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KATRIEN DE VOS ET AL: "Label-free biosensors on silicon-on-insulator optical chips based on microring cavities and surface plasmon interferometry", TRANSPARENT OPTICAL NETWORKS, 2008. ICTON 2008. 10TH ANNIVERSARY INTERNATIONAL CONFERENCE ON, IEEE, PISCATAWAY, NJ, USA, 22 June 2008 (2008-06-22), pages 88-91, XP031306272, ISBN: 978-1-4244-2625-6

DESCRIPTION

Field of the invention

[0001] The invention relates to the field of implantable sensors. More particularly, the present invention relates to implantable sensors for sensing substances and to corresponding continuous monitoring systems.

Background of the invention

[0002] According to the estimates of the World Health Organization (WHO), the number of people with diabetes will increase from 177 million in 2000 to 300 million by 2025. It is also estimated that 9% of all deaths worldwide are due to diabetes. Although diabetes is presently not curable, intensive insulin therapy in diabetic patients can dramatically delay the onset of serious complications.

[0003] The cornerstone to tight glycemic control is frequent or even continuous glucose monitoring, where blood glucose concentrations are measured to help administer proper levels of insulin and maintain euglycemic conditions. Continuous glucose monitoring (in practice a measurement every few minutes) is the prerequisite to enable strict glycemic control lowering the blood glucose levels within a "healthy" range (80-110 mg/dL) that prevents medical complications while avoiding dangerously low blood glucose concentrations (hypoglycemia). The ability to maintain blood glucose levels within this healthy range requires frequent measurements of glucose concentrations in the blood. Each measurement provides information that can be used to deliver the proper amount and type of insulin to maintain blood glucose levels within the targeted concentration range.

[0004] It is demonstrated that tight or continuous blood glucose control can introduce substantial reductions in overall medical care costs. Glucose sensing technology has advanced considerably in recent years, thereby providing excellent tools for home glucose monitoring and establishing opportunities for tight glycemic control. Unfortunately, the cost and pain associated with current glucose test-strip technology generally restrict the number of daily measurements performed by the average person with diabetes (on average 4-6 times a day).

[0005] Examples of next-generation sensors are implantable glucose bio-sensors. To date, implantable glucose sensors are all based on surface chemical reactions. Such sensors are very stable, accurate and sensitive in vitro. However, once the sensors are implanted, the stability and reliability reduces dramatically after a few days owing in large part to fouling of the sensor surface by proteinaceous material. They can therefore not be used for long term implantation. Alternative sensors under study are based on spectrometric devices which should allow long term in vivo operation thus justifying the surgical procedure to implant the device.

[0006] Some initiatives in the domain of subcutaneously implantable spectroscopic sensors are already reported. In US2007/0066877 A1, an implantable sensor device is established. In vitro testing confirms practicability of the invasive concept and the feasibility of target specifications. The device has a fluid inlet port, a measurement volume and a fluid outlet port. Bodily fluid and/or target analyte is forced to the measurement volume using micro-dialysis or ultra-filtration with vacuum source and analysed using a spectrometer. In "Optical Absorption Glucose Measurements Using 2.3- μm Vertical-Cavity Semiconductor Lasers" IEEE phot. Tech. lett., 20(11), pp. 930-933, 2008, the development of a 2.3 μm vertical-cavity semiconductor laser (VCSEL) is reported for applications wherein the tunable VCSEL and detector are packaged as an implantable design. However the finite tuning range of 5 nm that can be reached with the VCSEL limits the potential for in vivo use of the radiation source.

[0007] US5,833,603 describes a biosensing transponder for implantation in an organism. US2008/0186483 relates to an implantable product including an optical cavity structure with first and second parts.

[0008] "An integrated photonic sensor for in situ monitoring of hazardous organics" by Luo et al. in Sensors and Actuators 92 (2003) 121-126 describes an integrated photonic sensor based on single mode Mach Zehnder interferometry.

[0009] "Label-free Biosensors on Silicon-on-Insulator Optical Chips based on microring cavities and surface Plasmon interferometry" by De Vos et al. in Transparent Optical Networks (2008) 88 - 91, describes the use of microring resonators for biosensors. US2005/047702 describes an optical device based on a planar waveguide. US2004/0162470 describes a micro-optical-mechanical-electro-system based on a non-invasive blood glucose monitor comprising a micromachined infrared spectrometer array.

[0010] US2003/0209669 describes a miniaturized infrared gas analyzing apparatus fabricated by means of silicon micromachining technology.

[0011] US5,945,343 describes an optical sensing device comprising an urea sensing material. DE102009010955 describes a system and method for blood sugar detection using optical spectroscopy.

[0012] WO2009/156410 describes a photonic integrated circuit comprising a signal processing circuit.

[0013] EP1353200 describes an integrated optical circuit.

[0014] US6,997,879 and US2002/085784 illustrate integration of multiplexing structures in a photonic chip.

Summary of the invention

[0015] It is an object of embodiments of the present invention to provide good implantable sensors for sensing substances as well as corresponding monitoring systems. Sensing substances may include detecting or identifying targets of interest, but also may include sensing a sample for imaging it.

[0016] It is an advantage of embodiments according to the present invention that an implantable single-chip optical sensor for continuous monitoring, e.g. continuous glucose monitoring (CGM) is provided. It is an advantage of embodiments according to the present invention that the sensor can be made small, resulting in good implantation properties. It is an advantage of embodiments according to the present invention that a reagent-free, optical analysis method can be used, so that no direct contact between the sensor and the object (e.g. fluid or tissue) to be measured is required. It is an advantage of embodiments according to the present invention that the sensor can be made small, allowing optically good biocompatible packaging. The shape of the sensor may allow small thickness of the biocompatible packaging, so that absorption and diffraction by the packaging can be limited. The sensor may be substantially flat. Good biocompatible packaging may reduce or minimize bio-fouling. Furthermore, being an optical analysis method, a reduced or minimized bio-fouling might be less harmful, as the small bio-fouling results in substantial optical transparency, in contrary to biosensors for which minimal fouling often obstructs their activity.

[0017] It is an advantage of embodiments of the present invention that advanced optical processor may be provided in the sensor, allowing advanced and optionally complex radiation processing, e.g. allowing spectral and depth-resolved processing of radiation received or guided to a measurement region.

[0018] It is an advantage of embodiments according to the present invention that systems can be made such that there is no need for a stimulated flow or stimulated diffusion or stimulated displacement of material to enable sensing, i.e. that the sample or substance transport to the measurement region can be based on natural or spontaneous displacement. In this way, an extraction means for extracting fluid, a micro-cannula, a microdialysis probe, an ultrafiltration probe, etc. to extract material to a sample region can be avoided, resulting in significant advantages regarding amongst others ease of implantation and patient comfort, mechanical stability, reliability and need for powering. The latter is obtainable due to the miniaturisation of the sensor used, e.g. due to the miniaturisation of an optical processor as photonic integrated circuit.

[0019] It is an advantage of embodiments according to the present invention that the sensor has substantially direct access to the substance or sample under study.

[0020] It is an advantage of embodiments according to the present invention that it can assist in providing a closed-loop drug delivery system, such as a closed-loop insulin delivery system that is implantable within a patient's body. Sensors according to embodiments of the present

invention therefore may be coupled to a drug delivery system.

[0021] It is an advantage of embodiments according to the present invention that it can assist in non-invasive - after implantation - measurements e.g. glucose or urea measurements, allowing high frequency tests without patient discomfort.

[0022] It is an advantage of embodiments according to the present invention that substance sensing, e.g. glucose or urea sensing, can be performed in a disposable free manner, resulting in a reduced cost.

[0023] The above objective is accomplished by a device according to the appended claims.

[0024] The present disclosure relates to a sensor adapted for sensing of glucose, urea or lactate, the sensor being implantable in the body of a living creature or an object and configured for sensing in tissue or bodily fluids, the sensor comprising

- a radiation source configured for irradiating said tissue or bodily fluids in a measurement region, an integrated radiation processor and an integrated detection element, the sensor furthermore comprising a measurement region from which the radiation interacting with the glucose, urea or lactate is captured, characterised in that
- the integrated radiation processor is integrated in a silicon photonics integrated circuit and configured for spectrally processing radiation interacting with the glucose or urea or lactate , wherein the radiation processor comprises at least an integrated optical waveguide, a multiplexer and/or de-multiplexer adapted for obtaining spectrally resolved information from the spectrally processed radiation, and
- the integrated detection element is integrated in said silicon photonics integrated circuit and being configured for detecting the radiation processed by the radiation processor,

the radiation processor and the detection element forming an integrated spectrometer in said silicon photonics circuit and being configured for detecting integration or hybrid integration may result in an easy manufacturing. The detecting element may be fibre-coupled to the radiation processor.

[0025] The sensor may comprise a photonics integrated circuit compatible, integrated radiation source for irradiating a substance or a sample comprising the substance in a measurement region.

[0026] The radiation source may be a radiation source monolithically integrated with the radiation processor or heterogeneously integrated with the radiation processor or hybridly integrated with the radiation processor.

[0027] The radiation source may be fibre-coupled to the radiation processor.

[0028] The photonics integrated circuit based sensor may optionally be adapted for operating

in at least a wavelength region of 1560nm to 1850nm and/or is adapted for operating in at least a wavelength region of 2080nm to 2325nm.

[0029] The radiation processor may comprise a spectrometer for obtaining spectrally resolved information from the spectrally processed radiation after interaction. According to embodiments of the present invention, detecting spectral information regarding the absorption or scattering may allow for accurate detection of absorption bands of e.g. glucose. It is an advantage of embodiments according to the present invention that spectrally resolved information can be obtained as this allows for more accurate detection of glucose due to the possibility of detecting different absorption or reflection bands of glucose in the sample.

[0030] The sensor may have a sensor configuration such that a measurement region of the sensor is surrounded by components of the sensor. It is an advantage of some embodiments according to the present invention that transmission measurements, reflection measurements, absorption measurements as well as scattering measurements may be performed.

[0031] The sensor may have a sensor configuration such that a measurement region of the sensor lies substantially at one side of all components of the sensor. It is an advantage of embodiments according to the present invention that the measurement region may not be provided as channels, therefore being less prone to obstruction. spectral absorption bands of glucose, urea or lactate for determining a concentration of glucose, urea or lactate based thereon, and the radiation processor and the measurement region being configured for allowing substance-sampling free spectral measurements so that sensing can be performed without the need for extracting a sample or guiding a substance of interest in a forced manner to the measurement region.

[0032] In embodiments of the present invention, no extraction or probing must be performed.

[0033] The sensor may comprise a measurement region from which radiation is captured, the radiation processor and measurement region being adapted in size so as to allow for time-dependent substance measurements based on spontaneous displacement of the substance in the body. It is an advantage of embodiments according to the present invention that using a photonics integrated circuit based sensor, the sensor can be adapted in size such that time dependent measurements of the sample can be performed based on the natural flow of sample through the body of the living creature, without the need for a forced flow or displacement using a sampling means such as for example a pumping system such as a mechanical or electromechanical pump system, a fluid extractor, a micro-cannula, a microdialysis probe, an ultra-filtration probe, an implanted wick. It is an advantage of embodiments according to the present invention that more reliable and robust sensors can be obtained, with less or no mechanically moving components such as pumps.

[0034] The measurement region may be an open-space measurement region so that it is not substantially enclosed by sensor walls. The number of mechanical sensor walls around the

measurement region may be less than 2, e.g. only at one side a sensor wall may be present. The measurement region therefore may not be a closed room with an inlet and/or outlet.

[0035] It is an advantage of embodiments according to the present invention that the silicon-photonics based sensor can inherently be small so that only a small sample chamber of measurement region is required, resulting in smaller sample volumes being measurable. The latter can assist in continuous flow measurements because it allows on the one hand to use natural flow of the sample in the body and on the other hand provides more detailed results as smaller volumes can be probed.

[0036] It is an advantage of embodiments according to the present invention that integration of the sensor may result in a small footprint of the sensor.

[0037] The detecting element may be a detecting element monolithically integrated with the radiation processor or a heterogeneously integrated with the radiation processor or a hybridly integrated with the radiation processor. It is an advantage of embodiments according to the present invention that monolithic integration or heterogeneous integration or hybrid integration may result in an easy manufacturing. The detecting element may be fibre-coupled to the radiation processor.

[0038] The sensor may comprise a photonics integrated circuit compatible, integrated radiation source for irradiating a substance or a sample comprising the substance in a measurement region.

[0039] The radiation source may be a radiation source monolithically integrated with the radiation processor or heterogeneously integrated with the radiation processor or hybridly integrated with the radiation processor.

[0040] The radiation source may be fibre-coupled to the radiation processor.

[0041] The photonics integrated circuit based sensor may optionally be adapted for operating in at least a wavelength region of 1560nm to 1850nm and/or is adapted for operating in at least a wavelength region of 2080nm to 2325nm.

[0042] It is an advantage of embodiments according to the present invention that spectrally resolved information can be obtained as this allows for more accurate detection of glucose due to the possibility of detecting different absorption or reflection bands of glucose in the sample.

[0043] The sensor may have a sensor configuration such that a measurement region of the sensor is surrounded by components of the sensor. It is an advantage of some embodiments according to the present invention that transmission measurements, reflection measurements, absorption measurements as well as scattering measurements may be performed.

[0044] The sensor may have a sensor configuration such that a measurement region of the

sensor lies substantially at one side of all components of the sensor. It is an advantage of embodiments according to the present invention that the measurement region may not be provided as channels, therefore being less prone to obstruction.

[0045] The sensor configuration may be adapted for obtaining depth-related information regarding the sample. It is an advantage of embodiments according to the present invention that depth related sample information can be obtained, as the latter allows taking into account separation of the sample from the sensor through other tissue, such as for example collagen deposits. It is an advantage of embodiments according to the present invention that both spectrally and depth resolved measurements can be performed, allowing more accurate detection of a substance in the sample.

[0046] The sensor configuration may be configured for spatially resolved detection and for deriving said depth-resolved information regarding the sample based thereon.

[0047] The radiation processor may be adapted for spatially resolved detection of scattered or reflected radiation.

[0048] The radiation processor may comprise a plurality of cascading wavelength multiplexers or demultiplexers for increasing a number of channels for spectrally processing radiation.

[0049] The radiation processor may comprise a plurality of tuneable filters or filters for increasing a number of channels for spectrally processing radiation.

[0050] Frequency or time-domain multiplexing may be used for increasing a number of channels for spectrally processing radiation.

[0051] A Vernier-shifted spectral response may be used for increasing a number of channels for spectrally processing radiation.

[0052] The sensor may comprise an electronics component stacked with the sensing element and radiation source, wherein the connection between sensing element and radiation source on the one hand and the electronics on the other hand is made by through silicon vias.

[0053] The sensor may be adapted for sensing glucose.

[0054] The sensor may be adapted for sensing urea.

[0055] The sensor may be adapted for being implantable in a bioreactor.

[0056] The sensor may be provided with bodily fluid extraction means or radiation guiding means for extracting bodily fluid from the body or for guiding radiation to and from the sample, other components of the sensor being configured for extra-vivo use rather than being implantable.

[0057] The present invention also relates to a continuous monitoring system comprising an implantable sensor for sensing a substance as described above and a readout system for wirelessly receiving data sensed by the sensor.

[0058] The present invention also relates to the use of an implantable sensor as describe above as glucose sensor. Such use may be for sensing a glucose level in the body of a living creature.

[0059] The present invention also relates to the use of an implantable sensor as describe above as urea sensor. Such use may be for sensing a urea level in the body of a living creature.

[0060] In some embodiments, the present disclosure also relates to a method for sensing a substance, the method comprising receiving radiation interacting with a sample, prior or after said interacting, spectrally processing the radiation using a photonics integrated circuit based radiation processor. The method optionally further may comprise method steps corresponding with the functionality of the different components described for the sensor above.

[0061] Particular and preferred aspects of the invention are set out in the accompanying independent and dependent claims. Features from the dependent claims may be combined with features of the independent claims and with features of other dependent claims as appropriate and not merely as explicitly set out in the claims.

[0062] These and other aspects of the invention will be apparent from and elucidated with reference to the embodiment(s) described hereinafter.

Brief description of the drawings

[0063]

FIG. 1 illustrates a schematic example of components of a sensor according to an embodiment of the present invention.

FIG. 2A illustrates a 1x4 demultiplexer based on a planar concave grating, as can be used in an embodiment according to the present invention.

FIG. 2B illustrating an enlarged view of deeply etched teeth of an optical component as shown in FIG. 2A.

FIG. 3 illustrates a 1x4 multiplexer based on a planar concave grating, as can be used in an embodiment according to the present invention.

FIG. 4 illustrates a 1x23 multiplexer based on a laser array coupling to a waveguide, as can be used in an embodiment according to the present invention.

FIG. 5 illustrates a 1x32 demultiplexer based on an arrayed waveguide grating, as can be used in an embodiment according to the present invention.

FIG. 6 is a schematic cross-section of an exemplary post-dispersive sensor according to one embodiment of the present invention.

FIG. 7 is a schematic cross-section of an exemplary predispersive sensor according to one embodiment of the present invention.

FIG. 8 to FIG. 11 illustrate different examples of radiation processors, as can be used in embodiments of the present invention.

FIG. 12 illustrates the Vernier shift obtained in spectra when using a Vernier demultiplexer according to one embodiment of the present invention.

FIG. 13 illustrates a basic setup for an optical tomography system as can be used in embodiments according to the present invention.

FIG. 14 and FIG. 15 illustrates an example of a continuous monitoring system according to an embodiment of the present invention.

[0064] The drawings are only schematic and are non-limiting. In the drawings, the size of some of the elements may be exaggerated and not drawn on scale for illustrative purposes.

[0065] Any reference signs in the claims shall not be construed as limiting the scope.

[0066] In the different drawings, the same reference signs refer to the same or analogous elements.

Detailed description of illustrative embodiments

[0067] Where in embodiments of the present application reference is made to a photonics integrated circuit (PIC), this refers to a variety of forms and material systems such as for example low-index contrast waveguide platforms (e.g. polymer waveguides, glass/silica waveguides, $\text{Al}_x\text{Ga}_{1-x}\text{As}$ waveguides, $\text{In}_x\text{Ga}_{1-x}\text{As}_y\text{P}_{1-y}$ waveguides), high-index contrast waveguides (e.g. Silicon-on-Insulator, semiconductor membranes), plasmonic waveguides (e.g. metal nano-particle arrays, metal layers), also called Photonic Lightwave circuits (PLC). A photonic integrated circuit comprises at least one integrated optical component, such as for example but not limiting to an integrated optical cavity, an integrated optical resonator, an integrated optical interferometer, an integrated optical coupler, a waveguide, a taper, a tuneable filter, a phase-shifter, a grating, a modulator, a detector, a source, a multiplexer, a demultiplexer or a combination thereof. The optical components can be active or passive. The

components can be integrated for example monolithically, heterogeneously or hybridly. Monolithical integration is the integration technology that uses a single processing flow to process the diverse components potentially using different materials, e.g. integrated germanium detectors in silicon photonics IC. Heterogeneous integration is the integration technology for which the components are processed in separate process flows, which are then integrated at die or wafer level, e.g. BCB bonding, wafer bonding, and other bonding schemes, 3D integration. Hybrid integration is the integration of components or materials on processed photonic integrated platforms, e.g. flip-chipping of detectors, bumping, gluing, wire bonding, co-packaging, etc.

[0068] The devices and methods of the present invention are further described for the particular case of an SOI (Silicon-on-Insulator) material system, also referred to as silicon photonics system. However, the devices and methods of the present invention can be based on other material systems, such as for example III-V material systems, metallic layers, low index contrast material systems or a combination thereof.

[0069] Silicon-on-Insulator is a very interesting material system for highly integrated photonic circuits. The high refractive index contrast allows photonic waveguides and waveguide components with submicron dimensions to guide, bend and control light on a very small scale so that various functions can be integrated on a chip. Moreover SOI offers a flexible platform for integration with surface plasmon based components which in turn allows for even higher levels of miniaturization. Both waveguide types allow a high level of miniaturization, which is advantageous. Furthermore for both waveguide types light can be efficiently coupled in and out the PIC by use of e.g. a grating coupler or another coupling element.

[0070] Using Silicon-on-insulator also has some technological advantages. Due to the CMOS industry, silicon technology has reached a level of maturity that outperforms any other plane chip manufacturing technique by several orders of magnitude in terms of performance, reproducibility and throughput. Nano-photonic ICs can be fabricated with wafer scale-processes, which means that a wafer can contain a high amount of photonic integrated circuits. Combined with the commercial availability of large wafers at a relative moderate cost, this means that the price per photonic integrated circuit can be very low.

[0071] Where in the present application reference is made to "photonics integrated circuit compatible", reference is made to components that can be integrated in the semiconductor chip or platform.

[0072] Embodiments of the present invention typically may be used in pre-dispersive or post-dispersive applications. Where embodiments of the present invention refer to pre-dispersive applications, reference is made to embodiments wherein the radiation before interaction with the object to be measured is spectrally resolved. Where embodiments of the present invention refer to post-dispersive applications, reference is made to embodiments wherein the radiation after interaction with the object to be measured is split into individual components of different wavelengths. Where in embodiments of the present application reference is made to

integration, such integration may comprise monolithical, heterogeneous or hybrid integration. In some embodiments, such integration also may enclose fibre coupling of components to the silicon chip or platform.

[0073] Where in embodiments of the present application reference is made to radiation, reference is made to electromagnetic radiation. The radiation envisaged is radiation having a suitable wavelength or wavelength range for sensing, i.e. detecting or imaging, a substance. In some embodiments radiation used will be infrared radiation, e.g. near infrared radiation or mid infrared radiation. In some embodiments, the radiation has a wavelength or wavelength range between 1200nm and 2500nm, or between 2500nm and 10000nm, or a combination thereof, although the invention is not limited thereto.

[0074] Where in embodiments of the present application reference is made to subcutaneous there is meant "under the skin". Where in embodiments of the present invention reference is made to intramuscular there is meant "inside a muscle". Where in embodiments of the present invention reference is made to retroperitoneal, reference is made to "in the abdominal cavity". Where in embodiments of the present invention reference is made to intravascular, reference is made to "inside a blood vessel", and whereby in embodiments of the present invention reference is made to extra-vascular, reference is made to "close vicinity to a blood vessel". Where in embodiments reference is made to "interstitial", there is meant relating to or situated in the small narrow spaces between tissues or parts of an organ. Interstitial fluid is extracellular fluid that is present throughout the body and skin. It typically may be found in the outermost layers of the skin. Where in embodiments reference is made to tissue, the latter includes an aggregate of cells of a particular kind, together with their intercellular substance, that forms structural material. The substance of interest may be a target analyte being present in any sample such as for example in tissue, bodily fluid such as interstitial fluid, urine or blood, etc. Alternatively or in addition thereto, the substance also may be a tissue itself, whereby sensing may be performed for obtaining an image thereof.

[0075] In a first aspect, the present invention relates to a sensor for sensing a substance. Embodiments of the present invention are sensors for the sensing of a substance in the body of living creatures including the human being, but the invention is not limited thereto. The living creature may be any organism for which a sample containing a target substance can be obtained. The living creature may be any creature wherein the sensor can be implanted. It may for example be a plant or an animal, such as a mammal or non-mammal. It may be cold-blooded or warm-blooded. In some preferred embodiments, sensors are provided for sensing glucose, although also sensors are provided for sensing of other substances, such as for example urea, lactate, creatinine, triglyceride, protein, cholesterol, ethanol, etc. Alternatively or in addition thereto, the substance thus also may include tissue itself and sensing may be performed for imaging purposes, e.g. blood vessels, nerves, cancer tissue, cellular changes, etc. It is to be noticed that the wavelength at which sensing is performed mainly may be determined by the substance to be sensed. The selection of a different substance to be sensed, i.e. detected, imaged or monitored, thus may result in the need for using similar components as described for glucose, but having operability in another wavelength region or

converters therefore. For the sake of convenience, embodiments of the present invention will be further described with reference to glucose sensing, but it will be clear to the person skilled in the art that the description in the embodiments and examples is mutates mutandis applicable to embodiments of substance sensing in a different wavelength.

[0076] The sensor may be adapted - e.g. by a particular detecting element and/or radiation source as well as by optical components used in the optical processor- to be used in a the near infrared radiation wavelength range, e.g. in a range between 1200nm and 2500nm. The sensor may be adapted for use in those wavelength regions where glucose has particular absorption or scattering. For example, the sensor may be adapted for operating in the first-overtone band (1560nm to 1850 nm) and/or the combination band (2080nm to 2325nm) where glucose has numerous absorption bands and water has relative lower absorption. The selection of which wavelength range used could for example be based on the available radiation sources and detectors and on the degree of absorption of glucose occurring. For the different embodiments, especially if the combination wavelength range is used, optimization may be performed such that minimal propagation losses are obtained while maintaining a single-mode condition over the entire wavelength range of interest.

[0077] A sensor according to embodiments of the present invention is implantable in the body of a living creature. More particularly, the sensor according to embodiments of the present invention may be implantable in the human body, but the invention is not limited thereto. The sensor may be for example implanted subcutaneous, intramuscular, retroperitoneal, extra-vascular, intravascular, ocular, vesicular, or implanted in an organ. Subcutaneous and intramuscular implants may happen at different locations, e.g. in the fore arm, the upper, arm, the abdomen, etc. According to embodiments of the present invention, the sensor comprises a photonic integrated circuit based radiation processor, also referred to as radiation processing means, for spectrally processing radiation used for sensing a substance. Where in embodiments of the present invention reference is made to spectrally processing radiation, reference is made to processing of the radiation that influences the spectral behaviour of the radiation, such as for example splitting of different wavelength components into different radiation subbeams, merging of beams having a different spectral composition into a single beam. In other words the sensor may be adapted for capturing radiation that was directed to a sample and that has interacted therewith and processing that radiation, for processing radiation that is then directed to a sample and interacts therewith or for a combination thereof. It is an advantage of embodiments according to the present invention that photonics integrated circuit based radiation processors are used allowing miniaturization of the sensor. It is an advantage of embodiments according to the present invention that sensing, i.e. detecting or imaging, can be performed without substance-sampling, i.e. without the need for extracting sample or guiding the substance of interest, e.g. incorporated in the sample, in a forced manner to a measurement region. In this way, there is thus no longer need to actively induce a displacement of substance by stimulated flow, stimulated diffusion, etc. such as for example using microdialysis , micro-cannula, ultra-filtration or another sampling probe or extraction means. It is an advantage that in this way there is no need for using a fluid inlet and outlet port to guide a sample or substance to a separated measurement region. The measurement region

does not need to be enclosed by sensor walls. The number of mechanical sensor walls may be limited and optionally only at one side a mechanical sensor wall may be present. The miniaturization enables the device to be as compact that the natural flow of bodily fluids or the natural diffusion of substance, e.g. present in living creatures, e.g. in the human being, enable the possibility for sensing and for continuous monitoring the substance. It is also an advantage of embodiments of the present invention that sensing is performed using optical characterization, therefore not requiring reagents. These advantages result in a reliable and long term usable sensor, without the need for significant interference of operators.

[0078] By way of illustration, embodiments of the present invention not being limited thereto, an example of a sensor device comprising standard and optional components according to embodiments of the present invention is shown in FIG. 1.

[0079] The sensor 100 according to embodiments of the present invention comprises a photonics integrated circuit, e.g. silicon photonics integrated circuit, based radiation processor 110. Such a photonics integrated circuit based radiation processor advantageously is adapted for processing radiation spectrally, prior to directing it to a sample, also referred to as pre-dispersive, and/or received after interaction with the sample, also referred to as post-dispersive, in such a manner that one or more corresponding detecting element(s) 120 is fed with appropriate signals. The radiation processor 110 and the detecting element 120 are described as separate components, but these may form one part. The radiation processor 110 therefore also may be part of the detecting element 120. The photonics integrated circuit based radiation processor 110 may comprise a plurality of integrated components, such as for example waveguides, multiplexers, demultiplexers, couplers, splitters, filters, tuneable elements, laser sources, LEDs, etc. The photonics integrated circuit based radiation processor 110 is adapted for spectrally processing radiation, meaning that the photonics integrated circuit based radiation processor is adapted for processing the radiation in a wavelength dependent manner. In at least some embodiments of the present invention the radiation processor comprises optical components in the photonic integrated circuit. The photonics integrated circuit based radiation processor 110 may for example act as a multiplexer or demultiplexer or part thereof, an interferometer or part thereof, an integrated active or passive optical cavity, an integrated optical active or passive resonator, an integrated optical coupler, a waveguide, a grating, or a combination thereof. The radiation processor may for example comprise a coupler for coupling in the radiation on the chip. One example of a coupler may be an on-chip diffraction grating. Such a diffraction grating may be optimized using optical design techniques. Examples of grating couplers that may be used are diffractive gratings with a 1 dimensional (1D) or 2 dimensional (2D) binary lattice structure. The couplers, e.g. gratings, capturing the radiation on the chip may be optimized for capturing the optimum amount of light, e.g. by increasing the coupler size and by matching the other coupler parameters thereto. Furthermore the coupler, e.g. grating may be adapted for splitting the spectrum into sub-ranges. An etched diffraction grating can be used that utilizes the coherence properties of light to spatially separate different wavelengths. The latter may be performed by using a coupler that comprises a number of individual sub-couplers each operating in a particular wavelength range being a sub-range of interest. Each coupler may be connected to its own radiation

processor circuit. The circuit may be an interferometer, a tuneable filter, an arrayed waveguide grating (AWG) or a planar concave grating (PCG) or a combination thereof. While the diffraction grating together with the circuit spatially separates the different wavelengths, photodetectors have to be integrated on the photonic chip to convert the optical signals into electrical signals. By way of illustration, a 1x4 de-multiplexer based on a planar concave grating is shown in FIG. 2A and a 1x4 multiplexer based on a planar concave grating is shown in FIG. 3. In the latter case, an integrated laser array might be coupled to the respective channels of the multiplexer. The de-multiplexer of FIG. 2A and multiplexer of FIG. 3 illustrate a structure with a reference photonic wire 250 wherein no dispersive processing occurs and a photonic wire 240, or photonic waveguide 240, respectively guiding radiation of different wavelengths away from or towards a spectrally processing radiation processor. In FIG. 2A, a set of 500nm wide photonics wires is indicated for guiding radiation of different wavelengths away. The radiation processor in the de-multiplexer example is a structure having a dispersive concave grating, e.g. deeply etched teeth 220 also shown in enlarged view in FIG. 2B, for dispersively reflecting incident broadband radiation, a free propagation region 210 wherein the radiation can freely propagate and coupling structures 230, e.g. shallow-etch apertures, for coupling the dispersively reflected broadband radiation into the respective waveguides. The radiation processor in the multiplexer example is analogue due to reciprocity. In FIG. 2A arrow 270 gives the direction of the radiation coupling in the radiation processor and arrow 280 indicates the direction of the radiation being coupled out of the radiation processor. In FIG. 3 arrow 310 gives the direction of the radiation coupling in the radiation processor and arrow 320 indicates the direction of the radiation being coupled out of the radiation processor.

[0080] FIG. 4 and FIG. 5 illustrate a 1x23 multiplexer and a 1x32 de-multiplexer respectively de-multiplexer. The multiplexer 400 in FIG. 4 is based on integrated lasers 410, e.g. silicon photonics integrated lasers, e.g. ring lasers or microdisk lasers or DFB lasers or DBR lasers, light is directly coupled in a single silicon waveguide 420, such that serial multiplexing is intrinsic when using a PIC technology approach. Alternatively, also coupling of radiation from some or all of the integrated radiation sources to different waveguides may be used. A laser array of 23 lasers is shown as example in FIG. 4. The lasers may be tunable lasers, in the present example each covering about 2 to 4nm wavelength range. The light of the respective lasers are serially multiplexed on a single waveguide and coupled out of the circuit by a coupling element e.g. grating coupler 430. A monitoring diode might be integrated, i.e. the integrated power monitor 440, to monitor the circuit. Furthermore, sensitive photo-detectors 450 for detecting the radiation after interaction with the object under study is also shown.

[0081] The 1x32 de-multiplexer shown in FIG. 5 is based on an arrayed waveguide grating. An input coupler, such as for example an input star coupler 510, and an output coupler 530, such as for example an output star coupler, are used for guiding the radiation to the radiation processor, whereby the radiation processor in this configuration is an arrayed waveguide grating (AWG), which introduces a wavelength dependent phase delay. A set of dispersive delay lines 520 is shown. Depending on the number of channels and the width of the wavelength channels, either an AWG or a PCG is preferable in terms of performance or size. Arrow 540 indicates the in coupling direction for the radiation, while arrow 550 indicates the out

coupling direction for the radiation. By way of illustration a possible size of a delay line is indicated using a picture, embodiments of the invention not being limited thereby. Alternatively to a PCG or AWG based multiplexer, grating couplers to spatially multiplex the light of an integrated laser array might be used, or multiplexing by serially coupling the lasers to a single waveguide might be used. This approach is enabled by the fact that a photonic integrated circuit technology is used. Waveguides and gratings can be used to guide the light and couple the light out/in wherever necessary.

[0082] According to other embodiments of the present invention, the radiation processor may be an optical radiation processor, whereby optical components merge or split different spectral radiation components of the radiation beam. The sensor 100 furthermore may comprise one or more detecting elements 120 for detecting the processed radiation. Such one or more detecting elements 120 are photonics integrated circuit compatible detecting elements. The detecting elements 120 may for example be III-V material based detecting elements that can be integrated in the photonic integrated circuit platform. Integration of the detecting element may be performed in a number of ways : the detecting elements 120 may be monolithically, heterogeneously or hybridly integrated with the radiation processor 110 or coupled through optical fibre to the photonics integrated circuit radiation processor 110. In one example, one or more detecting elements 120 may be based on epitaxial grown layers or wafers, although the invention is not limited thereto. Conventional or designed bonding processes may be used for integrating the detecting elements. In case of a glucose sensor, the detecting element 120 may for example be an InGaAs epilayer detector, which is especially suitable in the overtone band, or an InGaAsSb epilayer detector which may be especially suitable for the combination band. Other detecting elements also could be used, as long as these can be integrated within the photonics integrated circuit platform in a suitable manner and as long as their detection characteristics are suitable for the sensing requirements set.

[0083] The sensor 100 also may comprise at least one radiation source 130 for generating a radiation beam for irradiating a sample. The radiation source may be integrated in the photonics device. The radiation source may be a single radiation source or may be an array of sources, such as for example an array of LED lasers or a laser array. The at least one radiation source 130 advantageously is a photonics integrated circuit compatible radiation source integrated in the sensor, although integration of the source on the photonics integrated circuit is not essential. In one embodiment, the at least one radiation source 130 may be homogeneously integrated with the sensor, for example with the radiation processor 110 as shown in FIG 4 or heterogeneously integrated with the sensor 100, for example with the radiation processor 110, although the invention is not limited thereto. The radiation source may be adapted for irradiating the sample in a wavelength range that is suitable for sensing the substance under study, e.g. in the overtone or combination band. In one embodiment, the radiation source may be a light emitting device (LED) integrated in a photonics integrated circuit platform used in the sensor 100. The radiation source 130 also may be any other suitable radiation source, such as for example a VCSEL, a solid state tunable laser, etc. Due to the small emission wavelength range wherein most tunable radiation sources can be tuned, the radiation source preferably is a wide wavelength range emitting radiation source or a a

laser array, covering a suitable range for characterizing substances.

[0084] The measurement configuration and principle of the sensor 100 typically may be defined by the detecting element, the radiation processor or part thereof and optionally also the radiation source. The sensor configuration may be adapted to accommodate for example spectral absorption measurements. Advantageously, embodiments of the present invention include a sensor configuration wherein the detected results are spectrally resolved, comprise depth-related information or preferably a combination thereof. It is an advantage of some embodiments according to the present invention, that advanced radiation processors can be provided allowing both spectral and spatial in-depth analysis and resulting in good sensors. Such advanced radiation processors allow for compact sensors with high accuracy. Obtaining depth-related information is especially suitable e.g. in case the response comes from a diffusely scattering medium. The latter may be especially suitable for sensing of media of interest separated from the sensor by tissue, such as for example collagen deposits. By way of illustration, a number of sensor configurations allowing particular measurement techniques will be described further in the description.

[0085] The sensor 100 may have a measurement chamber or measurement region 140 or may be adapted for measuring in an external measurement region 140. The position of the measurement region 140 typically may be determined by the sensor configuration. In case the sensor configuration allows measurement in transmissive or transreflective measurement, the measurement region typically may be surrounded by components of the sensor. Typically in such measurements, the at least one radiation source 130 is substantially diametrically opposed to the radiation processor 110 and the detecting element 120. Or in a predispersive approach, the at least one radiation source and the radiation processor is substantially diametrically opposed to the detecting element. Alternatively, the radiation source may be integrated in the photonics integrated circuit platform wherein the radiation processor is made and an additional mirror opposed substantially diametrically to the radiation source with respect to the measurement region 140 directs radiation that has passed the sample towards the radiation processor. In such a setup, the measurement system detects both the diffuse reflectance and the transmittance signal, which may be especially suitable in case dense biological suspensions are to be measured. In case a sensor with a measurement region surrounded by components is selected, the size of the measurement region, which typically may correspond with the internal diameter of the sensor through which the sample may pass, must be determined as function of the absorption coefficient of the sample or tissue relative to the absorption coefficient of glucose and the available power budget. By way of example for the combination band, an optical path length may be preferred between 1mm and 2 mm, implying an inner diameter between 0.5mm and 2 mm. One possible shape is a ring shape or doughnut shape, although the invention is not limited thereto. By implementing the sensor as a photonic integrated circuit based sensor a miniaturized sensor can be obtained having a small foot print in the order of square mm. The overall average diameter of the sensor may for example be in the range 4mm to 50mm . In case the sensor configuration is adapted for measuring in reflection, the measurement region 140 typically lies outside the solid portion of the sensor, i.e. on one and the same side of the sensor components. Diffuse scattered light

then can be detected. The actual preferred sensor shape may be defined by a number of factors, e.g. the chosen configuration such as measurement in reflection or in transmission, the body reaction - which shape causes the least tissue reaction -, etc. and can be chosen as function of the weight of these factors, e.g. a cylinder with height 0.5-30mm and diameter order 2-50 mm.

[0086] It is an advantage of embodiments according to the present invention that measurement regions without inlet and outlet, e.g. measurement regions being not substantially limited by walls of the sensor, can be used. The latter allows quick measurement of the substance, optionally reducing the instrumental delay time between actual concentration of the target analyte in the sample and the measured concentration of target analyte in the sample.

[0087] The required signal-to-noise ratio, the number of spectral measurements, the necessary resolution may depend on the sample, e.g. tissue that is measured and may for example be determined based on trial and error, a complex tissue model, by experimental test measurements, etc. The obtained signal to noise ratio SNR depend on the magnitude of the radiant power reaching the detector. As the thickness increases, the radiant power at the detector decreases because of scattering and absorption processes. The concentration sensitivity for the detection typically increases linearly with tissue thickness while the signal to noise ratio decreases exponentially. The sensor may be designed such that the spectrometric performance and power budget may be optimized, taking into account parameters such as the bandwidth, the resolution and sensitivity, etc.

[0088] The sensor 100 furthermore may comprise an electronic unit 150 for controlling and driving the radiation source 130 and/or the sensing elements 120. The electronic unit may be implemented in CMOS technology. Furthermore if tunable components are present in the radiation processor 110, these also may be driven by an electronic unit 150. The electronic unit may combine a plurality of control or drive functions or separate electronic units may be provided for each component to be driven. It is an advantage of embodiments according to the present invention that the electronic unit 150 optionally may be integrated in the same photonic integrated circuit chip as used for the radiation processor 110 and optionally the radiation source 130 and the sensing elements 120. Thus, although the invention is not limited thereto, the electronic unit may be integrated with the photonic integrated circuit. Such integration may be monolithically, i.e. electronics and photonics can be defined in the same process flow whereby either the photonics components or the electronics components can be performed in front-end processing. Alternatively, heterogeneous integration may be performed whereby the photonics wafer and the electronics wafer are processed in separate process flows and are then integrated. The electronic unit may be connected with the components to be controlled through interconnections, e.g. vias. In an advantageous embodiment, the electronic unit and the components may be stacked and connection may be performed by throughput vias e.g. copper nails. Other ways of integration may include bonding techniques such as for example BCB or wafer bonding, whereby both die to wafer or wafer to wafer bonding may be performed. Alternatively, the photonic integrated chip and the electronic chip can be positioned

close to each other on a printed circuit board, e.g. a thin flexible printed circuit board. The latter may be done prior or after packaging. The electronic unit may control components according to a predetermined algorithm, a programmable algorithm, preferably programmable from a distance, etc. The electronic unit may comprise a power source, e.g. battery, e.g. inductively powered, so that powering of the system can be performed from a distance.

[0089] The sensor 100 furthermore may comprise a data transmitter 160, for transmitting data from the sensing element(s) 120 to a read-out component outside the body. The data transmitter may comprise a memory for temporary storing the data before sending. The data transmitter 160 thus typically is linked through the sensing element(s) 120 for capturing data from the sensing elements. Nevertheless, other components, such as for example the electronic circuit or additional sensing elements present in the sensor, e.g. T-sensor, humidity sensor (e.g. detecting leakage), etc. also may be connected to the data transmitter for passing information to an external read-out component. Data to be transmitted may for example involve absorption, reflection, transmission or scattering data obtained with the sensor, timing data, data for reporting functionality of the sensor, etc. The data transmitter 160 also typically may comprise an antenna for transmitting the data.

[0090] The sensor may be packaged in a biocompatible packaging 170 such that good implantation properties are obtained. The latter may be a biocompatible packaging as known from prior art or a more dedicated biocompatible packaging, specifically designed for the sensor. The sensor may be packaged such that it is transparent for incident radiation. The packaging may also enable a bio-mimic interface with its environment.

[0091] Whereas according to some embodiments of the present invention the sensor may be adapted such that it can operate in a pump-free manner, the system may be adapted such that it nevertheless can be used with an extraction system for extracting bodily fluid using e.g. current or micro-cannula, with a microdialysis probe, with an ultra filtration probe, etc. The sensor could e.g. then be used to perform measurements on small amounts of bodily fluid, e.g. interstitial fluid extracted to a measurement chamber. Nevertheless, such embodiments may suffer from being less reliable with respect to longterm use.

[0092] By way of illustration, a schematic cross-section of a sensor comprising a silicon photonics integrated circuit based radiation processor and detecting element resulting in an integrated spectrometer is described with reference to FIG. 6 and 7 for a post-dispersive respectively pre-dispersive sensor, the present invention not being limited thereto. The illustrated sensor 600 shows a device packaged in a biocompatible packaging material 602. The photonics integrated circuit based sensor 600 comprises a silicon substrate 604, whereon an oxide layer 606, whereon a silicon layer and an oxide top cladding layer 608 is provided. In these materials an input grating 610, a waveguide 612 and an output grating 614 are provided being part of the optical processor and allowing incoupling of incident radiation 615 and direction of the radiation towards a detecting element 616, in the present example being a III-V detector, e.g. InGaAsSb. In the present example, the detecting element 616 is provided on the oxide layer 606 using a BCB bonding layer 618. Furthermore, at a backside of the silicon

substrate CMOS electronics 620 are provided comprising drivers for driving the detecting element, the radiation source, the tunable components, the data conversion means and transmission means for transmitting the data. The latter also is provided via a BCB bonding layer 623. Powering of the detecting element may be performed through a Cu nail through via 624 connected with the CMOS electronics which may be powered through a connection wire 622, or more preferably wireless. The through via may comprise a Au metallization 626 for actually connecting the through via with the detecting element, and at the other side may be connected with the CMOS electronics driver component via a Cu landing pad 628. Similar components can be seen in FIG. 7, but the component shown is a component for irradiating tissue whereby radiation is coupled out 702 and therefore a radiation source 704, in the present example being a laser, is provided coupling light into a waveguide and coupling out the radiation to tissue.

[0093] In order to further illustrate the principles and features of different embodiments of the present invention, a number of particular embodiments will be discussed in detail below.

[0094] In one particular embodiment, the sensor is adapted for spectral absorption, reflection or transmission measurements or for use with spectrally resolved scattering measurements. The sensor according to the particular embodiment therefore may comprise an integrated spectrometer that can measure the intensity of radiation in small wavelength intervals. The integrated spectrometer is then formed by the radiation processor 110 and the detecting element 120. In order to obtain the integrated spectrometer, the radiation processor 110 may comprise an on-chip wavelength demultiplexer which separates incoming radiation, after it has interacted with the sample, into its constituent wavelengths. The multiplexer and demultiplexer may be based on several techniques, such as for example resonators, diffraction gratings, dispersive delay lines, etc.

[0095] In further particular embodiments, the sensor is adapted for spectral measurements using an integrated spectrometer, whereby an increased number of channels compared to conventional spectrometers is obtained using one or more of the following techniques. A large number of wavelength channels in the spectrometer increases the resolution obtained. A number of techniques may advantageously be used to enlarge the resolution, further allowing to limit or prevent the increase of crosstalk levels. These techniques also may be combined with each other. The radiation processor may comprise cascading wavelength demultiplexers. Instead of splitting the spectrum in one operation, first a coarse splitting may be done, followed by a set of finer splitting with narrower wavelengths. In one example, the coarse splitting can be performed by grating couplers, i.e. by a first demultiplexer 810, while the narrower channel splitting can be done using an arrayed waveguide grating (AWG) or a planar concave grating (PCG), i.e. by second demultiplexers 820. The split radiation is guided to a plurality of detector elements 830. The latter is shown in FIG. 8. The radiation processor also may comprise cascading using swept tuneable filters 910 and a demultiplexer 920 : for finer resolution, the input or output of the spectrometer could be connected to a sharp wavelength filter, which is tuneable. By rapidly sweeping the filter and measuring the response a higher-resolution spectrum can be obtained which can be detected by detectors 930. The latter is shown

schematically in FIG. 9. A third technique that may be used for having a large number of channels is frequency or time-domain multiplexing the use of the spectrometer. Several types of spectrometers (especially the arrayed waveguide grating based spectrometers) can have multiple inputs, in fact about the same number as there are outputs. Using all inputs at the same time will blend together the spectra of all the inputs. This can be remedied by using fast switching at the inputs, so all inputs can be processed using the same spectrometer one at a time. Similarly, the signals at all the inputs could be modulated using a different RF frequency, which can then be split again by the electronics at the detector side. In this way more channels can be generated. The principle is illustrated in FIG. 10, illustrating a set of switches/modulators 1010 at the receiving side, followed by a demultiplexer 1020 and a set of detectors and demodulators 1030. A fourth exemplary method for increasing the number of channels may be by exploiting the Vernier-shifted spectral response, as illustrated in FIG. 11 and 12. In FIG. 11 a set of switches/modulators 1110 is shown directing radiation to a vernier demultiplexer 1120 and guiding radiation to a set of detectors 1130. FIG. 12 illustrates the demultiplexer output as function of wavelength for the different switches/modulators a, b and c shown in FIG. 11. Based on the previous technique, the same input could be analysed in more detail by inducing a Vernier-shifted spectral response. By carefully designing the spacing of the inputs and outputs, the spectral position of the output wavelength channels can be shifted for the different outputs. By combining the data from the different inputs, a much more detailed spectrum can be obtained. Or, in reverse, the channel count of the spectrometer could be reduced and still yield the same information. Advantageously, a sensor according to the present embodiment is equipped with a spectrometer that can handle up to 40-60 wavelength channels with 2-3nm resolution. In one example, a spectrometer platform, potentially low-cost, which can handle several tens of wavelength channels and >0.5 nm channel spacing is obtained.

[0096] A sensor using optical coherence tomography is also described. In one example, an optical coherence tomography (OCT) based sensor comprises a simple Michelson interferometer with a low temporal coherence source in one arm, a second reference arm, an object under study in the third arm and a registering element or spectrometer in the fourth arm. The source radiation is divided into the two arms and the backscattered light is interfered with the reference arm. A schematic drawing is shown in FIG. 13, indicating a radiation source 1310 in the present example being a superluminescent diode, a splitter 1320 splitting the radiation in one part directed to the sample through a focus point 1330 and a second part provided in a delay line 1340 in the present example being based on a loop mirror 1350. A combiner 1320 also typically is present (this may be the splitter) for combining the two parts of the radiation beam again whereby the radiation then is directed to a spectrometer 1360. Appropriate interferometric signals in an OCT system can be formed when the optical path length in the sample arm matches that in the reference arm within the coherence length of the source. The interference in OCT amplifies the backscattered signal and increases the sensitivity limit of the detection. In order to achieve a high resolution and depth range, a broadband radiation source, for example with a 100 nm bandwidth, may be used in combination with a high resolution spectrometer with a detector array of e.g. 1024 pixels. The bandwidth determines the axial resolution, and the imaging depth is either limited by attenuation of the medium or

spectrometer resolution of the system.

[0097] The sensor may consist of a group of sensors as described above. Alternatively or in addition thereto a sensor may comprise a plurality of detecting devices, e.g. a 1D or 2D array of detecting devices.

[0098] A sensor is also described adapted for performing spectrally resolved optical coherence tomography. The latter allows analyzing spectra of backscattered light a depth-resolved manner. SOCT is an extension of OCT imaging, analyzes not only the intensities, but also the spectra of backscattered light in a depth-resolved manner. This technique is capable of both qualitative contrast enhancement and quantitative concentration measurement. The system is based on a system as described above, whereby the interference spectrum is not fully combined in the processing, but whereby the interference spectrum is divided, prior to fourier transforming the spectrum, into several windows, each window being used to estimate the depth profile. The method implies a trade of between the axial resolution and obtaining wavelength dependent, depth resolved measurements. For some applications, depending on the volume distribution of the analyte, it may not be necessary to achieve very high spatial resolution, and few hundred microns axial resolution would be sufficient. Thus, sources with much smaller bandwidths can be used, or the spectrum can be analyzed by dividing it into smaller spectral windows. Windowing of the interference spectrum may be done using multiple demultiplexers, tunable filters, high resolution spectrometers, etc, some of these methods being discussed above. The latter may for example be used for imaging tissue using the scattering occurring when irradiating tissue. It therefore may provide a physiological imaging of the tissue.

[0099] In another particular embodiment, a sensor is described for absorption, scattering, reflection or transmission measurements, whereby a coupler in the optical processor may be used for extracting spatial information. The coupler may for example be a grating coupler. As the wavelength range coupled in is dependent on the angle of incidence of the radiation, from the detected spectrum an estimate of the incident angle of the radiation can be made, whereby the latter can be coupled to the origin or the optical path length that has been travelled in the tissue. Optimisation of the coupler, e.g. grating coupler may be performed using numerical simulation.

[0100] In still another embodiment, a sensor is provided with a spatially resolved spectroscopic setup. The object is illuminated at one position and the reflectance and/or backscattering is measured at different distances from the source. The signals captured and representative for different depths of the sample are detected by different detecting elements, resulting in a spatially resolved image.

[0101] The sensor may be powered in any suitable way, such as for example via a battery which could for example be powered inductively. Energy and power provision, control and use may be based on energy harvesting, e.g. energy scavenging. Furthermore data transmission from and to but also within the sensor may be performed in a wired or more preferably a

wireless manner.

[0102] In one aspect of the present invention, a continuous monitor - also referred to as continuous monitoring system - is described. Such a continuous monitor comprises a sensor as described in the first aspect. The continuous monitoring system may be a continuous glucose monitoring system. The sensor may comprise the same features and advantages as set out in the first aspect. The continuous glucose monitor may also include power electronics and data-transmission electronics for powering the device and for outputting data. These components may preferably be incorporated in the sensor, although the invention is not limited thereto. The power electronics may be inductive power electronics such that the sensor can be easily powered, without the need for surgical intervention or electrical contacts in mechanical contact with the sensor and present on the body. The data transmission electronics may be adapted for corresponding in a wireless manner with an external device. Such data may for example involve absorption or scattering data obtained with the sensor, timing data, data for reporting functionality of the sensor, etc. An example of a continuous glucose monitoring system is shown in FIG. 14 and 15. The present invention not being limited thereto. FIG. 14 illustrates a biocompatible packaged single-chip optical spectrometric sensor 1420, together with inductive power and wireless data-transmission electronics being implanted, e.g. subcutaneously in the upper arm. The sensor according to the present example is fed by and communicated with an external, wearable or portable read-out device 1410. In one example, the sensor may be coupled with an automatic insulin infusion system to enable a "closed loop" control, i.e. using an artificial pancreas system. The sensor may detect absorption or scattering in a measurement region close to the sensor, whereby no particular inlet or outlet is required. The latter may be advantageous, as the absence of inlet and outlet ports may result in better passage and reduced obstruction of the flow of the sample. FIG. 15 illustrate an overview for an implanted biosensor, indicating a handheld readout device wirelessly connected to 3D integrated chip package, enclosed in a biocompatible package, the package also comprising the coil antenna for power and signal transfer, an optical mirror for reflecting the optical signal in the current exemplary measurement setup and a measurement region comprising absorbing tissue or fluid. The diameter of the package typically may be in the range of 1 to 1.5cm, although embodiments of the present invention are not limited thereto. A more detailed picture of the 3-D integrated chip package also is shown, indicating an infrared light source, a coupler grating, a spectrometer portion, a SOI photonic chip and an electronics chip for driving and controlling. An example of a chip size may be in the range 2mm x 0.5mm, although embodiments of the present invention are not limited thereto.

[0103] In one aspect, the present invention also relates to the use of a sensor as described above or a continuous monitoring system as described above for sensing a substance, e.g. glucose in the body of a living creature. It is an advantage of such use that results can be obtained in a rapid and accurate manner, and in an automated and/or automatic way such that monitoring of the glucoses level can be done more appropriately.

[0104] Fabrication of the spectrometric sensor by e-beam or a photolithographic process, using CMOS technology, using silicon technology, and semiconductor etching steps and back-

end process steps like flip-chipping, bonding, metallisation are well described in literature and state-of-the-art technology. Processing of the dispersive sensor components, such as for example of the photonics integrated circuit, the detecting element, gratings, waveguides, the at least one radiation source, and/or the memory may thus be based on conventionally known techniques, although also more complex processing techniques described in literature may be applied.

[0105] Also the wireless unit is based on state-of-the-art technology. There are a lot of wireless communication standards like Zigbee, Bluetooth, Wibree, UWB etc. available on the market. Most of them are low power solutions and available in a small form factor. Depending on the application, e.g. read-out scanning rate, a power range and databit range, a communication protocol can be selected. A driver chip implementing the communication protocol will be connected to the spectroscopic chip or integrated to a single chip, e.g. via 3D packaging or the communication electronics might be homogeneously integrated with the photonics on a single chip in case of silicon photonics. Fabrication of electronic chips is well known to the skilled person.

[0106] Wireless power transmission based on inductive coupled coils might power the system. Wireless power transmission in the lower frequency band is well known with RFID applications. Depending on the application and related read-out scan rate, the power needed for the photonic sensor system might be much more than current RFID Transponder require, e.g. a power of 300mW-3W. Custom developed inductively coupled coils might be integrated, Alternatively, a miniature battery might be used. Today commercially available small batteries might have a lifetime spanning several months to years, depending on their use. In general any suitable powering method known to the skilled person for powering an implantable sensor can be selected.

[0107] The single-chip optical spectrometric sensor, together with power unit and wireless data-transmission electronics are packaged by e.g. moulding these components in a e.g. PDMS or PMMA based biocompatible package. The fabrication of PDMS or PMMA based material and the moulding of are well described in literature and state-of-the-art technology.

[0108] After production of the packaged sensor, including spectrometric sensor, power unit and wireless unit, the packaged sensor is implanted in the body under test.

[0109] In some embodiments of the present invention, a sensor and corresponding monitoring system is provided as described above, implanted in non-living objects, The sensor may for example be used in connection with a bioreactor to monitor levels of substances, e.g. nutrients and/or cellular waste products to maximize growth. It can also be used to monitor industrial chemical processes and/or environmental processes.

[0110] While the invention has been illustrated and described in detail in the drawings and foregoing description, such illustration and description are to be considered illustrative or exemplary and not restrictive. The invention is not limited to the disclosed embodiments. For

example, the present invention also relates to a corresponding method whereby radiation is received in the sensor and spectrally processed using a photonics integrated circuit based radiation processor. The method may comprise further method steps expressing the functionality of the different components described for the sensor above. The result of such a method may be a qualification of the presence or a quantification of the presence of a substance. The detection results do not necessarily include an evaluation of such detection results the method therefore not necessarily being a diagnostic method.

[0111] Other variations to the disclosed embodiments can be understood and effected by those skilled in the art in practicing the claimed invention, from a study of the drawings, the disclosure and the appended claims. In the claims, the word "comprising" does not exclude other elements or steps, and the indefinite article "a" or "an" does not exclude a plurality. A single processor or other unit may fulfil the functions of several items recited in the claims. The mere fact that certain measures are recited in mutually different dependent claims does not indicate that a combination of these measures cannot be used to advantage.

[0112] The algorithms implemented in the sensor may be implemented as software or as hardware. The algorithm may be implemented as a computer program performing control steps for controlling the sensor. Such a computer program may be stored/distributed on a suitable medium, such as an optical storage medium or a solid-state medium supplied together with or as part of other hardware, but may also be distributed in other forms, such as via the Internet or other wired or wireless telecommunication systems. Any reference signs in the claims should not be construed as limiting the scope.

[0113] The foregoing description details certain embodiments of the invention. It will be appreciated, however, that no matter how detailed the foregoing appears in text, the invention may be practiced in many ways, and is therefore not limited to the embodiments disclosed. It should be noted that the use of particular terminology when describing certain features or aspects of the invention should not be taken to imply that the terminology is being re-defined herein to be restricted to include any specific characteristics of the features or aspects of the invention with which that terminology is associated.

REFERENCES CITED IN THE DESCRIPTION

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- [US5833603A](#) [0007]
- [US20080186483A](#) [0007]
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- [US20040162470A](#) [0009]
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- LUO et al.Sensors and Actuators, 2003, vol. 92, 121-126 [0008]
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Implanterbar sensor**Patentkrav**

1. Sensor (100), der er tilpasset til registrering af glukose, urinstof eller laktat, hvor sensoren er konfigureret til at blive implanteret i kroppen af et levende væsen eller en genstand og er konfigureret til at registrere i væv eller kropsvæsker, idet sensoren omfatter
 - en strålekilde (130), der er konfigureret til at bestråle vævet eller kropsvæskerne i et måleområde (140), en integreret strålingsprocessor (110) og et integreret registrerings-element, (120) hvor integreret angiver monolitisk integration ved anvendelse af en enkelt processtrøm, heterogen integration, hvor komponenter behandles i separate processtrømme, men som er integreret på matrice- eller wafer-niveau, eller hybrid integration af komponenter eller materialer på behandlede integrerede fotoniske platforme, idet sensoren (100) yderligere omfatter måleområdet (140), hvorfra den stråling, der interagerer med glukose, urinstof eller laktat, fanges, kendetegnet ved, at
 - den integrerede stråleprocessor (110) er integreret i et integreret silicium-fotonik-kredsløb og konfigureret til spektral behandlingsstråling, der interagerer med glukose eller urinstof eller laktat, hvor stråleprocessoren i det mindste omfatter en integreret lysbølgeleder, en multiplexer og/eller de-multiplexer, der er tilpasset til at opnå spektralt opløste data fra den spektralbehandlede stråling, og
 - det integrerede registreringselement (120) er integreret i det integrerede silicium-fotonik-kredsløb og er konfigureret til at registrere den stråling, der behandles af stråleprocessoren, hvor stråleprocessoren og registreringselementet danner et integreret spektrometer i silicium-fotonik-kredsløbet og er konfigureret til at udføre spektrale absorptionsmålinger til registrering af spektrale absorptionsbånd af glukose, urinstof eller laktat til udførelse af en kvantificering af glukose, urinstof eller laktat, der er baseret derpå, og stråleprocessoren og måleområdet er konfigureret til at tillade frie spektralabsorptionsmålinger til substansprøvetagning, så der kan udføres registrering uden at skulle ekstrahere en prøve eller lede et interessant stof til måleområdet på en tvungen måde.

2. Sensor, der er tilpasset til registrering af et stof ifølge krav 1, hvor strålekilden er integreret i det integrerede silicium-fotonik-kredsløb.
3. Sensor ifølge et hvilket som helst af kravene 1 til 2, hvor stråleprocessoren og måleområdet er tilpasset i størrelse for at muliggøre tidsafhængige stofmålinger baseret på spontan forskydning af stoffet i kroppen.
4. Sensor ifølge et hvilket som helst af kravene 1 til 3, hvor måleområdet er et åbent måleområde, så det ikke i det væsentlige er omsluttet af sensorvægge.
5. Sensor ifølge et hvilket som helst af de foregående krav, hvor den integrerede sensor med fotonisk kredsløb er tilpasset til at fungere i mindst et bølgelængdeområde mellem 1560 nm og 1850 nm og/eller er tilpasset til at fungere i mindst et bølgelængdeområde mellem 2080 nm og 2325 nm.
6. Sensor ifølge et hvilket som helst af de foregående krav, hvor sensorkonfigurationen er tilpasset til at opnå dybderelaterede data om prøven.
7. Sensor ifølge krav 6, hvor sensorkonfigurationen er konfigureret til rumligt opløst registrering og til udledning af de dybderelaterede data om prøven, der er baseret derpå.
8. Sensor ifølge et hvilket som helst af de foregående krav, hvor stråleprocessoren omfatter en flerhed af kaskadebølgelængdemultiplexere, omfatter en flerhed af indstillelige filtre, bruger frekvens- eller tidsdomænemultiplexering eller bruger en noniusforskudt spektralrespons for at øge et antal kanaler til spektral strålebehandling.
9. Kontinuerligt overvågningssystem, der omfatter: en implanterbar sensor (1420) ifølge et hvilket som helst af kravene 1 til 8, der er tilpasset til registrering af et stof og omfatter trådløs datatransmissionselektronik og et udlæsningssystem (1410), der er konfigureret til trådløs modtagelse af data, som er registreret af sensoren.

DRAWINGS

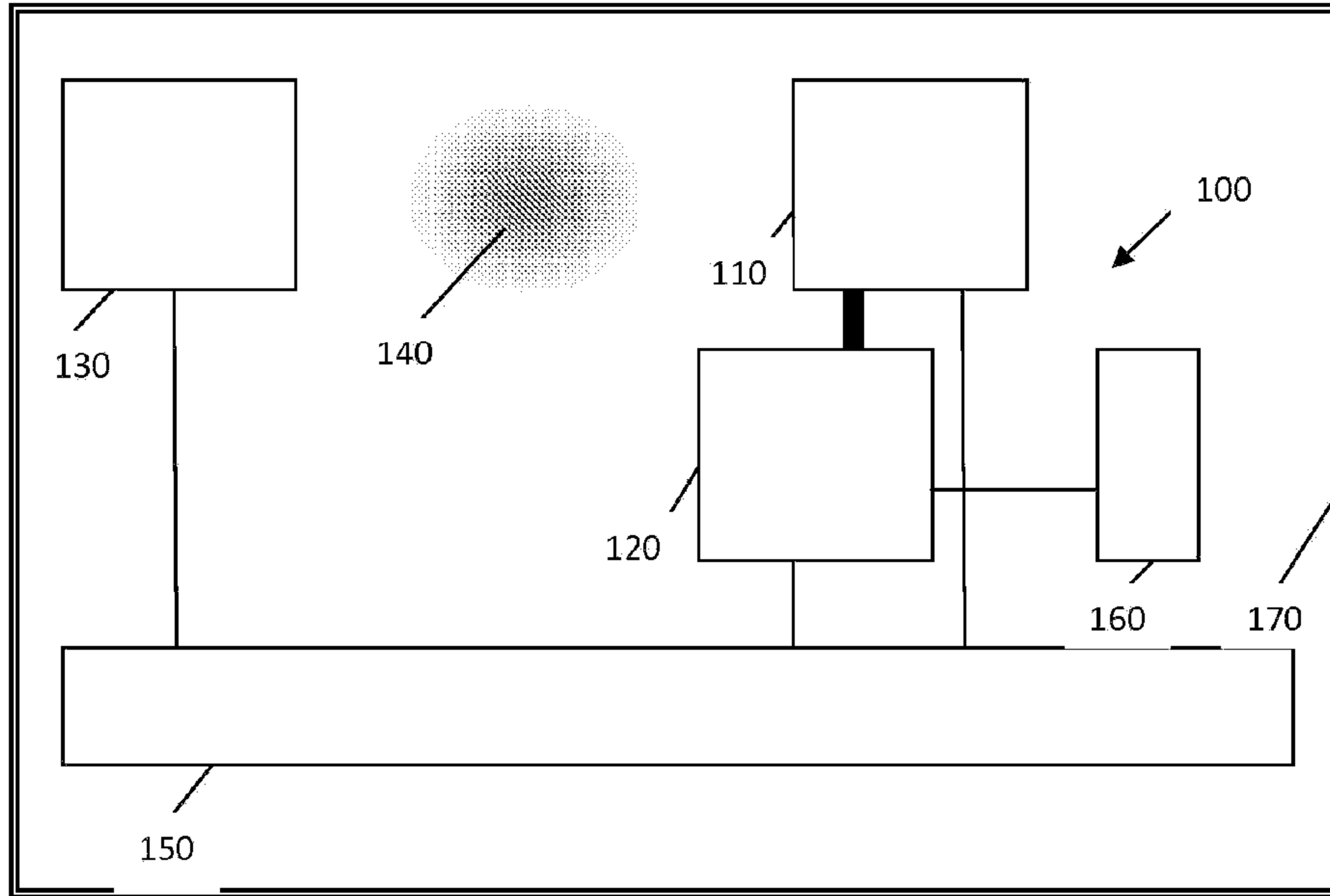


FIG. 1

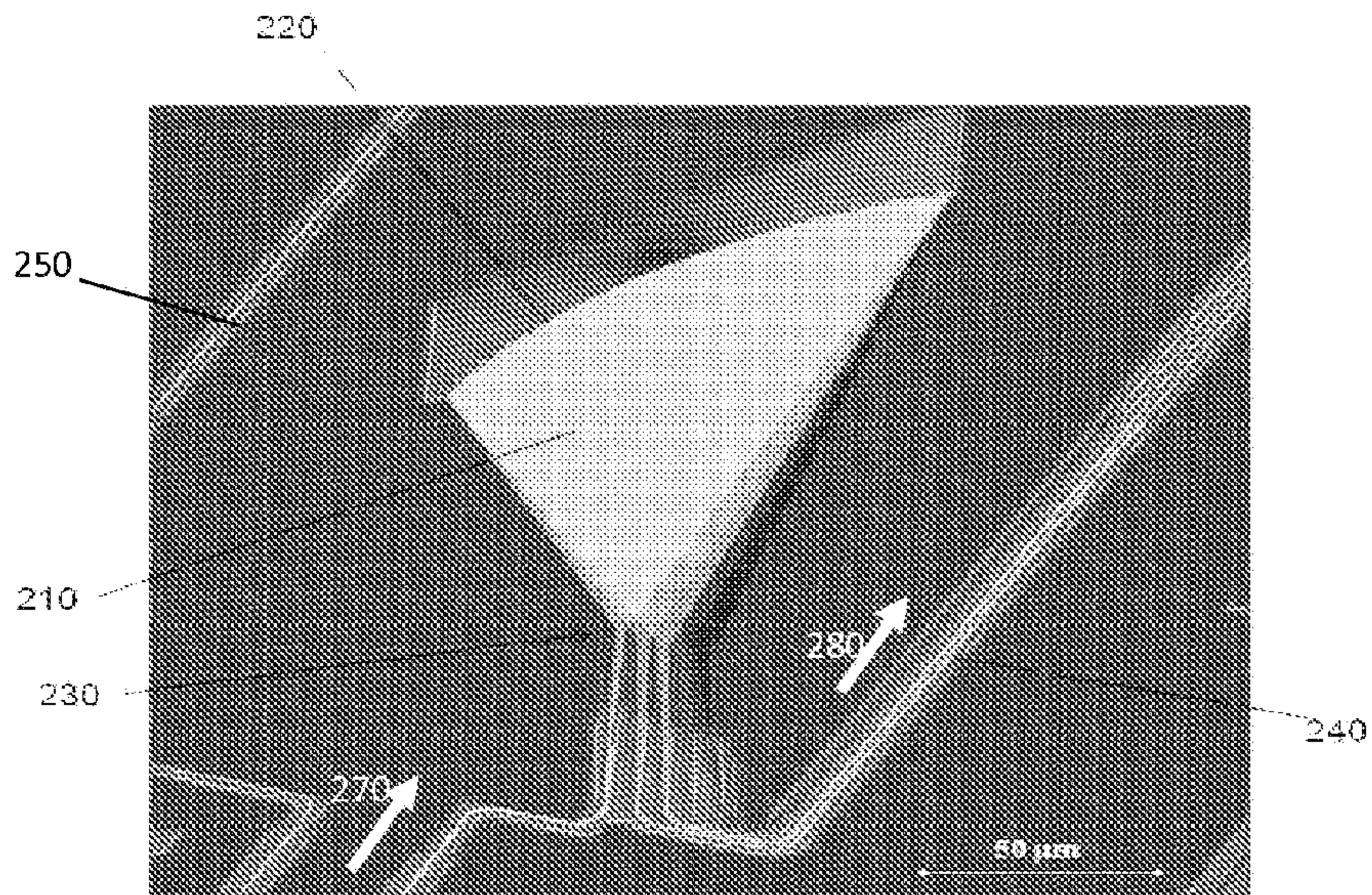


FIG. 2A

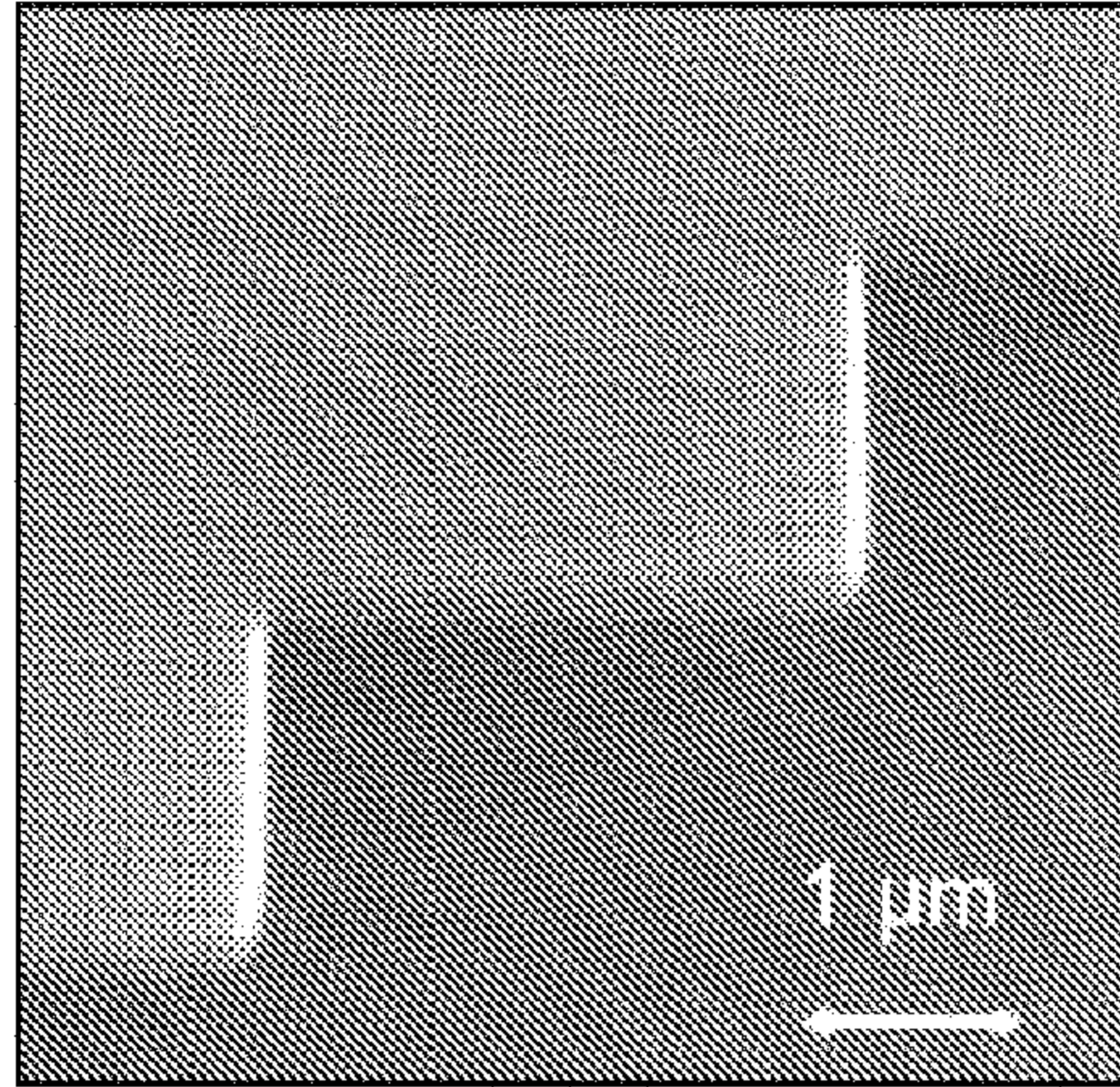


FIG. 2B

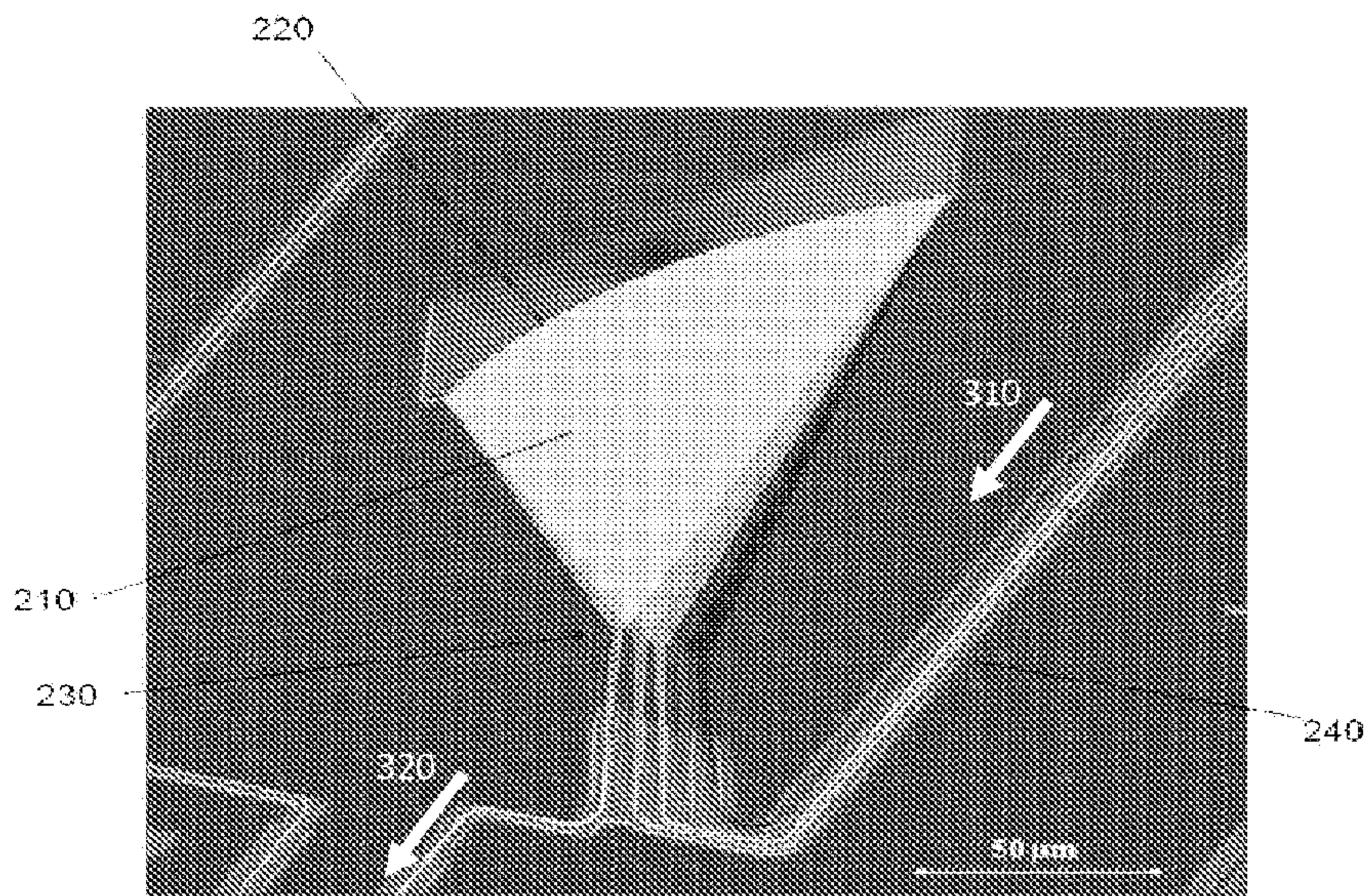


FIG. 3

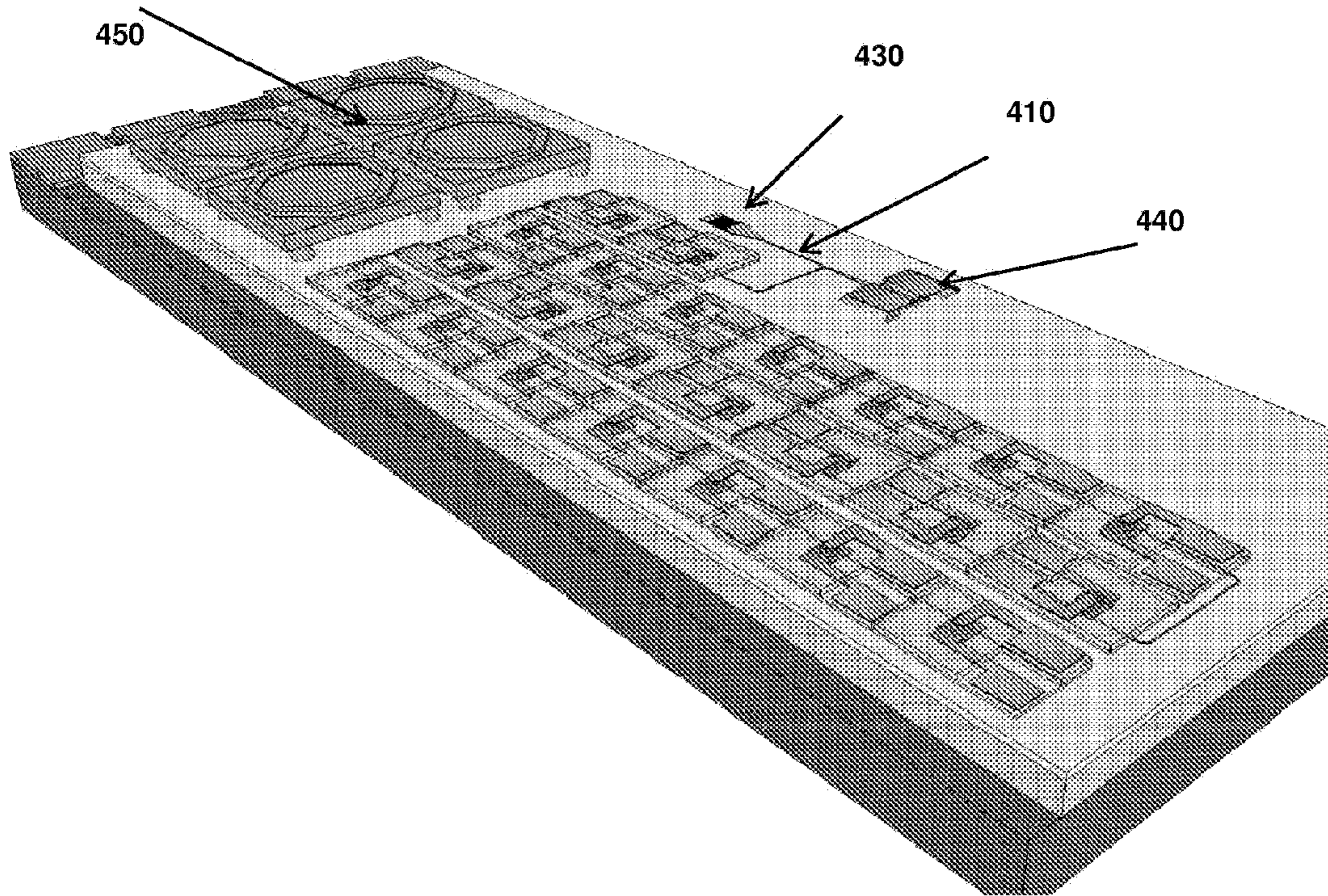


FIG. 4

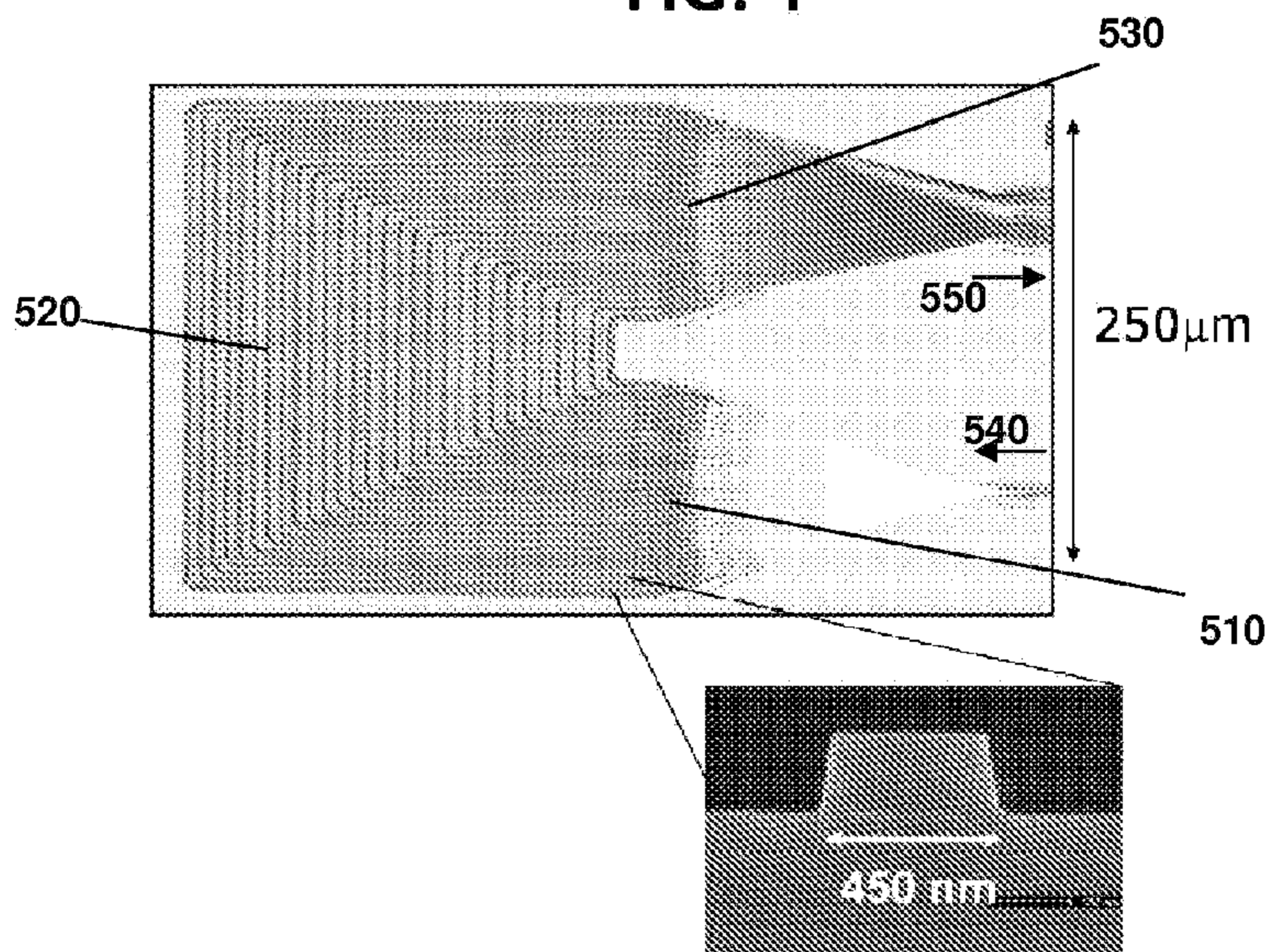


FIG. 5

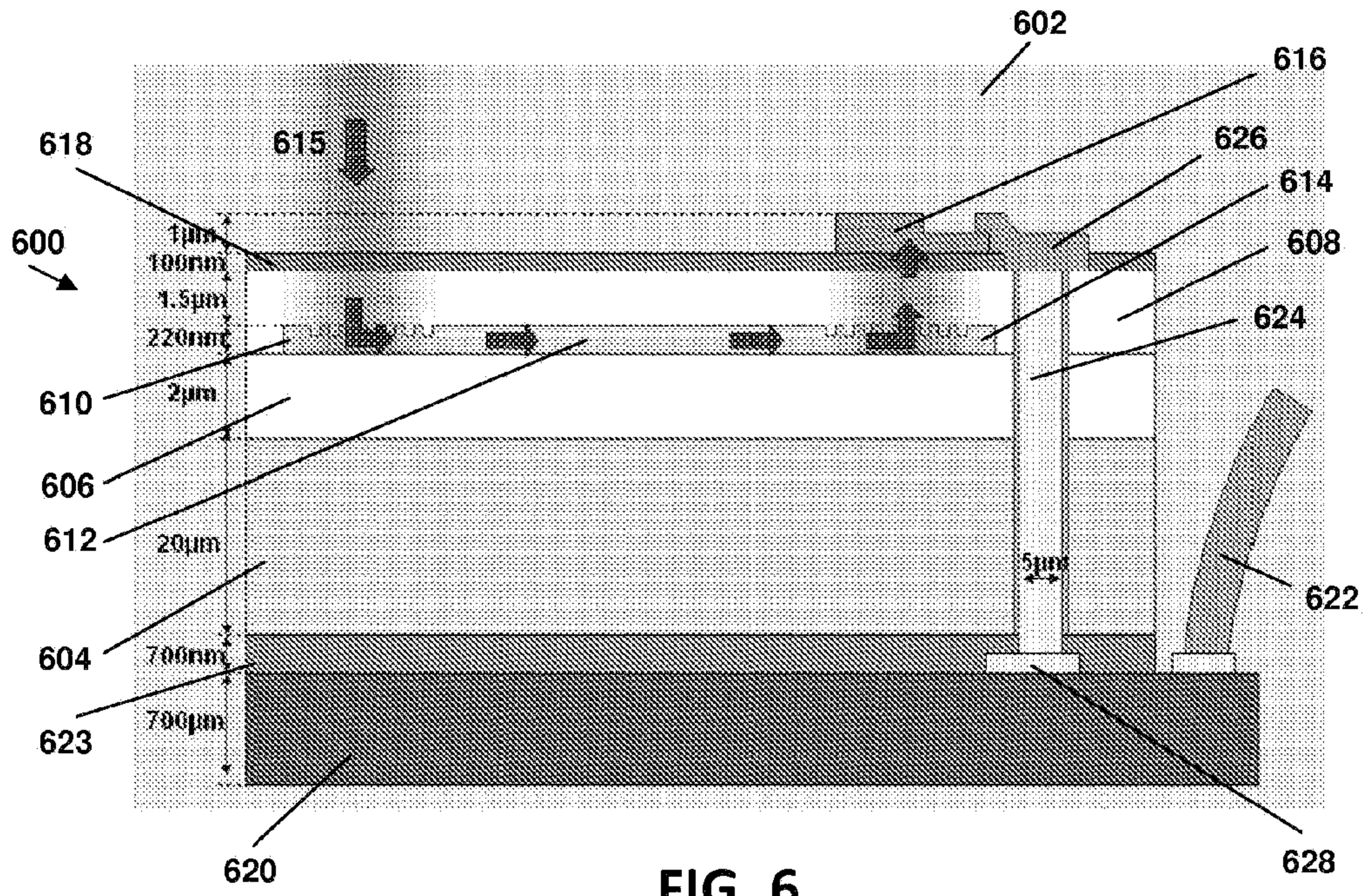


FIG. 6

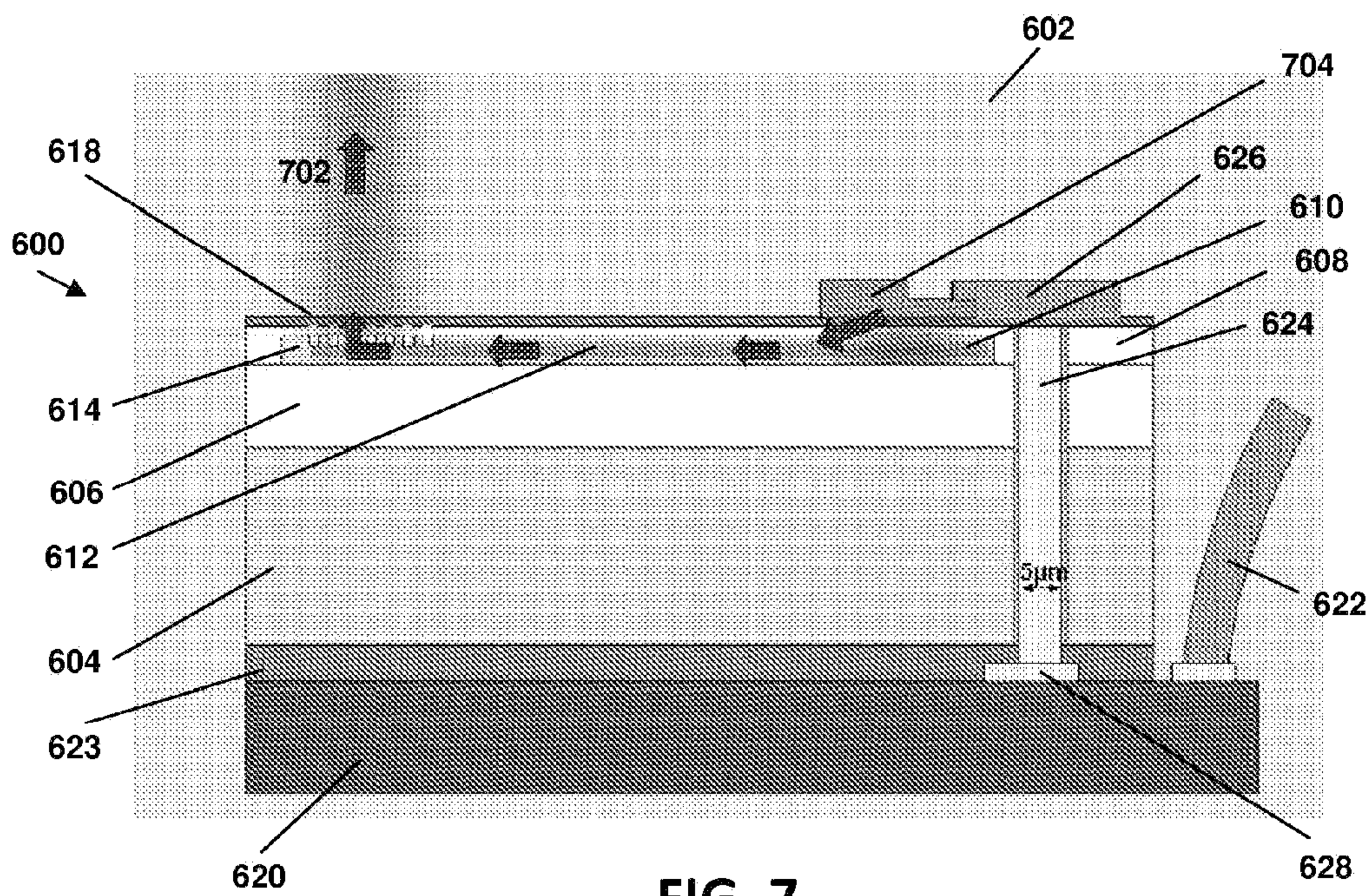


FIG. 7

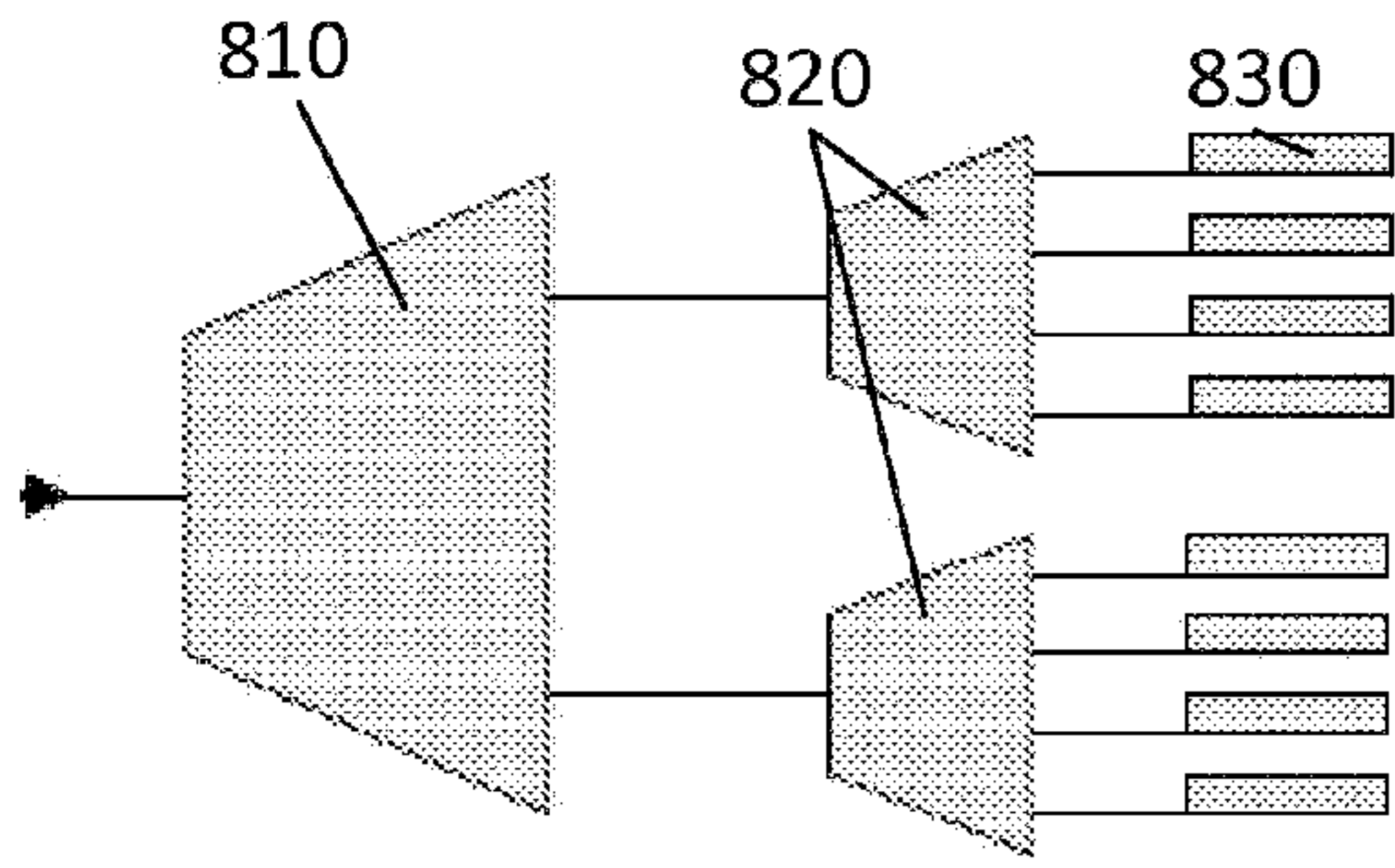


FIG. 8

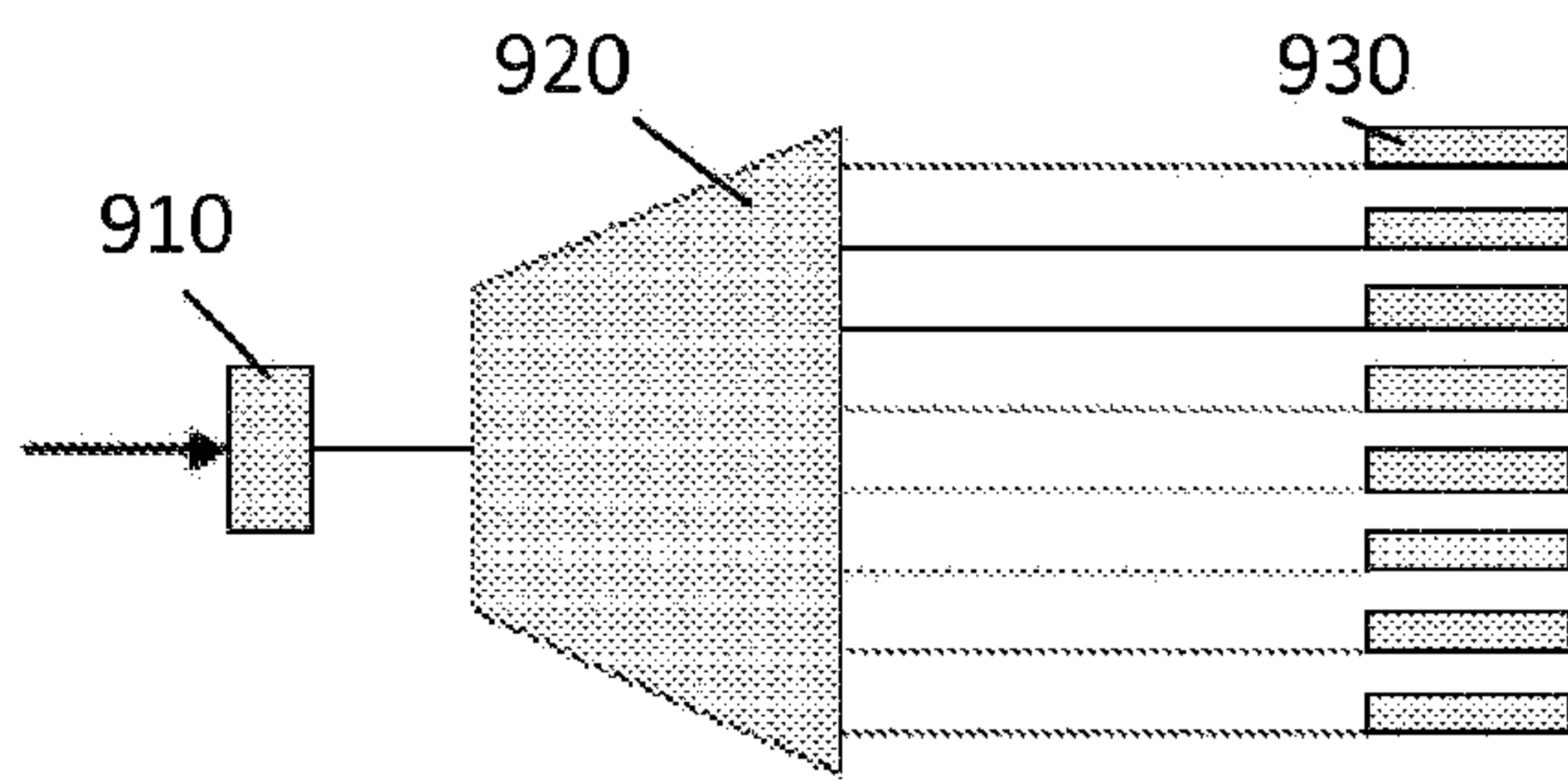


FIG. 9

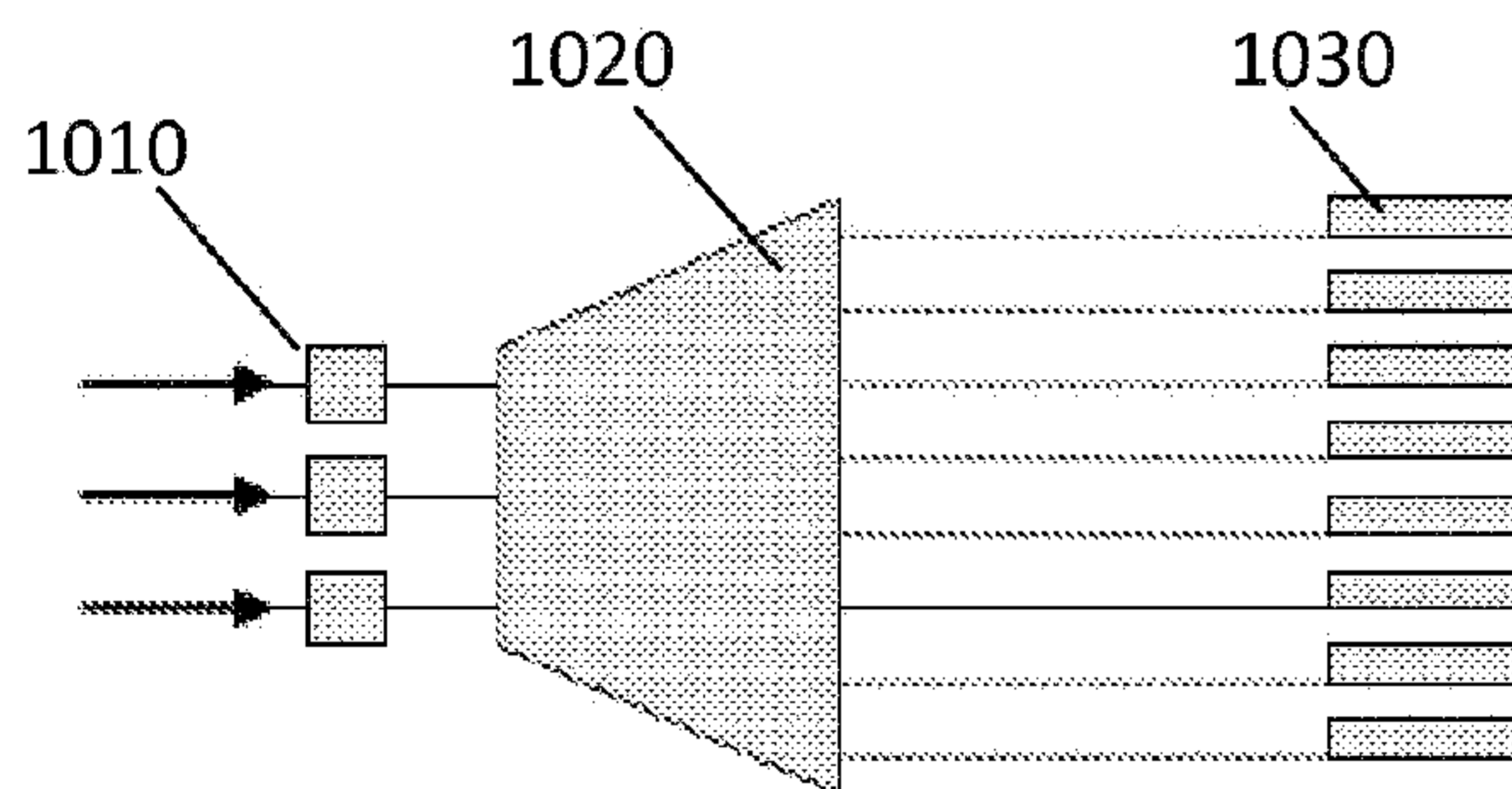


FIG. 10

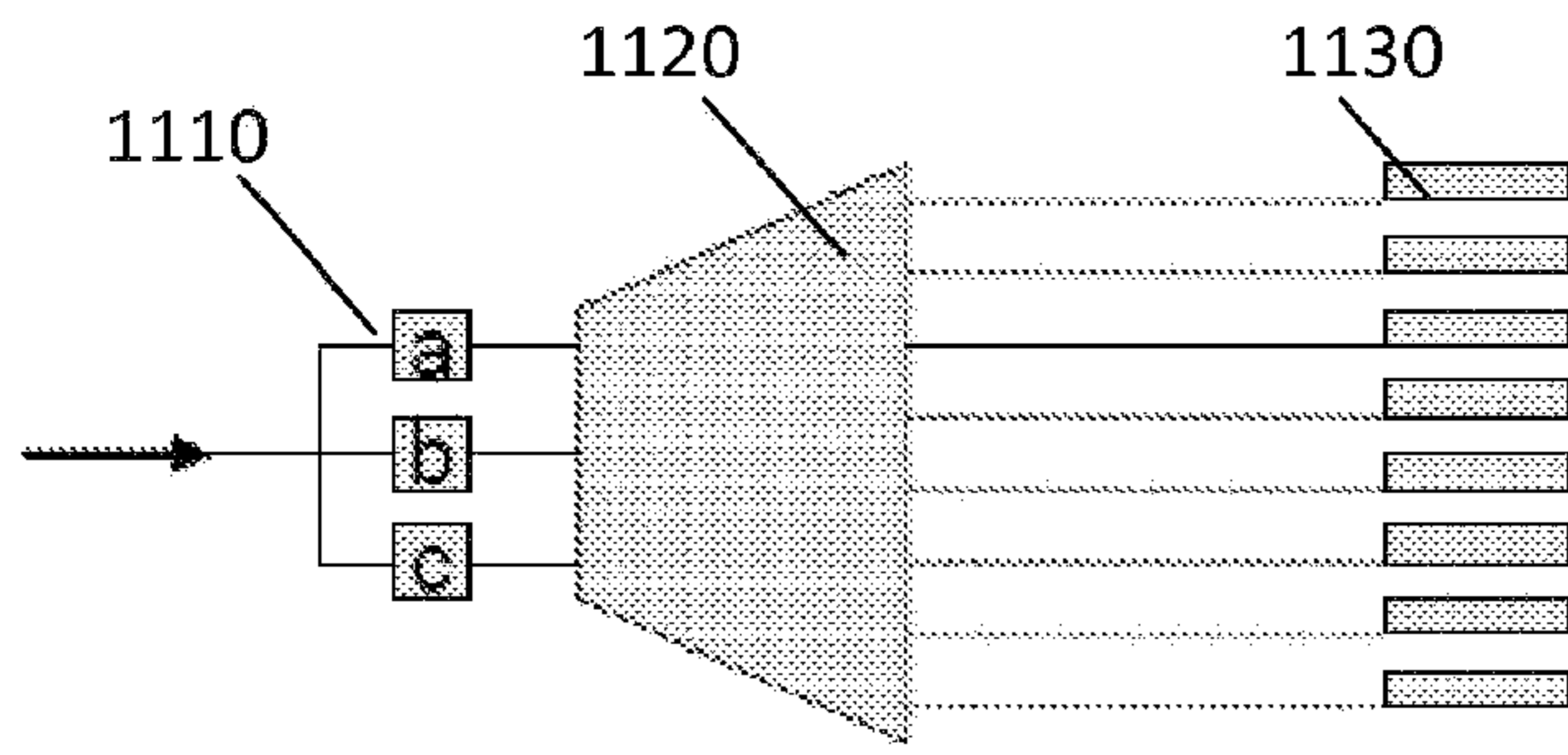


FIG. 11

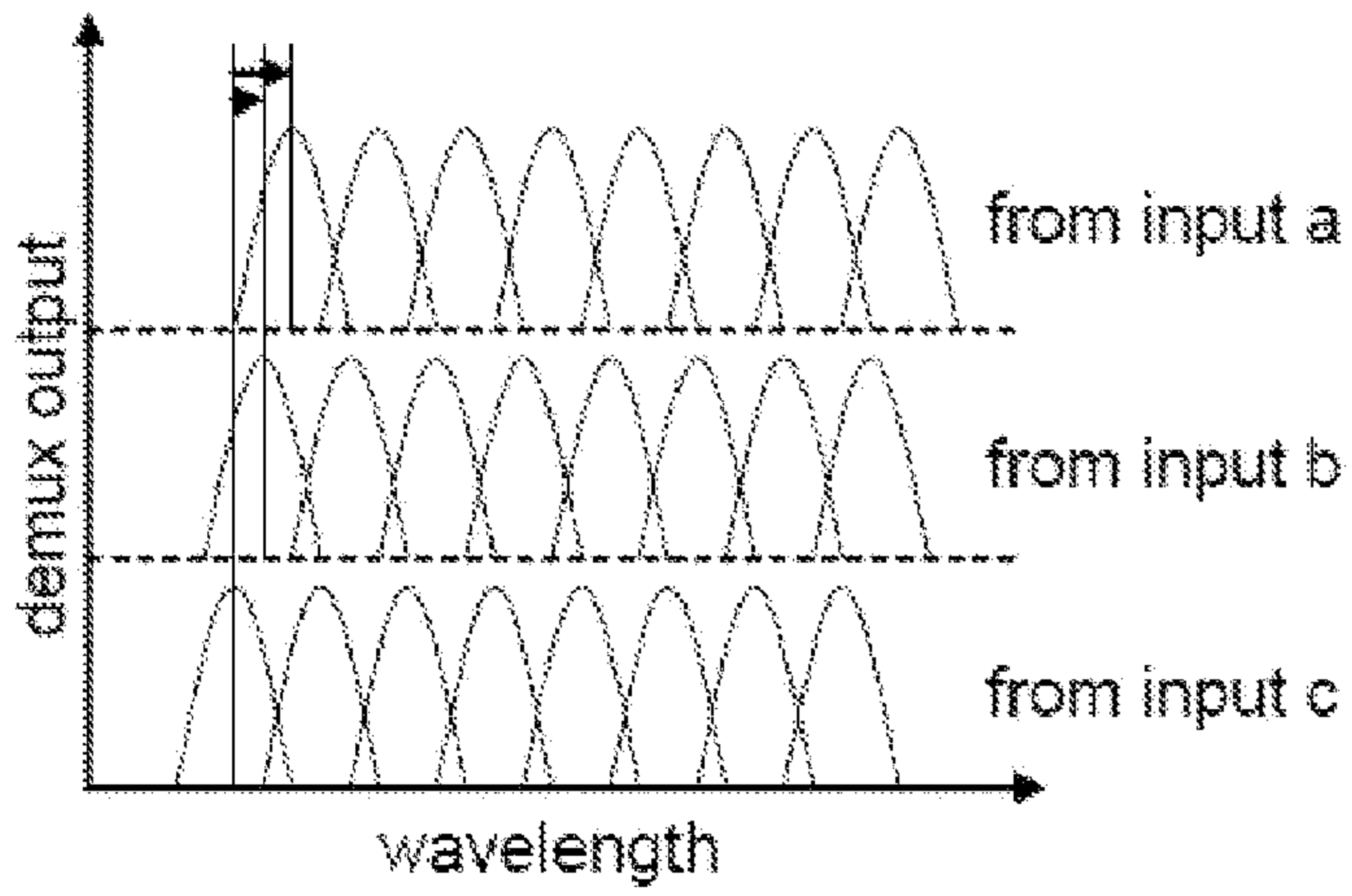


FIG. 12

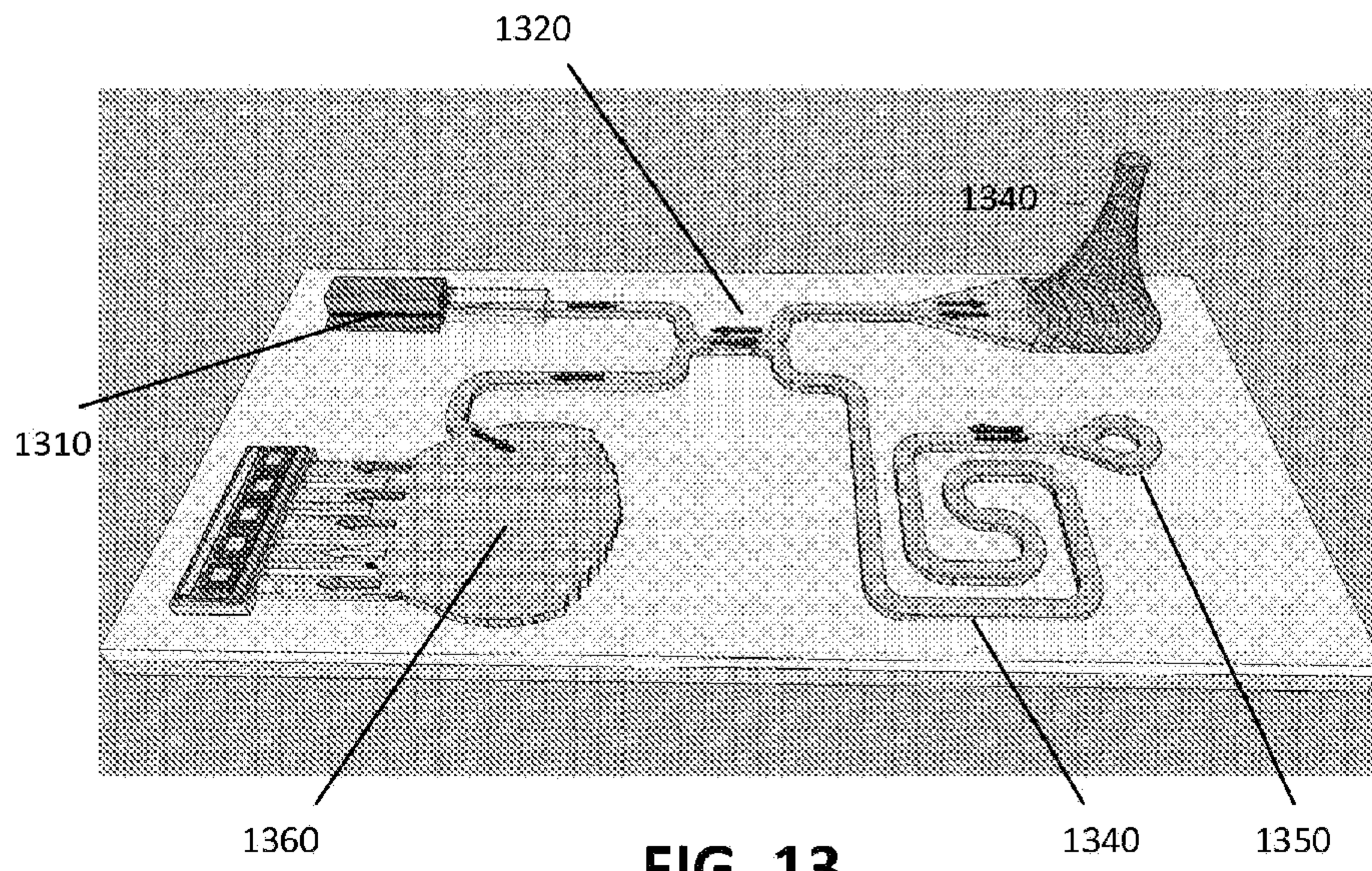


FIG. 13

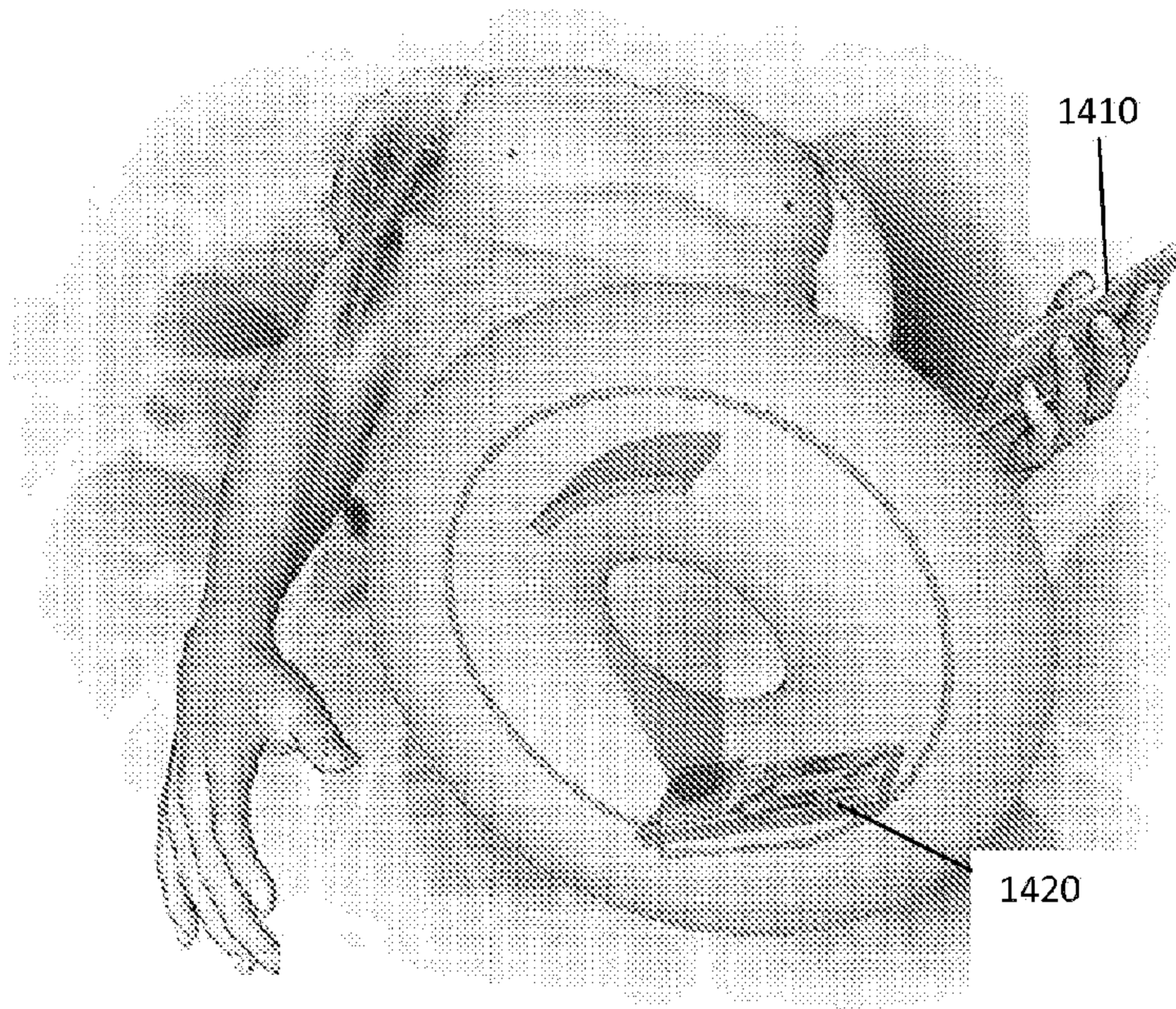


FIG. 14

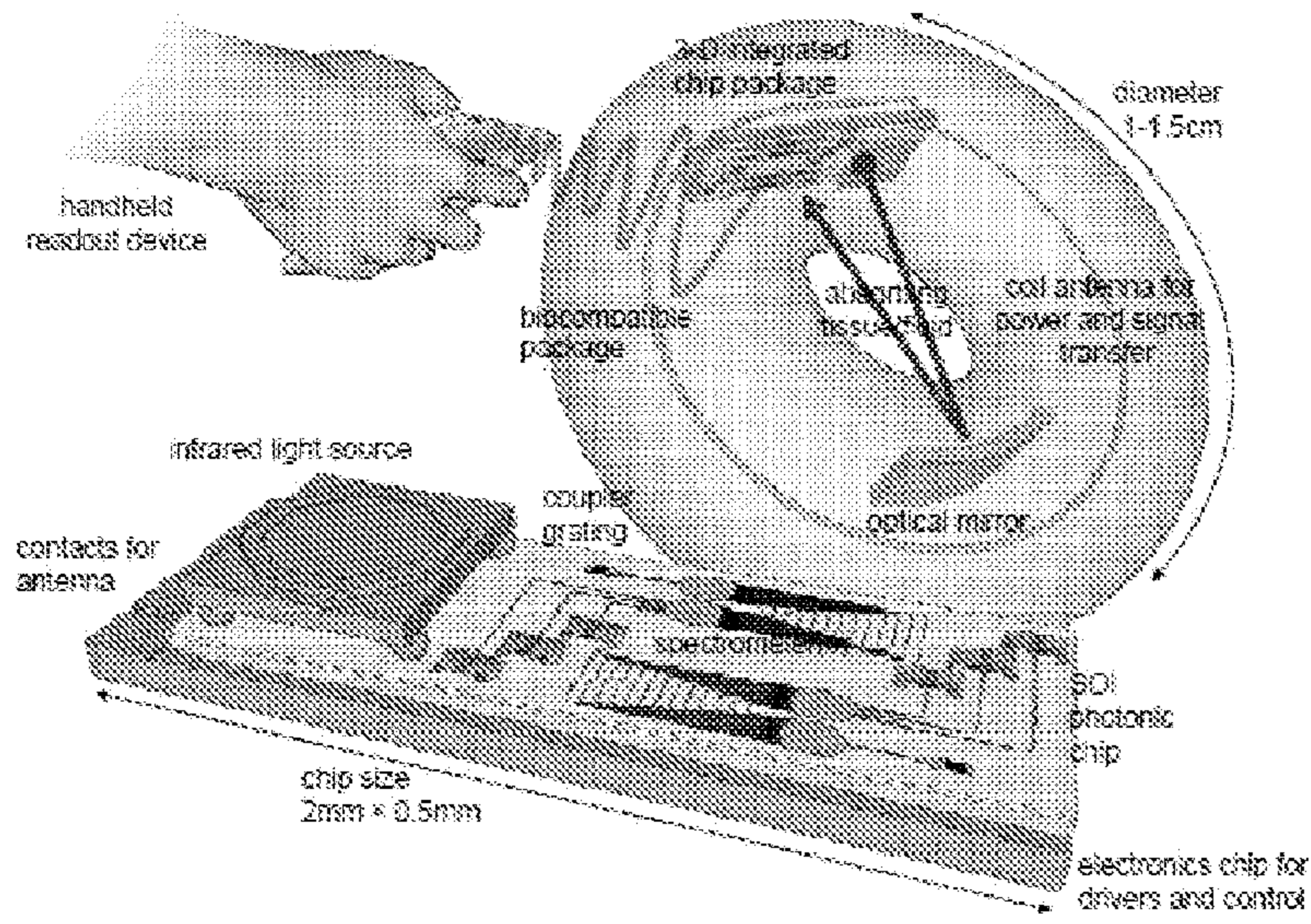


FIG. 15