(19) World Intellectual Property Organization

International Bureau



T TERRE BURNER IN BERNE HERE BERNE BERNE BERNE HER FIN BERNE BURNER BERNE BERNE BERNE BERNE BERNE BERNE BERNE

(43) International Publication Date 9 December 2004 (09.12.2004)

PCT

(10) International Publication Number WO 2004/105850 A1

(51) International Patent Classification⁷:

A61M 25/00

(21) International Application Number:

PCT/US2004/016595

(22) International Filing Date:

25 May 2004 (25.05.2004)

(25) Filing Language:

English

(26) Publication Language:

English

(30) Priority Data:

60/473,683

28 May 2003 (28.05.2003) US

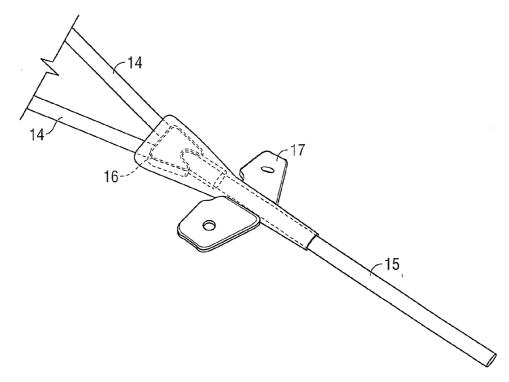
- (71) Applicant (for all designated States except US): C.R. BARD, INC. [US/US]; 730 Central Avenue, Murray Hill, NJ 07974 (US).
- (72) Inventors: KING, Eric; 3001 Chimney Rock Circle, West Jordan, UT 84084 (US). WORTLEY, Ron; 2680 Roxbury

Circle, Salt Lake City, UT 84108 (US). **DIAMOND, Jordan, P.**; 2552 South, 1300 East, Salt Lake City, UT 84106 (US).

- (74) Agents: WIGHT, Todd, W. et al.; Morrison & Foerster LLP, 555 W. Fifth Street, Suite 3500, Los Angeles, CA 90013 (US).
- (81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NA, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.
- (84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH,

[Continued on next page]

(54) Title: HIGH PRESSURE CATHETER AND METHODS FOR MANUFACTURING THE SAME



(57) **Abstract:** A catheter for high pressure applications may contain a rigid inner hub, forming a high pressure connection between a fluid path of a catheter shaft and extension tube assembly. The catheter may also contain a soft pliable outer hub with flexible suture wings positioned over the rigid inner hub. When used clinically, the catheter may function as both a standard catheter and a high-pressure catheter.

WO 2004/105850 A1



GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Published:

— with international search report

 before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments

For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

1

HIGH PRESSURE CATHETER AND METHODS FOR MANUFACTURING THE SAME

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] This application claims the benefit of United States provisional application Serial No. 60/473,683, filed May 28, 2003, which is expressly incorporated by reference as if fully set forth herein.

STATEMENT REGARDING FEDERALLY SPONSORED RESEARCH OR DEVELOPMENT

[0002] Not applicable.

5

10

15

20

25

REFERENCE TO A COMPACT DISK APPENDIX

[0003] Not applicable.

FIELD OF THE INVENTION

[0004] The invention generally relates to medical devices and methods for manufacturing such medical devices. In particular, the invention relates to catheters, methods for making such catheters, and methods for using such catheters. More particularly, the invention relates to power injection catheters, methods for manufacturing such catheters to address the high-pressure requirements and applications, and methods for using such catheters for high-pressure vascular access.

BACKGROUND OF THE INVENTION

Catheters and their use as medical devices are well known in the art. Some medical procedures, such as CT Scans, typically require rapid infusion of contrast media into the vascular system. These types of procedures are currently accomplished by accessing the vascular system with a needle and cannula that is connected to a power injection machine. The injection pressure of the machine is set to a clinically predetermined limit that is relatively high. When activated, the machine rapidly injects the media into the vascular system of the patient at a flow rate that will not exceed the predetermined pressure limit. The wide variation in the viscosity of different contrast media or medications, coupled with rapid flow rate requirements, can often result in a wide range of pressures.

2

A large number of patients that require the procedure described above already have a typical implanted catheter that is being used for other medical procedures. Typical catheter designs usually contain three major components: (1) the catheter shaft, (2) an extension tube assembly, and (3) a bifurcation in the case of multi lumen catheters or a hub in the case of a single lumen catheter. As used herein, the term "catheter" may refer to a device comprising each of said three major components. The catheter shaft is the portion of the catheter that is inserted into the vascular system. The extension tube assembly is the portion of the catheter that provides vascular access from outside of the body. The bifurcation or hub is the portion of the catheter that connects to the proximal end of the catheter shaft, connecting the catheter shaft to the extension tube assembly. The bifurcation or hub usually contains geometry required to secure the catheter to the body such as suture wings. The bifurcation or hub also provides a location to print instructions or logos on the catheter surface.

10

15

20

25

30

[0007] Typical catheters are usually designed and manufactured with flexible materials that are compliant. Using flexible materials increases patient comfort, especially when securing the catheter to the body, and also reduces trauma to the vascular system. As well, the catheter shaft and extension tube assembly are typically made of thin walled tubing. The strength of the tubing, especially for high pressure applications, can be increased (within certain limits) by increasing the durometer of the raw materials while retaining most of the flexibility and comfort of the assembly. Such an increase in strength by increasing the durometer of the raw material, however, is not possible with respect to the bifurcation and hub due to the relatively thicker geometry thereof. More particularly, due to the thicker geometry, any increase in the durometer of the raw material would greatly increase the stiffness of the bifurcation and hub, which increased stiffness would negatively affect patient comfort and the ability to attach the bifurcation and hub to the patient's body.

[0008] Thus, improving the pressure resistance of a typical catheter assembly, such as a venous access catheter assembly that can usually only withstand pressures of up to approximately 150 psi, has proved difficult due to the inability to provide a bifurcation and hub having a pressure resistance that matches that of the tubing. Accordingly, typical catheters do not exhibit the properties that are needed for the

3

high-pressure (i.e., power injection) medical procedures described above, meaning that the patient must undergo more invasive procedures, such as repeated vascular access (i.e., needle sticks).

BRIEF SUMMARY OF THE INVENTION

5

10

15

20

25

[0009] The present invention provides high pressure catheters, methods for manufacturing such catheters to address high-pressure requirements and applications, and methods for using such catheters for high-pressure vascular access. The high pressure catheters can be produced by maintaining the typical soft flexible exterior in the bifurcation, hub, and/or suture wings, while providing a more rigid high-pressure connection interior. The stiffer internal geometry transforms the typical catheter into a high-pressure catheter and allows a single implanted catheter to perform both standard and high-pressure functions, thereby reducing the number of vascular access procedures required during a course of therapy.

[0010] In one embodiment of the present invention a catheter comprises a catheter shaft, an extension tube assembly, an inner hub comprising a rigid hard material, connecting said catheter shaft to said extension tube assembly, wherein said catheter shaft is in fluid communication with said extension tube assembly, and an outer hub comprising a soft flexible material positioned around said inner hub.

[0011] In another embodiment of the present invention, a method for making a catheter comprising a catheter shaft and an extension tube assembly, comprises the steps of placing said catheter shaft and said extension tube assembly into a first mold, wherein a proximal end of said catheter shaft is positioned adjacent a distal end of said extension tube assembly within a first mold cavity, insert molding an inner hub comprising a rigid hard material over said proximal end of said catheter shaft and said distal end of said extension tube assembly, placing the combination of said inner hub, catheter shaft and extension tube assembly into a second mold, wherein said inner hub is placed within a second mold cavity, said inner hub being supported and centered therewithin, and insert molding an outer hub comprising a soft flexible material over said inner hub.

[0012] In yet another embodiment of the present invention, a method for making a catheter comprising a catheter shaft and an extension tube assembly, wherein said catheter shaft and said extension tube assembly each comprise a single lumen, comprises the steps of inserting a portion of an inner hub having a throughgoing lumen into a proximal end of said catheter shaft lumen and a distal end of said extension tube assembly lumen such that said inner hub is substantially contained within said catheter shaft and said extension tube assembly, wherein said catheter shaft is in fluid communication with said extension tube assembly, placing the combination of said inner hub, catheter shaft and extension tube assembly into a mold, wherein said inner hub is positioned within a mold cavity, and insert molding an outer hub comprising a soft flexible material over said catheter shaft and extension tube assembly.

10

15

20

25

[0013] These and other embodiments, features and advantages of the present invention will become more apparent to those skilled in the art when taken with reference to the following more detailed description of the invention in conjunction with the accompanying drawings that are first briefly described.

BRIEF DESCRIPTION OF THE DRAWINGS

- [0014] FIG. 1 is a side perspective view of a rigid single lumen inner hub, insert molded over a catheter shaft and extension tube assembly, according to one aspect of the present invention.
- [0015] FIG. 2 is a side perspective view of a soft flexible single lumen outer hub, insert molded over the rigid inner hub of FIG. 1;
- [0016] FIG. 3 is a side perspective view of a rigid dual lumen inner hub, insert molded over a catheter shaft and extension tube assembly, according to one aspect of the present invention.
- [0017] FIG. 4 is a side perspective view of a soft flexible dual lumen outer hub, insert molded over the rigid inner hub of FIG. 3.
- [0018] FIG. 5 is a side perspective view of a single lumen rigid inner hub, according to another aspect of the present invention.

5

[0019] FIG. 6 is a side perspective exploded view of a single lumen catheter shaft, extension tube assembly and rigid inner hub of FIG. 5.

[0020] FIG. 7 is a side perspective view of the components of FIG. 6 assembled.

FIG. 8 is a side perspective view of a soft flexible single lumen outer hub, insert molded over the rigid inner hub of FIG. 7.

[0022] FIGS. 1-8 illustrate specific aspects of the invention and are a part of the specification. Together with the following description, these figures demonstrate and explain the principles of the invention.

DETAILED DESCRIPTION OF THE INVENTION

10

· 15

. 20

25

. 30

The following description provides specific details in order to provide a thorough understanding of the invention. The skilled artisan, however, would understand that the invention can be practiced without employing these specific details. Indeed, the invention can be practiced by modifying the illustrated method and resulting product and can be used in conjunction with apparatus and techniques conventionally used in the industry. For example, the invention is described for a single or dual lumen catheter. The invention, however, could easily be adapted for three or four (or even more) lumen catheters. In another example, the manufacturing process of the invention is described primarily in terms of insert molding or solvent bonding relating to plastic as the base material in the context of catheter applications. However, the invention could be used with manufacturing processes that require snap fits using metal components as the rigid medical inner structure of the bifurcation or hub.

[0024] The invention provides a catheter capable of high-pressure applications while maintaining the look and feel of standard catheter devices. The high pressure catheter of the invention maintains the typical soft flexible exterior in the bifurcation, hub, and/or suture wings while providing a more rigid high-pressure connection interior. One example of such a catheter is illustrated in FIGS. 1-8. It should be appreciated in the following examples of the invention that the rigid inner hub (*i.e.*, inner hub 12, 16, 18) may be formed from a material such as medical grade

5

10

. 15

20

25

. 30

6

polyurethane (e.g., Tecoflex®, Carbothane®, Pelathane®, Chronoflex®, Tecoplast®, etc.) having a hardness in the range of approximately 90 Shore A durometer to 80 Shore D durometer, with the currently preferred polyurethane being Tecoflex® having a hardness in the range of approximately 70-75 Shore D durometer. The rigid inner hub may also be formed from other materials, such as metal (e.g., stainless steel, titanium, etc.), polyvinylchloride, nylon, polyester, and castable epoxy, provided the materials are sufficiently hard to withstand pressures present in typical high pressure catheter applications. The outer hub, on the other hand, may be formed from a much softer, flexible material, which is suitable for contacting the skin of a patient, such as medical grade polyurethane having a hardness rating in the range of approximately 35-80 Shore A durometer. The outer hub may also be formed from silicone or other materials discussed herein, provided that the material utilized is sufficiently soft to provide flexibility and patient comfort.

One aspect of the invention is illustrated in FIGS. 1-2. FIG. 1 depicts a [0025] single lumen rigid inner hub 12 that forms a rigid high pressure connection between the fluid paths of catheter shaft 11 and extension tube assembly 10. Inner hub 12 may be insert molded directly over both the catheter shaft 11 and the extension tube assembly 10, or may be separately molded as a pre-formed insert and attached to the catheter shaft 11 and extension tube assembly 10 manually (i.e., catheter shaft 11 and extension tube assembly 10 are respectively inserted into opposite ends of the inner hub 12). In the case of a separately molded inner hub 12, variations include having through holes with lead-in tapers, the use of adhesives, and or having barbs or other fittings that would ensure a tight fit of the catheter shaft 11 and extension tube assembly 10 within the inner hub 12. FIG. 2 depicts a soft pliable outer hub 13 that contains flexible suture wings substantially similar to those found on typical catheters. In one method of manufacture, the outer hub 13 can be insert molded over the inner hub 12, such that the geometry of the inner hub 12 is supported during the insert molding process by the outer hub 13 mold cavity, thereby keeping the inner hub 12 located in the center of the molded assembly.

[0026] Another aspect of the invention is illustrated in FIGS. 3-4. FIG. 3 depicts a dual lumen rigid inner hub (or inner connector) 16 that forms a rigid high pressure connection between the fluid paths of dual lumen catheter shaft 15 and the

extension tube assembly 14. Like inner hub 12, inner hub 16 may be insert molded directly over both the dual lumen catheter shaft 15 and the extension tube assembly 14, or may be separately molded as a pre-formed insert and manually attached to the dual lumen catheter shaft 15 and the extension tube assembly 14 in the same manner as described above in connection with inner hub 12. FIG. 4 depicts a soft pliable dual lumen outer hub 17 containing flexible suture wings substantially similar to those found on typical catheters. The outer hub 17 can be insert molded over the inner hub 16. As with the single lumen embodiment described above, the geometry of the inner hub 16 can be supported during the insert molding process by the outer hub 17 mold cavity, thereby keeping the inner hub 16 located in the center of the molded assembly.

[0027] Another aspect of the invention is illustrated in FIGS. 5-8, depicting an alternative method of design and manufacture of a high-pressure inner hub according to the present invention. As illustrated in FIG.5, an inner hub 18 contains distal barbs 19 for retention of the catheter shaft 11 and proximal barbs 20 for retention of the extension tube assembly 10, as well as a ring configuration 21 around a central portion thereof. FIG. 6 shows an exploded view of the inner hub 18 in relationship to the catheter shaft 11 and the extension tube assembly 10. FIG. 7 depicts the inner hub 18 with the catheter shaft 11 pressed over the distal retention barbs 19, and extension tube assembly 10 pressed over the proximal retention barbs 20, such that the proximal end of the catheter shaft 11 and the distal end of the extension tube assembly 10 abut the ring configuration 21. Such a configuration forms a rigid high-pressure connection between the fluid paths of the catheter shaft 11 and extension tube assembly 10.

[0028] In an alternate embodiment, a compression sleeve could be placed over the inner hub 18, following insertion into the catheter shaft 11 and the extension tube assembly 10, such that the compression sleeve covered the ring configuration 21 and portions of the catheter shaft 11 and the extension tube assembly 10. The compression sleeve could then be crimped onto the assembly to provide a smooth outer surface for the transition between the catheter shaft 11 and the extension tube assembly 10. FIG. 8 depicts a soft pliable single lumen outer hub 17 containing flexible suture wings substantially similar to those found on typical catheters. The

5

10

15

20

25

30

8

outer hub 17 can be insert molded over the inner hub 18 similar to that described above in connection with FIG. 2.

As described above, the high pressure catheters are made with a soft [0029] flexible exterior in the connector/hub while providing a more rigid high-pressure interior. Any manufacturing process known in the art that can provide this soft flexible exterior and rigid, high-pressure interior can be used to make the hub of the invention. In one aspect of the invention, the inner hub is made by inserting a ridged core pin between the extension tube assembly and the catheter shaft. As with standard insert molding practice, use of a core pin keeps the fluid path between the extension tube assembly and catheter shaft open during the molding process. The extension tube assembly, catheter shaft and core pin combination are loaded into a mold, which is machined to create a cavity having the desired shape and geometry of the inner hub. Molten high durometer (ridged) plastic is then injected into the mold cavity, encapsulating the extension tube assembly and catheter shaft. The core pin is then removed, leaving a ridged high-pressure connection between the extension tube assembly and catheter shaft. The outer hub is produced in a similar procedure. A ridged core pin is inserted into the ridged high-pressure connection described above and the combination is loaded into a mold, which is machined to create a cavity with the desired shape and geometry of the outer hub. Molten low durometer (soft) plastic is then injected into the mold cavity, encapsulating the ridged high-pressure connection. The core pin is then removed, leaving a soft flexible outer hub over the rigid high-pressure connection between the extension tube assembly and catheter shaft.

[0030] Using the hub of the invention, a typical catheter can be used in both standard pressure and high-pressure medical procedures. Thus, for example, a single catheter can be used for both procedures, saving equipment cost (using a single catheter in place of two or more catheters), physician time (needing only a single needle prick), and safer, less intrusive procedures (requiring only a single vascular access site).

[0031] In addition to any previously indicated variation, numerous other modifications and alternative arrangements may be devised by those skilled in the art

9

without departing from the spirit and scope of the invention and appended claims are intended to cover such modifications and arrangements. Thus, while the invention has been described above with particularity and detail in connection with what is presently deemed to be the most practical and preferred aspects of the invention, it will be apparent to those of ordinary skill in the art that numerous modifications, including but not limited to, form, function, manner of operations and use may be made without departing form the principles and concepts set forth herein.

10

CLAIMS

1. A catheter, comprising:

a catheter shaft;

an extension tube assembly;

an inner hub comprising a rigid hard material, connecting said catheter shaft to said extension tube assembly, wherein said catheter shaft is in fluid communication with said extension tube assembly; and

an outer hub comprising a soft flexible material positioned around said inner hub.

10

15

20

25

- 2. The catheter according to claim 1, wherein said catheter shaft and said extension tube assembly each comprise a single lumen.
- 3. The catheter according to claim 2, wherein a portion of said inner hub is inserted into a proximal end of said catheter shaft lumen and a distal end of said extension tube assembly lumen.
- 4. The catheter according to claim 3, wherein said inner hub is substantially contained within said catheter shaft and said extension tube assembly.
- 5. The catheter according to claim 3, wherein said inner hub comprises distal and proximal barbs.
- 6. The catheter according to claim 5, wherein said inner hub further comprises a central ring.
- 7. The catheter according to claim 2, wherein said inner hub comprises openings configured for receiving said catheter shaft and said extension tube assembly.
- 8. The catheter according to claim 7, wherein a lumen of said inner hub comprises tapered portions adjacent to said openings.
 - 9. The catheter according to claim 1, wherein said catheter shaft comprises an outer wall enclosing at least two lumens therein, and wherein said

11

extension tube assembly comprises at least two separate tubes in respective fluid communication with each of said at least two lumens.

10. The catheter according to claim 1, wherein said rigid hard material comprises a material selected from the group consisting of medical grade polyurethane, metal, polyvinylchloride, nylon, polyester, and castable epoxy.

- 11. The catheter according to claim 10, wherein said rigid hard material comprises medical grade polyurethane having a hardness in the range of approximately 90 Shore A durometer to 80 Shore D durometer.
- 12. The catheter according to claim 11, wherein said rigid hard material comprises Tecoflex® having a hardness in the range of approximately 70-75 Shore D durometer.
 - 13. The catheter according to claim 1, wherein said soft flexible material comprises a material selected from the group consisting of medical grade polyurethane, silicone, polyvinylchloride, nylon, polyester, and castable epoxy.
- 15 14. The catheter according to claim 13, wherein said soft flexible material comprises silicone having a hardness in the range of approximately 35-80 Shore A durometer.
 - 15. The catheter according to claim 1, wherein said rigid hard material is adapted to accommodate pressures higher than approximately 150 psi.
- 20 16. The catheter according to claim 1, wherein said outer hub comprises a pair of suture wings.

17. A method for making a catheter comprising a catheter shaft and an extension tube assembly, comprising the steps of:

placing said catheter shaft and said extension tube assembly into a first mold, wherein a proximal end of said catheter shaft is positioned adjacent a distal end of said extension tube assembly within a first mold cavity;

insert molding an inner hub comprising a rigid hard material over said proximal end of said catheter shaft and said distal end of said extension tube assembly;

placing the combination of said inner hub, catheter shaft and extension tube assembly into a second mold, wherein said inner hub is placed within a second mold cavity, said inner hub being supported and centered therewithin; and

insert molding an outer hub comprising a soft flexible material over said inner hub.

18. A method for making a catheter comprising a catheter shaft and an extension tube assembly, wherein said catheter shaft and said extension tube assembly each comprise a single lumen, comprising the steps of:

inserting a portion of an inner hub having a throughgoing lumen into a proximal end of said catheter shaft lumen and a distal end of said extension tube assembly lumen such that said inner hub is substantially contained within said catheter shaft and said extension tube assembly, wherein said catheter shaft is in fluid communication with said extension tube assembly;

placing the combination of said inner hub, catheter shaft and extension tube assembly into a mold, wherein said inner hub is positioned within a mold cavity; and

insert molding an outer hub comprising a soft flexible material over said catheter shaft and extension tube assembly.

10

5

15

20

25

WO 2004/105850

13

19. A method for making a catheter comprising a catheter shaft and an extension tube assembly, comprising the steps of:

providing an inner hub comprising a rigid hard material and at least one throughgoing lumen;

positioning a proximal end of said catheter shaft into an opening at a distal end of said inner hub;

positioning a distal end of said extension tube assembly into at least one opening at a proximal end of said inner hub;

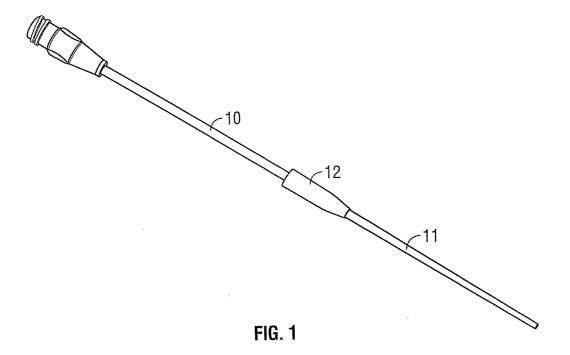
placing the combination of said inner hub, catheter shaft and extension tube assembly into a mold, wherein said inner hub is placed within a mold cavity, said inner hub being supported and centered therewithin; and

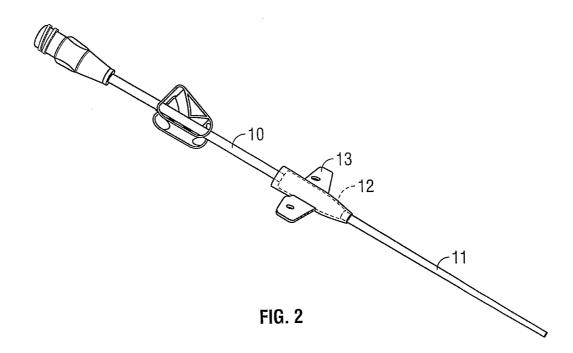
insert molding an outer hub comprising a soft flexible material over said inner hub.

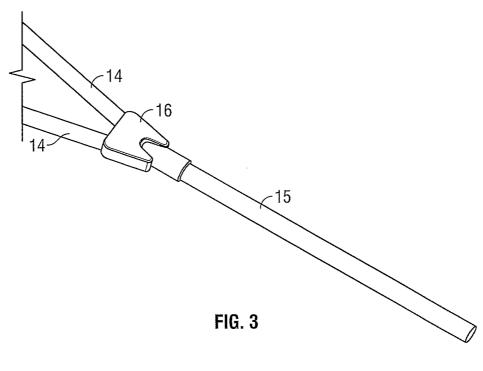
20. The method according to claim 19, wherein said inner hub comprises two proximal openings and said extension tube assembly comprises two separate tubes, wherein said step of positioning a distal end of said extension tube assembly comprises positioning a first of said tubes into a first of said openings and positioning a second of said tubes into a second of said openings.

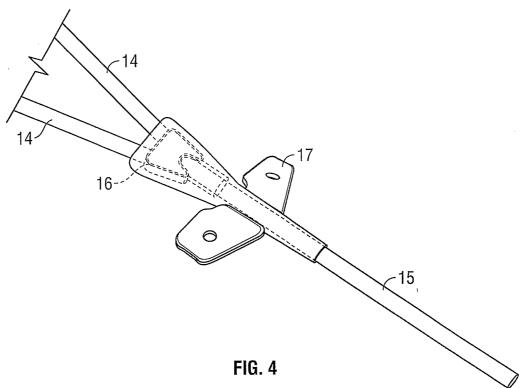
15

5









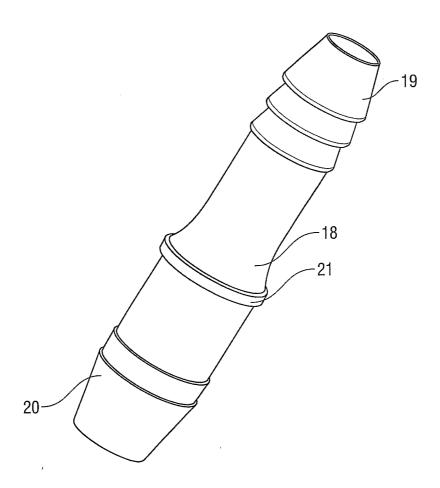
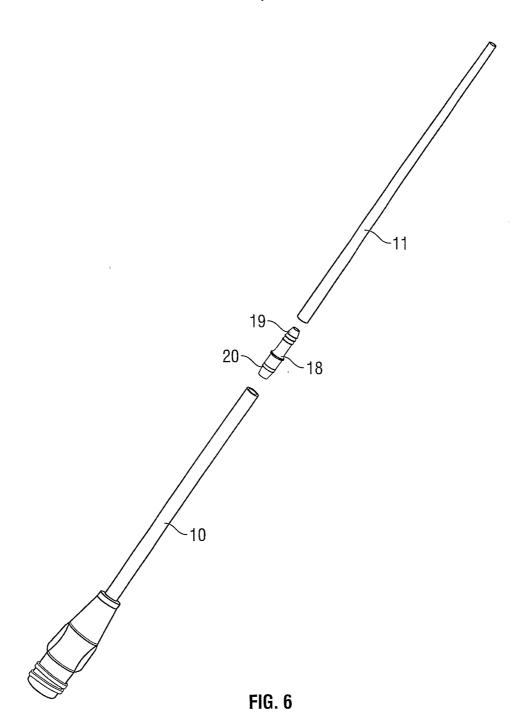


FIG. 5



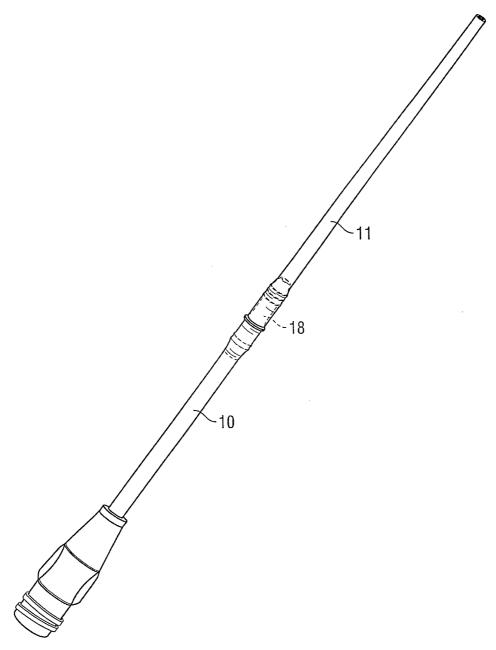
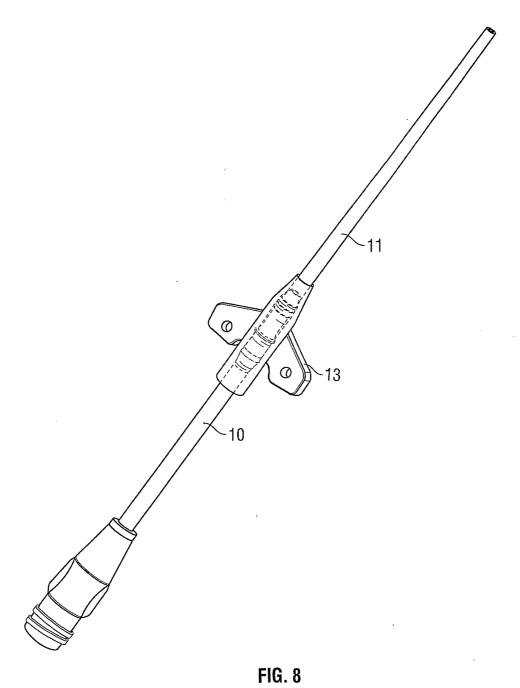


FIG. 7

PCT/US2004/016595 WO 2004/105850



Inte al Application No PC 1/ US2004/016595

A. CLASSIFI	CATION OF SUBJECT	T MATTER .
IPC 7	A61M25/00	A61M39/10

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

 $\begin{array}{ccc} \text{Minimum documentation searched (classification system followed by classification symbols)} \\ \text{IPC 7} & \text{A61M} \end{array}$

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

Category °	Criation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 160 325 A (NICHOLS COLIN J ET AL) 3 November 1992 (1992-11-03)	1,3,4,9, 10,13-16
Α	column 11, lines 36-62; compounds 20,21	18
Χ	US 4 588 402 A (IGARI AKIRA ET AL) 13 May 1986 (1986-05-13)	1-3,5,6, 13
Α	column 5, line 62 - column 10, line 12; figures	18
Х	WO 97/22374 A (ABRAHAMSON TIMOTHY ALAN ; QUINTON INSTR (US)) 26 June 1997 (1997-06-26)	1,2,7-9, 16
Y	page 16, line 15 - page 19, line 30; figure 17	10,11
Υ	US 5 718 678 A (FLEMING III JAMES ANTHONY) 17 February 1998 (1998-02-17) column 9, lines 5-25	10,11

Further documents are listed in the continuation of box C	Patent family members are listed in annex.
Special categories of cited documents A' document defining the general state of the art which is not considered to be of particular relevance E' earlier document but published on or after the international filing date L' document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) O' document referring to an oral disclosure, use, exhibition or other means P' document published prior to the international filing date but later than the priority date claimed	 'T' later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention 'X' document of particular relevance, the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone 'Y' document of particular relevance, the claimed invention cannot be considered to involve an invention to expect the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art '&' document member of the same patent family
Date of the actual completion of the international search 20 September 2004	Date of mailing of the international search report 01/10/2004
Name and mailing address of the ISA European Patent Office, P B 5818 Patentlaan 2 NL – 2280 HV Rijswijk Tel (+31-70) 340-2040, Tx 31 651 epo nl, Fax (+31-70) 340-3016	Authorized officer Vänttinen, H

Into al Application No
PC 1/ US 2004/016595

		PC1/u32004/016595
C.(Continua	ation) DOCUMENTS CONSIDERED TO BE RELEVANT	
Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X A	WO 99/16498 A (BOSTON SCIENT LTD) 8 April 1999 (1999-04-08) page 7, line 10 - page 9, line 6; figure 1	1,2,7, 10,16 19
Α	US 5 961 485 A (MARTIN GEOFFREY S) 5 October 1999 (1999-10-05) the whole document	1,17,19
Χ	US 5 797 869 A (LEBLANC MICHAEL R ET AL) 25 August 1998 (1998-08-25)	1,9
A	column 4, line 30 - column 10, line 65; figures	17,19
А	US 4 969 879 A (LICHTE LEO J) 13 November 1990 (1990-11-13) the whole document	1-6

In 'Application No
PCI/US2004/016595

Patent document		Publication		Patent family	Publication
cited in search report		date		member(s)	date
US 5160325		03-11-1992	US	4753640 A	28-06-198
00 0100020	/ `	00 11 1332	AU	607155 B2	
			AU	7773387 A	19-05-198
			CA	1319305 C	22-06-199
			DE	3752245 D1	
			DE	3786441 D1	
			DE	3786441 T2	
			EP	0263645 A2	
			EP	0537136 A2	
			ES	2005373 A6	
			JP	2571353 B2	
			JP	8098891 A	16-04-199
			JP	2533897 B2	
			JP	63095064 A	26-04-198
			US	4995863 A	26-02-199
US 4588402	Α	13-05-1986	JP	1380293 C	28-05-198
			ĴΡ	58152568 A	10-09-198
			ĴΡ	61048382 B	23-10-198
			ĴΡ	1380295 C	28-05-198
			JΡ	58163371 A	28-09-198
			ĴΡ	61050459 B	04-11-198
			ĂÜ	553449 B2	
			AU	8930482 A	15-09-198
			BE	894715 A1	
			CA	1188943 A1	
			DE	3238303 A1	
			DE	8229004 U1	
			DE	8237050 U1	
			FR	2522969 A1	
			SE	453887 B	14-03-198
			SE	8205642 A	04-10-198
UO 0700074		26.06.1007	A	1461207 4	14 07 100
WO 9722374	A	26-06-1997	ΑŬ	1461297 A	14-07-199
			WO	9722374 A1	
		- 	US 	6428513 B1	06-08-200
US 5718678	Α	17-02-1998	NONE		
WO 9916498	 А	08-04-1999	AU	735828 B2	19-07-200
5510750	^	OO OT 1999	AU	9671298 A	23-04-199
			CA	2304733 A1	
			EP	1019137 A1	
			JP	2001518327 T	16-10-200
			WO	9916498 A1	
			US	6358230 B1	
				0336230 DI	13-03-200
US 5961485	Α	05-10-1999	US	5480380 A	02-01-1990
			ΑU	6200294 A	11-10-199
			CA	2158139 A1	
			WO	9421315 A1	29-09-199
			DE	69403461 D1	
			DE	69403461 T2	
			ĒΡ	0689466 A1	
			ES	2106514 T3	
			ΗK	1007516 A1	
			JP	8507939 T	27-08-1996
			UF	000/303	2.1 00 1991

Patent document cited in search report		Publication date		Patent family member(s)	Publication date
US 5797869	A	25-08-1998	CA	1330285 C	21-06-1994
			US	5472417 A	05-12-1995
			US	6206849 B1	27-03-2001
			US	2001044594 A1	22-11-2001
			DE	3853058 D1	23-03-1995
			DE	3853058 T2	20-07-1995
			ΕP	0322225 A2	28-06-1989
			US	5195962 A	23-03-1993
			US	5135599 A	04-08-1992
US 4969879	<u></u> -	13-11-1990	NONE		