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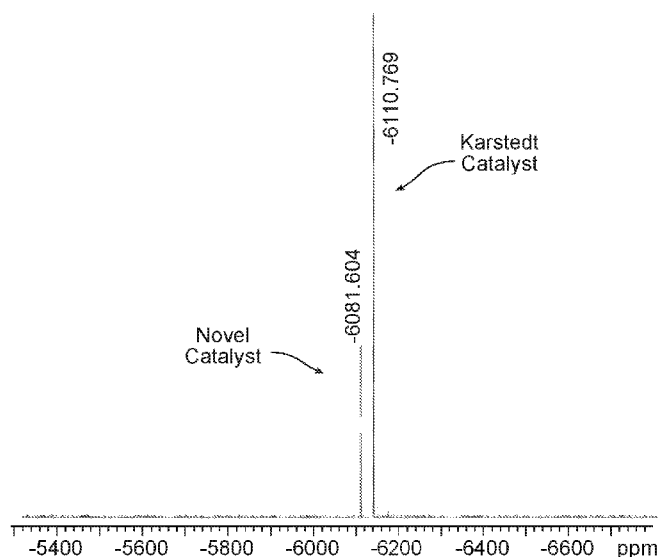
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(54) Title: NOVEL ANTIMICROBIAL TOPICAL SKIN CLOSURE COMPOSITIONS AND SYSTEMS

FIG. 1



(57) Abstract: Novel compositions and systems for closure of wounds with antimicrobial effectiveness are disclosed. The compositions provide devices of improved flexibility and elasticity and are readily applied to wound sites or over wound closure devices. The present invention is also directed to a novel platinum catalyst for use in such compositions. The catalyst provides for rapid curing on topical surfaces such as skin and bonds to such surfaces in about 2 -5 minutes.



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Novel Antimicrobial Topical Skin Closure Compositions and Systems

CROSS-REFERENCE TO RELATED APPLICATION(S)

This application is related to U.S. Non-Provisional Application Nos. 16/885,413
5 (Attorney Docket No. ETH6068USNP1), 16/885,426 (Attorney Docket No.
ETH6069USNP1), 16/885,361 (Attorney Docket No. ETH6070USNP1), 16/885,375
(Attorney Docket No. ETH6085USNP1) all filed on May 28, 2020 and _____ (Attorney
Docket No. ETH6070USCIPI, being filed concurrently herewith) and all the foregoing patent
10 applications having a common assignee the contents of which are herein incorporated by
reference in their entirety for all purposes.

TECHNICAL FIELD

The field of art to which this invention pertains is silicone-based wound closure
compositions and devices silicone-based topical skin adhesives (TSA's) and systems.

BACKGROUND OF THE INVENTION

15 There is a need for elastomeric topical skin adhesives, especially for skin closure of
the moving body joints such as knees, wrists, elbow, etc.

Elastic versions of the TSA are especially needed in orthopedic surgery. Aggressive
motion of joints may compromise the quality of the closure at the interface between the
adhesive and the skin. Watertight closure is also desirable in a product in order to lessen the
20 possibility of post-surgical infections. Silicone types of adhesives are one solution for both
these two key customer requirements due to its elasticity and sealing properties.

Silicone is known for its inertness and commonly used as OTC scar reduction
products. Reducing skin reactions and improvement of cosmesis are the extra benefits
provided by silicone-based TSA.

25 Thus, there is a need for elastomeric topical skin adhesives, especially for the closure
of the moving body parts and joints, such as knees, wrists, elbows, etc.

Because there is a potential for microbial contamination and infection of the wound,
there is also a further need in providing antimicrobial agents as a part of any novel TSA.

There is also a need to absorb liquid discharge from the wound during its healing process. Typical TSA seal the wound and it is difficult for wound discharge or exudate to escape. There is also a need to detect the state of the wound especially for exudate discharge. Indication of the wound state is important for addressing potential issues with wound management, including anti-infection treatments, dressing replacement, etc.

SUMMARY OF THE INVENTION

Accordingly, novel catalytic compositions, silicone based curable adhesive compositions, and wound closure systems are disclosed, further containing an antimicrobial agent and/or an indicator such as for detecting wound exudate discharge or wound moisture.

The compositions comprise a mixture of vinyl terminated polydimethylsiloxane, and polydimethylhydro-co-polydimethylsiloxane cross linker, surface treated silica particles as bonding agent, and a novel, non-conventional platinum catalyst, optionally with common low boiling point organic solvent such as aliphatic organic solvent such as hexane or its commercial derivatives, and SiH terminated polydimethyl siloxane chain extender, further comprising an antimicrobial agent. The proposed silicone adhesive can be dried on skin at body temperature in less than 3 minutes. The skin holding forces between the proposed silicone adhesive and skin is comparable or better than the typical cyanoacrylate-based TSA products. Unlike the traditional cyanoacrylate-based TSA products, the invented silicone-based TSA when combined with traditional wound closure devices can be stretched 160% of its original length and fully recover to its original unstretched dimension. When treated with the antimicrobial agent, triclosan, a traditional wound closure device, as hereinafter demonstrated, was stretched to 145% of its original length and fully recovered to its original unstretched dimension.

The bonding formation is enabled by the condensation reaction between the silanol functions on the surface of silica particle and the OH functions on the skin. Silanol condensation tends to be sluggish at ambient temperature and the novel non-conventional catalyst enables this reaction to occur in a short period of time. The platinum based novel catalyst also activates vinyl silylation reaction to allow vinyl terminated silicone polymer to cross link simultaneously to the condensation reaction.

In one embodiment, the invention relates to a composition comprising:

a cross-linkable silicone polymer having reactive functionalities;

a silica-containing composition;

a silicone cross-linking agent;

5 a catalyst, wherein said catalyst comprises a platinum tetramethyldivinyl disiloxane diethyl maleate complex having the formula:

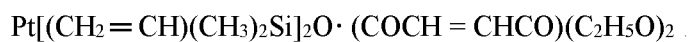


an antimicrobial agent.

10 In the foregoing embodiment, the silica-containing composition may be added as a separate component, but more preferably it is contained in the cross-linkable silicone polymer. The coating compositions may also contain a platinum catalyst.

Another aspect of the present invention is an antimicrobial medical device having a surface, wherein at least part of the surface is coated with the above-described novel silicone coating composition.

15 Still yet another aspect of the present invention is a novel platinum catalyst for use with cross-linkable silicone coatings. The catalyst comprises a platinum complex having the following formula:



20 A further aspect of the present invention is use of the compositions of this invention as a topical skin adhesive and as a topical skin adhesive in conjunction with wound closure devices as systems or kits to close wounds, further having an antimicrobial agent and/or an indicator such as for detecting wound exudate discharge or wound moisture incorporated therein.

25 These and other aspects and advantages of the present invention will become more apparent from the following description.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is an NMR peak comparison of the Karstedt Catalyst compared with the NMR peak of the novel catalyst of this invention.

5 FIGS. 2a, 2b and 2c show the steps of a stretch test used to demonstrate to elasticity of the present invention without an antimicrobial agent.

FIGS. 3a, 3b and 3c show the steps of a stretch test used to demonstrate to elasticity of the present invention with an antimicrobial agent.

FIGS. 4a and 4b show the Zone of Inhibition comparatives for antimicrobial- and nonantimicrobial-containing compositions in *S. aureus*.

10 FIGS. 5a and 5b show the Zone of Inhibition comparatives for antimicrobial- and nonantimicrobial-containing compositions in *E. Coli*.

FIGS. 6a , 6b and 6c show that absorbents and/or indicators may be incorporated within the compositions of this invention in or on the surfaces of underlying wound closure device.

15 FIG. 7 is a schematic showing water ingress into the lower surface films of this invention; changes in color of embedded absorbent/indicator particles upon absorption into the film of water or moisture; and moisture repellency on the upper surface of the film.

20 FIGS. 7a and 7b show color change for the compositions of the present invention before and after exposure to moisture when absorbents and/or indicators are included in the compositions.

FIG. 7c shows the hydrophobicity of the surfaces of the compositions of this invention.

25 FIGS. 7d, 7e, and 7f show the flexibility and stretching capabilities of the compositions of this invention for embodiments when absorbents and/or indicators are included in the compositions.

FIG. 7g and 7h show the water absorption and indicator capabilities of the compositions of the present invention when absorbents and/or indicators are included in the compositions,

DETAILED DESCRIPTION OF THE INVENTION

The terms silicone and siloxane are conventionally used interchangeably in this art, and that usage has been adopted herein.

Topical Skin Adhesive Compositions & Wound Closure Systems

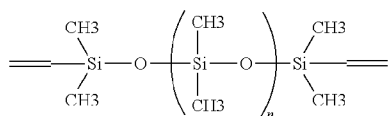
5 One aspect of the present invention is directed to novel wound closure compositions which are particularly useful for closing lacerations and surgical incisions. These compositions are suitable for use as topical skin adhesives and as adhesives in conjunction with wound closure devices.

10 In one embodiment, the compositions include a mixture of a cross-linkable siloxane polymer and a silica-containing composition which may be added as a separate component, but more preferably contained in the cross-linkable silicone polymer, a conventional silicone cross-linking agent, and a platinum catalyst. The silicone polymer components are blended with conventional aromatic organic solvents, including, for example, aliphatic organic solvents (such as, for example, hexane, heptane or its commercial derivatives) to form
15 coating solutions or compositions. Other solvent suitable for coating solution includes and not limited to low molecular weight siloxane, e.g., hexamethyldisiloxane.

The cross-linkable siloxane polymers useful in the compositions of the present invention will have reactive functionalities or terminal functional groups, including but not limited to vinyl terminated, hydroxyl and acrylate functional groups. The cross-linkable
20 siloxane polymers that can be used in the compositions of the present invention preferably include vinyl terminated polydialkylsiloxane or vinyl terminated polyalkarylsiloxane. Examples include but are not limited to the following vinyl terminated siloxane polymers: polydimethyl siloxane, polydiphenylsilane-dimethylsiloxane copolymer, polyphenylmethylsiloxane, polyfluoropropylmethyl-dimethylsiloxane copolymer and
25 polydiethylsiloxane. It is particularly preferred to use vinyl terminated cross-linkable polymethyl siloxane.

The cross-linking agents that can be used in the compositions of the present invention include conventional silicone cross-linking agents such as, for example, polymethylhydro siloxane, polymethylhydro-co-polydimethylsiloxane, polyethylhydrosiloxane,
30 polymethylhydrosiloxane-co-octylmethylsiloxane, polymethylhydrosiloxane-co-methylphenylsiloxane. The preferred conventional crosslinkers for use in the compositions of

the present invention are polymethylhydro siloxane and polymethylhydro-co-polydimethylsiloxane. Precise control of cross-link density in the coatings of the present invention is achieved by precise control of the ratio of non-cross-linkable silicone polymer (e.g., polydimethylsiloxane) to fully cross-linked polymer. The fully cross-linked polymer is formed by a reaction between the functionalized cross-linkable polymer and the cross-linking agent, for example, a vinylsilylation reaction between vinyl-terminated polydimethylsiloxane and polymethylhydrosiloxane optionally in the presence of a platinum complex catalyst. Examples of this polymer include but are not limited to: Gelest Product Code No. DMS-V31, DMS-V33, DMS V-35, DMS V42, DMS-V46, DMS-V52, etc., available from Gelest, Inc., Morrisville, Pa. 19067. The typical molecular structure of vinyl terminated polydimethyldisiloxane is the following:



wherein n is defined by the molecular weight.

The molecular weights of the silicone polymers used wherein can be estimated based on the relationship between viscosity and molecular weight (page 11, SILICONE FLUIDS: STABLE, INERT MEDIA ENGINEERING AND DESIGN PROPERTIES, Catalog published by Gelest, Inc. 11 East Steel Rd. Morrisville, PA 19067). Using A.J. Barry's relationship for molecular weights (M) >2,500 correlating the kinematic viscosity μ expressed in centistokes (cSt) at 25 C, the molecular weight M of silicones can be estimated as follows:

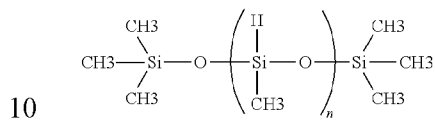
$$\log \mu_{\text{cSt}} = 1.00 + 0.0123M^{0.5}$$

(as published by A.J. Barry in the Journal of Applied Physics 17, 1020 (1946))

Vinyl terminated polydimethylsiloxane reacts with polymethylhydrosiloxane cross-linker in the presence of platinum catalyst under appropriate conditions; the vinyl terminated polydimethylsiloxane linear polymers are fully cross-linked to each other as the result of this reaction. The amount of polymethylhydrosiloxane cross-linker is in large stoichiometric excess compared to vinyl terminated polydimethylsiloxane base polymer. It is believed that the extra SiH functions in the cross-linker react with the OH functions on the surface such as human skin, e.g., polymeric sutures, to form Si—O—C bonds at elevated temperature or in

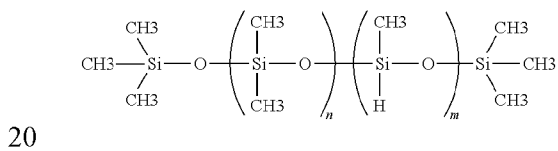
the case of steel needles, to form Si—O—Fe bonds. Covalent bonds thus created between the silicone coating and the device, as the result of this reaction, result in the adhesive attachment of the coating to a given surface.

The polymethylhydrosiloxane cross-linkers, or cross-linking agents, used in the practice of the present invention will have a molecular weight between about 1000 and about 3000, and preferably between about 1400 and about 2100. An example of this polymer cross-linker includes, but is not limited to, Gelest Product Code No. HMS-991, HMS-992, available from Gelest, Inc., Morrisville, Pa. 19607. The typical molecular structure of the polymethylhydrosiloxane cross-linker is the following:



wherein n is defined by the molecular weight.

Polymethylhydro-co-polydimethylsiloxane can also be used as cross-linker or cross-linking agent in the novel coatings of the present invention. Examples of this polymer include, but are not limited to, Gelest Product Code No. HMS-301, HMS-501. The molecular weight of this siloxane polymer cross-linking agent will typically be between about 900 and about 5,000, and preferably about 1,200 to about 3,000. The typical molecular structure of polymethylhydro-co-polydimethylsiloxane cross linker is the following:

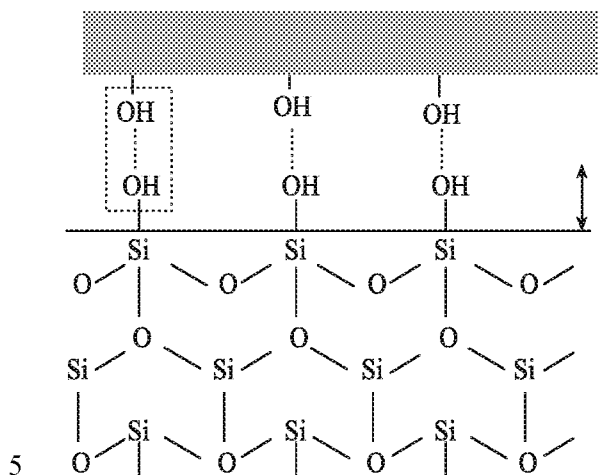


wherein n and m are defined by the molecular weight.

Silica-Containing Compositions

As used herein, the silica-containing compositions described for use with this invention include silica materials as a separate component (such as surface treated silica) or from commercially available compositions that contain silica in a cross linkable silicone polymer mixture.

As a separate component, silica is incorporated into composition of this invention to act as a bonding agent to skin and other substrate materials. It is believed that the OH groups on the surface of silica particles react with the OH functions on the surface of substrate material including human skin under a certain condition, as illustrated below.



Silica particles were incorporated into the cross linkable silicone polymers. Hexamethyl silyl surface treatment is needed for the silica particles to enable its compatibility to the polysiloxane polymer matrix which prevents phase separation. An example of treated silica includes hexamethyldisilazane treated silica i.e., trimethyl silyl surface treated silica filler (Gelest SIS6962.0).

10

In the case of silicone polymers already containing silica, these may be obtained from commercially available sources such as silica-containing composition selected from reactive silica-containing silicone bases including HCR (high consistent rubber) bases and LSR (liquid silicone rubber) bases, preferred are LSR bases. Other commercial examples of this material include and is not limited to Wacker 401-10, 401-20, 401-40 base; and a liquid silicone rubber base, a commercial example of this material includes and is not limited to Bluestar Silbione LSR 4370 base. These types of commercial silicone rubber bases are prepared by mixing a surface-treated silica filler with various molecular weights of vinyl terminated polydimethylsiloxane polymer. In-situ surface treatment may be performed during the mixing process to improve the compatibility between filler and polysiloxane polymer.

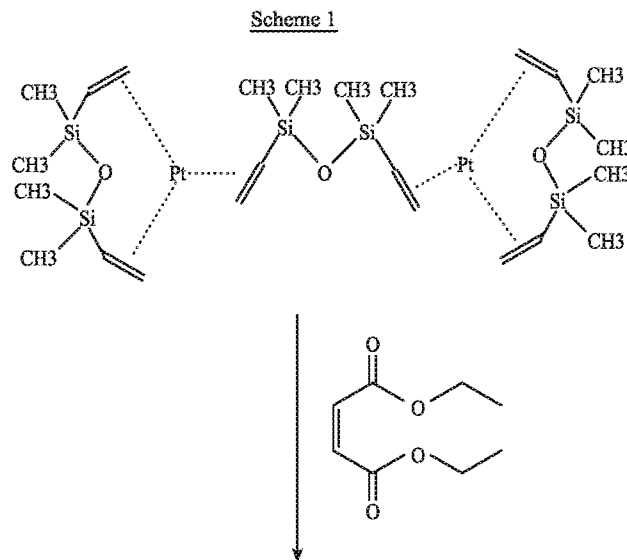
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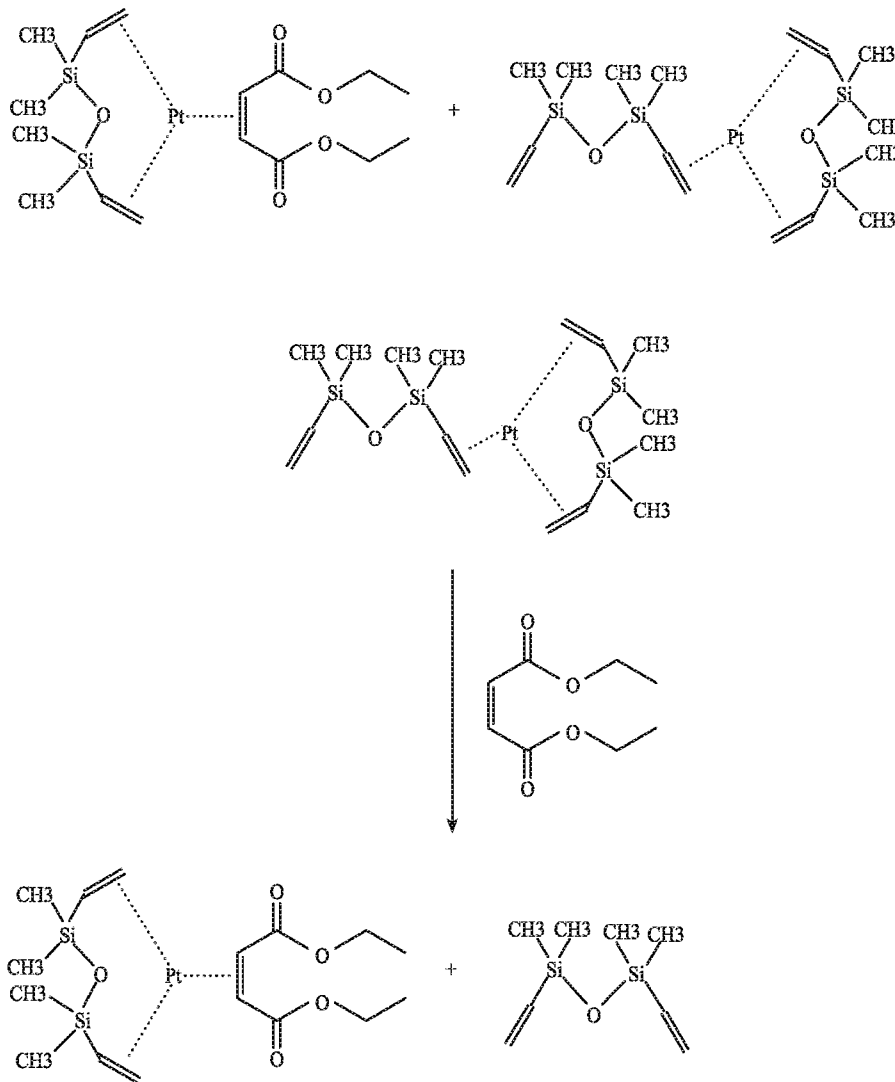
Catalyst

Karstedt of GE Silicone invented a highly active platinum catalyst at the beginning of the 1970's (US 3775452). Vinyl terminated polydimethylsiloxane can react with polymethylhydrosiloxane containing cross linker in less than 1 minute at ambient temperature with as little as 10 ppm of the Karstedt catalyst. The traditional platinum catalyst does not enable the reaction between OH groups on the surface of silica particles reacts and the OH functions on the surface of substrate. This type of condensation reaction tends to be slow at ambient condition and the typical catalyst for this reaction including organic amine and catalyst such as tin dilaurate. Trace amount of condensation catalyst will terminate the catalytic ability of platinum catalyst which is referred as platinum poisoning in the silicone industry. A novel platinum comparable catalyst is needed to activate the OH condensation between silica particle and substrate material, to enable rapid adhesion formation between silicone and a given substrate material. A platinum based novel catalyst of the present invention is able to activate both vinyl silylation and OH condensation simultaneously.

The novel catalyst is prepared by reacting Karstedt's catalyst with diethyl maleate according to scheme 1. The novel platinum tetramethyldivinyl disiloxane diethyl maleate catalyst enables both vinyl silylation and condensation reaction. This is referred to as "dual functional silicone catalyst".



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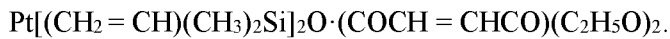


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The novel catalyst of the present invention may be prepared in the following manner. Karstedt catalyst in xylene solution is mixed with a low concentration of vinylcyclohexanol in a xylene solution at ambient temperature for a sufficiently effective time to complete the reaction, e.g., a half an hour, and completion of the reaction is indicated by a change of the color of the reaction mixture, from clear to light brown.

The resulting catalyst solution containing the novel catalyst of the present invention is ready to use in a composition useful as a topical skin adhesive. The formula of the resulting platinum complex catalyst (platinum tetramethyldivinyl disiloxane diethyl maleate complex) is:

15



It should be noted that the resulting catalyst reaction mixture will contain a small amount of the reaction product divinyltetramethyldisiloxane. This component does not affect the catalyst and is a low boiling point component that is rapidly evaporated. Accordingly, purification of the catalyst mixture to remove divinyltetramethyldisiloxane is optional, and it is believed that its presence at ultra-low concentrations will not affect the cross-linking reaction of a cross-linkable silicone polymer. The novel catalyst of the present invention also activates the bonding formation between silanol groups on the surface of silica fillers and OH functions on a given surface, that is, the catalyst is capable to activate two reactions. This allows for curing the cross-linkable components in silicone coatings to rapidly form coating films at desired curing temperatures and provides bonding to a given substrate such as human skin.

Solvents for Viscosity Reduction

Some commercially produced filler reinforced cross linkable silicone polymers (silicone base rubber) have high viscosity, typically higher than 500,000 and up to many millions of cPs. It is impossible to mix and spread such high viscosity material onto skin and low hazardous organic solvent is needed to reduce its viscosity.

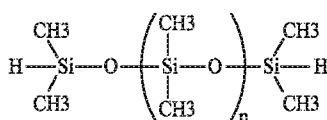
Low temperature aliphatic solvents are used for this purpose. Typical examples include, but are not limited to, pentanes, heptanes, hexanes and their mixtures. The organic solvents are added at a concentration sufficient to allow effective blending of the silicone polymer components into a homogeneous solution. The total solvent concentration is between 10% and 30%, depending upon the original viscosity of the base rubber. Ultra-low boiling point solvent such as n-butane and isopentane can also be used to provide sprayable formulation of silicone adhesive.

Chain Extender for Low Viscosity Vinyl Terminated Polydimethylsiloxane Base Polymer

For those commercially produced filler reinforced cross linkable silicone polymers (silicone base rubber) that have a high viscosity in the range from 100,000 centipoise (cP) to several million cP (e.g., 1-20 million cP) viscosity, (low molecular weight) vinyl terminated polydimethylsiloxane (<300 cP) may be also added together with low temperature aliphatic solvents to improve its mixability and spreadability. A SiH terminated polydimethylsiloxane

is added as a chain extender to polymerize the low molecular weight vinyl terminated polydimethylsiloxane. The SiH terminated polydimethylsiloxane base polymer has molecular weight between 1000 and 100,000, preferably between 3,000 to 10,000.

5 Examples of this type of polymer include, but are not limited to: Gelest Product Code No. DMS-H21, DMS-H31, etc. The typical molecular structure of SiH terminated polydimethylsiloxane is illustrated below



10

The above silicone polymers and novel platinum catalyst are dispersed into low boiling point organic solvents to form the coating solution. Low temperature aliphatic solvents are used for the silicone dispersion. Aromatic solvents and hexamethyldisiloxane are commonly used for silicone dispersion. Typical examples include, but are not limited to, pentane, heptanes, hexane and their mixtures. The organic solvents are added at a concentration sufficient to allow effective blending of the silicone polymer components into a homogeneous coating solution. The total solvent concentration is from about 80 wt.% to about 99 wt.%, and is more typically from about 85 wt. % to about 93 wt. %, depending upon the coating thickness requirement. Those skilled in the art will appreciate that the coating thickness can be engineered by changing the solids content of the coating solution.

20

Antimicrobial Agent

The compositions as described above further comprise at least one antimicrobial agent. The antimicrobial agent can be any medicant having antibiotic or antimicrobial or antipathogen function, including triclosan, chlorhexidine, polyhexamethylene biguanide (PHMB), octenidine, elemental silver, and silver salts, for example. In a preferred embodiment, the inventive composition comprises triclosan.

25

Wound Exudate/Moisture Absorbent Particles and Indicator(s)

The compositions described above may further comprise at least one wound exudate or wound moisture absorbent and/or indicator.

Suitable absorbents are those that have water or moisture or exudate absorbent particles that are capable to absorb water, in quantities of at least 10% the weight of particles, more preferably at least 30% absorbed water vs. the weight of particles. The absorbent particles when presence in the composition of this invention may possess the property to
5 change color to indicate presence of wound exudate or moisture as herein after described.

Advantageously, silica-based desiccant particles with an indicator have been incorporated into the silicone matrix described above prior to curing. After curing, the composition forms a thin layer suitable as a TSA/dressing having good adherence, absorbency and indicator properties.

10 Examples of absorbent materials include silica and anhydrous inorganic salts, Examples of anhydrous inorganic salts include copper copper(II) sulfate and cobalt(II) chloride. These types of absorbent materials change color when they contact water and are used as indicator for commercial desiccants with indicating property, which is typically a mixture of silica and an inorganic salt indicator such as cobalt(II) chloride.

15 Examples of commercial desiccant include t.h.e.® Desiccant produced by EMD Millipore Corporation. Drierite™ Indicating Absorbents produced by W.A. Hammond

Advantageously, superabsorbent materials may be utilized instead or in combination with the salt-based desiccants and absorbent materials. Color-changing is due to the salt hydration, but most of the water absorption is by the superabsorbent particles. In some
20 embodiments, superabsorbent materials can be utilized as absorbent particles or desiccant particles of the present invention, including (a) cross-linked polyacrylates and polyacrylamides; (b) hydrolyzed cellulose-polyacrylonitrile, c) cross-linked copolymers of maleic anhydride. Materials useful for such application are exemplified by cross-linked sodium polyacrylate, various acrylonitrile and acrylamide-based polymers, e.g., starch-g-
25 polyacrylonitrile. Other superabsorbent materials that can be useful are based on various polysaccharides, such as starch, chitosan and guar gum. Also, composite superabsorbents, can be utilized made by incorporating kaolin, attapulgite, humates, mica, bentonite, montmorillonite and sodium silicate.

Typically the amount of the absorbent/indicator will range from 5 to 25 % by weight
30 of the total formulation.

The inventors have discovered as hereinafter described that incorporating silica-based desiccant particles (with or without an indicator) into the films formed from the cured silicone matrix compositions of this invention result in films having a hydrophobic upper surface and a water permeable lower surface (substrate facing) side of the film. Fig. 7 is a schematic that indicates water ingress into the lower surface of the film (for example, the surface that would be in constant, intimate contact with a substrate such as a moisture-containing or exudate-generating wound or tissue surface,); changes in color of the embedded absorbent/indicator particles upon absorption into the film of water or moisture such as from wound exudate; and moisture repellency on the upper surface of the film . The intimate and prolonged contact of the lower surface with wound discharge/moisture will allow absorption into the silicone film over time while the hydrophobic upper surface will repel moisture provided that the film is not immersed in water for a prolonged period of time. The moisture-resistant properties of the upper surface of the film are ideally suited for patients that may wish to shower after the film cures.

15

Referring to Fig. 7a, 7b and Fig. 7c, the above principals may be observed with the compositions of this invention. In one instance, a silica-containing composition of this invention was immersed in water to simulate the intimate contact with a source of moisture on its surface. Prior to immersion blue coloration was observed (Fig. 7a). After immersion, the coloration had changed to red/pink, indicating water ingress (Fig. 7b). Further, the hydrophobic nature of the compositions of this invention for instances simulating contact that is not prolonged and intimate (such as splashing with water in a shower) is illustrated by viewing the surface of the cured composition, as in Fig. 7c, where drops of moisture (for example, element 500) are seen to bead.

25

In various embodiments the absorbent/indicator components may be incorporated into the compositions of this invention in various ways. Referring to Fig. 6a, wound 360 of tissue 340 is approximated with wound closure device 300. Over the top and sides of wound closure device 300 is applied a topical skin adhesive 320 containing the absorbent/indicator particles. Alternately as shown in Fig. 6b, the absorbent/indicator particles may be applied to wound closure device 400 or applied as coating 450 onto wound closure device 400 as shown in Fig. 6c.

30

Sequence

The sequence of the addition of components is important. The typical coating composition is prepared in the following manner. In the case when the silica is added as a separate component, the vinyl terminated polydimethylsiloxane is dispersed into the first solution such as hexamethyldisiloxane together with surface treated silica for up to two hours
5 until fully homogeneous (solution 2). Heptane is then added (solution 3) and further mixing for one hour prior to the addition of polymethylhydrosiloxane cross linker. The solution is fully blended for one more hour after all of the catalyst is added as the final component

In the following paragraph, the wt. % is the wt. % of total solid content in the coating solution. The novel coating compositions of the present invention will contain sufficient
10 amounts of the polymeric components, silica-containing composition, cross-linking agent, catalyst, and solvent to effectively provide a silicone coating having high flexibility and durability.

Typically, the amount of the silica in the coating solution will be about 5 wt. % to about 40 wt. % (total solids), more typically about 10 wt. % to about 30 wt. % (total solids),
15 and preferably about 15 wt. % to about 25 wt. % (total solids). The amount of the cross-linkable silicone polymer will typically be about 60 wt. % to about 95 wt. % (total solids), more typically about 70 wt. % to about 90 wt. % (total solids), and preferably about 75 wt. % to about 85 wt. % (total solids). The amount of the silicone cross-linking agent will typically be about 1 wt. % to about 15 wt. % (total solids), more typically about 2 wt. % to about 10
20 wt. % (total solids), and preferably about 3 wt. % to about 8 wt. % (total solids). The amount of the platinum catalyst is based upon the total solids in the novel silicone coating compositions (platinum element in total solids) of the present invention will typically be about 0.06 wt. % to about 0.003wt. %, more typically about 0.04 wt. % to about 0.008 wt. %, and preferably about 0.03 wt. % to about 0.01 wt. %. The amount of the antimicrobial agent
25 is based upon the total solids in the novel silicone coating compositions present invention will typically be about 0.05 wt. % to about 2 wt. %, more typically about 0.1 wt. % to about 1.5 wt. %, and preferably about 0.2 wt. % to about 1 wt. %.

The amount of organic solvent in the compositions of the present invention will typically be about 0wt. % to about 30 wt. %, more typically about 10 wt. % to about 20 wt.
30 %, and preferably about 12 wt. % to about 18 wt. %. Those skilled in the art will appreciate that the amount of solvent present in the novel coating compositions of the present invention will vary with several factors, and that the solvent quantity in the coating compositions will

be selected to engineer an efficacious coating. The factors typically considered include the method of application, the method of cure, the coating equipment utilized, ambient conditions, thickness, etc. It will be appreciated that each of the components of the coating compositions of the present invention may consist of blends of those components. For
5 example, two or more cross-linkable silicone polymers having different functionalities and/or molecular weights may be used, etc.

In practice and similar to most of commercially available platinum cured silicone materials, the silicone-based topical skin adhesive of this invention is delivered in a two-part kit by mixing equal volumes of the Part A and Part B components as hereinafter described.

10 As an overview, vinyl terminated polydimethylsiloxane is mixed with Platinum tetramethyldivinyl disiloxane diethyl maleate catalyst, silica particles and optionally aliphatic organic solvent using a high-speed mixer to form part A of the kit. Vinyl terminated polydimethylsiloxane are mixed with polymethylhydro-co-polydimethylsiloxane cross linker, silica particle, antimicrobial agent (when desired) and optionally aliphatic organic solvent
15 using high speed mixer to form part B of the kit.

When applied to a substrate, equal amounts of the two-part kit were mixed using a static mixer and then spread onto the surface of a substrate, such as skin. The compositions of this invention are well suited for wound closure applications such as topical skin adhesives. Generally, these compositions have been demonstrated to cure to a non-tacky nature or touch
20 at temperatures at about 19 C. At temperatures of about 28 C, the compositions cure in about 2-5 minutes.

As noted above and as would be appreciated by one of skill in the art, the silicone compositions of this invention cure in several minutes to films that are neither sticky nor tacky. In contrast, some silicone adhesives, such as silicone pressure sensitive adhesives
25 (PSA's), are by nature sticky or tacky and are intended to be such for the entire usable life of the adhesive. Such useable life of the tacky silicone PSA's may be upwards to several years. The non-tackiness of the compositions and examples of this invention is measured by ASTM C679.

In general ASTM C679 consists of lightly touching a surface of a curing sealant with
30 a polyethylene film at regular intervals until the sealant does not attach itself to the film and the film appears clean when peel from the surface. More specifically a strip of polyethylene film is placed on the surface of the curing elastomer and a 30g weight is placed on the film.

The weight is left in place for 30 seconds, then removed and the polyethylene strip is removed and examined for sealant attachment to the film. The length of time from when the sealant was first applied onto a given surface until the time the sealant is no longer picked up by the film is called tack-free time and is the time point at which the film exhibits a non-tacky nature which evidences that the sealant has cured.

Upon curing the curable compositions of the present invention exhibit stretchable, flexible and elastic properties especially useful for applications over wound closure on bendable joints, such as knees, elbows. The curable compositions of the present invention, optionally in combinations with various wound closure devices can be applied over any wound closures, including wounds over bendable joints or wounds not over bendable joints, such general surgical closures such over any tissue area, e.g., body, abdominal, arm, leg, shoulder, back areas and similar.

The compositions of this invention can be applied onto wounds directly as a curable liquid or semi-liquid, flowable composition, or applied over a porous, flowable composition-permeable wound closure device.

Wound Closure Systems

As noted above, the compositions of this invention are suitable for use in combination with wound closure devices.

Wound closure devices suitable for use in this invention comprise any device that is configured to close a wound. The wound closure devices most useful are wound closure strips, tapes, patches or any other materials suitable for closing a wound, most preferably a strip. Preferably, the wound closure device is porous and will allow a flowable, polymerizable adhesive to permeate the device and to allow adequate bonding of the device to a tissue surface being bonded.

The wound closure device comprises a wound facing side and a top side. The wound facing side may further comprise an adhesive such as a pressure sensitive adhesive (PSA) applied over at least a portion of the wound facing side. The PSA is useful for initially approximating the wound. The wound closure device is preferably porous. By "porous" is meant herein either that the bulk of the wound closure device has pores, such that subsequently applied polymerizable adhesive composition is soaked up or absorbed by the bulk material, or that the bulk of the wound closure device has voids (like a net or screen),

such that the subsequently applied polymerizable adhesive composition passes directly through the bulk material, with or without being soaked up or absorbed by the bulk material.

For example, in the case of textile materials, “porous” is generally used to mean that the applied adhesive composition permeates and passes through interstices between the fibers but does not necessarily pass into and through the fibers themselves. Preferably the wound closure device is a mesh strip.

Such porosity (or other properties such as hydrophobicity or hydrophilicity) will also allow a polymerization initiator or rate modifier to be loaded in or on the wound closure device prior to use, to initiate the subsequently applied polymerizable adhesive composition. Such porosity will also preferably allow air and fluid to pass through the wound closure device, either through pores per se, or through voids in the bulk material. Depending upon the degree of porosity and/or the size of the openings, such porosity of the mesh or ability of air and fluid to permeate through the mesh may be tailored either to remain after a final composite material is formed, or to be absent therefrom. The wound closure device is also preferably non-toxic, as it is intended to be used cover a wound, such as on biological tissues. As such, the wound closure device should be biologically compatible with the desired substrate (such as tissue, skin, organ, or the like), and is preferably a material that is governmentally approved or generally regarded as safe for the desired purpose. By way of example, suitable wound closure devices are mesh materials and are disclosed in United States Patent Applications 2006/0009099 and 2005/0182443, incorporated herein by reference in their entirety.

The wound closure device may be a textile or mesh/web material. Suitable textile materials may be formed of either synthetic or natural materials. Such textile material may be formed of either woven or non-woven fabrics or materials. The wound closure device may be, for example, any suitable polymeric film, plastic foam (including open celled foam), a woven fabric, knitted fabric, a non-woven fabric, mixture thereof, or the like. In particular, suitable wound closure devices may thus be prepared, for example, from nylons, polyolefins such as polyethylene, polypropylene, ethylene propylene copolymers, and ethylene butylene copolymers, acrylics, rayons, polyurethanes, polyurethane foams, polystyrenes, plasticized polyvinylchlorides, polyesters such as polyethylene terephthalate (PET), polyamides, polylactic acids, polyglycolic acids, polycaprolactones, copolymer mixtures of the above, natural materials such as cotton, silk and linen, polytetrafluoroethylene (PTFE), biovascular material, collagen, Gore-Tex®, DACRON®, etc. The preferred wound closure device

materials are those that contain an OH functionality on its surface whether occurring naturally or by surface treatment to impart an OH functionality (“OH surface-treated”). These materials include and are not limited to polyesters, nylons, acrylic, rayon, polyurethanes, polyurethane foams, polystyrenes, polyesters, polyethylene terephthalate (PET), polyamides, poly(lactic acid), polyglycolic acid, polycaprolactone, copolymer mixtures of the above, and cotton, silk and linen. Suitable OH surface-treated materials that impart an OH functionality to their surfaces include but are not limited to OH surface-treated PTFE, OH surface-treated polypropylene and OH surface-treated polyethylene.

The wound closure device may be formed of a synthetic, semi-synthetic, or natural organic material. Thus, for example, the mesh may be formed of a synthetic or natural polymer material, but not from a material such as metal (such as silver, steel or the like) or glass or ceramic. The wound closure device may be either biodegradable, or not biodegradable. The wound closure device is preferably resistant to tearing.

The thickness of the wound closure device may be from about 0.1 mm to about 25 mm. In another embodiment, the thickness of the wound closure device is from about 0.5 mm to about 20 mm, preferably from about 0.7 mm to about 10 mm, most preferably from about 1 mm to about 5 mm.

When the wound closure device is a strip, the strip may be from about 2 cm to about 40 cm, preferably from about 10 to about 30 cm, most preferably 25 cm in length. The strip may be from 0.1 to about 8 cm, preferably from about 2 to 6 cm, more preferably about 4 cm in width.

The wound closure device may be selected to be elastic or have some memory effect. In such embodiments, the elastic properties of the mesh may desirably provide a degree of pressure or stress at the application site, for example, to maintain wound edge approximation. Likewise, in embodiments where such additional degree of pressure or stress at the application site is not desired, the mesh may be selected to have less or no elasticity.

The wound closure device may be either biodegradable, or not biodegradable. By “biodegradable” is meant that the mesh biodegrades over time in vivo, such that it does not require physical removal of the mesh after a set period of time. Thus, for example, a biodegradable mesh is one that, in the in vivo environment, will biodegrade over a period of from about one week to about five years. A nonbiodegradable material is one that does not biodegrade in an in vivo environment within about five years. Such a nonbiodegradable

material thus would require physical removal of the wound closure device at a desired time, rather than slowly deteriorating over time or may slough off naturally from the tissue.

The wound closure device may include one or more chemical materials located in or on it. For example, one or more chemical substances may be dispersed in or on the wound closure device, such as being chemically bound, physically bound, absorbed, or adsorbed to it. Such chemical materials that may be present in or on the wound closure device include, but are not limited to, any suitable and preferably compatible additive that enhances performance of the composite structure. Such additional chemical substances may be bioactive or non-bioactive. Suitable other chemical substances thus include, but are not limited to, colorants (such as inks, dyes and pigments), scents, protective coatings that do not chemically detach, temperature sensitive agents, drugs, wound-healing agents, anti-microbial agents and the like.

Examples

15 Example 1, Novel Platinum Catalyst (Synthesis Procedure)

44.50g of Gelest SIP 6831.2 (2.2% platinum divinyl tetramethyldisiloxane complex in xylene, Karstedt catalyst) was mixed with 2g of diethyl maleate for 24 hours at ambient temperature. Samples were taken out after 3 hours, 18 hours, and 24 hours for NMR testing and the NMR spectra for the 3 hour sample is shown in FIG. 1.

20 The formation of the novel catalyst is the evidence for scheme 1, which rests on NMR spectroscopic identification. Karstedt catalyst is known with a characteristic ^{195}Pt signal at approximately -6111 ppm.

After 3 hours of mixing of the mixtures of Example 1, a new ^{195}Pt signal at -6082 ppm was observed along with the original signal for the Karstedt catalyst at -6111 ppm as illustrated in the NMR spectra of this mixture at 3 hours in FIG. 1. The intensity of the new signal increases over time while the intensity of the Karstedt catalyst signal reduced at the same time.

Preparation of Test Sample Compositions

As describes above, the silicone-based topical skin adhesive is delivered in a two-part kit by mixing equal volumes of the Part A and Part B components. The following examples

describe the components of each part of the compositions which were prepared and which are subsequently mixed together.

Example 2. Preparation of Silicone-Based Topical Skin Adhesive -No Antimicrobial Agent

5 Part A

40g of vinyl terminated polydimethylsiloxane (Gelest DMSV41) was mixed with 10g of surface treated silica particles (Gelest SIS6962.0), together with 2.6g of the resulting catalyst of Example 1 using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

10 Part B

40g of vinyl terminated polydimethylsiloxane (Gelest DMSV41) was mixed with 10g of surface treated silica particles (Gelest SIS6962.0), together with 3.34g of Polymethylhydro-co-polydimethylsiloxane (Gelest HMS301) using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

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Example 3. Preparation of Silicone-Based Topical Skin Adhesive using Commercial Silica - containing Silicone Raw Material -No Antimicrobial Agent

Part A

20 90g of Elkem 44 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 4.72g of the resulting catalyst of Example 1, 9.0g of low molecular weight vinyl terminated polydimethyl silicone base polymer (Gelest DMS V21) and 26g of hexane using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

25 Part B

81g of Elkem 44 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 8.1g of polymethyl hydro siloxane cross linker (Gelest DMS H991), 2.7g of SiH terminated polydimethylsiloxane chain extender (Gelest DMS H21) and 10.2g of hexane using a high speed centrifugal mixer
30 (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Control Example: Control Example without Silica Bonding Agent and Using Conventional Karstedt Catalyst – No Antimicrobial Agent

5 Part A

40g of vinyl terminated polydimethylsiloxane (Gelest DMSV41) was mixed with 2.6g of Karstedt catalyst xylene solution (1% of Gelest SIP 6831.2 in xylene) using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Part B

10 40g of vinyl terminated polydimethylsiloxane (Gelest DMSV41) was mixed 3.34g of Polymethylhydro-co-polydimethylsiloxane (Gelest HMS301) using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

EXAMPLE 4A. Preparation of Inventive Silicone-based Antimicrobial Topical Skin Adhesive with 0.25% Loading of Triclosan

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Part A

90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 0.62g of example 1, 0.90g of Gelest SIP 6831.2 (2.2% platinum divinyl tetramethyldisiloxane complex in xylene), 9.0g of low molecular weight vinyl terminated polydimethyl silicone base polymer (Gelest DMS V21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Part B

25 90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 9.0g of polymethylhydro-co-polydimethyl siloxane cross linker (Gelest DMS H301), 3.0g of SiH terminated polydimethylsiloxane chain extender (Gelest DMS H21) and 0.5g of triclosan using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

EXAMPLE 4B. Preparation of Inventive Silicone-based Antimicrobial Topical Skin Adhesive with 0.50% Loading of Triclosan

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Part A

90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 0.62g of example 1, 0.90g of Gelest SIP 6831.2 (2.2% platinum divinyl tetramethyldisiloxane complex in xylene), 9.0g of low molecular weight vinyl terminated polydimethyl silicone base polymer (Gelest DMS V21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Part B

90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 9.0g of polymethylhydro-copolydimethyl siloxane cross linker (Gelest DMS H301), 3.0g of SiH terminated polydimethylsiloxane chain extender (Gelest DMS H21) and 1.0g of triclosan using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Example 4C. Preparation of Inventive Silicone-based Antimicrobial Topical Skin Adhesive with 0.75% Loading of Triclosan

Part A

90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 0.62g of example 1, 0.90g of Gelest SIP 6831.2 (2.2% platinum divinyl tetramethyldisiloxane complex in xylene), 9.0g of low molecular weight vinyl terminated polydimethyl silicone base polymer (Gelest DMS V21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Part B

90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 9.0g of polymethylhydro-copolydimethyl siloxane cross linker (Gelest DMS H301), 3.0g of SiH terminated polydimethylsiloxane chain extender (Gelest DMS H21) and 1.5g of triclosan using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Example 4D. Control Example: Preparation of Silicone-based Topical Skin Adhesive with 0% Loading of Triclosan

Part A

90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 0.62g of example 1, 0.90g of
5 Gelest SIP 6831.2 (2.2% platinum divinyl tetramethyldisiloxane complex in xylene), 9.0g of low molecular weight vinyl terminated polydimethyl silicone base polymer (Gelest DMS V21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Part B

10 90g of Elkem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 9.0g of polymethylhydro-copolydimethyl siloxane cross linker (Gelest DMS H301), 3.0g of SiH terminated polydimethylsiloxane chain extender (Gelest DMS H21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

15 Example 5, Preparation of Test Samples and Description of Test Procedures Test Procedures Wound Closure Strip Testing Sample Preparation:

An 8 inch by 11 inch synthetic substrate (or bio substrate) was cut in two halves with dimensions of 4 inches by 11 inches. A 1 inch wide PSA (pressure sensitive adhesive) coated
20 polyester mesh was placed along the cutting line to hold the two half pieces together. The two-part silicone TSA compositions described above were mixed and applied onto the mesh evenly to cover the entire area of the mesh using a conventional rubber spatula.

Holding Strength Test:

This test evaluated the force required to separate the substrate approximated with the
25 PSA coated mesh and the applied silicone TSA compositions. This method was based on ASTM F2458: Standard test method for wound closure strength in tissue adhesive and sealant.

Synthetic substrate (Mylar) was used for the test, selected samples were also tested on porcine skin. The width of the synthetic substrate was 1 inch and porcine skin was 2 inches and the strain rate was 20 inches per minute.

30 Peel Test.

The T-peel strength test was performed following ASTM F2256: Standard test method for Strength Properties of Tissue Adhesives in T-Peel by Tension Loading.

The average peel strength of mesh coated with silicone-based TSA in T-peel configuration is performed at a strain rate of 10 inches per minute.

5 Zone of Inhibition Test:

The triclosan containing silicone TSA test article is placed into an agar medium that is inoculated with the test organism. Where the antimicrobial agent triclosan diffuses through the silicone carrier into the agar medium, and as long as the concentration of the
10 antimicrobial agent is above the minimum inhibitory concentration (MIC), none of the susceptible organisms will grow on or around the disk for some distance. This distance is called a Zone of Inhibition (ZOI). Assuming the antimicrobial agent has a diffusion rate in the medium, the presence of a ZOI around a test article indicates that the organism is inhibited by the presence of the antimicrobial agent in the otherwise satisfactory growth
15 medium. The diameter of the ZOI is inversely proportional to the MIC.

The triclosan containing silicone coated test articles were tested for antimicrobial properties utilizing this ZOI test. ZOI testing is a conventional method for estimating the inhibitory effects of antimicrobial substances against specific bacterial strains of interest. ZOI assays are useful for testing diffusible agents. As the agent diffuses away from the disk, the
20 concentration decreases logarithmically. The sensitivity of the organism to the agent is judged by the appearance and size of a zone where no growth occurs, i.e., the Zone of Inhibition.

The triclosan containing silicone coated test articles were aseptically placed in individual sterile Petri dishes and challenged with 100 micro liters of inoculum containing 10
25 colony-forming units (CFU) of Staphylococcus aureus or Escherichia coli. Trypticase soy agar was poured into each dish and allowed to solidify. The plates were incubated at 37° C. for 48 hours. After incubation, the plates were examined under a darkfield colony counter and the Zones of Inhibition were measured.

30 Holding Strength Test Sample

Synthetic Substrate, Polyester film (0.05 inch thick Duralar® film), Grafix Plastics, Maple Heights, OH

A 1.0 inch wide PSA (pressure sensitive adhesive) coated polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed along the cutting line to hold together the two half pieces of the Duralar film of 4 inches by 11 inches described above. The two-part silicone TSA compositions in each of the following examples were respectively mixed (Example 2, 5 Example 3, Control Example, Examples 4A - 4C and Control Example 4D) and evenly applied onto the mesh to cover the entire area of the mesh using a conventional rubber spatula. The samples were dried between 2 to 5 minutes at 31 C. 5, 1 inch wide strips of each of the covered mesh samples were cut for testing.

Bio Substrate (Porcine skin)

10 A 2 inch by 8 inch sample of porcine skin was cut in two halves with the dimensions of 2 inches by 4 inches. A 1.5 inch wide PSA (pressure sensitive adhesive) coated polyester mesh was placed along the cutting line to hold the two half pieces together. The two-part silicone TSA composition was mixed (Example 3) and evenly applied onto the mesh to cover the entire area of the mesh using a conventional rubber spatula.

15 Peel Test Sample

Synthetic substrate (Polyester film, 0.05 inch thick Duralar® film, Grafix Plastics, Maple Heights, OH)

A 5 inch by 5 inch PSA (pressure sensitive adhesive) coated on polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed on the polyester substrate of the same dimensions. 20 The two-part silicone TSA compositions of each of the following examples were respectively mixed (Example 2, Example 3, Control Example, Examples 4A , 4B, 4C and Control Example 4D) and applied onto the mesh evenly to cover the entire area of the mesh using a conventional rubber spatula. 5, 1 inch wide specimens were cut for testing after each of the covered mesh samples were dried and maintained at 31C over night (i.e., at least 8 hours).

25 Bio substrate (Arm of a 55 year-old Asian male)

A 3 inch by 1 inch PSA (pressure sensitive adhesive) coated on polyester mesh was placed on the left arm of a 55 year old Asian male. The two-part silicone TSA compositions of each of the following examples were respectively mixed (Example 3 and Control Example) and applied onto the mesh evenly to cover the entire area of the mesh using a 30 conventional rubber spatula.

Bio substrate (porcine skin)

A 5 inch by 1.5 inch PSA (pressure sensitive adhesive) coated on polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed on a piece of porcine skin with approximately the same dimension. The two-part silicone TSA composition of examples 2 and 3 was mixed and applied onto the mesh evenly to cover the entire area of the mesh using a conventional rubber spatula.

Stretch Test Samples

A 5 inch by 5 inch PSA (pressure sensitive adhesive) coated polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed on a Teflon substrate. The two-part silicone TSA composition was mixed (Example 3 and Example 4C) and applied onto the mesh evenly to cover the entire area of the mesh using a conventional rubber spatula. The silicone coated polyester mesh was peeled off from the Teflon substrate after 1 hour. 5, 1 inch -wide silicone coated mesh specimens were cut for testing.

Performance Testing Results:15 1a: Holding Test Results (Synthetic Substrate)

Holding test on Polyester film was performed for the compositions of Example 2 and 3, along with the Control Example; the results are summarized in Table 1.

Table 1

<u>Sample</u>	<u>Holding Strength (lb/in)</u>
Example 2	13.4
Example 3	17.9
Control Example	0.7
Examples 4A	11.6
Example 4B	11.0
Example 4C	10.5
Example 4D	13.1

Referring to Table 1, it can be seen that the holding force for the polyester substrate is significantly better in the inventive examples made from polysiloxane polymer and commercial bases, compared to conventional cross-linked silicone polymer using the Karstedt catalyst (Control Example). Additionally, a decrease in holding force is observed
 5 between the antimicrobial containing examples (Examples 4A, 4B, and 4C) and the non-antimicrobial containing examples (Examples 2, 3, and 4D).

1b: Holding Test Results (Bio Substrate)

Holding test on porcine skin was performed on the composition of Example 3
 10 and the results are summarized in Table 2

Table 2

<u>Sample</u>	<u>Holding Strength (lb)</u>
Example 3	10.2

Referring to Table 2, one sees that the holding force of the silicone- based TSA on porcine skin is comparable to cyanoacrylate based commercial product holding strength
 15 which is about 10 lbs.

2a: Peel Test Results (Synthetic Substrate)

Peel tests of TSA compositions on a synthetic substrate (polyester) was performed using the compositions of Examples 2 and 3, along with Control Example and Examples 4A-
 20 4C and Control Example 4D. The results are summarized in Table 3.

Table 3

<u>Sample</u>	<u>Average Peel Strength (lb/in)</u>	<u>Maximum Peel Strength (lb/in)</u>
Example 2	1.3	2.1

Example 3	2.6	3.1
Control Example	0.1	0.2
Example 4A	1.3	2.4
Example 4B	1.1	2.0
Example 4C	1.2	2.3
Example 4D	1.6	2.8

Referring to Table 3, it is seen that the average and maximum peel force for polyester substrate is significantly better in the inventive examples made from polysiloxane polymer and commercial bases, compared to conventional cross-linked silicone polymers using the Karstedt catalyst. (Control Example). Additionally, the peel force is observed to be nearly equal or slightly lower between antimicrobial containing examples (Examples 4A, 4B, and 4C) and the non-antimicrobial containing examples (Examples 2, 3, and 4D)

2b: Peel Test Results (Bio Substrate)

Peel tests of TSA on human skin was performed on Example 3 and Control Example and the results are summarized in Table 4.

Table 4

<u>Sample</u>	<u>Average Peel Strength (lb/in)</u>	<u>Maximum Peel Strength (lb/in)</u>
Example 3	2.5	3.5
Control Example	0.1	0.3

The peel force of silicone TSA made in inventive Example 3 is significantly higher than the Control Example. Also, the peel force of silicone TSA on human skin is very similar to the peel force of the same material on polyester substrate (see Table 3).

2b: Peel Test Results (Bio Substrate)

Peel tests of TSA on porcine skin was performed on Example 3 and the results are summarized in Table 4a.

Table 4a

<u>Sample</u>	<u>Average Peel Strength (lb/in)</u>	<u>Maximum Peel Strength (lb/in)</u>
Example 3	0.42	1.04

5

3: Stretch Test Results

Example 3 was stretched to 160% of its original length. The dimensions of the testing sample were measured before and after the stretch and the image is shown in FIGS. 2a, 2b and 2c.

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Example 4C was stretch to 145% of its original length. The dimensions of the testing sample were measured before and after the stretch and the image is shown in FIGS. 3a, 3b and 3c.

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Referring to these figures, the testing results indicate that Example 3 can be elongated to 160% of its original dimensions and recover fully, while the sample of Example 4C could be stretched to 145% and fully recover without . In a separate test not depicted, a cyanoacrylate coated polyester mesh sample could only be elongated to 101% of its original dimension. That is a 1% stretch was sufficient to create permanent deformation.

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EXAMPLE 6: Zone of Inhibition Tests

Two sets of test articles cut from each example (1x1cm silicone coated polyester mesh specimens) were aseptically placed in individual sterile petri dishes and challenged with 100 micro liters of inoculum containing 10 colony-forming units (CFU) of Staphylococcus aureus (S. aureus) or Escherichia coli (E coli). Trypticase soy agar was poured into each dish and allowed to solidify. The plates were incubated at 37° C. for 24

25

hours. After incubation, the plates were examined under a darkfield colony counter and the Zones of Inhibition were measured. The results are summarized in Table 4 and Table 5.

Table 4: Zone of Inhibition (mm) - S.aureus

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Sample ID	Zone of Inhibition (mm)				Average
	4 measurements around the sample				(mm)
Example 4A, replicate 1	9.7	9.7	10.1	10.2	9.9
Example 4A, replicate 2	10.4	10.2	10.2	10.4	10.3
Example 4B, replicate 1	11.9	11.9	11.4	11.9	11.8
Example 4B, replicate 2	11.2	11.3	11.3	11.2	11.3
Example 4C replicate 1	13.2	13.1	13.4	13.1	13.2
Example 4C, replicate 2	11.4	12.2	12.2	11.8	11.9
Control Example 4D, replicate 1	0	0	0	0	0.0
Control Example 4D, replicate 2	0	0	0	0	0.0

Referring to Table 4, one sees that compositions containing an antimicrobial agent (Examples 4A - 4C) are effective against S. aureus versus the non-antimicrobial composition (Control Example 4D) which is not effective against S. aureus.

10

FIG. 4a and FIG. 4b depict the ZOI with respect to Example 4C (0.75% loading of triclosan) and Control Example – 4D (no antimicrobial), respectively, on a trypticase soy agar plate challenged with A. aureus. As can be seen in comparing these 2 figures, Example 4C demonstrates that the compositions of this invention are able to effectively carry antimicrobial agents

15

Table 5: Zone of Inhibition (mm) - E.coli

Sample ID	Zone of Inhibition (mm)				Average
	4 measurements around the sample				(mm)
Example 4A, replicate 1	5.4	5.3	5.9	5.6	5.6

Example 4A, replicate 2	6.5	6.2	6.4	6.1	6.3
Example 4B, replicate 1	7.2	7.3	6.8	6.2	6.9
Example 4B replicate 2	7.1	7.8	6.4	7.2	7.1
Example 4C, replicate 1	10.1	9.7	9.7	9	9.6
Example 4C, replicate 2	10.1	10.2	9.9	9.6	10.0
Control Example 4D, replicate 1	0	0	0	0	0.0
Control Example 4D, replicate 2	0	0	0	0	0.0

Referring to Table 5, one sees that compositions containing an antimicrobial agent (Examples 4A - 4C) are effective against E. coli versus the non-antimicrobial composition (Control Example 4D) which is not effective against E. coli.

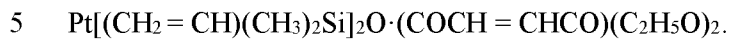
FIG. 5a and FIG. 5b depict the ZOI with respect to Example 4C (0.75% loading of triclosan) and Control Example – 4D (no antimicrobial), respectively, on a trypticase soy agar plate challenged with E colic. As can be seen in comparing these 2 figures, Example 4C demonstrates that the compositions of this invention are able to effectively carry antimicrobial agents.

Examples – Solvent Free (SF)

In some embodiments, use of organic solvent free mixing compositions are more desirable. Such embodiments include situations where contents of a mixing device, such as a dual-barrel syringe, may be made with a solvent in which contents of the syringe leak past seals of the syringe or the solvent evaporates. We have found that suitable compositions are possible without use of organic solvents by substituting a low molecular weight (3000 to 9000) vinyl terminated polydimethylsiloxane and/or low molecular weight (3000 to 9000) hydride terminated polydimethylsiloxane. Both these types of low molecular vinyl terminated or hydride terminated polydimethylsiloxane compounds have viscosities in the 40-150 cPs range. We have demonstrated that these solvent free formulations are capable of lowering viscosity of high viscosity silicone bases that that have viscosities typically higher than 500,000 and up to several million centipoise.

In these embodiments, the Part A compositions will typically comprise a silicone base (containing vinyl terminated polydimethyl silicone base polymer and fumed silica particles) ranging from 60 to 95 wt. % when controlling to a Part A viscosity of a 45,000 to 75,000 cPs

(or 30 to 100 wt.% when controlling to a Part A viscosity of a 15,000 – 45,000 cPs , or 0 to 40 wt. % when controlling to a Part A viscosity of a 75,000 to 105,000 cPs); 5 to 15 wt. % 3000 to 9000 cPs vinyl terminated polydimethylsiloxane; and 100 to 250 ppm of elemental platinum contributed from the catalyst of this invention:



Part B compositions will typically comprise a silicone base (containing vinyl terminated polydimethyl silicone base polymer and fumed silica particles) ranging from 60 to 80 wt. % when controlling to a Part B viscosity of 45,000 to 75,000 cPs base, (or 0 to 30 wt.% when
10 controlling to a Part B viscosity of 15,000 – 45,000 cPs base, or 70 to 100 wt. % when
controlling to a Part B viscosity of 75,000 to 105,000 cPs base); 10 to 40 wt.%
polymethylhydro-co-polydimethyl siloxane cross linker; and 3 to 12 wt. % hydride
terminated polydimethylsiloxane.

Typically, the viscosity of both the Part A and Part B compositions will independently range
between 25,000 and 100,000 cPs prior to mixing and will be of similar viscosity when Part A
15 and Part B are used in conjunction with each other around a low, medium or high viscosity
level.

Example 1-SF: Novel Platinum Catalyst (Synthesis Procedure)

2.7g of diethyl maleate was mixed with 3.6g of diethyl ether and 3.6g of Gelest SIP 6830.3
(3.0% platinum divinyl tetramethyldisiloxane complex in vinyl terminated
20 polydimethylsiloxane, Karstedt catalyst – xylene solvent free) at ambient temperature for 24
hours. 64.9g of Gelest SIP 6830.3 was then added into the above mixture and mixed for an
additional 72 hours while the lid of the container remained open. Finally, 928.8g of vinyl
terminated polydimethylsiloxane (Gelest DMS V21) was added and mixed for an additional
4 hours. The novel platinum catalyst master batch contains the novel catalyst having 2055
25 ppm of elemental platinum with essentially the remainder being vinyl terminated
polydimethylsiloxane .

Example 2 -SF, (Low Viscosity) (15,000 to 45,000 cPs)

Part A

30 90g of Elkem 55 experimental base (also known as Elkem Silbione 4020-55,
containing vinyl terminated polydimethyl silicone base polymer and fumed silica particles)

was mixed with 10g of Example 1-SF using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 3 minutes. This composition had a viscosity of 32,090 cPs (see Example7a-SF).

Part B

5 90g of Elkem 55 experimental base was mixed with 9.0g of polymethylhydro-co-polydimethyl siloxane cross linker (Gelest HMS H301), 3.0g of SiH terminated polydimethylsiloxane chain extender (Gelest DMS H21) using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 3 minutes. This composition had a viscosity of 31,160 cPs (see Example7a-SF).

10 Example 3- SF, Mid- viscosity (45,000 to 75,000 cPs)

Part A

15 115g of Elkem 55 experimental base was mixed with 20g of Elkem 44 experimental base (also known as Elkem Silbione 4020-44, containing vinyl terminated polydimethyl silicone base polymer and fumed silica particles) and 15g of Example 1-SF using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 3 minutes. This composition had a viscosity of 57,900 cPs (see Example7a-SF).

Part B

20 80g of Elkem 44 experimental base was mixed with 20g of Elkem 55 experimental base, 42g of polymethylhydro-co-polydimethyl siloxane cross linker (Gelest HMS 151), 8.0g of SiH terminated polydimethylsiloxane chain extender (Gelest DMS H21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 3 minutes. This composition had a viscosity of 61,500 cPs (see Example7a-SF).

25 Example 4 -SF , High viscosity (75,000 to 105,000 cPs)

Part A

 90g of Elkem 55 experimental base was mixed with 45g of Elkem 44 experimental base and 15g of Example 1-SF using a high-speed centrifugal mixer (FlackTek DAC150 FV-

K) at 3470 rpm for 3 minutes. This composition had a viscosity of 84,000 cPs . (see Example7a-SF).

Part B

100g of Elkem 44 experimental base was mixed with 42g of polymethylhydro-co-
5 polydimethyl siloxane cross linker (Gelest HMS H151), 8.0g of SiH terminated
polydimethylsiloxane chain extender (Gelest DMS H21) using a high-speed centrifugal mixer
(FlackTek DAC150 FV-K) at 3470 rpm for 3 minutes. This composition had a viscosity of
94,800 cPs (see Example7a-SF).

10 Example 5- SF: Preparation of Adhesion Performance Test Samples :

Holding Strength Test Sample

Synthetic Substrate, Polyester film (0.05 inch thick Duralar® film), Grafix Plastics, Maple
Heights, OH

15 A 1.5 inch wide PSA (pressure sensitive adhesive) coated polyester mesh (Lot#
16204, Innovize, St Paul, MN) was placed along the cutting line to hold together the two half
pieces of the Duralar film of 4 inches by 11 inches described above. The two-part silicone
TSA compositions in each of the following examples were respectively mixed (Example 2-
SF, Example 3-SF, Examples 4-SF) and evenly applied onto the mesh to cover the entire area
20 of the mesh using a conventional rubber spatula. The samples were cured between 1 to 3
minutes at 31 deg C and maintain at this temperature overnight. 5 pieces of 1 inch wide
strips of each of the covered mesh samples were cut for testing.

Peel Test Sample

25 Synthetic substrate (Polyester film, 0.05 inch thick Duralar® film, Grafix Plastics, Maple
Heights, OH)

A 5 inch by 5 inch PSA (pressure sensitive adhesive) coated on polyester mesh (Lot#
16204, Innovize, St Paul, MN) was placed on the polyester substrate of the same dimensions.
The two-part silicone TSA compositions of each of the following examples were respectively
30 mixed (Example 2-SF, Example 3-SF, Examples 4-SF) and applied onto the mesh evenly to

cover the entire area of the mesh using a conventional rubber spatula. 5, 1 inch wide specimens were cut for testing after each of the covered mesh samples were cured and maintained at 31degC over night (i.e., at least 8 hours).

5 Stretch Test Samples

A 5 inch by 5 inch PSA (pressure sensitive adhesive) coated polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed on a polyethylene substrate. The two-part silicone TSA composition was mixed (Examples 2-SF, 3-SF and 4-SF) and, applied onto the mesh evenly to cover the entire area of the mesh using a conventional rubber spatula. The silicone coated polyester mesh was peeled off from the Teflon substrate after 1 hour. 5, 1 inch -wide silicone coated mesh specimens were cut for testing.

15 Example 6-SF. Description of testing procedures

Viscosity measurement:

Viscosity measurements were performed on Examples 2-SF, 3-SF and 4-SF, using a Brookfield DV II+CP viscometer. Spindle 12 was used for all measurements and the speed was 1RPM.

20

Cure time measurement

ASTMC679: Standard test method for tack-free time of elastomeric sealants. The test consists of lightly touching a surface of a curing sealant with a polyethylene film at regular intervals until the sealant does not attach itself to the film and the film appears clean when peeled from the surface. More specifically a strip of polyethylene film is placed on the surface of the curing elastomer and a 30g weight is placed on the film. The weight is left in place for 30 seconds, then removed and the polyethylene strip is removed and examined for sealant attachment to the film. The length of time from when the sealant was first applied onto a given surface until the time the sealant is no longer picked up by the film is call tack-

free time and is the time point at which the film exhibits a non-tacky nature which evidences that the sealant has cured.

Peel Test.

5 The T-peel strength test was performed following ASTM F2256: Standard test method for Strength Properties of Tissue Adhesives in T-Peel by Tension Loading.

The average peel strength of mesh coated with silicone-based TSA in T-peel configuration is performed at a strain rate of 10 inches per minute.

Holding Strength Test:

10 This test evaluated the force required to separate the substrate approximated with the PSA coated mesh and the applied silicone TSA compositions. This method was based on ASTM F2458: Standard test method for wound closure strength in tissue adhesive and sealant.

Synthetic substrate (Mylar) was used for the test. The width of the synthetic substrate was 1 inch and the strain rate was 20 inches/minute.

15

Examples 7-SF. Performance Testing Results:

7a-SF. Viscosity Measurement.

The result of viscosity measurements of Examples 2-SF, 3-SF and 4-SF are summarized in Table 1a-SF.

20

Table 1a-SF

<u>Sample</u>	<u>Part A Viscosity (cPs)</u>	<u>Part B Viscosity (cPs)</u>
Example 2-SF	32090	31160
Example 3-SF	57900	61500
Example 4-SF	84000	94800

7b-SF. Cure time measurement

Cure time measurements were performed for the compositions of Examples 2-SF, 3-SF and 4-SF, during peeling test sample preparation; the results are summarized in Table 1b-SF.

5

Table 1b- SF

<u>Sample</u>	<u>Cure Time (sec)</u>
Example 2-SF	110
Example 3-SF	90
Examples 4-SF	70

The foregoing demonstrates that the inventive compositions are able to cure under 2 minutes.

7c-SF: Holding Test Results (Synthetic Substrate)

10

Holding test on Polyester film was performed for the compositions of Example 2-SF, 3-SF and 4-SF; the results are summarized in Table 1c-SF.

Table 1c-SF

<u>Sample</u>	<u>Holding Strength (lb/in)</u>
Example 2-SF	11.5
Example 3-SF	14.9
Example 4-SF	15.2
Control Example (see Table 1)	0.7

15

Referring to Table 1c-SF, it can be seen that the holding force for the polyester substrate is significantly better in the inventive examples made from polysiloxane polymer and commercial bases, compared to conventional cross-linked silicone polymer using the Karstedt catalyst (Control Example, Table 1).

7d-SF: Peel Test Results (Synthetic Substrate)

Peel tests of TSA compositions on a synthetic substrate (polyester) was performed using the compositions of Examples 2-SF, 3-SF and 4-SF. The results are summarized in Table 1d-SF.

5

Table 1d-SF

<u>Sample</u>	<u>Average Peel Strength (lb/in)</u>
Example 2-SF	1.2
Example 3-SF	1.5
Example 4-SF	1.6
Control Example (See Table 3)	0.1

Referring to Table d-SF, it is seen that the average peel force for polyester substrate is significantly better in the inventive examples made from polysiloxane polymer and commercial bases, compared to conventional cross-linked silicone polymers using the Karstedt catalyst.\ (Control Example, Table 3)

10

7e-SF: Stretch Test Results

Examples 2-SF, 3-SF and 4-SF were able to be stretched to 160% of its original length and recover to its original dimensions.

15 As demonstrated, the novel compositions, wound closure systems and catalyst of the present invention have many advantages compared with the prior art. The compositions allow for the formation of medical grade silicone adhesive, in particular suitable for human skin. The compositions provide a durable elastic structure, which provides both mechanical properties and adhesion properties. The catalyst provides dual cured catalytic action, enabling the cross

20 link of polysiloxane chains to form a film rapidly while forming adhesion properties on a given hydroxyl containing substrates. The silanol functions on the surface of silicone fillers in the compositions reacts with the hydroxyl functions on a given surface in the presence of

this novel dual functional catalyst provide the adhesion properties on this novel silicone based adhesive.

Example 7 - Wound Exudate/Moisture Absorbent Particles and Indicator(s)

5 The following examples demonstrate the feasibility of embodiments of the compositions of this invention incorporating wound exudate/moisture absorbent particles and/or indicators to absorb moisture when in intimate contact with a source of moisture (and to indicate such moisture absorption) while maintaining critical adherence and flexibility characteristics required for use as a wound closure device.

10 Similar to most commercially available platinum cured silicone materials, the water absorbable silicone based topical skin adhesives (TSA) of this invention is delivered in an equal 1 to 1 volume two-part kit.

 Preferably, the foregoing composition are made with the solvent-free silicone compositions hereinbefore described above.

15 In general, vinyl terminated polydimethylsiloxane is mixed with platinum tetramethyldivinyl disiloxane diethyl maleate catalyst, silica particles and optionally aliphatic organic solvent using a high- speed mixer to form part A of the kit. Vinyl terminated polydimethylsiloxane is mixed with polymethylhydro-co-polydimethylsiloxane cross linker, silica particles and optionally aliphatic organic solvent using a high-speed mixer to form part
20 B of the kit. The silica desiccant particles are blended into part B during its preparation process. These water absorbable particles are available commercially with an indicating property, the color change indicates absorbed water/moisture.

25 Example 7a: Preparation of silicone-based, water absorbable TSA with 23% loading of desiccant

Water absorbable TSA with 23% Desiccant-

Part A

90g of E-Kem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fumed silica particles) was mixed with 0.62g of Example 1, 0.60g of Gelest SIP
30 6830.3 (3% platinum divinyl tetramethyldisiloxane complex in vinyl terminated

polydimethyl siloxane), 9.0g of low molecular weight vinyl terminated polydimethyl silicone base polymer (Gelest DMS V21) using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

5 Part B

32g of E-Kem 55 experimental base (containing vinyl terminated polydimethyl silicone-based polymer and fumed silica particles) was mixed with 20.5g of polymethylhydro-co-polydimethyl siloxane cross linker (Gelest DMS H071), 1.6g of SiH terminated polydimethylsiloxane chain extensor (Gelest DMS H21) and 45.8g of silica desiccant (t.h.e.®
10 Desiccant, 100% indicating, EMD Millipore Corporation, Billerica, MA) using a high-speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Control Example- 7b: Preparation of Silicone-based TSA with 0% Loading of Desiccant

Part A

15 90g of E-Kem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fumed silica particles) was mixed with 0.62g of example 1, 0.62g of Example 1, 0.60g of Gelest SIP 6830.3 (3% platinum divinyl tetramethyldisiloxane complex in vinyl terminated polydimethyl siloxane), 9.0g of low molecular weight vinyl terminated
20 polydimethyl silicone base polymer (Gelest DMS V21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Part B

64g of E-Kem 55 experimental base (containing vinyl terminated polydimethyl silicone base polymer and fume silica particles) was mixed with 41g of polymethylhydro-co-polydimethyl siloxane cross linker (Gelest DMS H071), 3.2g of SiH terminated polydimethylsiloxane chain
25 extensor (Gelest DMS H21) using a high speed centrifugal mixer (FlackTek DAC150 FV-K) at 3470 rpm for 5 minutes.

Example 7c – Preparation of Test Samples

Holding Strength Test Sample

Synthetic substrate (Polyester film, 0.05 inch thick Duralar film, Grafic Plastics, Maple Heights, OH) 8 inch by 11 inch was cut in two halves with the dimension of 4 inch by 11 inch. A 1 inch width PSA (pressure sensitive adhesive) coated polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed along the cutting line to hold the two half pieces together.

- 5 The two-part silicone TSA compositions in each of the following examples were respectively mixed (Example 7a and Control Example 7b) and evenly applied onto the mesh to cover the entire area of the mesh using a conventional rubber spatula. The samples dried in 3 minutes at 31 C, according to ASTM 678. A 1- inch wide strip was cut for testing after being placed at 31 C for 1 hour.

10 Peel Test Sample

Synthetic substrate (Polyester film, 0.05 inch thick Duralar film, Grafic Plastics, Maple Heights, OH)

- 15 A 5 inch by 5 inch PSA (pressure sensitive adhesive) coated polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed on a Mylar substrate with the same dimension. The two-part silicone TSA compositions in each of the following examples were respectively mixed (Example 7a and Control Example 7b) and evenly applied onto the mesh to cover the entire area of the mesh using a conventional rubber spatula. 1 inch-wide specimens were cut for testing after the samples were dried and placed at 31 C overnight.

Stretch Test Sample

- 20 A 5 inch by 5 inch PSA (pressure sensitive adhesive) coated polyester mesh (Lot# 16204, Innovize, St Paul, MN) was placed on a Teflon substrate. The two-part silicone TSA compositions in each of the following examples were respectively mixed (Example 7a and Control Example 7b) and evenly applied onto the mesh to cover the entire area of the mesh using a conventional rubber spatula. The silicone coated polyester mesh was peel off from
25 Teflon substrate after the 1 hour. 1x5 inch silicone coated mesh specimens were cut for stretch testing.

Example 7d – Performance Test Results

Holding Test (Synthetic Substrate)

- Holding tests on Polyester film were performed on the test samples of Example 7a and
30 Control Example 7b the results are summarized below.

Sample	Holding Strength (lb/in)
Example 7a	11.5
Control Example 7b	11.1

The holding force on the polyester substrate for the water absorbable silicone-based TSA (Example 7a, desiccant containing) is comparable the holding force of the non-desiccant silicone-based TSA (Control Example 7b)

5

Peel test (Synthetic Substrate)

Peel tests of TSA on a synthetic substrate was performed for test samples using the compositions of Example 7a and Control Example 7b the results are summarized below.

10

Sample	Average Peel Strength (lb/in)
Example 7a	0.9
Control Example 7b	1.1

As observed, the peel force of the water absorbable silicone-based TSA (Example 7a) on polyester substrate is slightly lower than the peel force of the non-desiccant silicone-based TSA (Control Example 7b).

15

Stretch Test

The sample of Example 7a was stretched to 150% of its original length. The dimensions of the testing sample were measured before and after the stretch and the images of this is shown in Fig. 7d Fig. 7e and Fig. 7f.

20

Water Absorption Test

A test specimen of Example 7a with the dimension of approximately 3.5 X 3.5 X 0.1 cm was immersed into water at ambient temperature for 24 hours. 4.82% weight gain was observed after water immersion. A specimen of Control Sample 7b was tested at the same time and no weight gain was observed. The color of the specimen (Example 7a) changed from blue to brown, as illustrated in Fig. 7g and Fig. 7h.

25

As illustrated in the examples above, incorporation of silica-based desiccants into silicone TSA is capable of indicating color changes when immersed in water. Quite

unexpectedly, the hydrophobicity of the cross-linked polydimethylsiloxane appears not to prevent water ingress into the matrix of silicone TSA, when the silicone TSA is fully contacted with water by immersion and one would expect the same to be true with intimate contact over a period of time with a source of moisture such as a wound closure device in contact with wound exudate/discharge. Very noteworthy is the finding that the incorporation of desiccant appears not to impact the adhesion and mechanical properties of the silicone-based TSA when compared to control examples not containing the desiccant.

As demonstrated, the novel compositions, wound closure systems and catalyst of the present invention have many advantages compared with the prior art. The compositions allow for the formation of medical grade silicone adhesive, in particular suitable for human skin. The compositions provide a durable elastic structure, which provides both mechanical properties and adhesion properties. The catalyst provides dual cured catalytic action, enabling the cross link of polysiloxane chains to form a film rapidly while forming adhesion properties on a given hydroxyl containing substrates. The silanol functions on the surface of silicone fillers in the compositions reacts with the hydroxyl functions on a given surface in the presence of this novel dual functional catalyst provide the adhesion properties on this novel silicone-based adhesive. Additionally, as illustrated in the examples provided above, triclosan containing silicone TSA provides an effective means to deliver the antimicrobial agent via skin closure devices. The incorporation of triclosan appears not to significantly impact the adhesion properties of the adhesive and surgical performance of the silicone-based TSA.

Although this invention has been shown and described with respect to detailed embodiments thereof, it will be understood by those skilled in the art that various changes in form and detail thereof may be made without departing from the spirit and scope of the claimed invention.

We claim:

1. A composition comprising:

a cross-linkable silicone polymer having reactive functionalities;

a silica-containing composition;

a silicone cross-linking agent;

a catalyst, wherein said catalyst comprises a platinum tetramethyldivinyl disiloxane diethyl maleate complex having the formula:



an antimicrobial agent.

2. The composition of claim 1, wherein the cross-linkable silicone polymer is selected from the group consisting of vinyl terminated polydialkylsiloxane, vinyl terminated polydimethylsiloxane, vinyl terminated polydiphenylsilane-dimethylsiloxane copolymer, vinyl terminated polyphenylmethylsiloxane, vinyl terminated polyfluoropropylmethyl-dimethylsiloxane copolymer, vinyl terminated polydiethylsiloxane, and SiH terminated polydimethyldisiloxane.

3. The composition of claim 1, wherein the cross-linkable silicone polymer comprises vinyl terminated polydimethylsiloxane.

4. The composition of claim 1, wherein the silica-containing composition comprises a trimethyl silyl surface treated silica filler.

5. The composition of claim 1, wherein the silica-containing composition is selected from the commercially available reactive silica-containing silicone bases including HCR (high consistent rubber) bases and LSR (liquid silicone rubber) bases.

6. The composition of claim 5, wherein the silica-containing composition is a liquid silicone rubber base.

7. The composition of claim 1, wherein the silicone cross-linking agent is selected from the group consisting of polymethylhydrosiloxane, polymethylhydro-co-polydimethylsiloxane,

polyethyhydrosiloxane, polymethylhydrosiloxane-co-octylmethylsiloxane, and polymethylhydrosiloxane-co-methylphenylsiloxane.

8. The composition of claim 1, wherein the silicone cross-linking agent comprises polymethylhydrosiloxane, polymethylhydro-co-polydimethylsiloxane and combinations thereof.

9. The composition of claim 1, wherein the composition additionally comprises about 0 wt. % to about 30 wt. % of an organic solvent, based upon the weight of the composition.

10. The composition of claim 1, wherein the composition comprises about 1 wt. % to about 15 wt. % of the silicone cross-linking agent based on total solids, wherein the coating composition additionally comprises about 0 wt. % to about 30 wt. % of an organic solvent, based upon the weight of the coating composition.

11. The composition of claim 1, wherein the coating composition comprises about 0.003 wt. % to about 0.06 wt. % of the platinum catalyst, based on total solids, wherein the coating composition additionally comprises about 0 wt. % to about 30 wt. % of an organic solvent, based upon the weight of the coating composition.

12. The composition of claim 1, wherein the coating composition additionally comprises a solvent selected from the group consisting of pentane, hexane, heptanes, mixtures of low molecular weight olefins, and combinations thereof.

13. The composition of claim 1, wherein the antimicrobial agent is selected from the group consisting of triclosan, chlorhexidine, polyhexamethylene biguanide (PHMB), octenidine, elemental silver and silver salts.

14. The composition of claim 13, wherein the antimicrobial agent is triclosan.

15. The composition of claim 14, wherein the triclosan comprises about 0.05 wt. % to about 2.0 wt. % of the composition,

16. The composition of claim 15, wherein the triclosan comprises about 0.1 wt. % to about 1.5 wt. % of the composition.

17. The composition of claim 16, wherein the triclosan comprises about 0.2 wt. % to about 1.0 wt. % of the composition.

18. The coating composition of claim 1, wherein the composition is curable at temperatures at about 19 C.

19. The coating composition of claim 18, wherein the composition is curable at temperatures of about 28 C in about 2-5 minutes.

20. A kit comprising:

a) a wound closure device; and

b) the composition of claim 1.

21. The kit of claim 20, wherein the wound closure device is a wound closure strip.

22. The kit of claim 21, wherein the wound closure strip is selected from the group consisting of meshes, polymeric films, plastic foams (including open celled foam), woven fabrics, knitted fabrics, a non-woven fabrics, and combinations thereof.

23. The kit of claim 22 wherein the wound closure strip is a mesh.

24. The kit of claim 23, wherein the wound closure device comprises materials selected from the group consisting of polyesters, nylons, acrylics, rayons, polyurethanes, polyurethane foams, polystyrenes, polyesters, polyethylene terephthalate (PET), polyamides, polylactic acids, polyglycolic acids, polycaprolactones, and mixtures thereof; cotton, silk and linen; and surface-treated materials that impart an OH functionality to their surfaces including but not limited to OH surface-treated PTFE, OH surface-treated polypropylene and OH-surface treated polyethylene.

25. The kit of claim 24, wherein the antimicrobial is triclosan.

26. A composition comprising:

a cross-linkable silicone polymer having reactive functionalities;

a silica-containing composition;

a silicone cross-linking agent;

a catalyst, wherein said catalyst comprises a platinum tetramethyldivinyl disiloxane diethyl maleate complex having the formula:

$\text{Pt}[(\text{CH}_2 = \text{CH})(\text{CH}_3)_2\text{Si}]_2\text{O} \cdot (\text{COCH} = \text{CHCO})(\text{C}_2\text{H}_5\text{O})_2$; and

a wound exudate or wound moisture absorbent and/or indicator.

27. The composition of claim 26, wherein the absorbent and/or indicator is silica.

28. The composition of claim 26, wherein the absorbent and/or indicator is a superabsorbent.

29. The composition of claim 26, wherein the absorbent and/or indicator is an anhydrous inorganic salt.

30. A kit comprising:

a) a wound closure device; and

b) the composition of claim 26.

31. The kit of claim 30, wherein the wound closure device is a wound closure strip.

32. The kit of claim 31, wherein the wound exudate or wound moisture absorbent and/or indicator is applied or coated on the wound closure strip.

FIG. 1

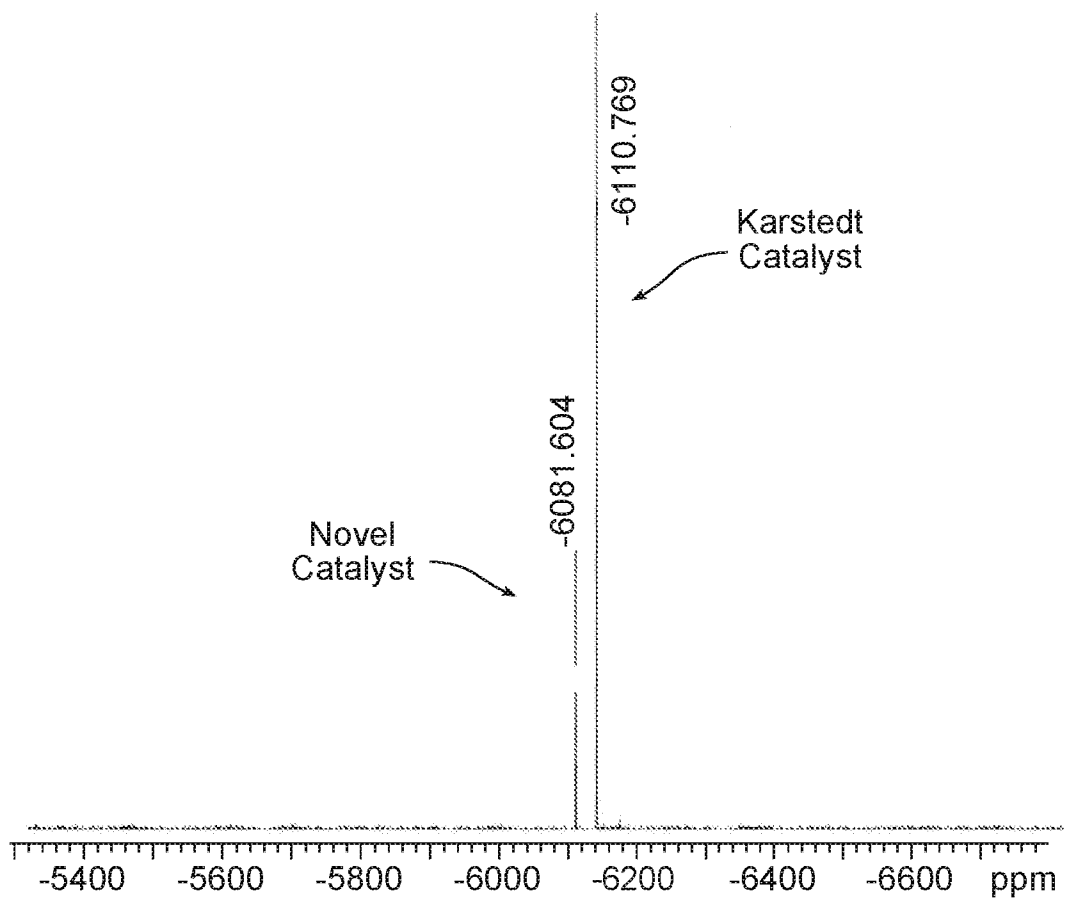


FIG. 2a

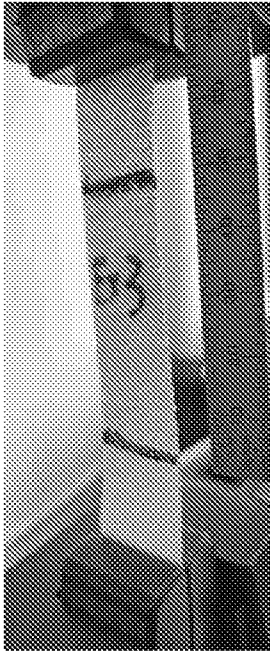


FIG. 2b

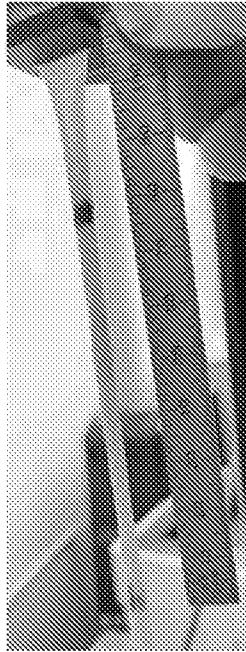


FIG. 2c

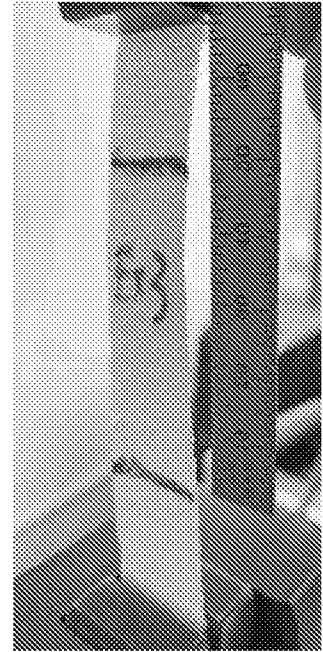


FIG. 3a

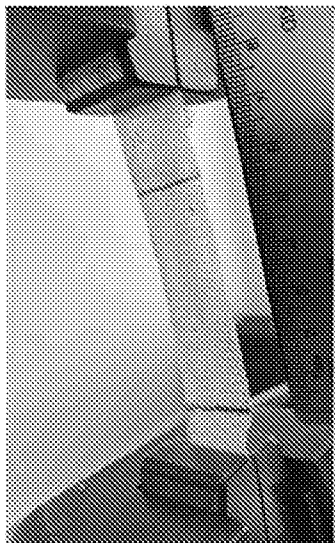


FIG. 3b

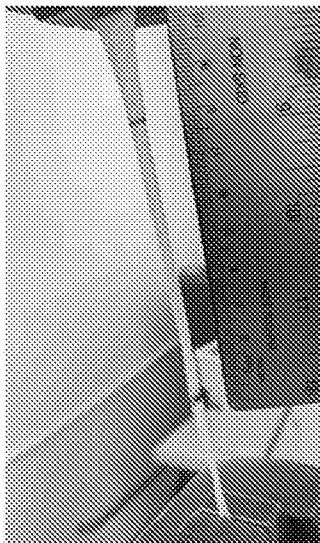


FIG. 3c

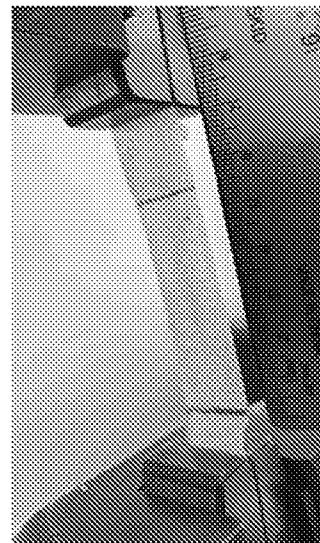


FIG. 4a

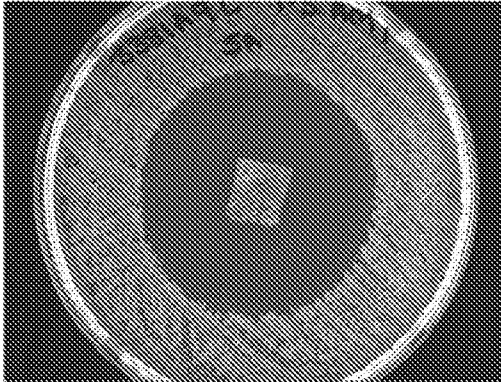


FIG. 4b

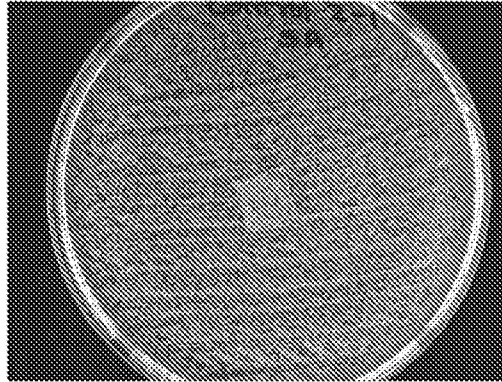


FIG. 5a

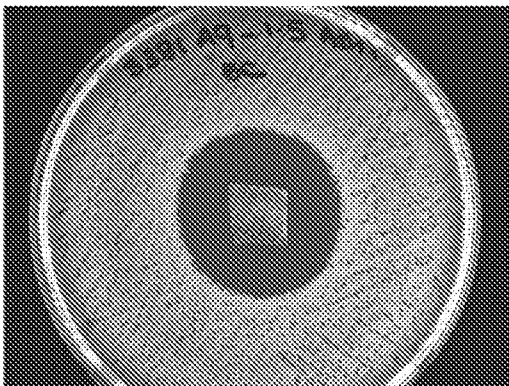


FIG. 5b

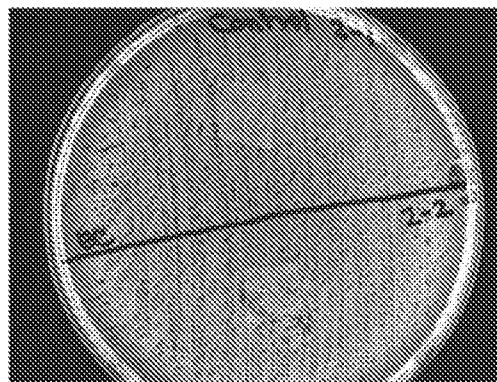


FIG. 6a

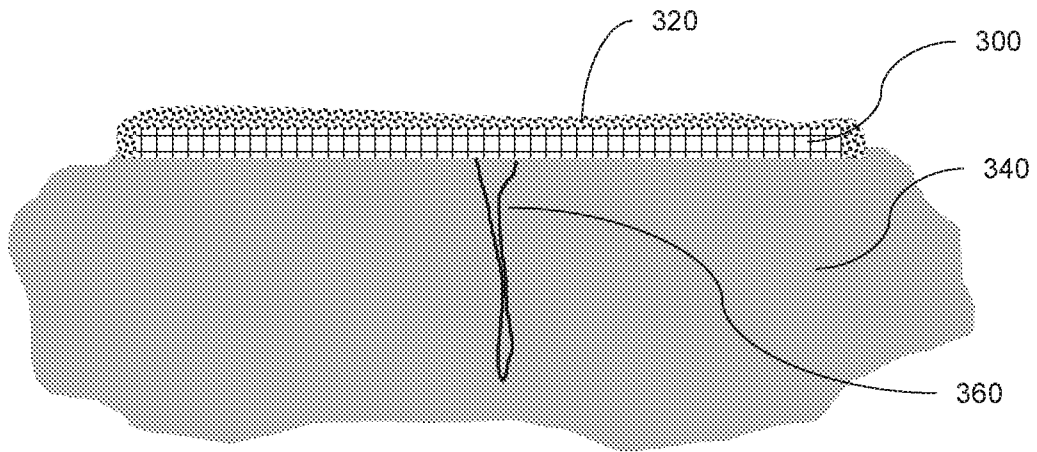


FIG. 6b

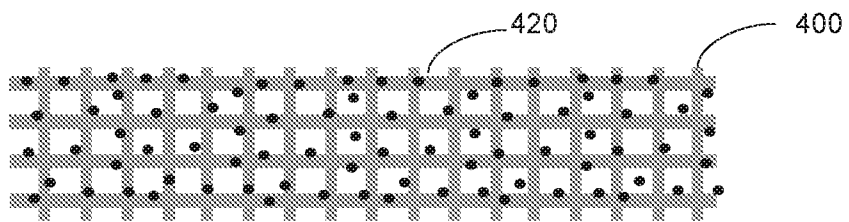


FIG. 6c

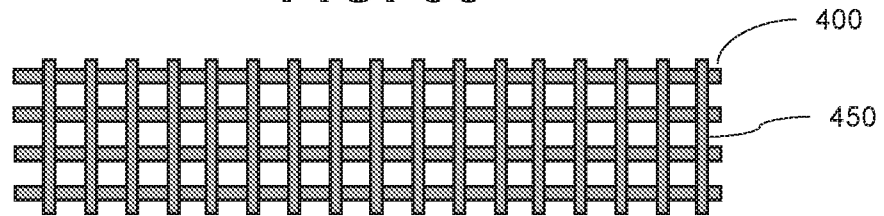


FIG. 7

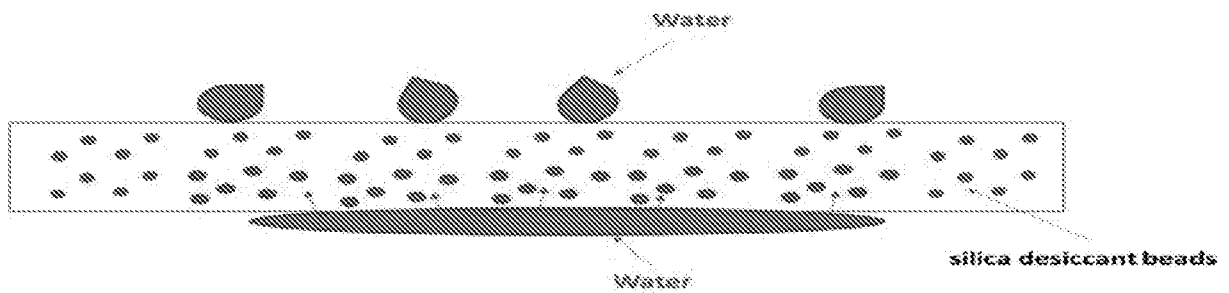


FIG. 7a

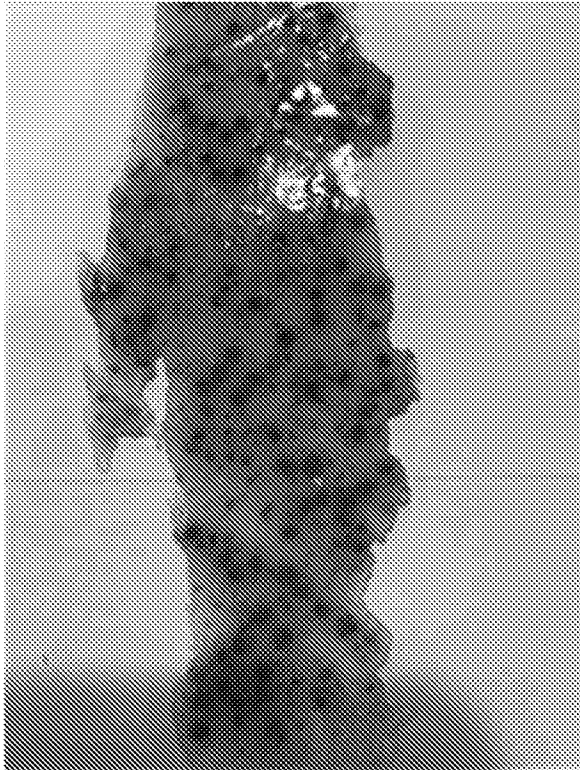


FIG. 7b

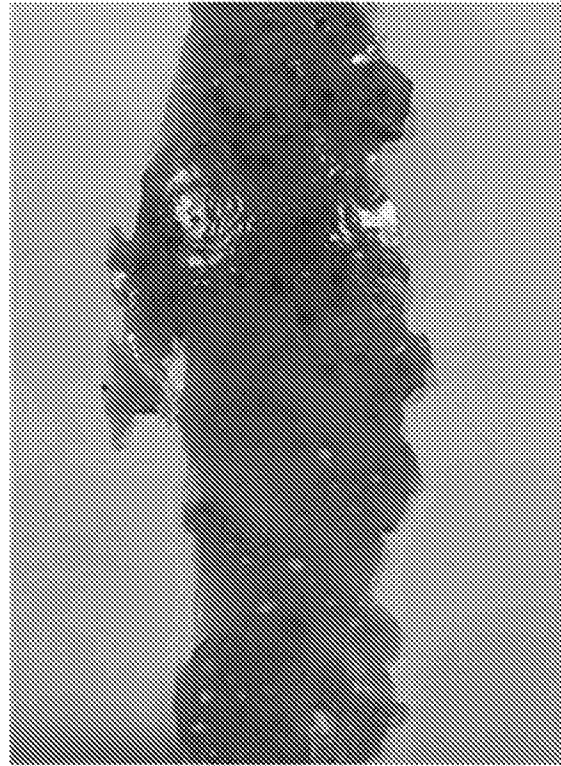


FIG. 7c

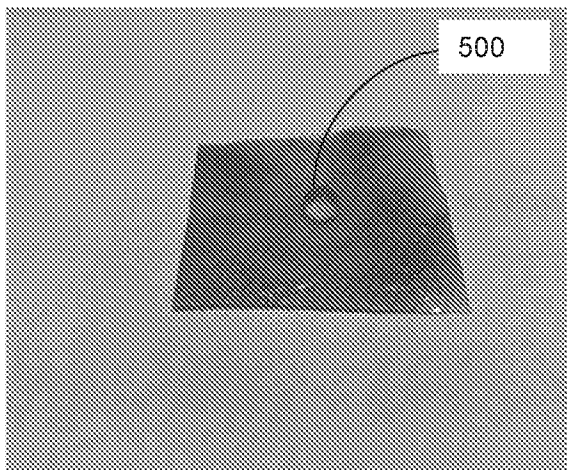


FIG. 7d

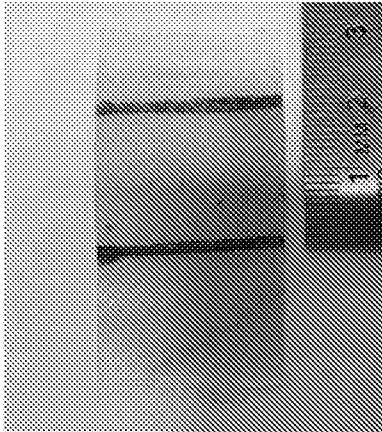


FIG. 7e

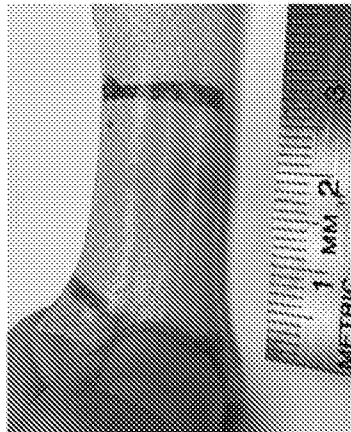


FIG. 7f

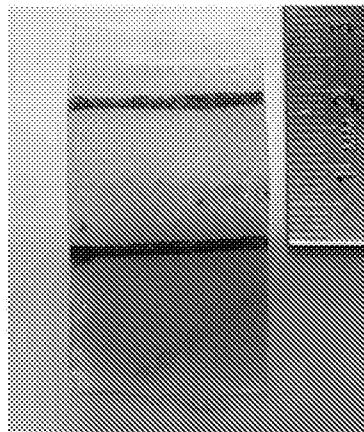


FIG. 7g

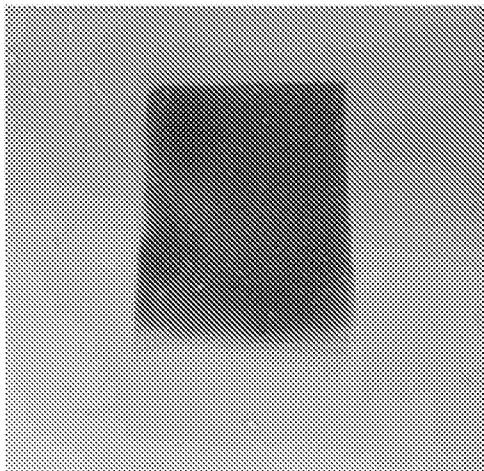
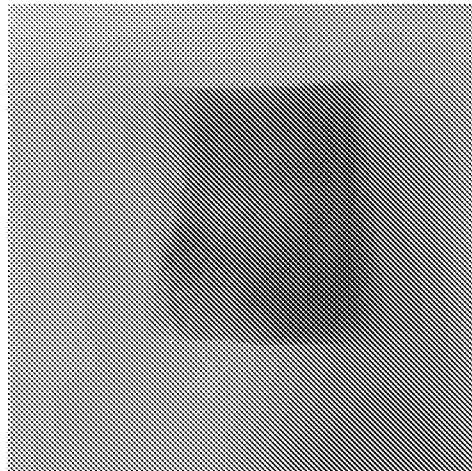


FIG. 7h



INTERNATIONAL SEARCH REPORT

International application No
PCT/IB2021/054518

A. CLASSIFICATION OF SUBJECT MATTER
 INV. A61L15/46 A61L15/58 A61L15/60 A61L26/00 B01J23/42
 C07F15/00 C08F4/60
 ADD.
 According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED
 Minimum documentation searched (classification system followed by classification symbols)
 B01J C07F C08F A61L

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)
 EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2012/237461 A1 (YU BETTY [US] ET AL) 20 September 2012 (2012-09-20) page 1, paragraph 8-10 page 5, paragraph 70 page 8, paragraph 100 page 9, paragraph 104 page 10, paragraphs 115,122 page 11, paragraph 139 - page 12, paragraph 141 claims	1-32
A	----- US 9 511 034 B1 (GARRETT SHIEN-LIN [US]) 6 December 2016 (2016-12-06) column 6, lines 31-63 column 7, lines 51-57 column 8, lines 47-48 column 10, line 60 - column 13, line 32 claims ----- -/--	1-32

Further documents are listed in the continuation of Box C.

See patent family annex.

* Special categories of cited documents :

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Date of the actual completion of the international search 22 July 2021	Date of mailing of the international search report 30/07/2021
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Name and mailing address of the ISA/ European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Fax: (+31-70) 340-3016	Authorized officer Van den Bulcke, H
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INTERNATIONAL SEARCH REPORT

International application No
PCT/IB2021/054518

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 2003/077316 A1 (NICHOLS JANE [US] ET AL) 24 April 2003 (2003-04-24) page 6, paragraph 38 page 7, paragraph 54-56 claims	1-32
A	----- US 2013/122314 A1 (OU DUAN LI [US]) 16 May 2013 (2013-05-16) page 2, paragraph 18-22 page 4, paragraph 30 claims	1-32
A	----- WO 2017/158340 A1 (TRIO HEALTHCARE LTD [GB]) 21 September 2017 (2017-09-21) page 3, lines 8-22 page 9, line 23 - page 10, line 10 page 14, line 17 - page 15, line 12 claims	1-32
A	----- US 5 026 768 A (LILES DONALD T [US]) 25 June 1991 (1991-06-25) column 3, lines 18-39 column 4, lines 16-41 column 6, lines 10-44 example 1	1-32
A	----- EP 3 388 037 A1 (TRULIFE LTD [IE]) 17 October 2018 (2018-10-17) claims	1-32

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No PCT/IB2021/054518

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2012237461	A1	20-09-2012	NONE

US 9511034	B1	06-12-2016	US 9511034 B1 06-12-2016
			US 2017049925 A1 23-02-2017

US 2003077316	A1	24-04-2003	NONE

US 2013122314	A1	16-05-2013	AU 2012340465 A1 01-05-2014
			BR 112014011731 A2 09-05-2017
			CA 2855664 A1 23-05-2013
			CN 104105765 A 15-10-2014
			EP 2780425 A1 24-09-2014
			JP 6147759 B2 14-06-2017
			JP 2015504467 A 12-02-2015
			RU 2014124158 A 27-12-2015
			US 2013122314 A1 16-05-2013
			US 2016348025 A1 01-12-2016
			US 2017028391 A1 02-02-2017
			US 2018345262 A1 06-12-2018
			WO 2013074732 A1 23-05-2013
			ZA 201404391 B 28-09-2016

WO 2017158340	A1	21-09-2017	AU 2017232433 A1 27-09-2018
			CA 3016845 A1 21-09-2017
			EP 3429644 A1 23-01-2019
			JP 6752896 B2 09-09-2020
			JP 2019509812 A 11-04-2019
			US 2019083677 A1 21-03-2019
			WO 2017158340 A1 21-09-2017

US 5026768	A	25-06-1991	NONE

EP 3388037	A1	17-10-2018	NONE
