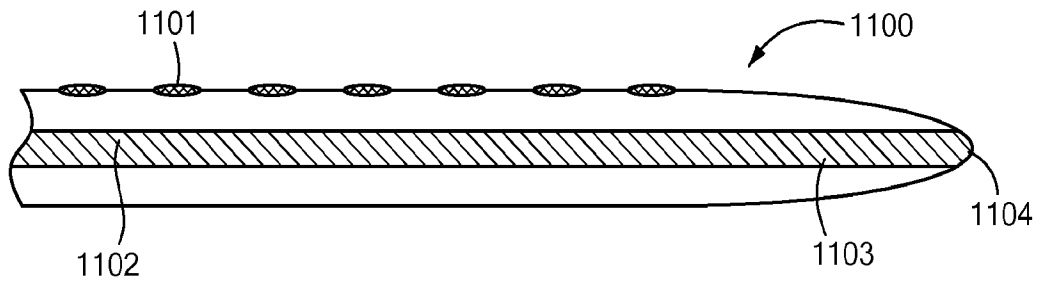


FIG. 11(B)

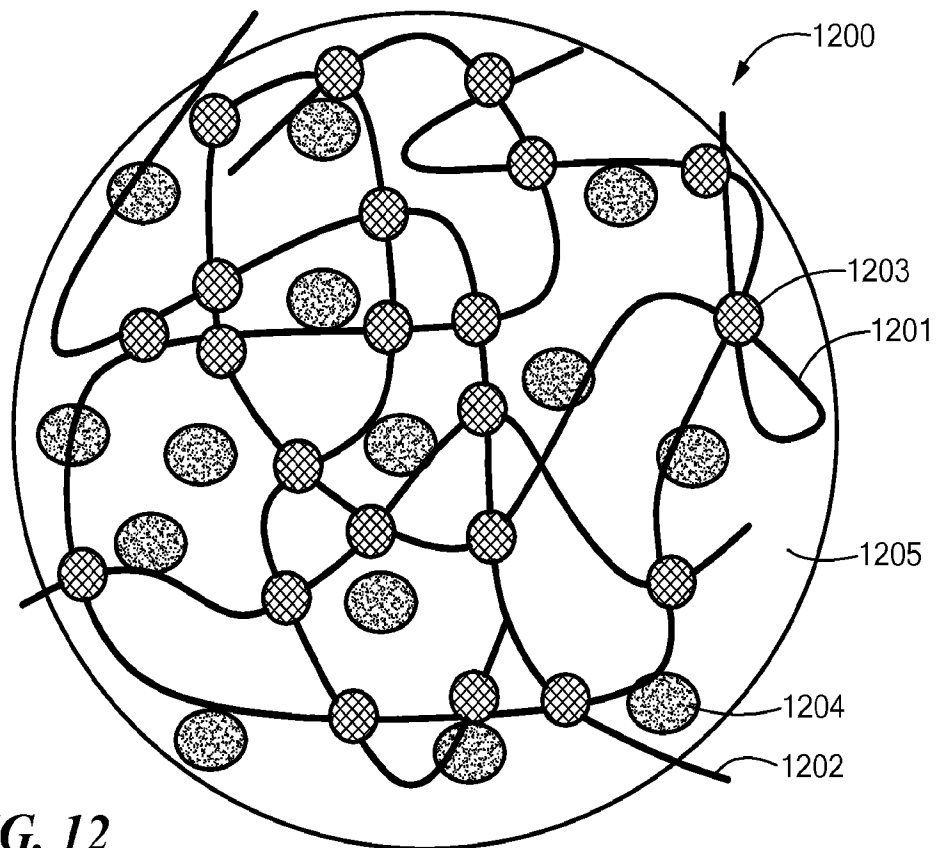


FIG. 12

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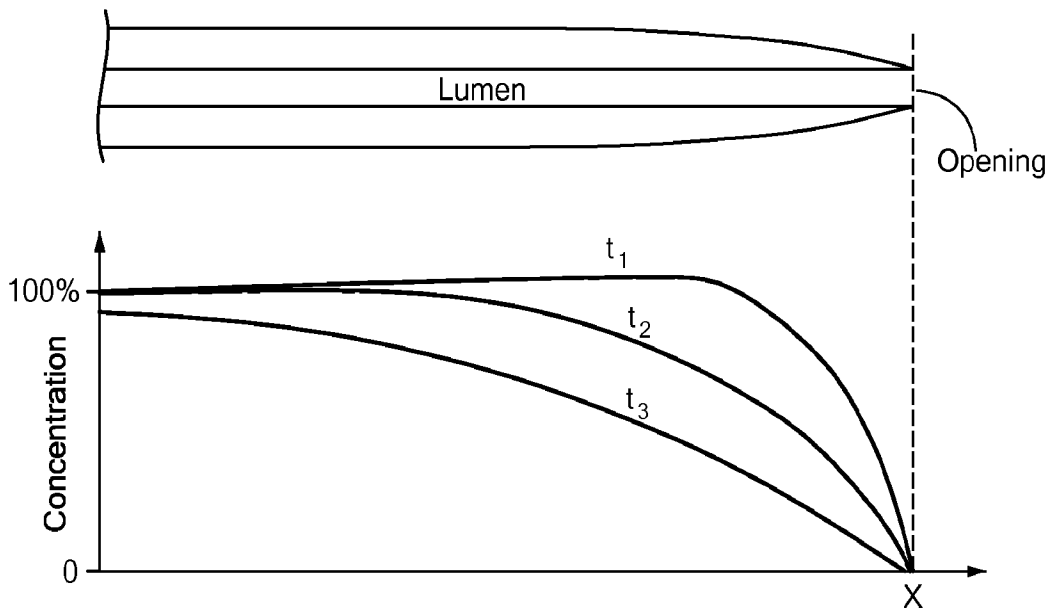


FIG. 13(A)

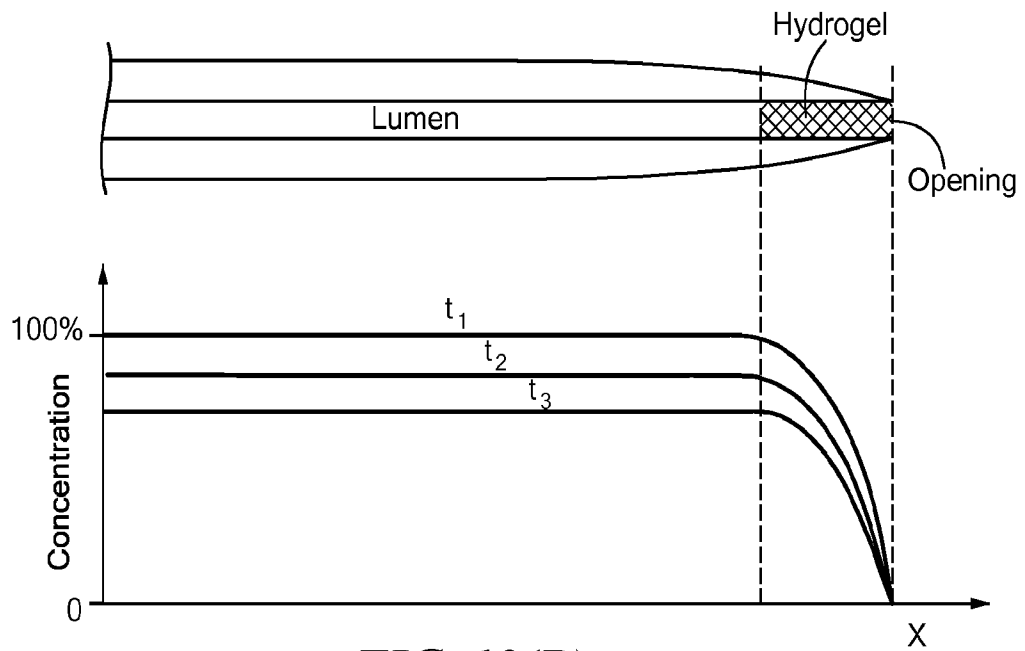


FIG. 13(B)

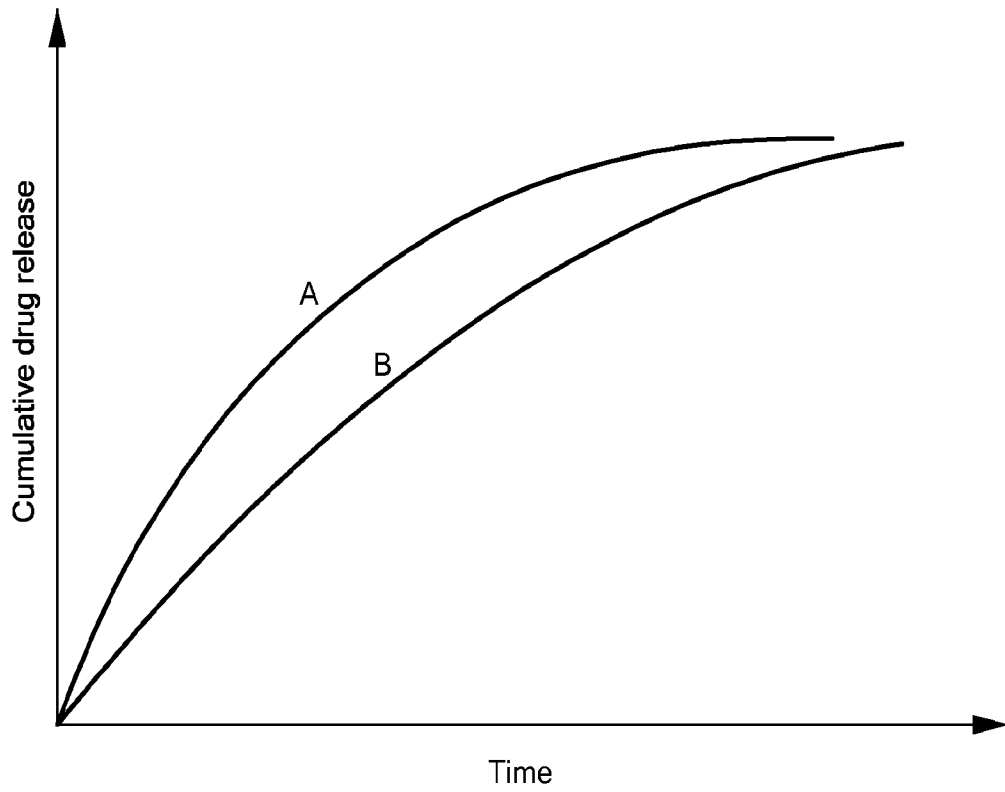


FIG. 14

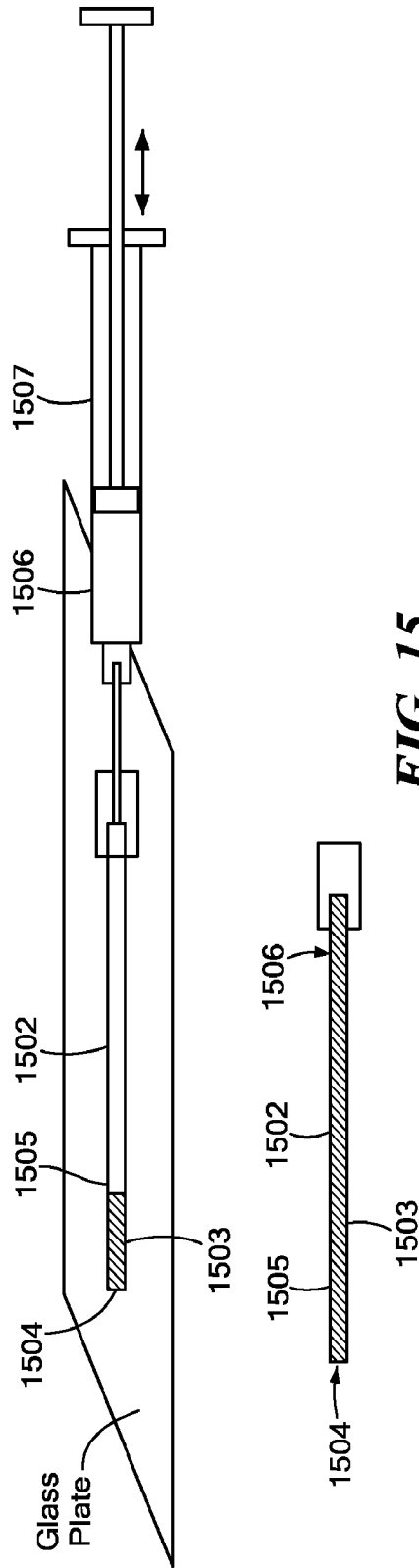


FIG. 15

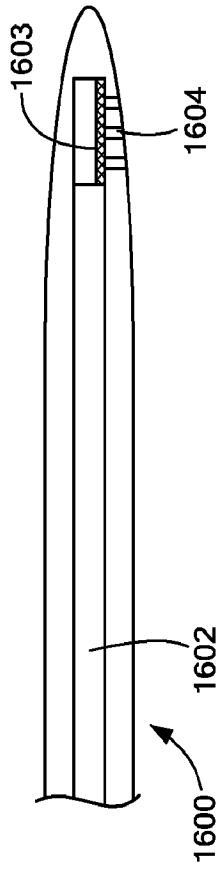


FIG. 16(A)

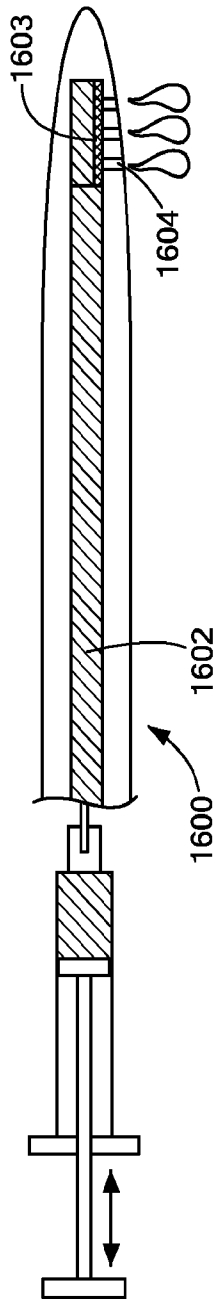


FIG. 16(B)

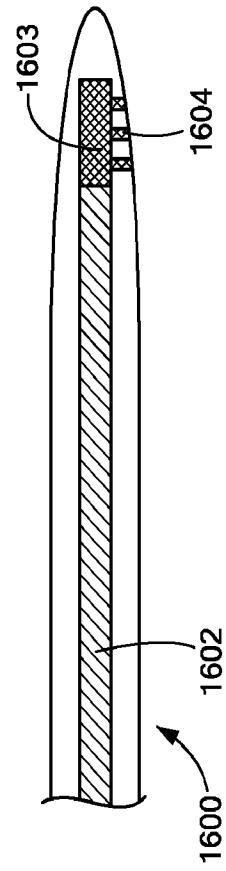


FIG. 16(C)

INTERNATIONAL SEARCH REPORT

International application No
PCT/US2009/063721

A. CLASSIFICATION OF SUBJECT MATTER
INV. A61N1/05

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
A61N

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)
EPO-Internal, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US 2007/088335 A1 (JOLLY CLAUDE [AT]) 19 April 2007 (2007-04-19) paragraphs [0123], [0132] - [0137]; figures 39-41	1-9
Y	US 2006/009806 A1 (HERUTH KENNETH T [US] ET AL) 12 January 2006 (2006-01-12) paragraphs [0046], [0051] - [0053], [0067], [0070], [0073]	1-9
P, X	EP 2 047 884 A (COCHLEAR LTD [AU]) 15 April 2009 (2009-04-15) the whole document	1-9
A	US 2007/255237 A1 (LOBL THOMAS J [US] ET AL) 1 November 2007 (2007-11-01) the whole document	1-9

Further documents are listed in the continuation of Box C.

See patent family annex.

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Date of the actual completion of the international search

11 December 2009

Date of mailing of the international search report

29/12/2009

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Monogyiou, Efstratia

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/US2009/063721

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