[54] CRYOSURGICAL APPARATUS

Stumpf et al.

[45] Apr. 30, 1974

[56] References Cited UNITED STATES PATENTS 3,393,679 7/1968 Crump et al				
Conn. [22] Filed: June 14, 1972 [21] Appl. No.: 262,543 [52] U.S. Cl	[75]	Inven	tors: Jo	seph C. Stumpf, Fairfield; Joseph Andera, Trumbull, both of Conn.
[21] Appl. No.: 262,543 [52] U.S. Cl	[73]	Assig		
[52] U.S. Cl. 128/303.1, 62/293, 62/51 [51] Int. Cl. A61b 17/36, A61f 7/1 [58] Field of Search 62/293, 514; 128/303.1 128/400, 40 [56] References Cited UNITED STATES PATENTS 3,393,679 7/1968 Crump et al. 128/303.3,502,081 3/1970 Amoils 128/303.3,575,176 4/1971 Crump et al. 128/303.	[22]	Filed	Ju	ine 14, 1972
[51] Int. Cl	[21]	Appl.	No.: 26	52,543
UNITED STATES PATENTS 3,393,679 7/1968 Crump et al. 128/303. 3,502,081 3/1970 Amoils 128/303. 3,575,176 4/1971 Crump et al. 128/303.	[51]	Int. C	7 .	A61b 17/36, A61f 7/12
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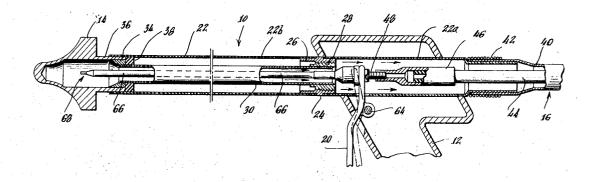
Primary Examiner—Channing L. Pace Attorney, Agent, or Firm—Buckles and Bramblett

57] ABSTRACT

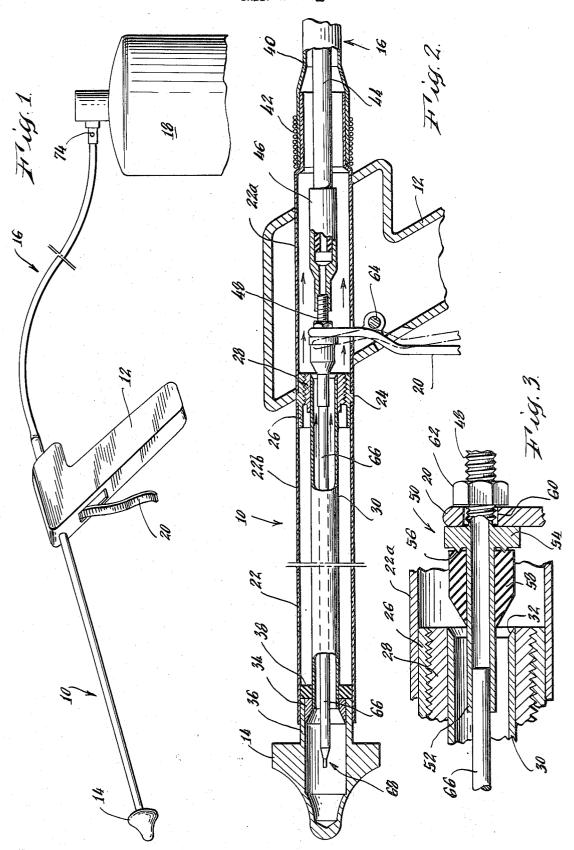
There is disclosed a cryosurgical apparatus of the type which operates from a source of compressed gas. It includes an improved nozzle which is substantially less critical tnan prior art nozzles and permits simplified and less expensive construction. A defrost valve in the exhaust conduit permits easy and quiet operation by the surgeon. An insulator tube is resiliently secured to the probe to allow thermal expansion and contraction without stress.

The foregoing abstract is not to be taken either as a complete exposition or as a limitation of the present invention. In order to understand the full nature and extent of the technical disclosure of this application, reference must be had to the following detailed description and the accompanying drawings as well as to the claims.

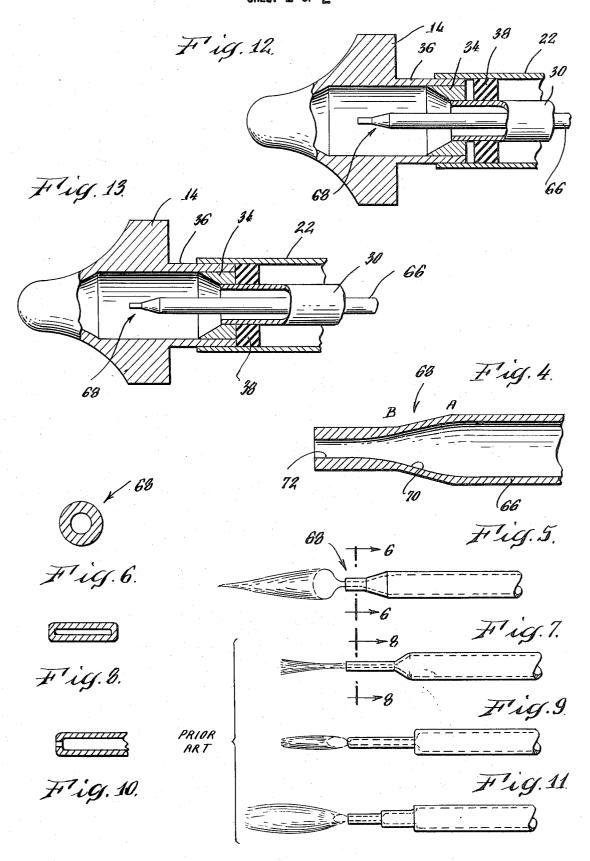
6 Claims, 13 Drawing Figures



SHEET 1 OF 2



SHEET 2 OF 2



CRYOSURGICAL APPARATUS

BACKGROUND OF THE INVENTION

This invention pertains to cryosurgical instruments of 5 the type which are cooled under the influence of high pressure gas escaping from an orifice. Instruments of this type are well known in the art and are widely employed for a number of surgical procedures such as the necrosis of diseased tissue. Several gases exhibit the 10 Joule Thomson effect and may be used in the operation of the instrument. The most common, however, are nitrous oxide and carbon dioxide.

In instruments of this type, the gas expansion orifice is of an extremely small size and in all prior art instruments the spacing between the orifice and the inner wall of the cooling tip is extremely critical. For example, with prior art instruments, the orifice is positioned approximately 0.050 inch from the inner wall of the tip and the permitted tolerance is only 0.010 inch. This results in such instruments being difficult and costly to manufacture. For example, the parts of such instruments are commonly threaded so that they may be factory adjusted prior to shipment.

Another problem connected with prior art instru- 25 ments of this type is found in the exhaust valve of intruments which have controlled defrost. For example, one such instrument is normally warm, which means that the exhaust valve is normally closed and the device is filled with compressed gas at bottle pressure. As the 30 bottle gas prssure may be commonly as high as 800 psi, it will be quite apparent that this creates an explosion hazard. The exhaust valve used in this prior art device comprises a cylindrical piston which seats against a small exhaust orifice and is retained in the seated posi- 35 tion by means of a heavy spring. The piston is raised against the force of a spring by means of a finger operated toggle. When the surgeon wishes to cool the probe tip, he must apply substantial force to depress the toggle which is, itself, detrimental, particularly in the case 40 of very delicate surgical procedures. Secondly, as soon as the piston begins to leave the orifice, the full bottle pressure, which was formerly applied only to a small area of the piston, is now applied to the full area of the piston end, slamming the piston open with an explosive-like report.

Still another problem with prior art devices arises from the fact that they are subject to considerable thermal stress. For example, it is usually desirable to provide an insulated housing to prevent adherence to healthy tissue. This housing should preferably remain at room temperature. However, the tip and exhaust conduit may be cooled to temperatures as low as -89°C. The resultant contraction may result in substantial stresses at the junctures of the cold and warm parts.

Accordingly, it is a primary object of the present invention to provide an improved cryosurgical instrument of the gas operated type having much less critical tolerances, permitting it to be assembled in a much less expensive manner such as by electron beam welding. Other objects are to provide such an instrument which is only intermittently exposed to full bottle gas pressure, which has a substantially silent and easily operated exhaust valve, and which has substantially no thermal stresses between the cooled parts and the insulator housing. The manner in which these objects are

achieved will be apparent from the following description and appended claims.

SUMMARY OF THE INVENTION

The invention comprises a gas operated cryosurgical instrument including a tubular exhaust conduit terminating at one end in a hollow probe tip of high thermal conductivity. A high pressure gas delivery conduit extends through the exhaust conduit and terminates at a nozzle within the probe tip. The nozzle has a cylindrical gas discharge passage of smaller diameter than the delivery conduit and a smoothly curved reduction passage therebetween. A normally open valve is connected in fluid flow relationship with the exhaust conduit. An insulator tube surrounds but is spaced from the exhaust conduit and is connected thereto by a resilient connection.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a perspective view of a cryosurgical instrument in accordance with the present invention shown connected to a source of bottled gas;

FIG. 2 is an enlarged cross section taken through the instrument of FIG. 1;

⁵ FIG. 3 is an enlarged cross section of the exhaust valve of FIG. 2;

FIG. 4 is a greatly enlarged cross section of the nozzle portion of the apparatus;

FIG. 5 is an illustration of the gas jet obtained with 0 the nozzle of FIG. 4;

FIG. 6 is a cross section taken substantially along the line 6—6 of FIG. 5;

FIG. 7 is an illustration of one type nozzle used in the prior art;

FIG. 8 is a cross section taken substantially along the line 8—8 of FIG. 7;

FIG. 9 is an illustration of another type of nozzle used in the prior art;

FIG. 10 is an enlarged cross section showing the orifice of the FIG. 9 nozzle;

FIG. 11 shows still another type of nozzle used in the prior art;

FIG. 12 illustrates the resilient connection between the warm insulator tube and the cold portions of the probe; and

FIG. 13 is an illustration similar to FIG. 12 showing the manner in which the resilient connection operates.

DESCRIPTION OF THE PREFERRED EMBODIMENT

With particular reference to FIG. 1, there is disclosed an instrument of the type utilized in treating cervicitis. It comprises an elongated probe 10 mounted in a handle 12 and terminating in a substantially conical applicator tip 14. The other end of the probe extends from the handle and is connected to a line 16 which, in turn, is connected to a suitable source 18 of pressurized gas. A trigger 20 extends from the handle for selective defrosting as will be explained.

Turning now to FIG. 2, the handle 12 will be seen to support the rear portion 22a of a stainless steel insulator tube 22. The rear portion 22a and a forward portion 22b are each welded to the circumferential flange 24 of an internally threaded sleeve 26. Threaded into sleeve 26 is a bushing 28 which is welded to the end of an exhaust tube 30. The end of exhaust tube 30 has a bev-

elled valve seat 32 as shown in FIG. 3. The other end of exhaust tube 30 is welded to a bushing 34 which, in turn, is welded to the cylindrical stem 36 of the hollow copper tip 14. The forward end of the insulator tube 22 extends over the surface of stem 36 but is not secured 5 thereto. Instead, a resilient bushing 38 frictionally engages both the exhaust tube 30 and the insulator tube 32.

The line 16 is a coaxial conduit comprising a silicon coated fiberglass exhaust line 40 secured by a spring 42 10 to the end of insulator tube 22. Carried within the exhaust line is a high pressure delivery line 44 secured by means of a high pressure connector 46 to the threaded end 48 of a steel valve member 50 which is illustrated in more detail in FIG. 3.

The valve member 50, in addition to the threaded end 48, has an unthreaded forward portion 52 and a central circumferential flange 54. The forward surface of flange 54 carries a circular knife edge 56. A Teflon valve member 58 is press fitted over the forward por- 20 shown in an exaggerated manner in FIG. 13 wherein it tion 52 and has a flat rear surface which engages the knife edge 56. The forward surface of valve seat 58 is tapered to engage the valve seat 32 on exhaust tube 30. The upper end of trigger 20 defines a drilled opening 50 extends. It is held in place by a nut 62. The trigger 20 is mounted on a pivot 64 positioned approximately one inch below its upper end. The length of trigger 20 below the pivot 64 is approximately 4 inches in the described embodiment. Welded to the unthreaded for- 30 ward portion 52 of valve member 50 is the end of a delivery tube 66 which in one embodiment is a 15 gauge stainless steel hypodermic tube having an internal diameter of 0.059 inch. The forward end of delivery tube 66 has a reduced diameter portion forming a nozzle 68 35 positioned within the hollow probe tip 14.

The construction of nozzle 68 will be best understood by reference to FIG. 4. As will be seen therein, the internal diameter of the delivery tube 66 is reduced via a smooth wall reduction passage 70 to a cylindrical gas discharge passage 72. This configuration is achieved by inserting into the end of the hypodermic tube a hardened wire having an external diameter equal to the desired diameter of the gas discharge passage. The end of the tube is then swaged onto the wire and the wire is removed. In one actual embodiment, the tube 66 has an internal diameter of 0.059 inch and the internal diameter of the gas discharge passage 72 is 0.01065 inch. The distance from the nozzle to the beginning of reduction ("A" FIG. 4) is 0.20 inch and the distance between the nozzle tip and the end of reduction ("B") is 0.12 inch.

The performance of the nozzle 68 is strikingly superior to those of the prior art. The reason for this is not fully understood but is believed to be due to the smooth continuous inner surface formed by the reduction passage 70 and the gas discharge passage 72. This is believed to prevent gas turbulence and permit laminar flow out of nozzle 68.

FIG. 5 illustrates the gas flow from the nozzle 68 as actually observed in practice. As will be seen, it presents an elongated "flame like" appearance and shape. FIGS. 7-11 illustrate three prior art nozzle constructions and the jets obtained thereby. FIGS. 7 and 8 illustrate a pinched tube configuration. FIGS. 9 and 10 illustrate a rolled end construction and FIG. 11 illustrates a type of orifice known as a "double reduction" orifice which comprises a series of tubes of reduced di-

ameter. The jets from these prior art nozzles appear as indicated. In these prior art nozzles the distance from the orifice to the wall of the applicator tip is very critical and the spacing must be quite close. As an example, this distance may be 0.050 inch with a tolerance of + or -0.010 inch. In contrast, when utilizing the nozzle of this invention, the distance from the nozzle tip to the wall may be 0.250 inch with a tolerance of + or -0.060inch. Accordingly, by means of this invention, manufacture and assembly are greatly simplified, resulting in a highly effective instrument at a much lower cost.

The resilient tip construction is illustrated in detail in FIGS. 12 and 13. As seen in FIG. 12, the insulator tube 22 is spaced from exhaust tube 30, providing an insulat-15 ing air space therebetween. The end of the insulator tube 22 slidingly encircles the stem 36 of tip 14. A resilient bushing 38 engages both the insulator tube and the exhaust tube. As the probe tip is cooled, the tip 14 and the exhaust line 30 will both cool and contract. This is will be seen that the normal resilience of bushing 38 compensates for expansion and contraction and prevents stresses from building up in the instrument.

The nozzle and the resilient tip construction may be 60 through which the threaded end 48 of valve member 25 utilized in connection with either a non-defrostable or a defrostable cryosurgical probe. The probe illustrated herein is of the defrostable type. Defrosting is obtained by means of the valve illustrated in detail in FIG. 3. When the valve is in its normally open position, high pressure gas entering through delivery line 44 passes through the hollow passage in the valve member 50 an through delivery tube 66 to nozzle 68. From the nozzle it expands into tip 14, causing the tip to be cooled by the Joule Thomson effect. The expanded gas then passes rearwardly through exhaust tube 30 and out the exhaust line 40. It may then be exhausted to atmosphere through any suitable opening such as the vent 74 shown in FIG. 1. The high pressure exhaust gas tends to maintain the exhaust valve in its normally open position without the need for springs or similar devices. In order to defrost the instrument, the trigger 20 is depressed by the surgeon, whereupon it assumes the dashed line position illustrated in FIG. 2 and forces the Teflon valve member 58 against the bevelled valve seat 32 of the exhaust tube 30. The circular knife edge 56 forms a gas tight seal with the rear of the valve member. With the exhaust valve closed, the gas pressure within tip 14 rises to bottle pressure and the heat of compression causes rapid defrosting of the probe tip. In one embodiment, the diameter of the valve member 58 which is exposed to gas pressure is approximately 0.187 inch. With a bottle pressure of 800 psi, this results in 27 pounds force tending to drive the valve member to the rear. The 4:1 lever ratio of the trigger 20 results in only 6.8 pounds of force being required to close the valve and maintain it in the closed position. As the valve is normally open, it will be closed only for the period of time during which the surgeon desires to defrost the probe tip. Therefore, the instrument is exposed to full bottle pressure only intermittently and for short periods of time, greatly increasing the safety of the apparatus.

> It is believed that the construction and operation of this invention will now be apparent to those skilled in the art. It will also be apparent that a number of variations and modifications may be made in this invention without departing from its spirit and scope. Accord

ingly, the foregoing description is to be construed as illustrative only, rather than limiting. This invention is limited only by the scope of the following claims.

We claim:

- 1. A gas operated cryosurgical instrument which 5 comprises: a tubular exhaust conduit terminating at one end in a hollow probe tip of high thermal conductivity; a remote source of high pressure gas; a gas delivery conduit extending through said exhaust conduit in fluid flow communication with said source and terminating at a nozzle within said probe tip; normally open valve means connected in fluid flow relationship between said exhaust conduit and atmosphere; and means for controllably closing and opening said valve means.
- 2. The instrument of claim 1 wherein said valve means comprises: a stationary valve seat defined by said exhaust conduit; and a moveable valve member carried by said delivery conduit.
- 3. The instrument of claim 2 wherein said closing 20 means comprises a manually operable trigger connected to advance both of said delivery conduit and valve member.
 - 4. A gas operated cryosurgical instrument which

comprises: a tubular exhaust conduit terminating at one end in a hollow probe tip of high thermal conductivity; a gas delivery conduit extending through said exhaust conduit and terminating at a nozzle within said probe tip, said nozzle including a cylindrical gas discharge passage of smaller diameter than said delivery conduit and a smoothly curved reduction passage therebetween; normally open valve means connected in fluid flow relationship between said exhaust conduit and atmosphere; an insulator tube surrounding, but spaced from, said exhaust conduit; resilient means interconnecting said insulator tube and exhaust conduit; and means for controllably closing and opening said valve means.

- 5 5. The instrument of claim 4 wherein said resilient means comprises an annular bushing encircling said exhaust conduit adjacent said probe tip and frictionally engaging both of said exhaust conduit and insulator tube to permit relative motion therebetween.
- 6. The instrument of claim 5 wherein said probe tip includes a substantially cylindrical stem and said insulator tube encircles one end of said stem in sliding relationship therewith.

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UNITED STATES PATENT OFFICE CERTIFICATE OF CORRECTION

Patent No. 3,807,403	Dated April 30, 1974
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Inventor(s) Joseph G. Stumpf and Joseph F. Andera

It is certified that error appears in the above-identified patent and that said Letters Patent are hereby corrected as shown below: In Title Page, Column 1, change inventor's name from "Joseph C. Stumpf" to --Joseph G. Stumpf--; change address of Assignee from "Skelton" to --Shelton--. In Abstract, Line 4, change "tnan" to --than--. Column 3, line 49, after "nozzle" insert --tip--. Column 4, line 31, change "an" to --and--. Column 5, line 20, after "closing" insert --and opening--.

Signed and sealed this 3rd day of September 1974.

(SEAL) Attest:

McCOY M. GIBSON, JR. Attesting Officer

C. MARSHALL DANN Commissioner of Patents